



Proceedings Normal range of motion of lower extremity joints in Mongolian subjects⁺

Batbayar Khuyagbaatar,* Tserenchimed Purevsuren and Ganbat Danaa

4

5

6 7

8

19 20

21

3

2

Biomechanical Research Laboratory, School of Mechanical Engineering and Transportation, Mongolian University of Science and Technology, Ulaanbaatar 14191, Mongolia * Correspondence: batbayarkh@must.edu.mn; Tel.: +976-86075099

+ Presented at the title, place, and date.

Abstract: It is important to identify the normal range of motion (ROM) of the human joints for both 9 biomechanical and clinical applications. For health care providers, including physicians and thera-10 pists, the restoration of normal ROM is a difficult task. The severity of impaired joint mobility or the 11 postoperative rehabilitation process must be evaluated in comparison with a normal reference 12 value. However, there is no studies have reported the ROM of the Mongolian subjects. In this study, 13 we measured the hip, knee, and ankle joint angles using a multiple wearable inertial sensor. Ten 14 healthy young subjects participated. The three-dimensional (3D) motion data were collected during 15 the walking with normal speed. In our knowledge, it is first to analyze the normal ROM of the 16 Mongolian male subjects. The collected data can be reference values for evaluating the disability of 17 the motion and performance in rehabilitation programs. 18

Keywords: normal range of motion; Mongolian; wearable sensors

1. Introduction

Identification of the natural gait characteristics of people is important from both the biomechanical and clinical perspective [1]. Many diseases and injuries can impair joint mobility, which results in a decline in ROM or changes the gait characteristics. Furthermore, the abnormal gait characteristics are associated with aging and abnormal lifestyle. Joint motion varies with age and is generally more restricted in the older age group [2].

For health care providers, including physicians and therapists, the restoration of nor-27 mal ROM is a difficult task. The severity of impaired joint mobility or postoperative reha-28 bilitation process must be evaluated in comparison with normal gait patterns. These nor-29 mal gait parameters have been investigated extensively in a variety of countries including 30 the United States [3], Sweden [2], Korean and Western [1], Japanese [4], and Chinese [5]. 31 However, there is no studies have reported the ROM of the Mongolian subjects. Further-32 more, the video-based motion analysis systems cannot provide the details of the joint mo-33 tions during the movements. Since the 3D joint angle measurement is an important re-34 quirement, notably in the orthopaedic and rehabilitation fields [6]. 35

Recent developments in sensor technology allow us to precisely measure the human movements. There are several studies that have used the inertial measurement unit (IMU) sensor for analyzing the kinematics of the lower extremity during normal walking and other motions in a variety of countries [6–9]. In this study, we investigated the joints angles of the hip, knee, and ankle during the walking using wearable IMU sensors. 40

41 42 43

44

Citation: Lastname, F.; Lastname, F.; Lastname, F. Title. *Proceedings* **2021**, 68, x. https://doi.org/10.3390/xxxxx

Published: date

Publisher's Note: MDPI stays neutral with regard to jurisdictional claims in published maps and institutional affiliations.



Copyright: © 2021 by the authors. Submitted for possible open access publication under the terms and conditions of the Creative Commons Attribution (CC BY) license (https://creativecommons.org/license s/by/4.0/).

2. Materials and Methods

3.1. Participant Information

Ten male subjects (age, 26.1 ± 7.8 years; height, 177 ± 7 cm; weight, 76.4 ± 17.6 kg), 3 who had no had no musculoskeletal injuries within the past year, were recruited in this study. All subjects were recruited with informed consent from the Mongolian University of Science and Technology (MUST). 6

3.2. Experiment Procedure

Each subject performed three times of walking under supervision. Subjects were 8 asked to perform the walking with normal speed to minimize the speed differences. Prior 9 to the experiment, each participant was asked to perform several times of walking as a warm-up. The experiment was conducted in the indoor laboratory at the MUST. The sub-11 jects were wearing IMU sensors, a training suit and sports shoes. In total, 6 IMU sensors 12 (Wearnotch, Notch Interface Inc) were used to record the right lower extremity motion 13 during the normal walking. The sensors were attached on the chest, tummy, right thigh, 14 shank, and foot using the straps. The IMU sensor includes 3-axis acceleration and 3-axis 15 gyroscope with ±16 g and ±2000 °/s with a sampling rate of 100 Hz. The sensors' locations 16 were described in Figure 1. 17



Figure 1. This is a figure. Schemes follow the same formatting.

