

Improving brain targeting efficiency by noseto-brain delivery of lipidic and polymeric nanoparticles: a focus on depression and anxiety treatments

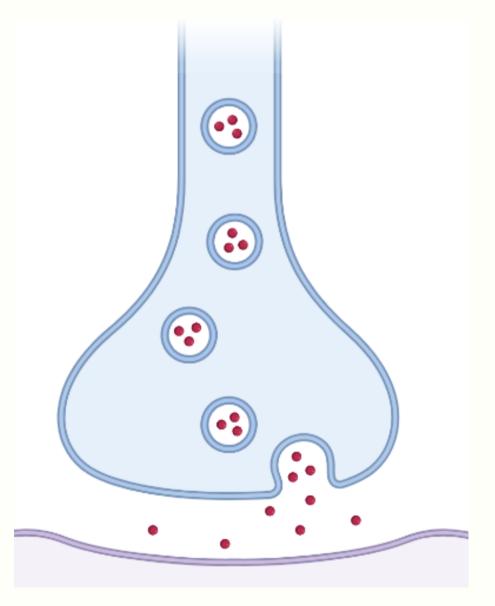
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INTRODUCTION: DEPRESSION AND ANXIETY

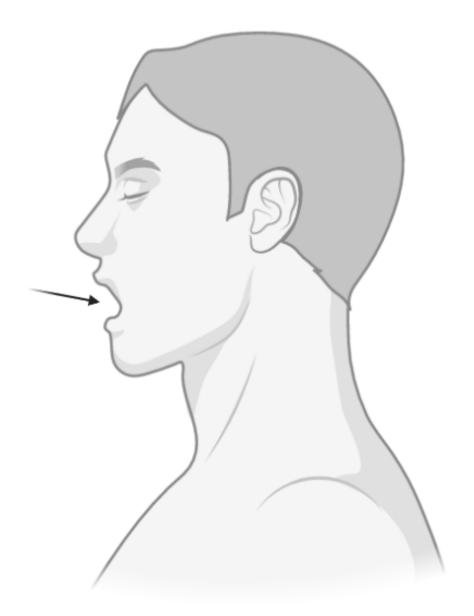
The most accepted theory for the pathogenesis of depression is based on a monoaminergic transmission disorder due to the complex interaction of several social, psychological and biological factors. Most drugs used in the treatment of depression increase the availability of these neurotransmitters in the synaptic cleft.

Anxiety is associated with the inhibition of the synaptic transmission of y-aminobutyric acid (GABA). Pharmacological treatment of anxiety includes anxiolytic drugs such as benzodiazepines.



TREATMENT: DEPRESSION AND ANXIETY

Root of administration used for the treatment



Disadvantages of oral administration of drugs:

- Exposition of the drug to the first pass hepatic metabolism;
- Regular administrations needed to ensure the constant presence of the drug at the site of action;
- The amount of drug that reaches the site of action is restricted by the action of the blood brain barrier and bloodcerebrospinal fluid that act as a barrier,
- Fluctuations in plasma concentrations lead to side effects and loss of efficacy

INTRANASAL ADMINISTRATION: A possible alternative for the treatment of depression and anxiety

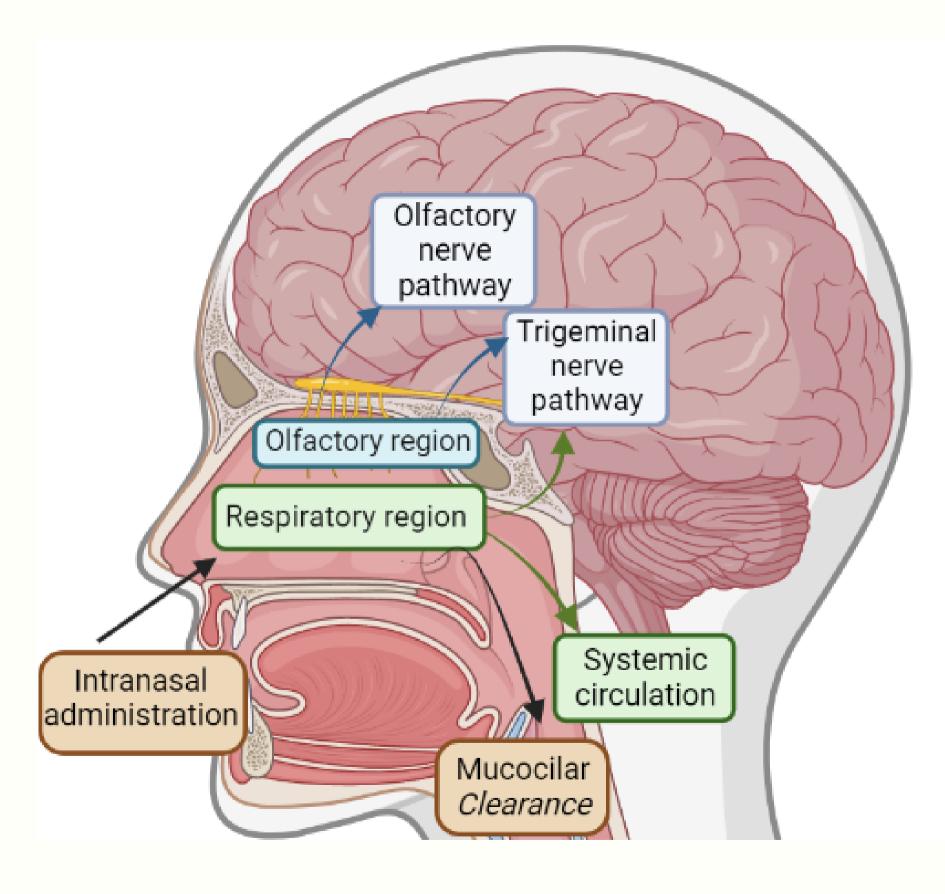
Advantages:

