

# **Wearable Multi-Frequency and Multi-Segment Body Impedance Spectroscopy (**WM\_BIS**) in Sports and Rehabilitation Medicine**

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# Background

Body Impedance Spectroscopy (BIS)  
may assess the composition of body districts  
noninvasively and quickly.

For this reason, BIS can provide  
important physiological or clinical information  
for sport-medicine studies  
or rehabilitation protocols.

# Background

However, available instruments do not **simultaneously** satisfy the demanding needs that exercise/rehabilitation tests often requires, i.e.,

- \* recording BIS unobtrusively
- \* over a broad frequency range
  - \* for long periods
- \* in different segments at the same time
  - \* with high measurements rate.

# Aim

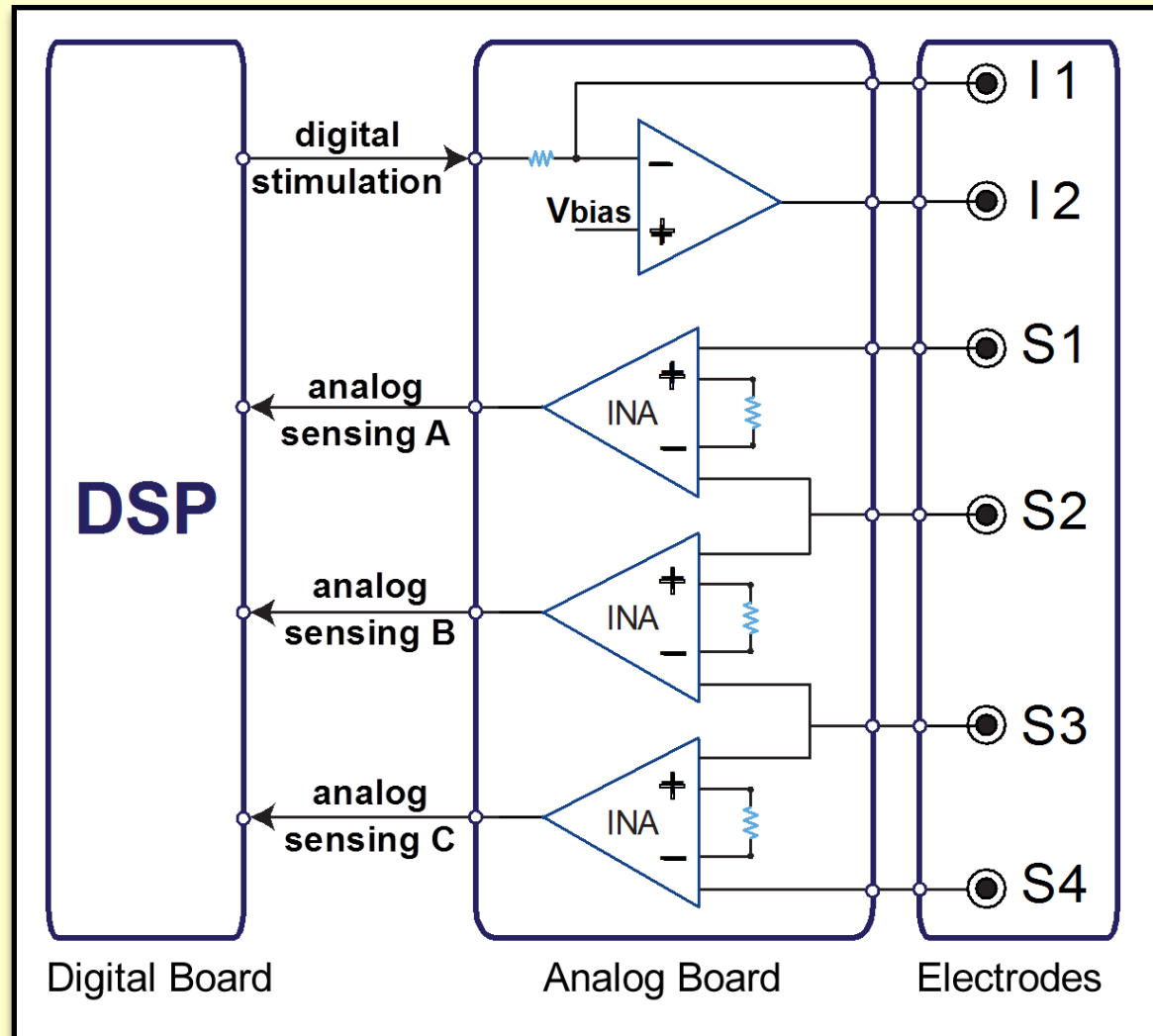
Therefore our aim is to present a new prototype:

- 1) designed for monitoring multi-segment, multi-frequency BIS, unobtrusively over long periods
- 2) that guarantees wearability with its low weight, small size and low power consumption.

Our prototype, **WM\_BIS**, should meet the needs required for rehabilitation or sport-medicine studies:

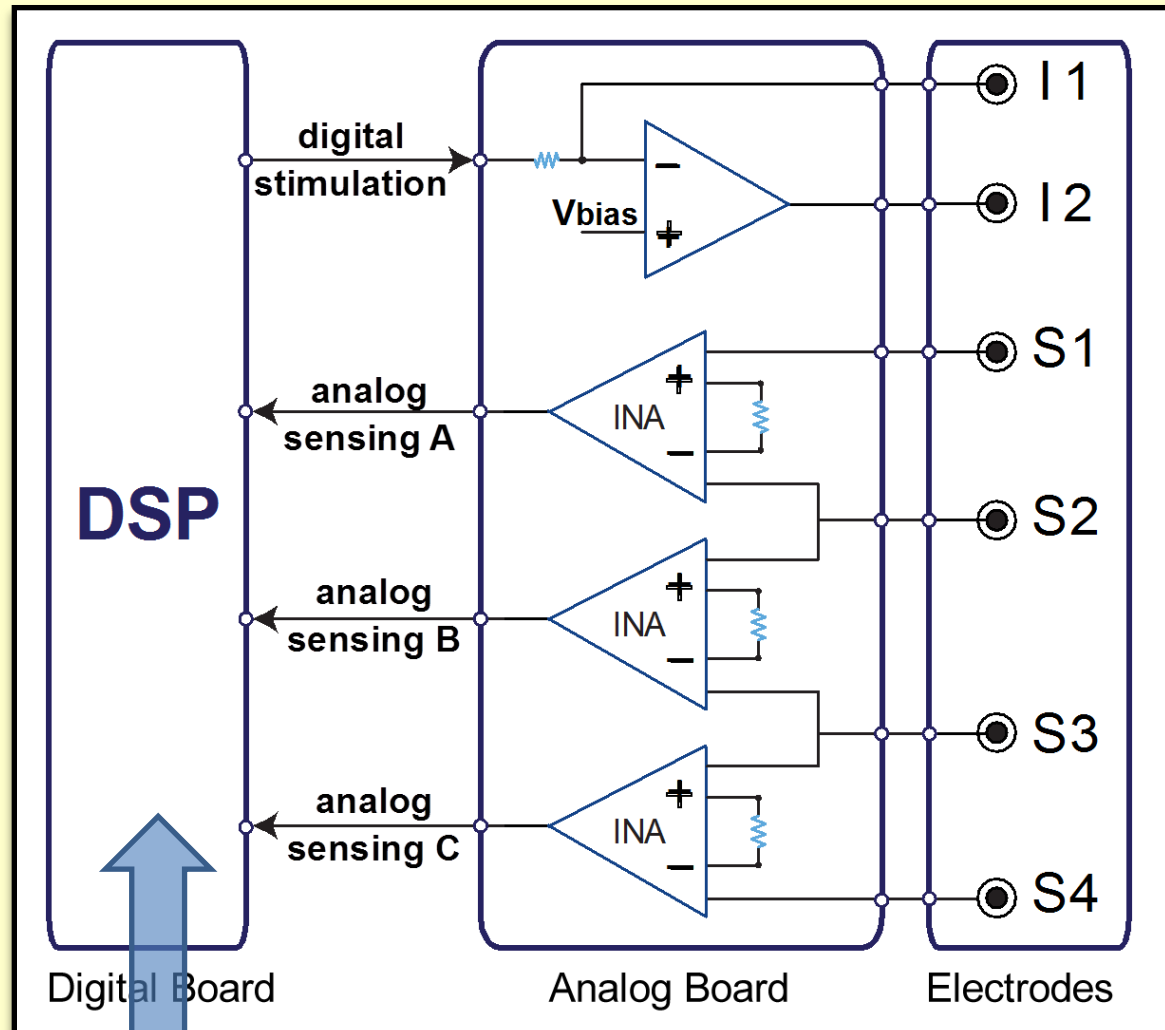
for this reason, its performance is illustrated with an application in the field of sports and rehabilitation medicine.

