

Cost-Effective Flexible CSRR-Based Sensor for Noninvasive Measurement of Permittivity of Biomaterials [†]

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Abstract: A novel, cost-effective, flexible microwave sensor is proposed to facilitate point-of-care testing (POCT) methods for medical diagnosis. The sensor is based on the complementary split-ring resonator (CSRR) for accurately measuring the permittivity of biomaterials over a wide range of frequencies. This capability can be used to characterize various materials under test (MUT) such as blood, saliva, tissue samples, etc. The flexibility of the proposed sensor makes it possible to use it when the accessibility of the sample has technical difficulties, such as curved surfaces. Firstly, the optimized structure and coupling to the readout transmission line are evaluated using finite element method (FEM) simulations. Then, the prototype of the optimized structure is fabricated on thin polydimethylsiloxane (PDMS) substrate as a biocompatible economical polymer, and Aluminium is carefully chosen for the fabrication of CSRR and readout parts. The proposed flexible sensor is tested to compare to conventional rigid CSRR sensors. Not only the proposed structure withstood the different bending positions well, it is also showed an improvement in the results for curved MUT.

Keywords: Biosensor; Microwave sensor; Split-ring resonator; Biomaterial; Permittivity; Flexible

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1. Introduction

Point-of-care testing (POCT) emerges as an alternative to traditional laboratories-based diagnostic tests due to cost considerations and available medical equipment, particularly in areas of resource-limited requirements [1,2]. Simplified operation without the requirement of skilled operators, reduced analytical time and faster systematic procedures, uncomplicated and cost-effective manufacturing process, ease of use, especially in regions that have limited resources, and low energy consumption and reagent are POCT's distinct advantages [1–4].

Modern biosensors have played a significant part in realizing POC ideas based on the concept of reduced diagnostics times and processes [2]. Microwave resonator-based sensors, such as the complementary split-ring resonator (CSRR), have recently emerged as a promising technique for the fabrication of biosensors and biodevices [5,6]. For point-of-care testing, planar structures have proved to be the ideal sensing choice among other microwave resonators. This is due to their simplicity design, cost-effectiveness, compactness, label-free, portability, non-invasive nature, CMOS compatibility, and ease of sample preparation [5–10]. With recent progress in research [5–7], planar CSRR was established as a leading instrument among a broad variety of disciplines, from medical and biomedical sensing applications [7,11,12] to the oil and gas industry [13], from materials characterisation, process control to environmental monitoring [14].

A typical CSRR consists of a high-conductive metal that is fabricated on a rigid dielectric substrate surface [10]. Their design geometry and the physical parameters of the environment in which they are placed impact the resonant features of these microwave

37 resonators. The resonant features variation versus the change in the materials under
38 test (MUT) permittivity placed on the sensor surface is used to determine sensitivity for
39 these types of sensors [5,6,9,12]. The air gap effect between the sample and the sensor in
40 these structures is a common and unavoidable issue. By properly tightening the sample
41 and the sensor together, a fraction of the error due to air gap may be reduced [5,15]. This
42 is while nearly all CSRR-based biosensors proposed so far are rigid devices, limiting
43 their applicability to MUT with curved surfaces such as fingers. Flexible structures can
44 enhance the particularly crucial conditions, especially in wearable electronic applications.
45 To the best of our knowledge, the only flexible devices proposed are the glucose moni-
46 toring device suggested by Daneshman's group in [12] and the glaucoma monitoring
47 device proposed by Ekinici et al. in [10], where both of them used microfabrication
48 procedures. Microfabrication processes, as is widely known, involve specialized labo-
49 ratory equipment and materials such as deposition or lithographic equipment utilized
50 by professionals. Given the expense of cleanroom treatment and the time needed, this
51 approach is not only complex and expensive but is not even available to many research
52 groups or organizations [16,17].

53 Here the possible solution to this difficulty with a simple, flexible, and cost-effective
54 resonator microwave sensor using a novel manufacturing approach for non-invasive
55 biomaterial permittivity measurements is provided. This approach eliminates complex
56 microfabrication processes, lowering total costs and making it a viable choice for POCT
57 outside of hospitals or health centers for outpatient monitoring, as well as revitalizing
58 medical and health care in resource-limited locations. Furthermore, the suggested
59 device is built from thin polydimethylsiloxane (PDMS) substrate as an inexpensive
60 biocompatible and flexible polymer, making it applicable when the sample accessibility
61 has technical challenges, such as curved surfaces or liquid samples such as saliva or urine.
62 The proposed sensor is designed and simulated using the numerical electromagnetic
63 solver, the Computer Simulation Technology (CST). The proposed sensor is tested
64 in terms of flexibility and sensitivity using in-vitro setups and is compared with the
65 typical rigid CSRR sensors. In comparison to the standard SRR, there is a substantial
66 improvement in sensitivity and performance. The structures and results are described in
67 the following.