- Overcome the blood brain barrier,
- Avoid the first pass hepatic metabolism;
- Minimize the side effects caused by drugs administered though the systemic circulation;
- Reduce the dosage necessary to achieve the therapeutic effect;
- Direct the active molecule to the site of action;
- Direct contact with the CNS.

INTRANASAL ADMINISTRATION: A possible alternative for the treatment of depression and anxiety

Disadvantages:

- Physical removal of the drug from the nasal cavity by mucociliary clearance mechanisms;
- Enzymatic degradation in the mucus and nasal epithelium layer;
- Volume of formulation that can be administered that is limited to 25 -200μ l, which turns this route of administration more appropriate for potent drugs.



NASAL CAVITY ANATOMY AND TRANSPORT

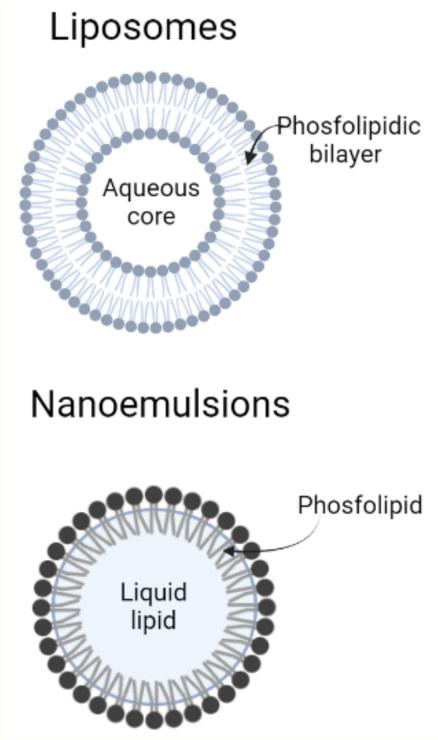
There is a direct connection between the nasal cavity and the CNS, which allows the transport of several substances to the brain, being the only place in the human body where the nervous system is in direct contact with the surrounding environment.

NANOMETRIC DRUG TRANSPORT SYSTEMS

Nanometric drug transport systems are formulations that help transporting the drug to the place of action, allowing to modulate the time and quantity of drug released.

Main types of nanometric systems:

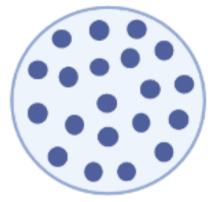
- Liposomes,
- Nanoemulsions,
- Polymeric nanoparticles (nanocapsules and nanospheres)
- Lipidic nanoparticles (solid lipid nanoparticles (SLN) and nanostructured lipid transporters (NLC)).



Polymeric Nanoparticles

Nanocapsules

Nanospheres



NLC

Lipidic Nanoparticles

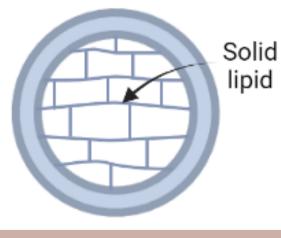
Liquid

lipid and

Solid

lipid

SLN



PURPOSE OF THE WORK

This work approaches, in summary, studies already developed with the goal of formulating nanoparticles for intranasal administration of drugs for the treatment of these pathologies.

METHODS

On 10 of August of 2022, a pubmed database review with the keywords "nanoparticle AND (depression OR anxiety) AND (intranasal OR nasal)" revealed 28 results. Applying exclusion criteria 12 articles of fundamental research were included in this work.