# Design of the wearable BIS system



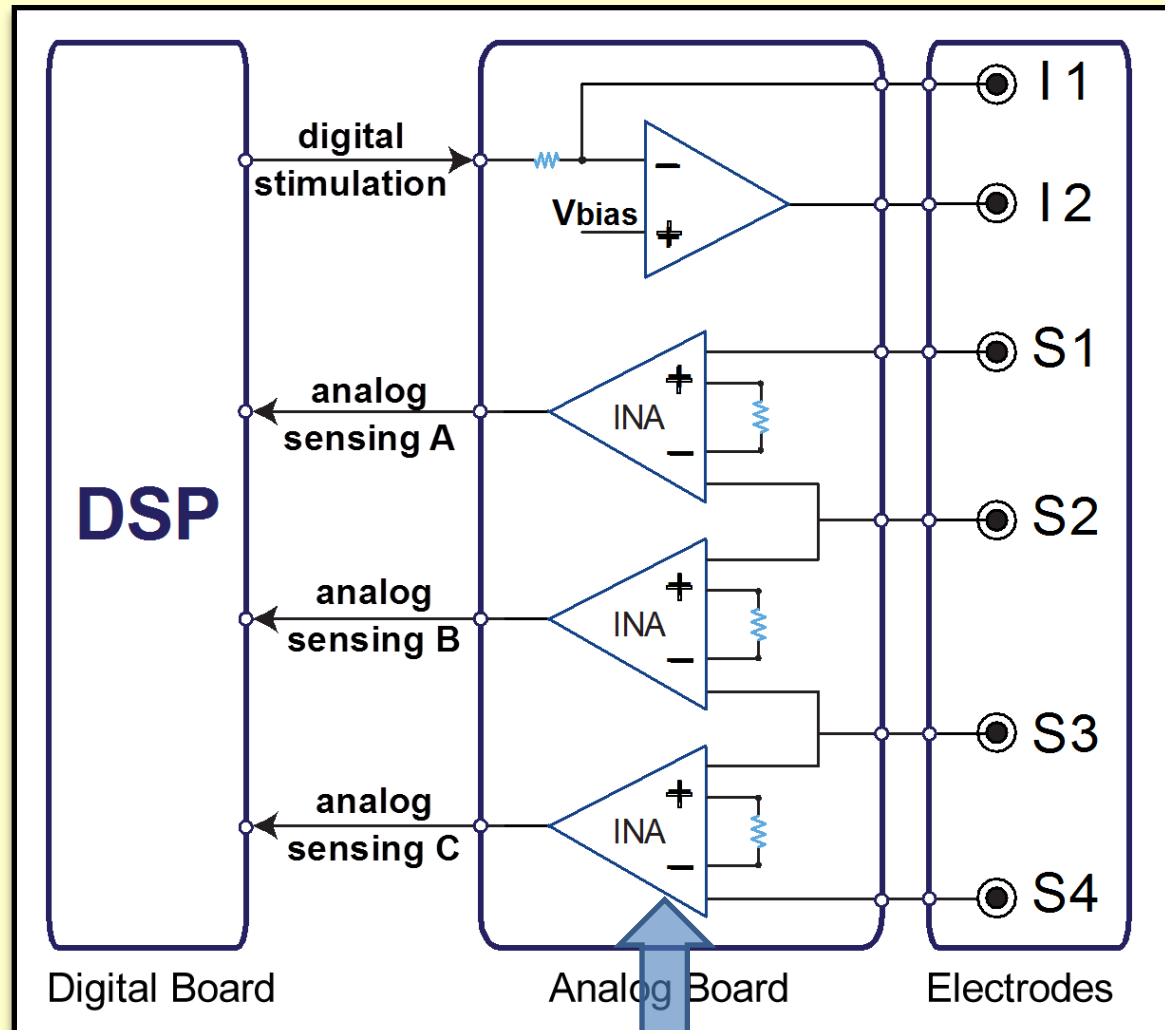
The system consists in two boards: a digital board with a DSP (Texas Instrument C2000 "Piccolo family", 80 MHz clock) and a custom analog board

# Design of the wearable BIS system



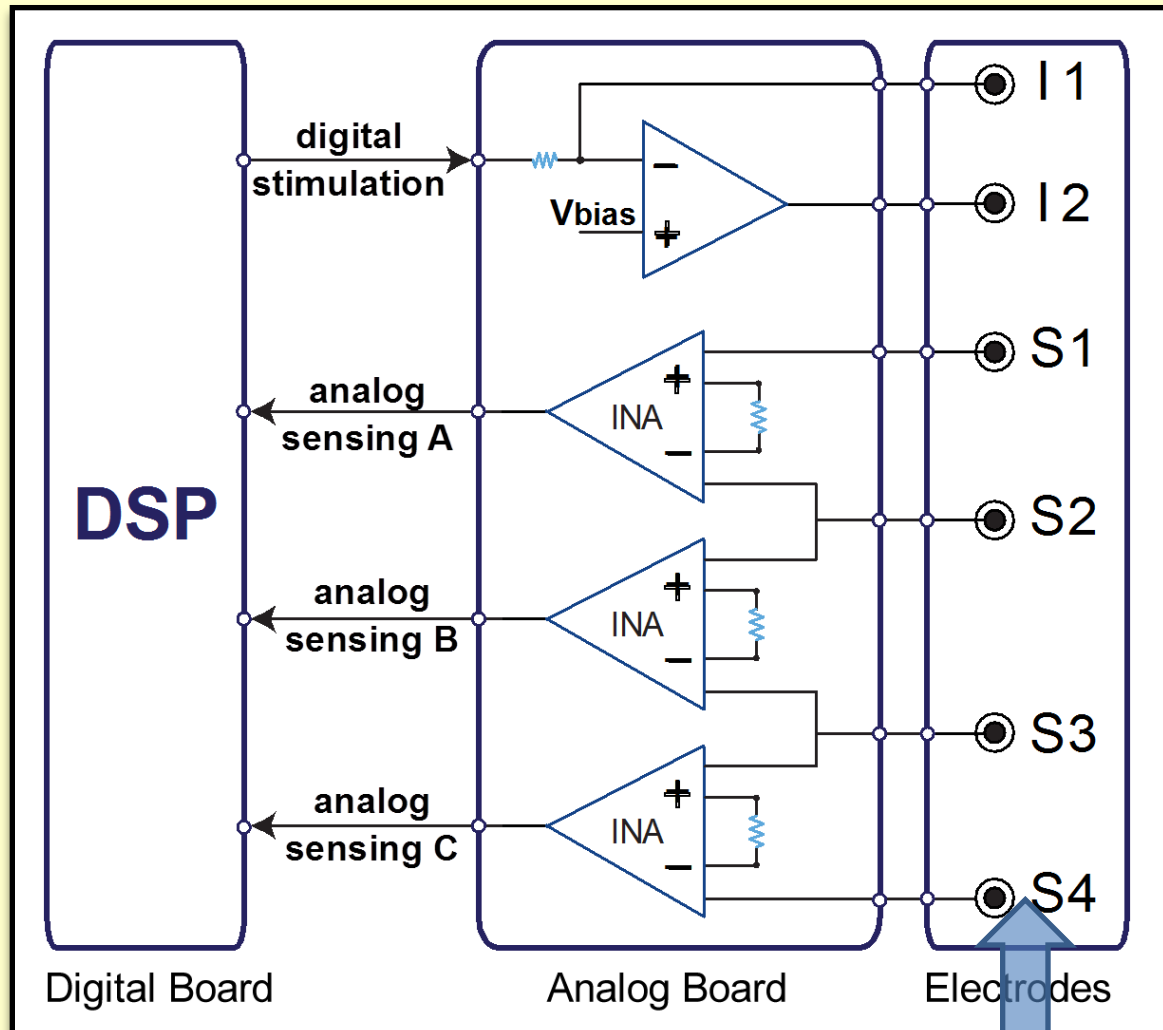
The DSP generates the stimulus waveforms, samples and digitalizes the voltage across three body segments with its 12-bit Analog to Digital Converter (ADC) and computes magnitude and phase of impedance,  $Z(f)$ .