68 2. Materials and Methods

69 CSRRs typically consist of one or more rings etched out from a flat conductive layer.
70 The rings can be in different shapes, such as circles as one of the popular ones, with
71 small gaps on one side or two opposite sides (Figure 1 (a)). A circuit can model the
72 CSRR's electrical behavior with equivalent resistance, capacitance, and inductance. The
73 gaps can be interpreted as capacitors (C), and the rings can be considered as inductors
74 (L) and resistors (R) [6,18]. Accordingly, the resonance frequency can be calculated with
75 $f_0 = a/2\pi\sqrt{L \times C}$ while $C \propto \epsilon_0\epsilon_r$, where ϵ_0 and ϵ_r are permittivity of free space and
76 relative permittivity of the resonator's environment, respectively [7,9]. Therefore, it
77 can be stated that the sensor's resonance frequency is inversely associated with the
78 MUT's relative permittivity as its most critical characteristic in the context of microwave
79 engineering. Placing MUT on the resonator's surface changes the total effective permit-
80 tivity; consequently, the sensor's resonance frequency, which can be utilized as a sensing
81 parameter to distinguish different materials [5,10,12].

82 An electric field (E) perpendicular to the CSRR plane is required to excite the
83 structure, done with a microstrip transmission line [9,19]. The CSRR biosensors' function
84 can be easily evaluated by measuring the device's scattering parameters by using the
85 transmission line. So typically, the sensor comprises a substrate including metal layers
86 on both sides, one as a ground layer from which the rings are etched out, and the other
87 as a transmission line on the opposite side (Figure 1 (b)). To be analyzed, the biosensor
88 is connected to the vector network analyzer (VNA) through coaxial cables and SMA
89 connectors. Then the transmission spectra S_{21} is measured, which strongly depends on

90 the frequency. Notably, when compared to other scattering parameters, the influence of
 91 sample material permittivity is more significant on the S_{21} behavior [5,18,19].

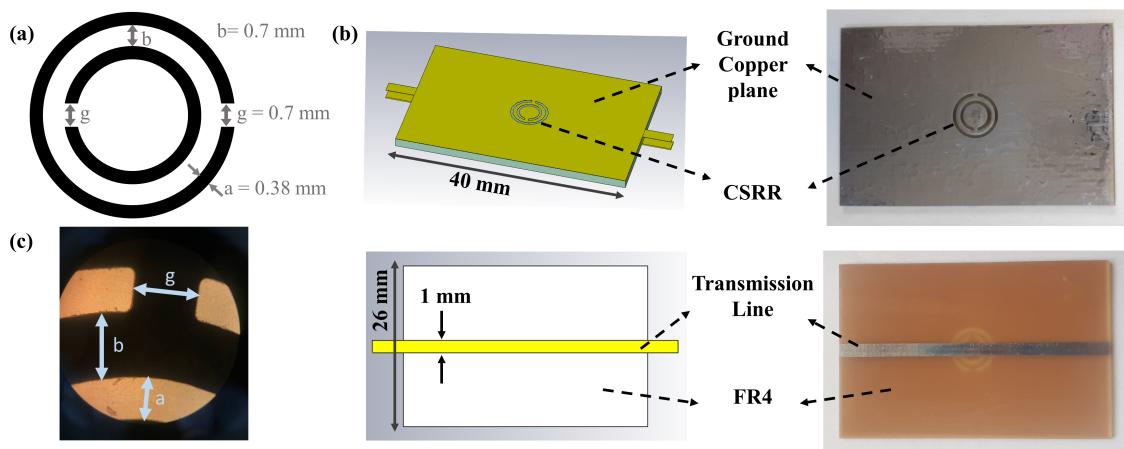


Figure 1. (a) Schematic of circular CSRR with design parameters. (b) Perspective view of simulated and fabricated model of Rigid device. (c) Dimensions of fabricated device.