3.3. Data Processing

At the beginning of the walking, subjects did a steady pose as a calibration. After 22 sensor calibration, each participant performed a normal walking. The sensor's raw data 23 sent to server computer and processed by using Matlab® R2015a (The Mathworks Inc., 24 USA) [10]. After data processing, the quaternions of the 6 sensors were estimated using 25 the 3-axis acceleration and 3-axis gyroscope data based on the Madgwick filter algorithm 26 [11]. Then, the joint angles were estimated based on the orientation difference between 27 the adjusting two sensors. The joint angles were represented as the Euler angles of the 28 distal segment reference frame relative to the proximal segment reference frame using 29 sensor's orientation [12]. The 3D rotations of the joints in sagittal, transverse, and coronal 30 planes were expressed as extension-flexion (Ex-Fl), internal-external (Int-Ext) rotation, 31 and adduction-abduction (Add-Abd), respectively (Figure 2). After calculating the 3D 32 joint angles, the one walking cycle was defined and normalized. The start and end of the 33 cycle were from a right heel strike to the next right heel strike. 34

1 2

4 5

7

10

18

19

20

21

1

2

3

4

5

6

7

8

9

10



Figure 2. Joint angle definition for hip, knee and ankle joints

3. Results

3.1. Joint angles of hip, knee and ankle joint

The hip, knee, and ankle joint angles during walking are shown in Figures 3. The maximum extension-flexion angles of the hip and knee were $30.8\pm3.5^{\circ}$ and $55.2\pm3.4^{\circ}$. In the ankle joint, the dorsiflexion-plantar flexion angle was $13.5\pm6.0^{\circ}$. The maximum adduction-abduction angles of the hip, knee, and ankle joints were $5.3\pm4.8^{\circ}$, $16.6\pm10.2^{\circ}$, and $10.3\pm5.8^{\circ}$. The maximum internal-external rotation angles of the hip, knee, and ankle joints were $5.5\pm4.5^{\circ}$, $7.3\pm10.2^{\circ}$, and $6.3\pm3.8^{\circ}$ (Figures 3).



Figure 2. Joint angles of hip, knee and ankle joint

3.2. Comparison with previous studies

The maximum flexion angles of the hip, knee, and ankle joints were compared to the previous studies. The results were summarized in Table 1. The total joint angle data were similar with previous studies[1,5,13,14]. Especially, the joint angular motion of this study was similar to Asian countries. It is because of the anthropometric similarities between the Asian countries. 18

12 13

11

Throughout flexion motions, the maximum difference of hip, knee, and ankle joints 1 between the current and the previous studies was 14.9°, 11.0°, and 14.8°, respectively. The 2 dissimilarity may be from the use of different motion capture systems. Our study utilized 3 the wearable motion capture system, while other studies have been used the conventional 4 marker-based system. Of course, the difference was occurred due to the gait characteristics of different nationalities. 6

	Hip	Knee	Ankle
Our study	30.8±5.5°	55.2±3.4°	13.5±6.0°
United States [13]	43.2°	56.7°	25.5°
Korea [1]	45.7°	58.0°	28.3°
China [5]	34.7°	66.2°	13.7°
Italy [14]	39.8°	65.3º	33.5°

Table 1. Maximum flexion angles comparison with previous studies

4. Conclusion

In this study, we utilized the wearable IMU sensor for measuring the normal ROM 10 of the lower extremity during the walking for Mongolians. The wearable sensor technol-11 ogy can be applied to both indoor and outdoor environments without any restrictions. 12 The raw sensor data was processed using the in-house developed algorithm based on the 13 Mahony filter. In my knowledge, it is first to analyze the 3D normal ROM of the Mongo-14 lian male subjects. But, the subjects were the only male, and a small number of the group 15 participated. Therefore, future work will need to include a large number of subjects as 16 well as different sex and age groups. Future work will also focus on the gait characteristics 17 of the nomadic peoples. This study provides fundamentals of the normal gait characteris-18tics during the walking, which can be reference values for evaluating the disability of the 19 motion and performance in rehabilitation programs. 20

Author Contributions: "Conceptualization, B.K. and T.P.; methodology, B.K. and T.P.; writing—original draft preparation, B,K.; writing—review and editing, G.D. All authors have read and agreed to the published version of the manuscript.