# Design of the wearable BIS system



The analog board interfaces the DSP with the electrodes. A transimpedance amplifier is connected to two injecting electrodes; three instrumentation amplifiers (INAs) read the voltages across three body segments by means of four sensing electrodes.

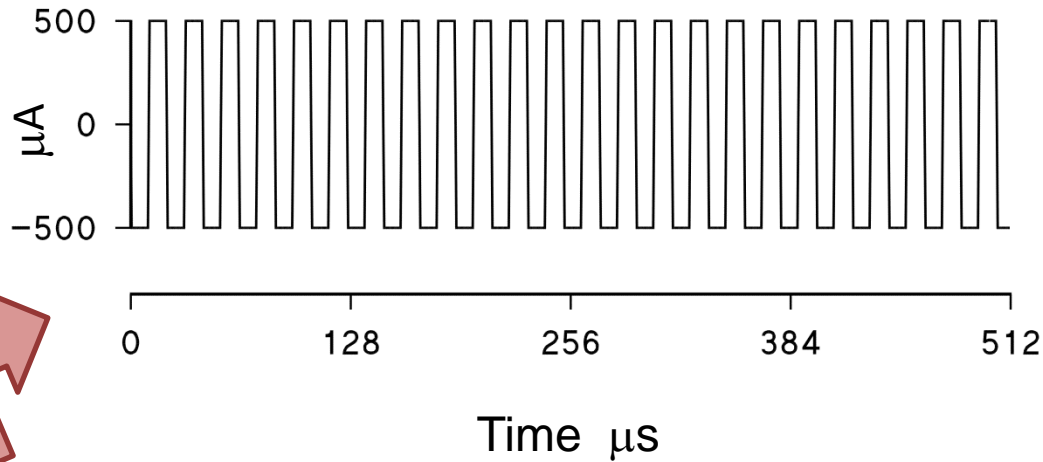
# Design of the wearable BIS system



By using separate injection and sensing electrodes, measures are independent from the electrode impedance (this allow using small disk electrodes, avoiding band electrodes of larger area)