IN VIVO PHARMACOKINETIC STUDIES

Different parameters were calculated:

 $Entrapment \ efficiency \ (EE\%) = \frac{(Total \ drug - free \ drug)}{Total \ drug} \times 100$

 $Drug \ loading \ (DL\%) = \frac{(Total \ drug - free \ drug)}{Total \ weight \ of \ nanoparticles} \times 100$

Drug targeting efficiency

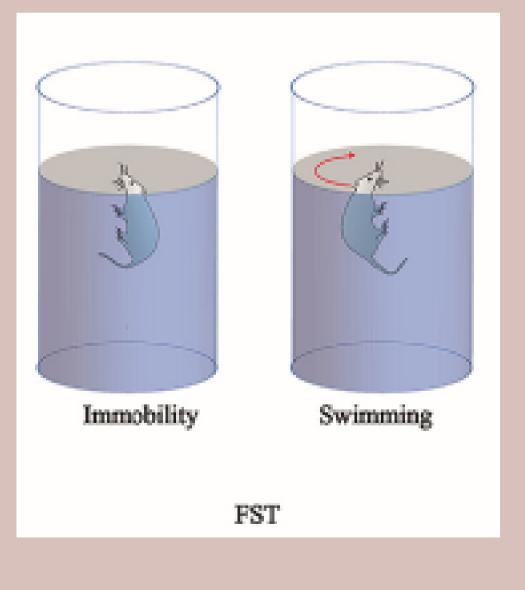
Direct transport percentag

 D_{iv} is the AUC_{0-72h} (brain) intravenous route. Piv is the AUC_{0-72h} (blood) intravenous route. D_{in}, is the AUC_{0-72h} (brain) intranasal route. Pip. is the AUC_{0-72h} (blood) intranasal route

$$(DTE\%) = \frac{\left(\frac{AUCbrain}{AUCblood}\right)i.n}{\left(\frac{AUCbrain}{AuCblood}\right)i.v} \times 100$$

$$(e (DTP\%) = \frac{Di.n - ((Di.v./Pi.v.) \times Pi.n.)}{Di.n.} \times 100$$

IN VIVO PHARMACODYNAMIC STUDIES

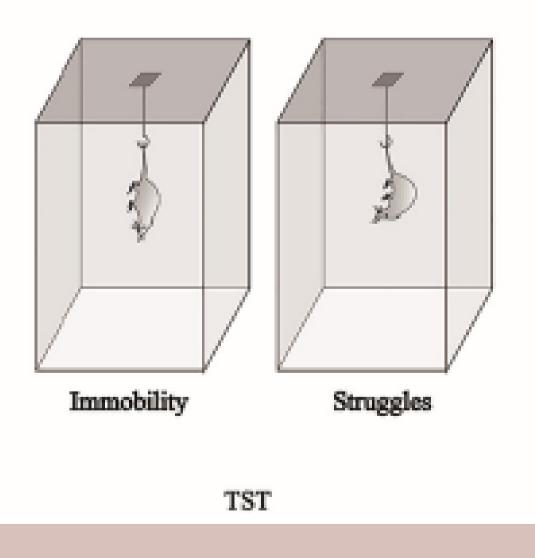


1) Forced Swim Test (FST) Analyses the response of the animal model to the treat of drowning. It measures:

- Immobility time
- Climbing time
- Swimming time
- Locomotor activity

The results allow to assess the efficacy of the antidepressive drug.

IN VIVO PHARMACODYNAMIC STUDIES



2) Tail suspension test (TST)

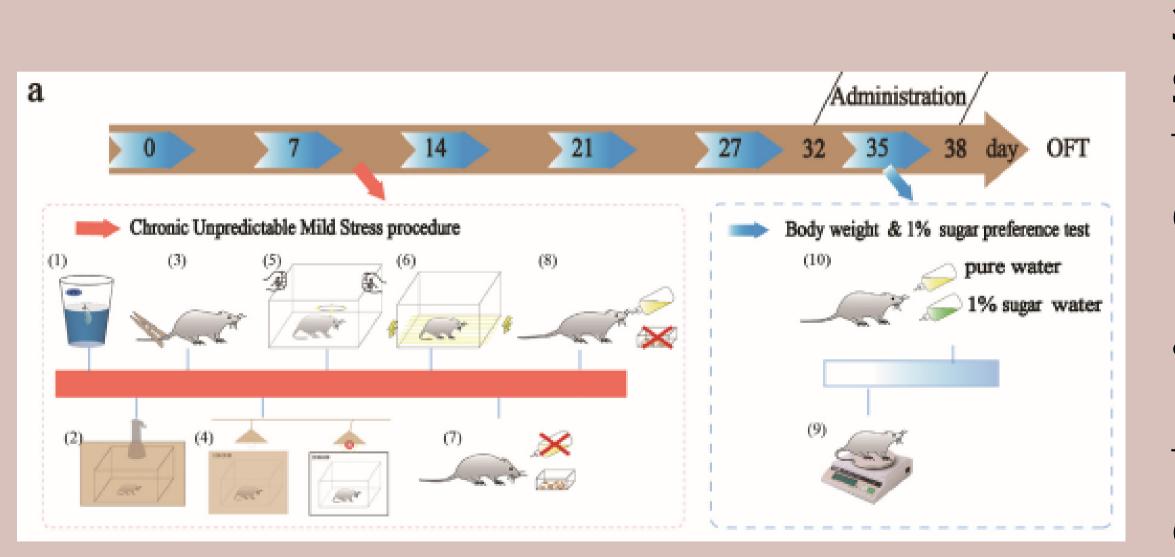
Analyses the response of the animal model when they are suspended and can not escape. It measures:

- Immobility time
- Locomotor activity

drug.