Informed Consent Statement: Informed consent was obtained from all subjects involved in the 25 study. 26

Acknowledgments: Authors would like to acknowledge the financial support from the Mongolian University of Science and Technology.

Conflicts of Interest: The authors declare no conflict of interest.

References

- Ryu, T.; Soon Choi, H.; Choi, H.; Chung, M.K. A comparison of gait characteristics between Korean and Western people for establishing Korean gait reference data. *Int. J. Ind. Ergon.* 2006, *36*, 1023–1030, doi:10.1016/j.ergon.2006.09.013.
- Roaas, A.; Andersson, G.B.J. Normal range of motion of the hip, knee and ankle joints in Male subjects, 30-40 years of age.
 Acta Orthop. 1982, 53, 205–208, doi:10.3109/17453678208992202.
 34
- Boone, D.C.; Azen, S.P. Normal range of motion of joints in male subjects. J. Bone Jt. Surg. Ser. A 1979, 61, 756–759, 35 doi:10.2106/00004623-197961050-00017.
- Shimada, T., Takemasa, S., Kawakami, K., Inoue, Y. and Susuki, K. Normal range of motion of joints in young Japanese 37 people. *Bull. allied Med. Sci.* 1988, 61, 756–759.
 38
- 5. Han, S.; Cheng, G.; Xu, P. Three-dimensional lower extremity kinematics of Chinese during activities of daily living. J. Back 39

8

21

22

23

24

27

28

29

30

7

	Musculoskelet. Rehabil. 2015, 28, 327–334, doi:10.3233/BMR-140523.	1
6.	Favre, J.; Aissaoui, R.; Jolles, B.M.; de Guise, J.A.; Aminian, K. Functional calibration procedure for 3D knee joint angle	2
	description using inertial sensors. J. Biomech. 2009, 42, 2330–2335, doi:10.1016/j.jbiomech.2009.06.025.	3
7.	Kim, K.J.; Agrawal, V.; Bennett, C.; Gaunaurd, I.; Feigenbaum, L.; Gailey, R. Measurement of lower limb segmental excursion	4
	using inertial sensors during single limb stance. J. Biomech. 2018, 71, 151–158, doi:10.1016/j.jbiomech.2018.01.042.	5
8.	Tadano, S.; Takeda, R.; Miyagawa, H. Three dimensional gait analysis using wearable acceleration and gyro sensors based	6
	on quaternion calculations. Sensors (Switzerland) 2013, 13, 9321–9343, doi:10.3390/s130709321.	7
9.	Vargas-Valencia, L.S.; Elias, A.; Rocon, E.; Bastos-Filho, T.; Frizera, A. An IMU-to-body alignment method applied to human	8
	gait analysis. Sensors (Switzerland) 2016, 16, 1–17, doi:10.3390/s16122090.	9
10.	Choi, Y.C.; Khuyagbaatar, B.; Cheon, M.; Batbayar, T.; Lee, S.; Kim, Y.H. Kinematic Comparison of Double Poling Techniques	10
	Between National and College Level Cross-Country Skiers Using Wearable Inertial Measurement Unit Sensors. Int. J. Precis.	11
	Eng. Manuf. 2021 , 22, 1105–1112, doi:10.1007/s12541-021-00511-3.	12
11.	Madgwick S. An efficient orientation filter for inertial and inertial/magnetic sensor arrays.	13
12.	Khuyagbaatar, B.; Purevsuren, T.; Park, W.M.; Kim, K.; Kim, Y.H. Interjoint coordination of the lower extremities in short-	14
	track speed skating. Proc. Inst. Mech. Eng. Part H J. Eng. Med. 2017, 231, doi:10.1177/0954411917719743.	15
13.	Kadaba, M.P, Ramakrishnan, H.K, Wootten, M.E. Measurement of lower extremity kinematics during level walking. J. Orthop.	16
	<i>Res.</i> 1990 , <i>8</i> , 383–392, doi:10.1007/978-1-4471-5451-8_100.	17
14.	Benedetti, M.G.; Catani, F.; Leardini, A.; Pignotti, E.; Giannini, S. Data management in gait analysis for clinical applications.	18
	Clin. Biomech. 1998, 13, 204–215, doi:10.1016/S0268-0033(97)00041-7.	19
		20