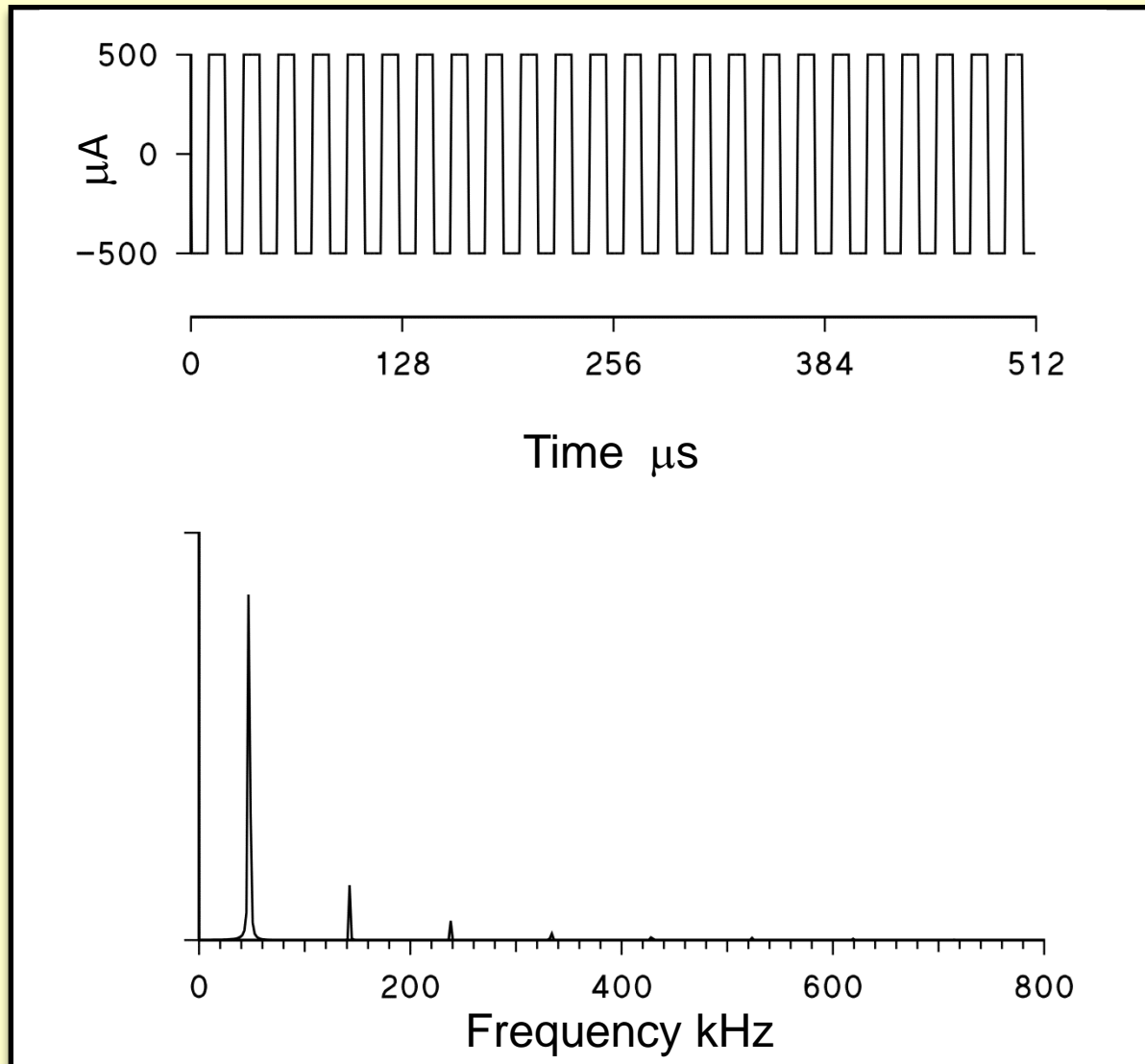
# Design of the wearable BIS system



Example of  
waveform with  
period = 1/48 kHz

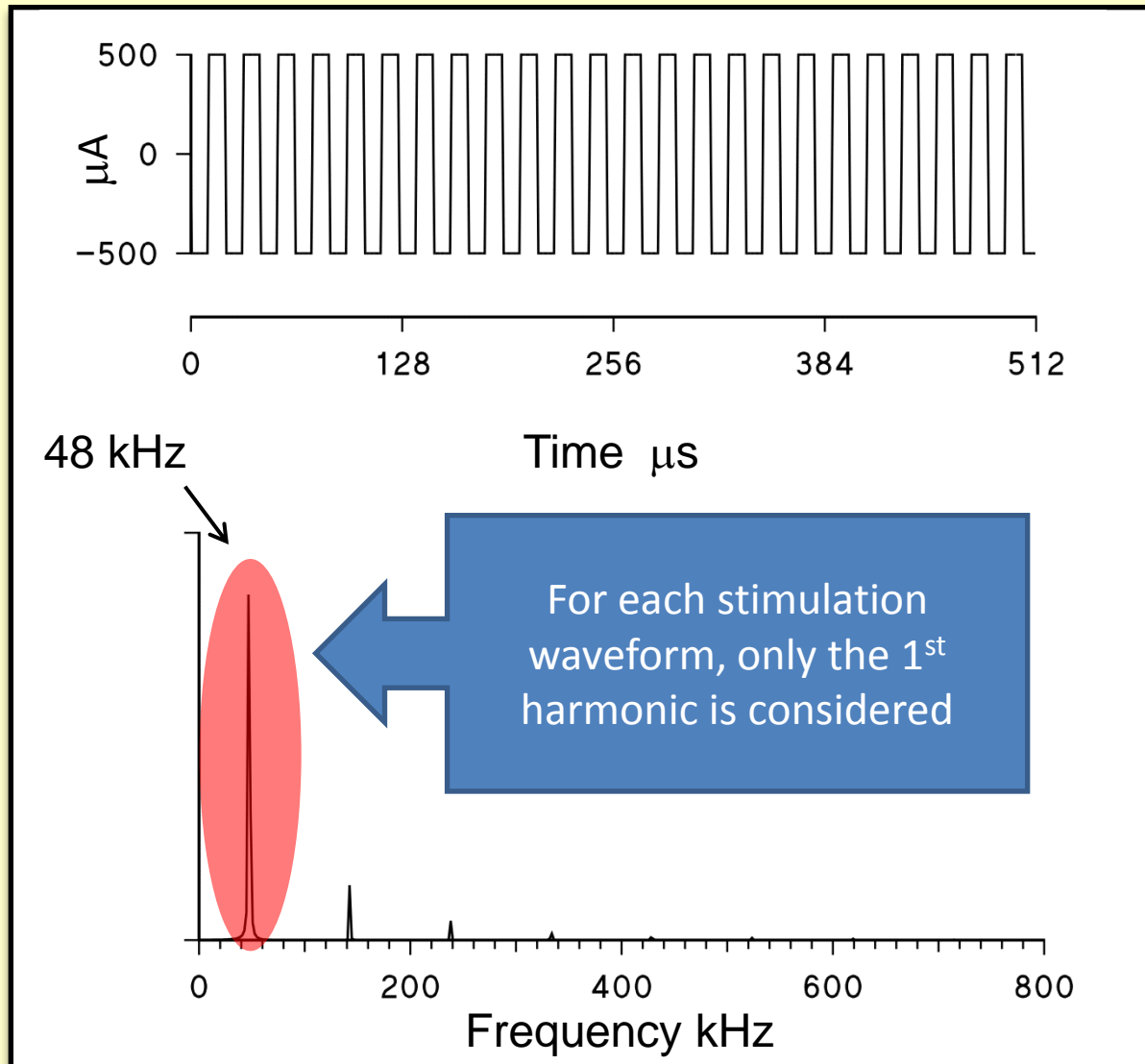
The stimulation waveform is not a sinusoid (as in commercial BIS devices) but a square wave. DSPs easily generate square waves and this waveform allows minimizing power consumption, size and cost

# Design of the wearable BIS system



The DSP extracts magnitude and phase of  $Z(f)$  by FFT of the sensed voltage

# Design of the wearable BIS system



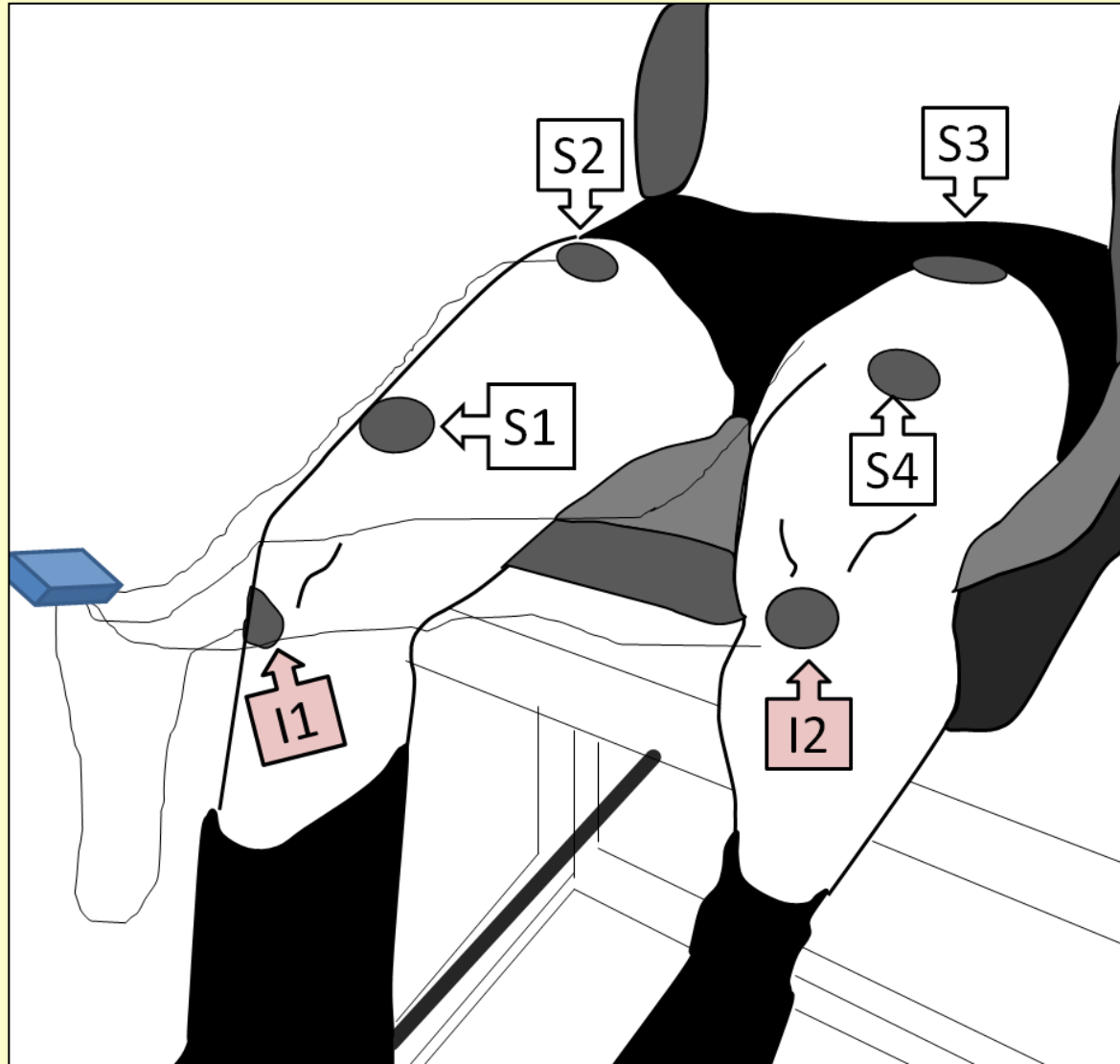
The DSP extracts magnitude and phase of  $Z(f)$  by FFT of the sensed voltage

# Realized Prototype



size =  $8.5 \times 5.5 \times 2 \text{ cm}^3$ ;  
weight <100 g;  
total power consumption <100 mW

# Experimental Set-Up



We instrumented a volunteer with an injecting electrode on each knee (I1 and I2), sensing electrodes on distal and proximal endings of the rectus femoris muscle belly of the two thighs. Monitored segments were right (S1-S2) and left (S3-S4) thighs and pelvis (S2-S3).