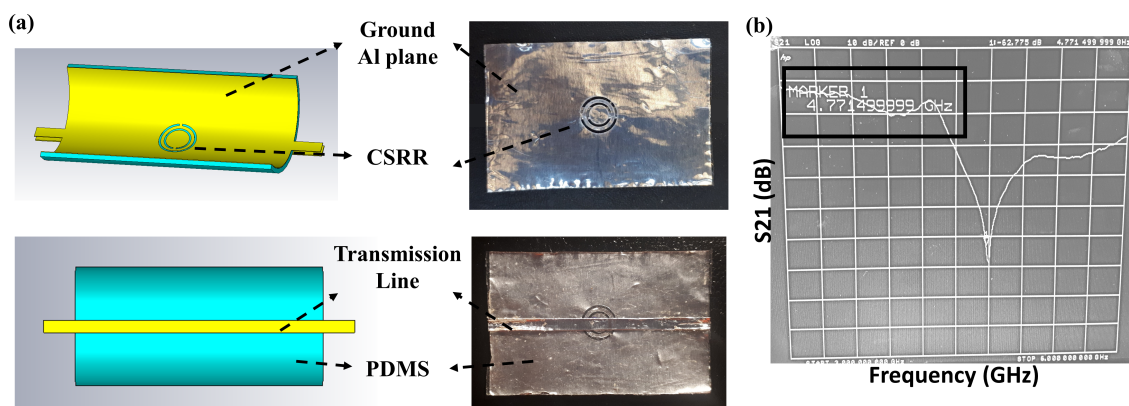


Figure 2. (a) Perspective view of simulated and fabricated model of flexible device. (b) Measured transmission coefficients as a function of frequency for flexible device without MUT.

92 Since the objective sensors operate at different resonance frequencies, the results
 93 should be normalized to the relevant frequency to allow a more realistic performance
 94 comparison. In this regard, the quantity that helps us is their sensitivity, defined as the
 95 relative frequency shift vs. permittivity changes of MUT for a given volume. Because the
 96 tests are performed on similar materials, we choose parameter S defined as $S = \Delta f / f_0$
 97 where $\Delta f = f - f_0$ to compare different devices. Here f and f_0 indicate the resonant
 98 frequencies in the cases with and without MUT, respectively [5,7,12].

99 The primary goal of this work is to examine the fabrication process and performance
 100 of a flexible CSRR-based biosensor to reduce the air gap effect between the sample and
 101 the sensor, which is a common yet unavoidable problem. A rigid structure is also
 102 considered to compare its performance as the standard technology to that of the flexible
 103 one. So, it is fabricated on a conventional printed circuit board (PCB) for the experimental
 104 investigation, see Figure 1 (b). The ground copper plane is printed on one side of the
 105 FR4 substrate, with the rings etched out of it, and the copper transmission line is printed
 106 on the other side. The shape of the CSRR is chosen to be circular based on Ansari et al.
 107 comprehensive sensitivity study [5], which reveals that the circular CSRR gives higher
 108 sensitivity than the rectangular CSRR with the same unit area. The dimensions and
 109 configuration of the device are shown in Figure 1 (a), (b), and (c).

110 As illustrated in Figure 2 (a), the proposed flexible device is fabricated from Poly-
 111 dimethylsiloxane (PDMS) as its substrate and Aluminum as the metal parts. Because of
 112 PDMS's biocompatible nature and mechanical impedance near to that of soft tissues, it
 113 has been widely used in biomedical applications [17,20]. Aluminum tape is chosen to
 114 implement the ground plane and transmission line in this structure because it is not only
 115 inexpensive and readily available, but it can also withstand various bending positions
 116 without damage. After that, to make patterns on Aluminum tape, a conventional laser
 117 engraver was used. The suggested methodology eliminates traditional microfabrication
 118 procedures, which are complicated and expensive to fabricate microfeature-sized de-
 119 signs. Therefore, the proposed flexible biosensor is low-cost and easy to use, proper for
 120 POCT applications.

121 Both rigid and flexible structures are modeled in the CST studio suite for the
 122 simulation phase to acquire the two-port scattering parameters in the specified frequency
 123 band with and without MUT. After analyzing the simulation results, they are fabricated
 124 to compare experimentally. Figure 1 and Figure 2 show the overall structure of both
 125 devices in simulation and experiment.

126 3. Results

127 For evaluating the proposed structure, the simulation results were first compared.
 128 By using the suggested model for rigid and flexible sensors in CST Microwave Studio,
 129 S_{21} profile and sensitivity of sensors for different materials such as wood and rubber as
 130 reference samples are analyzed. Firstly, to consider the influence of device flexibility in
 131 analyzing samples with curved surfaces, two devices with similar characteristics such as
 132 geometry and material (PDMS and Al) in flat (rigid) and bend (flexible) structures were
 133 simulated. The results with and without MUT are shown in Figure 3 (a). The frequency
 134 change in the sensor's transmission spectra is obvious by positioning a specific volume of
 135 wood as MUT on the resonator's surface. In this case, the sensitivity of rigid and flexible
 136 devices are 0.042 and 0.062, respectively, corresponding to 48% sensitivity improvement.
 137 Consequently, as expected, the flexible structure performs better for samples with curved
 138 surfaces.