The results allow to assess the efficacy of the antidepressive

IN VIVO PHARMACODYNAMIC STUDIES



3) Chronic Unpredictable Mild Stress model (CUMS model)

- This model submits the animal to different stressful situations, leading to the loss of body weight and reducing the sugar preference of the animal.
- The results allow to assess the efficacy of the antidepressive drug.

RESULTS AND DISCUSSION

The analysis of the studies revealed that several drugs have been researched in order to verify the efficacy of intranasal administration of nanoparticles for the treatment of depression and anxiety.

The results of the analyzed articles are described in summary form and for each drug, the most relevant results will be presented.

ICARIIN AND ALBIFLORIN

Icariin:

Particle size: 73,80 nm PDI: 0,15 Zeta potencial: -19,2mV

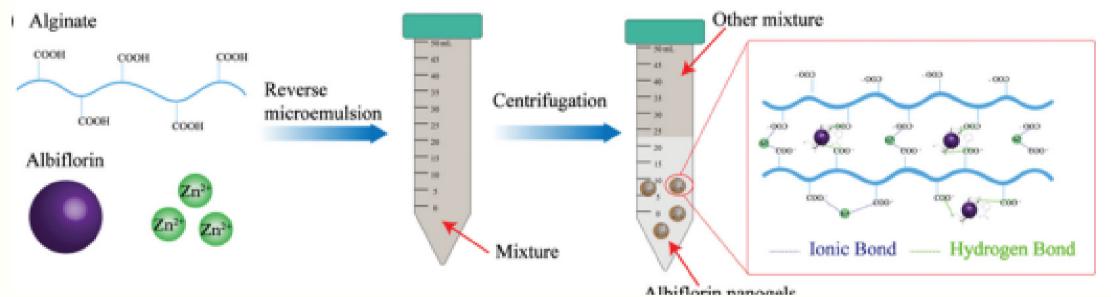
Albiflorin:

Particle size: 45,6 nm PDI: 0,20 Zeta potencial: -19,8 mV

Composition of the nanoparticules:

Alginate-Polymer Poloxamer-Surfactant





In both studies the FST, TST and CUMS model were applied. For all the tests performed, the nanoparticules developed, when administrated via intranasal, obtained better results.

FLUOXETINE

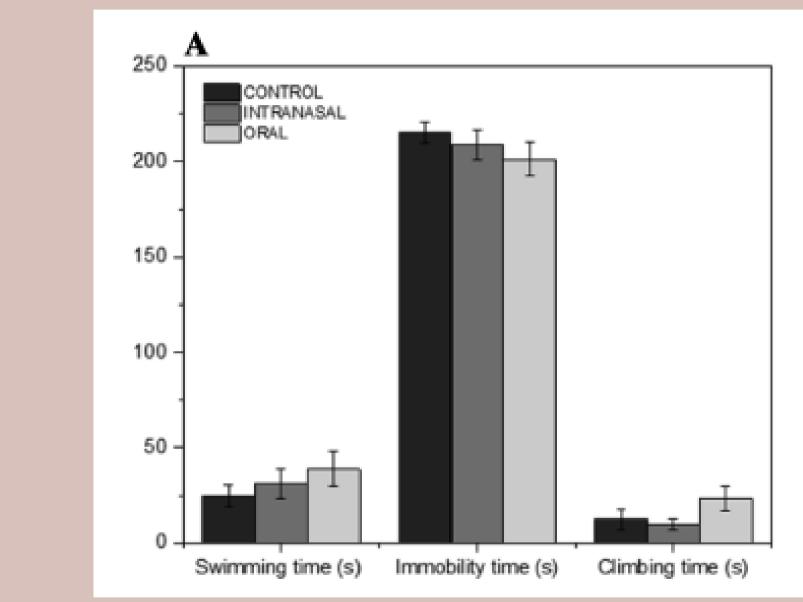
Composition of the nanoparticles:

Glyceryl palmitostearate- Solid lipid Propylene glycol monocaprylate (type I)- Liquid lipid Polysorbate 80- Surfactant

RESULTS

Particle size: 154 nm PDI: 0,514 Zeta potencial: 19,7 mV EE%: 74% DI%: 12,9%

FST applied to mice when treated with an **oral** solution vs **intranasal** nanoparticles:



Although there is no comparative superiority, the formulation can be used when the oral route is not available (vomits, intubation, convulsions...).