# Experimental Set-Up

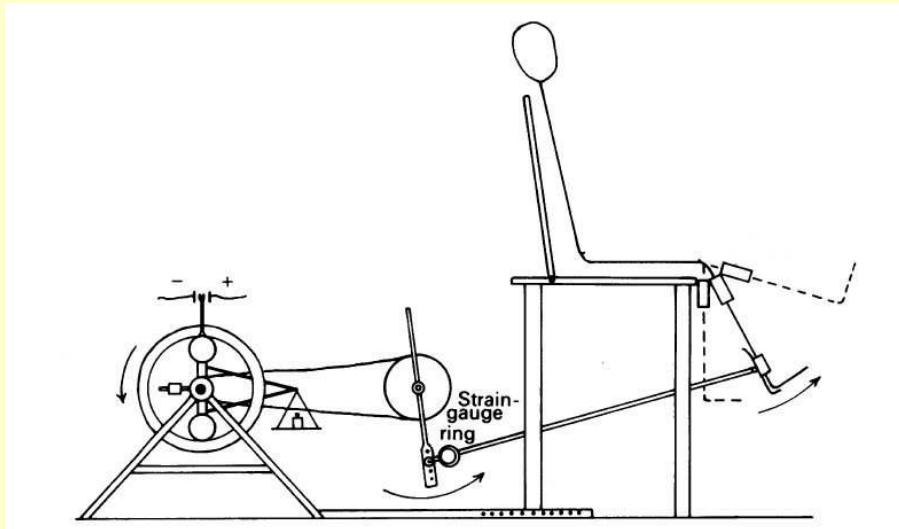
Baseline  
7 minutes

Exercise  
20 minutes

Recovery  
20 minutes

Standing  
7 minutes

Volunteer sitting on a one-legged knee-extensor ergometer



# Experimental Set-Up

Baseline  
7 minutes

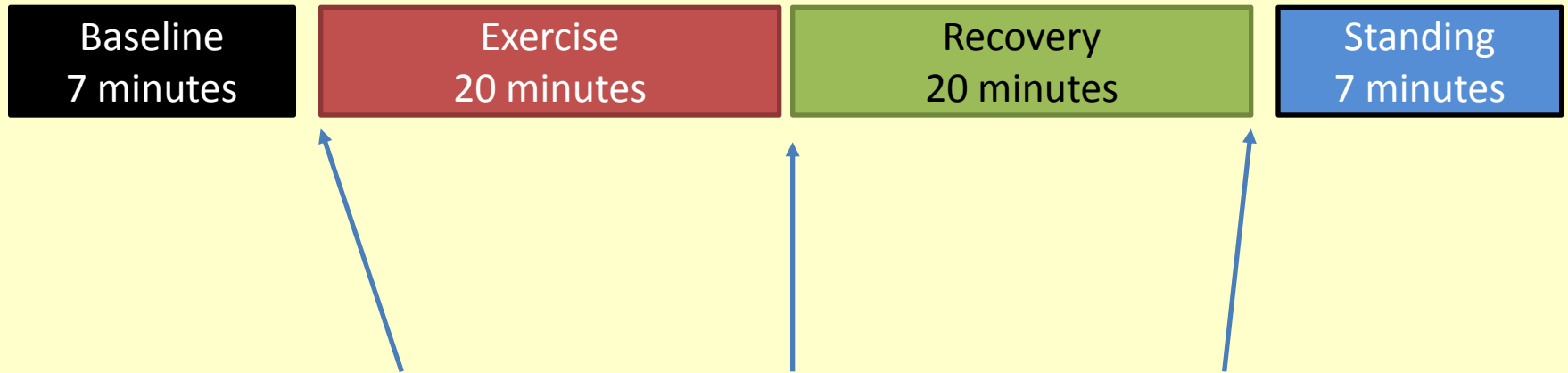
Exercise  
20 minutes

Recovery  
20 minutes

Standing  
7 minutes

EXERCISE= repeated kicking extending the knee of the right (dominant) leg, at 60 extensions/minute. The ergometer load was set at 25 watts with the exclusion of the initial warm-up (10 watts) and of the last 2 minutes (50 watts).