139 Following that, two structures with identical dimensions and materials to that of the
 140 fabricated devices, a flexible Al-PDMS sensor and a rigid Cu-FR4 device, were simulated.
 141 It is worth noting that due to fabrication faults, there is a slight variation between f_0
 142 of two devices, which is also taken into account in the simulation. The results of both
 143 devices for different MUT are compared in Figure 3 (b). Rigid sensor sensitivity for
 144 wood and rubber samples was 0.040 and 0.136, respectively, whereas these were 0.060
 145 and 0.149 for the flexible sensor. Here, there are also a 50% and 9.6% improvement in
 146 sensitivity for flexible structure for wood and rubber, respectively.

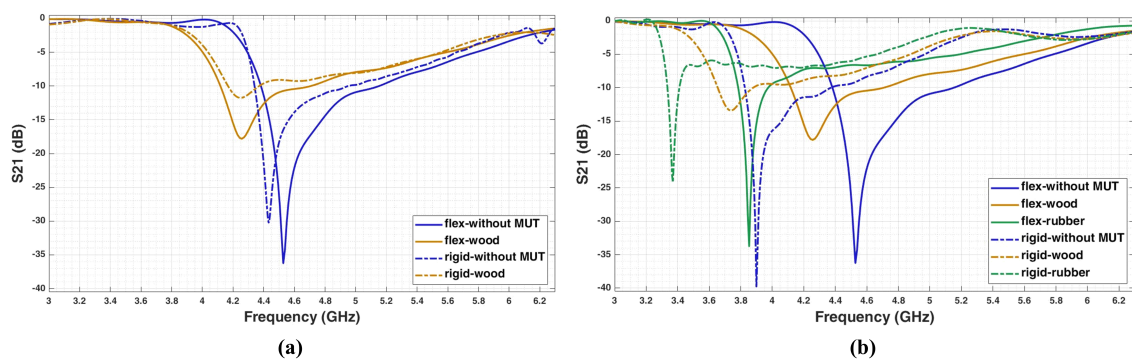


Figure 3. Simulation of S_{21} as a function of frequency for (a) rigid and flexible devices with similar characteristics such as geometry and material (PDMS and Al). (b) a flexible Al-PDMS sensor and a rigid Cu-FR4 device.

147 Now that the simulation results are desirable, the fabricated flexible device was
 148 examined in practice. During the test phase, it was necessary to place the flexible

149 biosensor on a curved surface to check its performance in the bent position. Flexible
150 sensors were tested on curved surfaces with various bending angles to ensure that
151 bending does not damage the biosensors and that their sensing performance stays
152 unaltered. Then, the S_{21} parameter was measured experimentally by connecting the
153 device to the VNA via SMA connectors. The sensor response is steady and reproducible.
154 Also, based on experimental results, the resonant frequency for bent flexible biosensor
155 was 4.77GHz (Figure 2 (b)) which is close to the simulation results. Even though a
156 frequency shift in the device's transmission spectra was observed by positioning MUT,
157 it should be optimized to improve sensitivity.

158 4. Discussion

159 In this study, a novel, cost-effective, flexible complementary split ring resonator
160 was proposed to facilitate POCT. We provided simulation and experimental results for
161 studying the effects of flexibility of sensor on its sensitivity. The results showed that
162 the proposed structure can improve sensitivity for the samples with curved surfaces.
163 This capability can be used to characterize various MUT such as blood, saliva, or when
164 the accessibility of the sample has technical difficulties, such as curved surfaces. A
165 comparison between traditional rigid microwave resonators and the proposed sensor
166 was provided here to present a meaningful understanding of sensitivity enhancement in
167 the proposed sensor.

168 In microwave resonator sensors, the electromagnetic fields interact with the MUT,
169 which is how the sensing mechanism works. It has been demonstrated in the literature
170 that the substrate stores a significant amount of electromagnetic energy; hence, increas-
171 ing the interaction of MUT with substrate is predicted to enhance its electromagnetic
172 interactions with the resonator, resulting in improved sensitivity [7]. With this argument,
173 we predicted that a flexible sensor could provide better results than a flat sensor for
174 curved specimens. This hypothesis was confirmed by the obtained results. Despite
175 the fact that flexible microwave resonators provide acceptable results, there are still a
176 number of difficult challenges to overcome.

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