AGOMELATINE

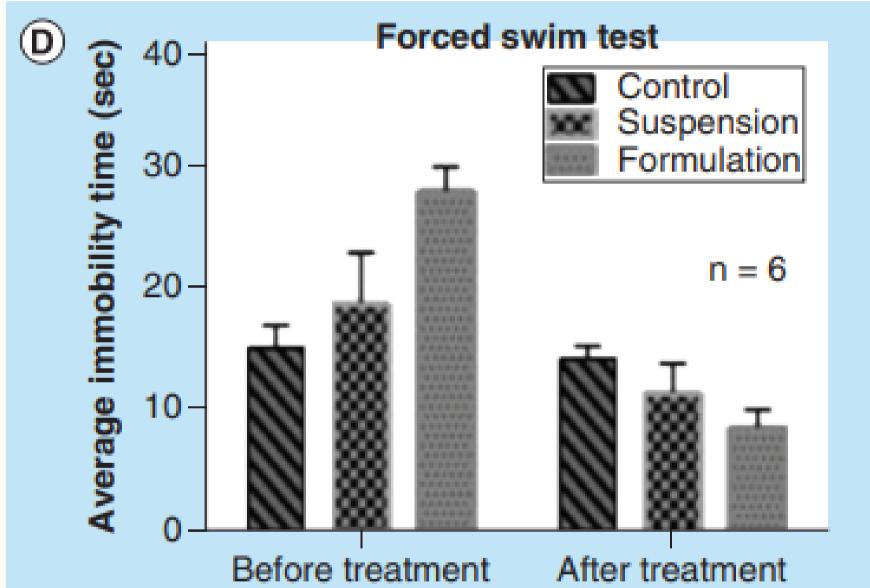
Composition of the nanoparticles:

PLGA (poly-lactic-coglycolic acid)- Polymer Poloxamer 407- Surfactant

RESULTS

Particle size: 116,06 nm, PDI: <0,3 Zeta potencial: -22,7 mV. EE%: 98,3% DL% 49,15%

FST applied to rats when treated with an **oral** suspension vs **intranasal** nanoparticles:



DESVENLAFAXINE

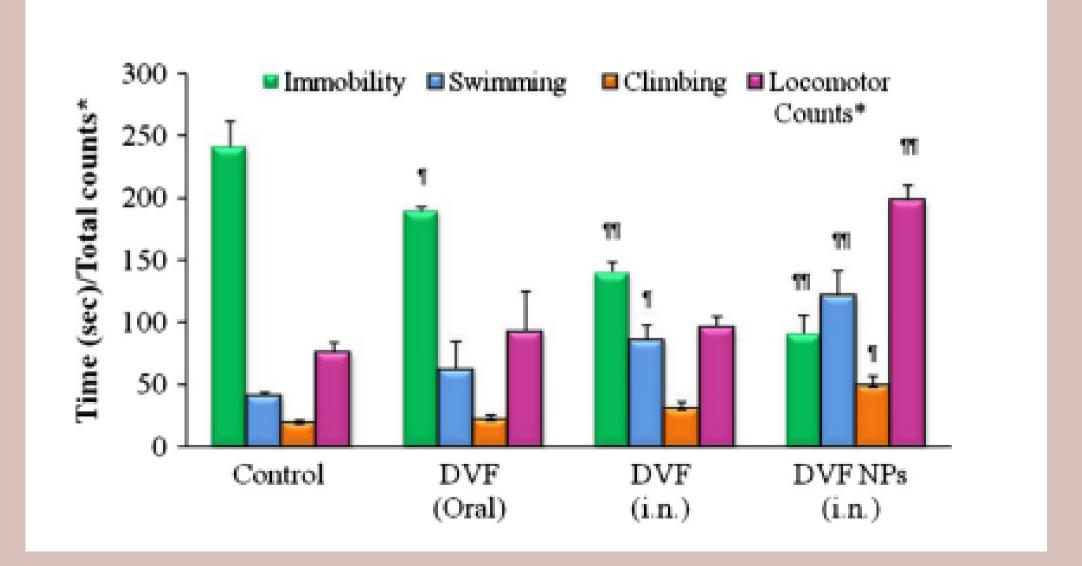
FST applied to rats when treated with an **oral** solution vs **intranasal** solution vs **intranasal** nanoparticles:

Composition of the nanoparticles:

PLGA- Polymer Chitosan- Polymer Polyvinyl alcohol- Surfactant

RESULTS

Particle size 172,5 nm PDI: 0,254 Zeta potencial: +35,63 mV EE%: 98,3% DL%: 49,15% DTE%: 554,23% DTP%: 81,62%



VENLAFAXINE 3 studies developed formulations with venlafaxine:

1	CHITOSAN TPP	PDI: 0,30	67	e: 167 nm tial : +23,83 mV	EE%: 79,3% DL%: 32,25% DTE%: 508,59% DTP%: 80,34%	<i>In vivo</i> p AUC, co formula • Nan			
2	ALGINATE CHITOSAN	Particle size: 173,7 nm PDI: 0,391 Zeta potential: +37,4 m			EE%: 85,6% DL%: 26,74% DTE%: 425,77% DTP%: 76,52%	 Solu Solu The bes adminis 			
	PLGA			PLGA + TF*/ PLGA + TFRP**		The ligands w and improve permeability f			
3	Particle size: 206,3 nm PDI: 0,190 Zeta potential: -26,5 mV EE%: 48 - 50% DL%: 10 - 12%			Particle size: 218,6/ 216,3 nm PDI: 0,078 / 0,067 Zeta potential: -19,5/ -19,6 mV EE%: 48 - 50% DL%: 10 - 12%		30 minutes higher conce nanoparticles take longer to			
	*transferin receptor								

*transferin receptor** specific peptide against Tf receptor

- pharmacokinetics studies compared results of oncentration and semi-life time of three different lations:
- noparticles (i.n.)
- lution (i.v.)
- lution (i.n.)
- est results were obtained after intranasal
- istration of the nanoparticles.

were used in order to modify the surface of the nanoparticles e their interaction with mucosal cells, favoring absorption and / through the mucosa.

after intranasal administration of the 3 formulations, the centration of drug in the brain was obtained with simple es, which allowed to conclude that functional nanoparticles to reach the brain.

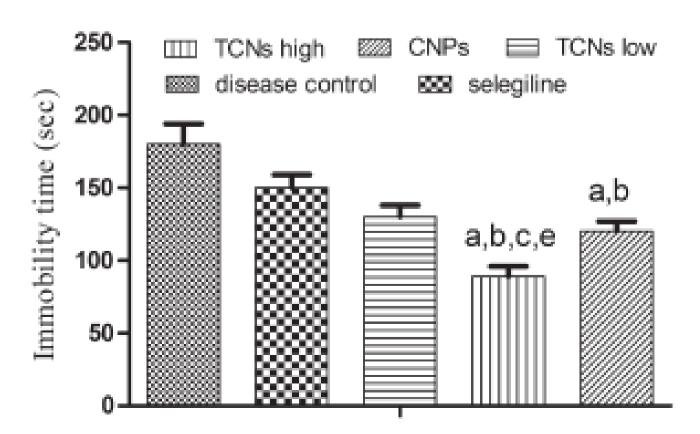
SELEGILINE

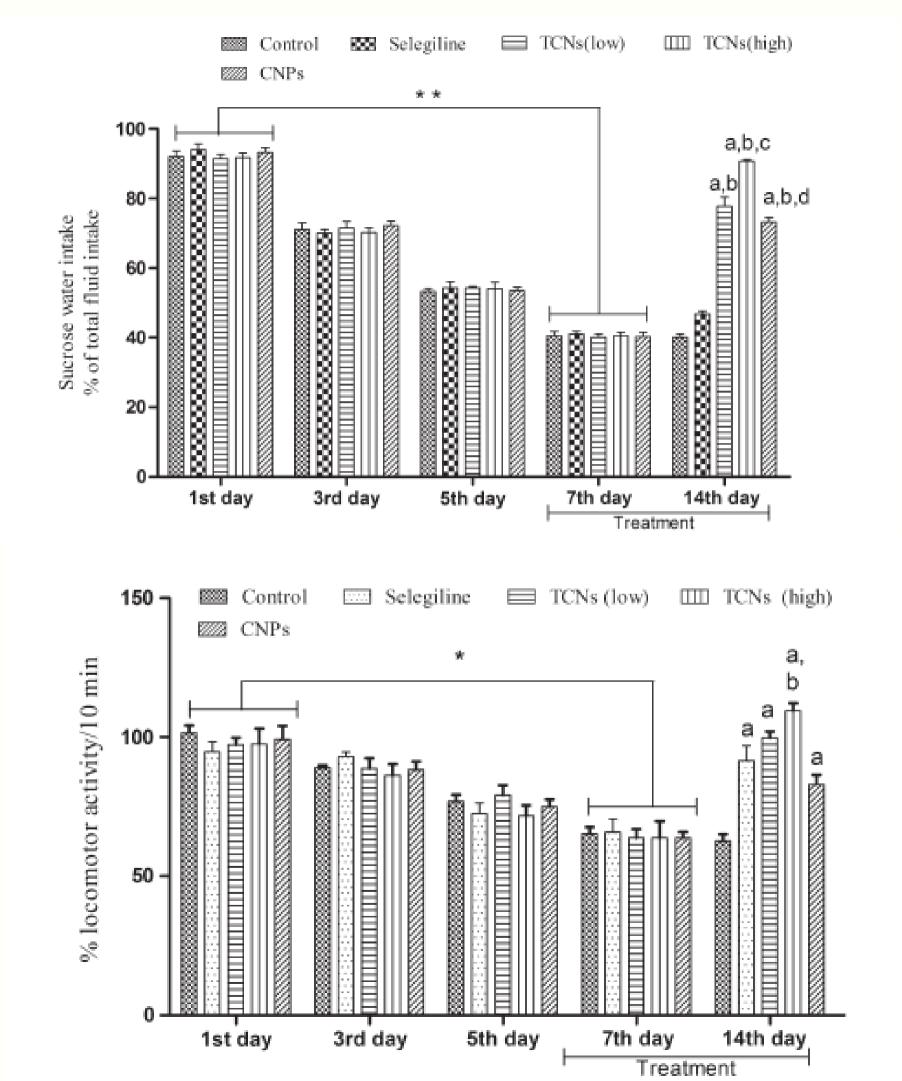
Composition of the nanoparticles:

Chitosan or tiolated chitosan- Polycation Tripolyphosphate (TPP)- Polyanion

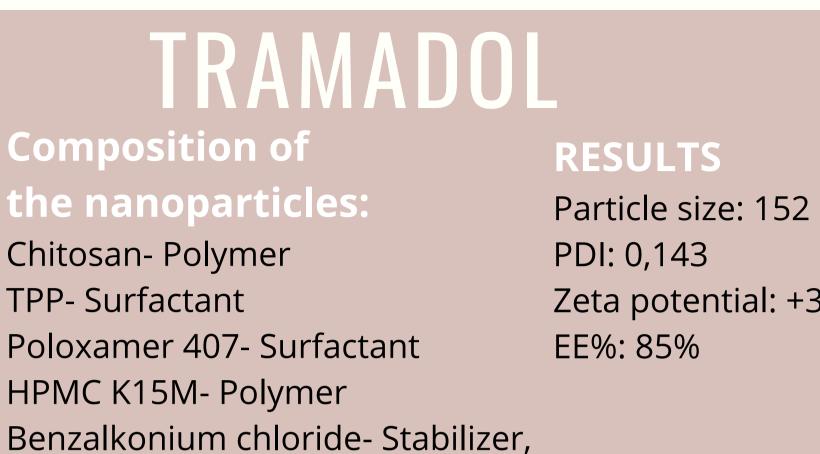
RESULTS (for thiolated chitosan nanoparticles)

Particle size: 215 nm PDI: 0,214 Zeta potential: +17,06 mV EE%: 70%





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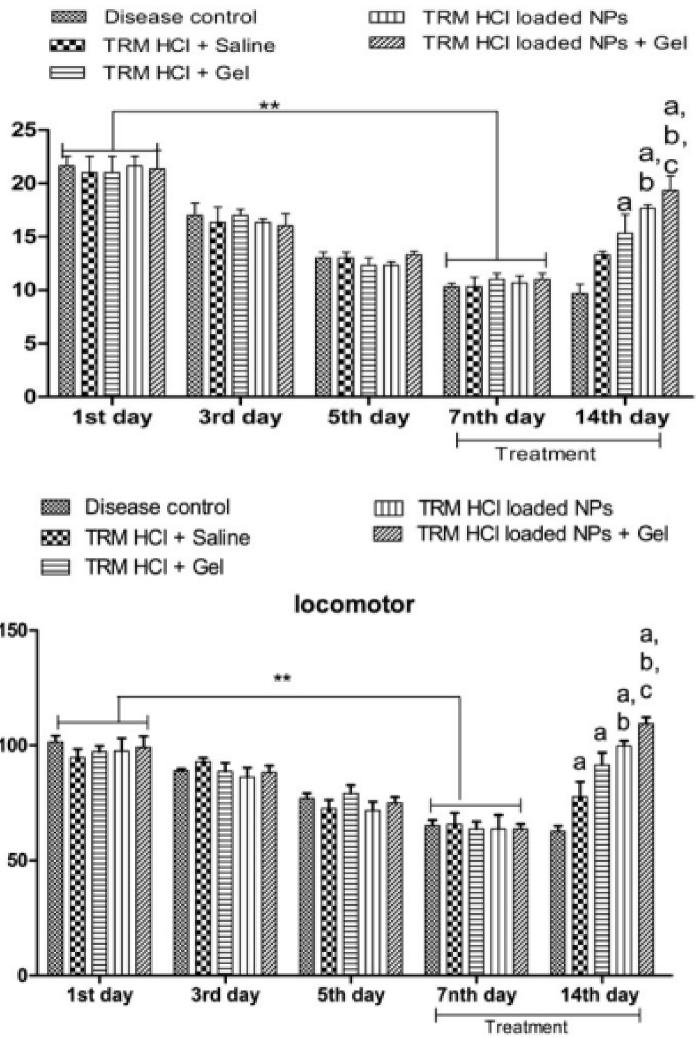
TRM HCI loaded NPs