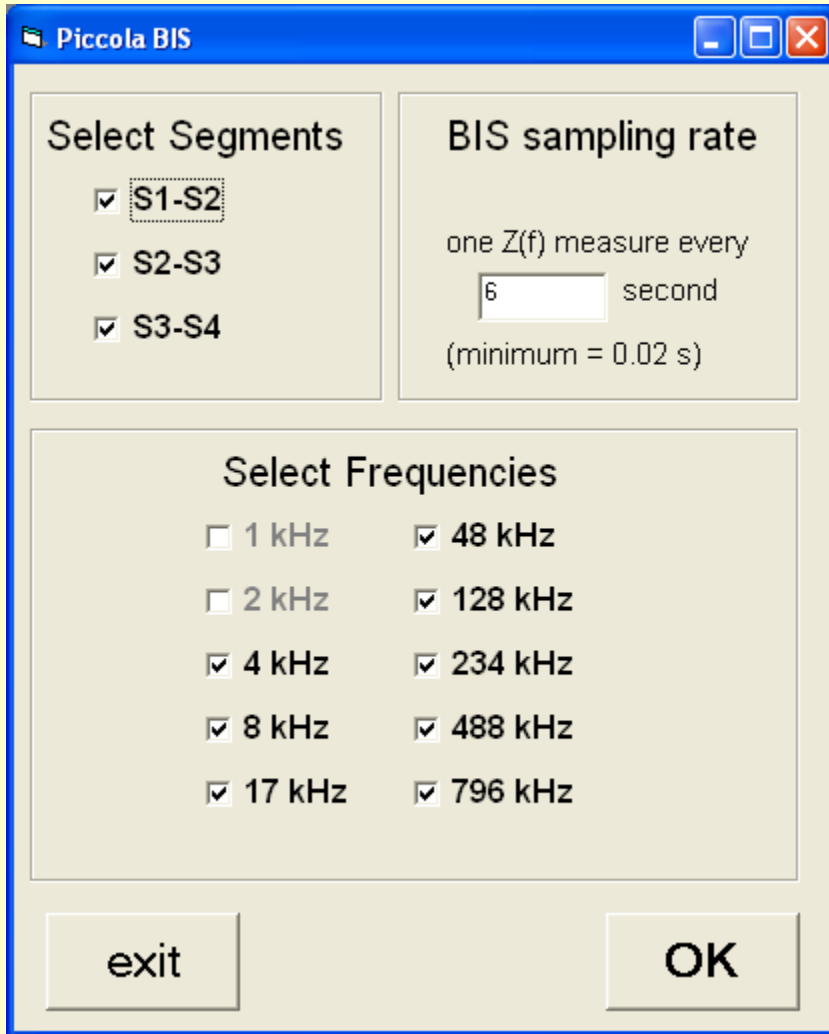
# Experimental Set-Up



Subsequent conditions were spaced by few minutes to exclude transition phases



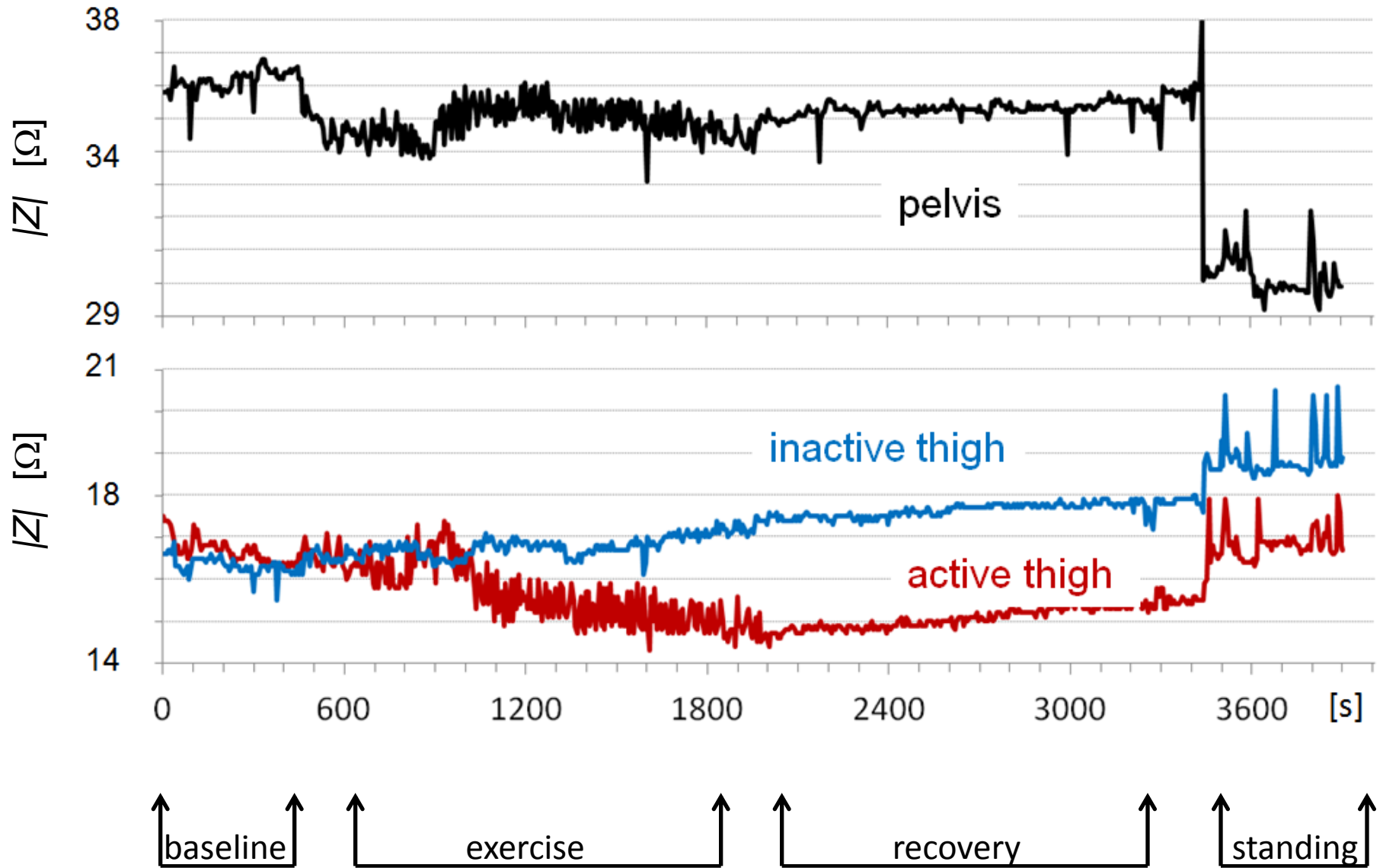
# Experimental Set-Up



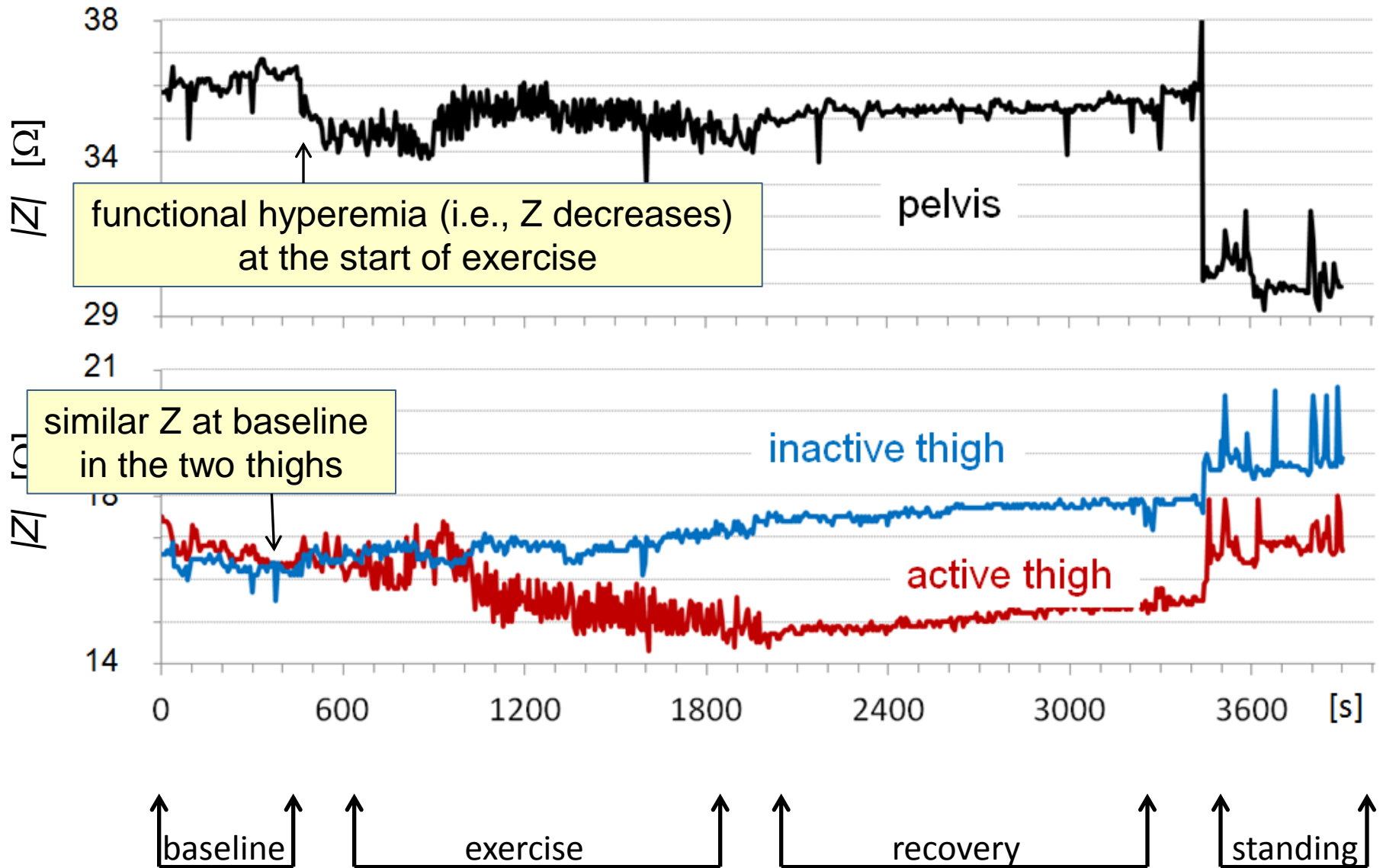
The device was set for providing  $Z(f)$  of the 3 body segments simultaneously every 6 s (maximum sampling rate = 50 Hz)

at 8 of a maximum of 10 frequencies equispaced in a log-scale between 1 kHz and 796 kHz

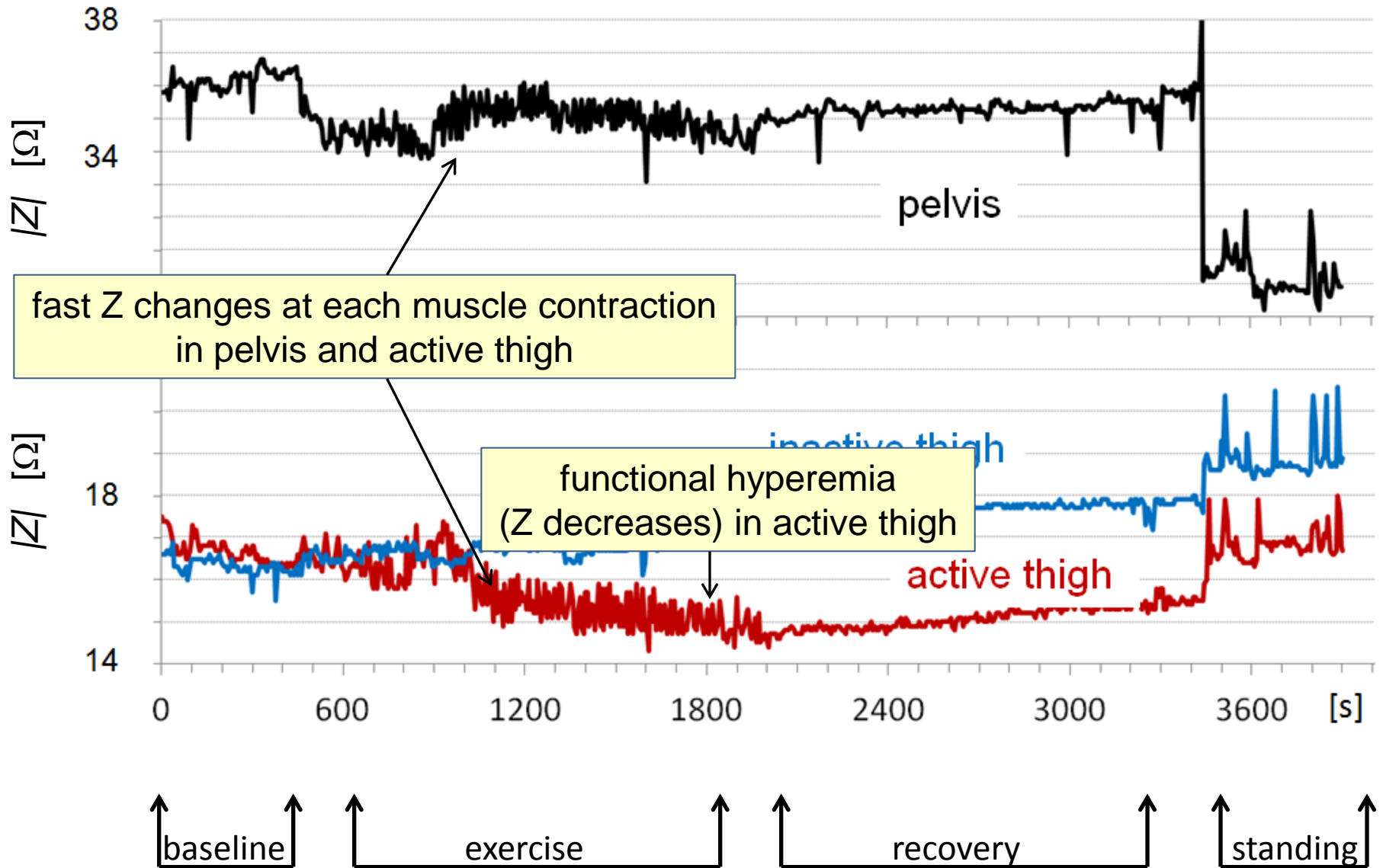
# Results: $|Z(f)|$ at $f=48$ kHz



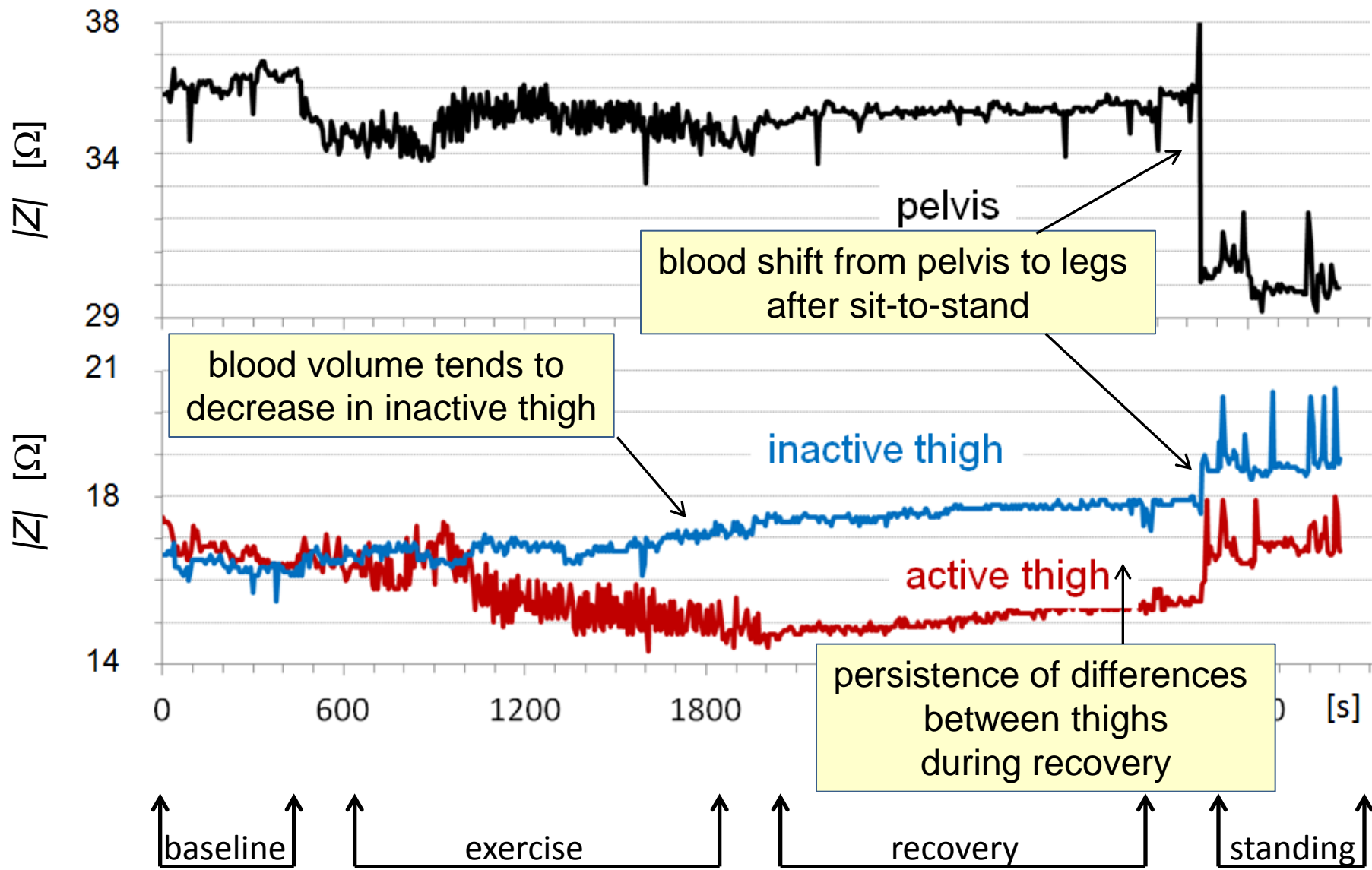
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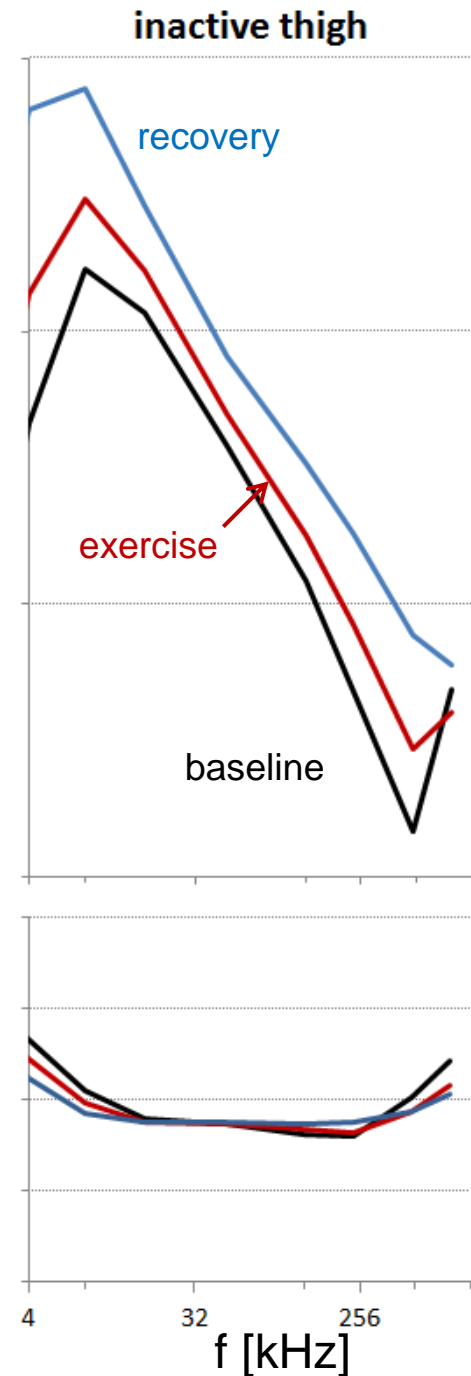
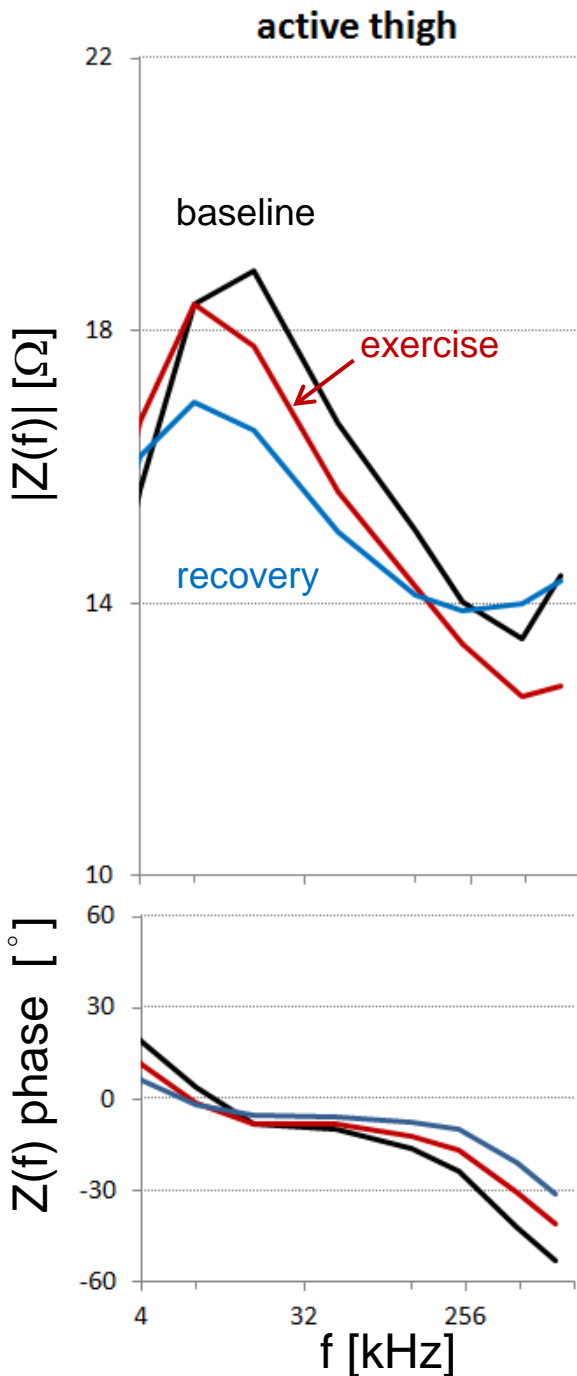


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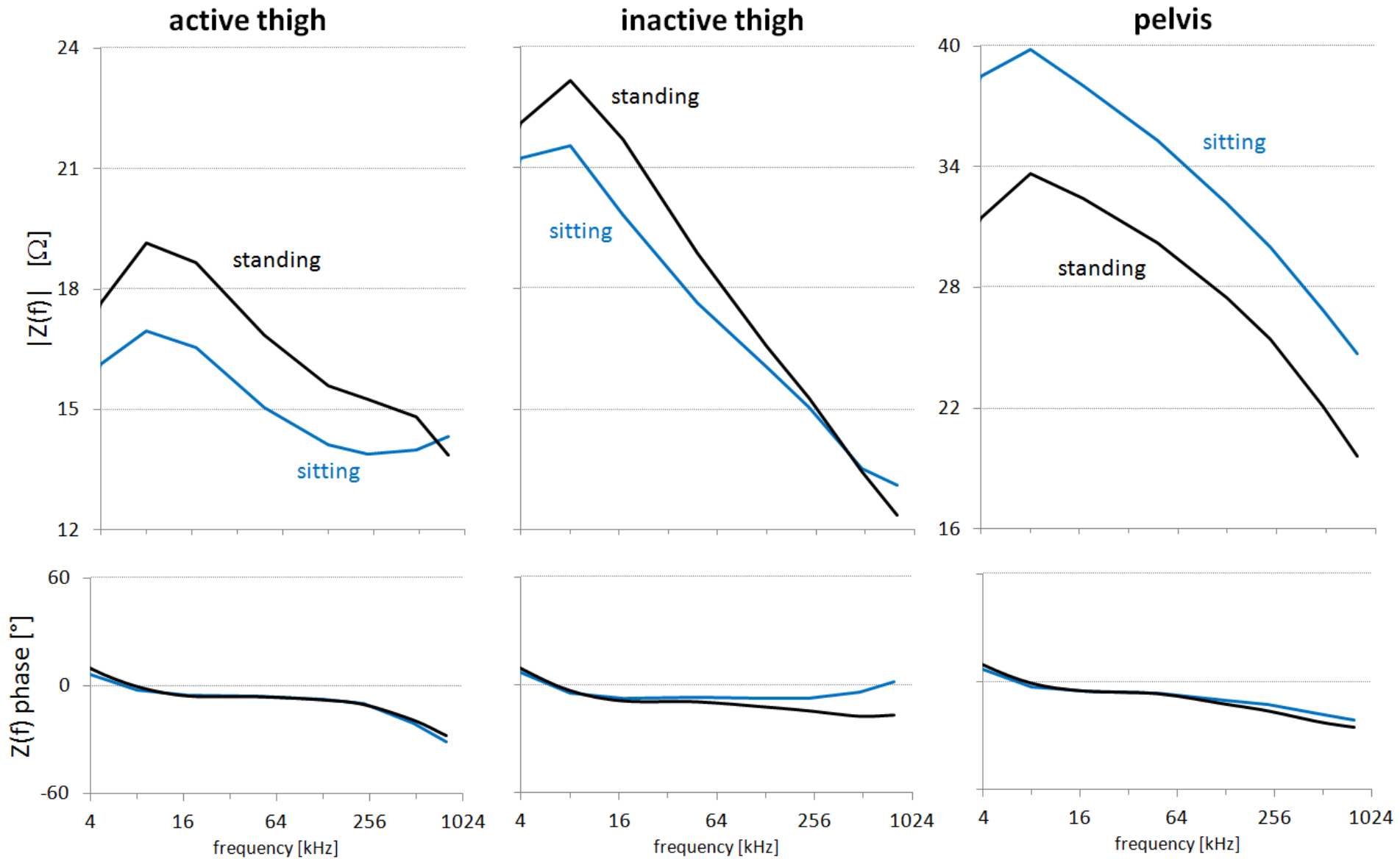


## $Z(f)$ in the thighs during the knee-extensor test

We found opposite trends from **baseline** to **exercise** and to **recovery**:

$|Z(f)|$  decreased in the active thigh  
 $|Z(f)|$  increased in the inactive thigh.

Changes are more pronounced between 16-64 kHz in the active thigh, between 4-16 kHz in the inactive thigh.



### **Z(f) from sit to stand during recovery.**

$|Z(f)|$  of thighs increased, mainly at the lower frequencies.

$|Z(f)|$  of pelvis decreased, uniformly over the whole frequency band

# Discussion

The exercise test illustrated the amount of information that our wearable BIS device may provide.

Actually, our system was able to **quantify BIS dynamics** over very different time scales, from the fast changes due to each muscle contraction up to long-term trends during recovery.

By monitoring different body segments simultaneously, it was able to detect shifts of blood volumes among contiguous districts.

In particular, it showed that the effect of the knee-extensor exercise regards different frequencies on the active and inactive thigh, **suggesting that the blood shift between legs changes the ratio between intra-cellular and extra-cellular liquids.**

This finding would not be observed with traditional mono-frequency systems.



# Conclusions

Our prototype has the lightness, wearability and unobstrusiviness required by “real field” studies of sports and rehabilitation medicine.

Specific technical solutions  
(DSP, square wave stimulations, small disk electrodes)  
allow monitoring more segments simultaneously  
and continuously for long periods.

This makes it possible  
describing different body segments at the same time,  
with frequency- and time-resolution  
not achievable by traditional BIS systems.