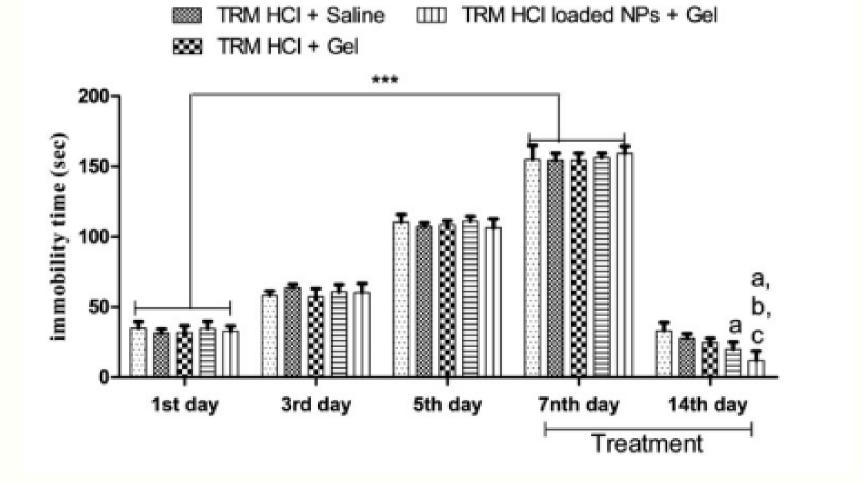


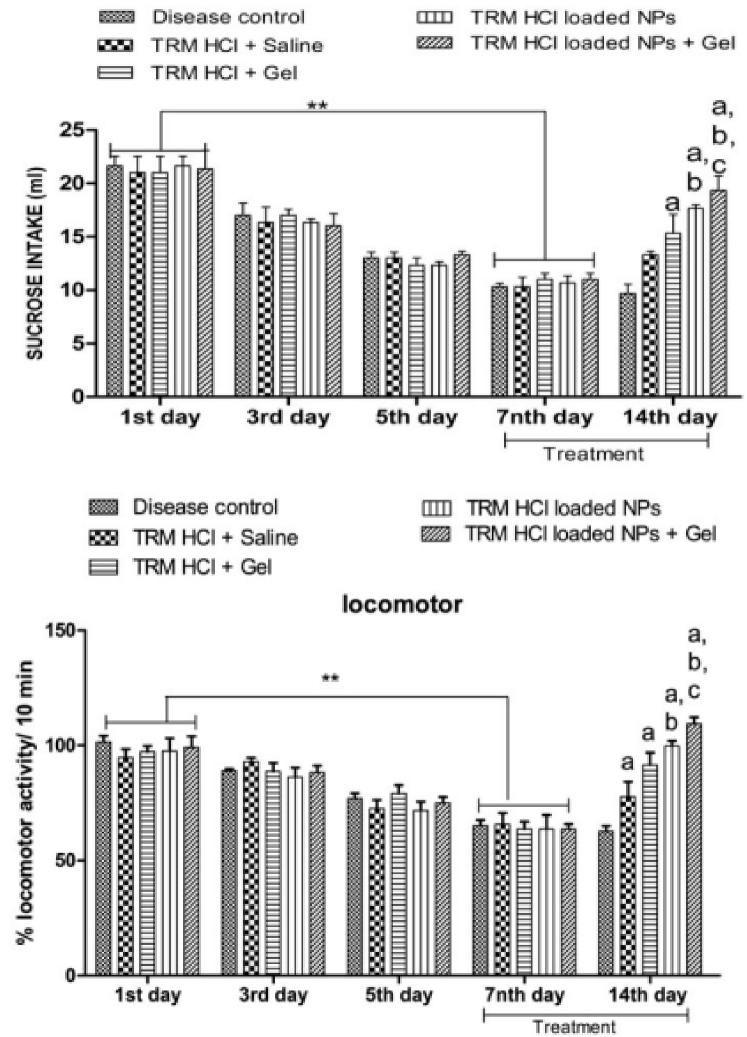
.....

Disease control

Particle size: 152 nm Zeta potential: +31 mV







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BUSPIRONE

Composition of the nanoparticles:

Chitosan-Polymer Cross-linker (alginate + TPP)

Results

Particle size: 195,7 nm PDI: 0,367

Composition of the nanoparticles:

Results

Particle size: 208,3 nm PDI: 0,253 DTE%: 95,97% DTP%: 78,94%

In vivo pharmacokinetics studies results:

BUH(i.v.)Brain 384.15 ± 13.42 2 1151.01 ± 54.78 1253.01 ± 10.32 BUH (i.n.)Brain 417.77 ± 19.24 2 2036.9 ± 51.62 3941.26 ± 26.99	Formulation	Organ/tissue	C _{max} (ng/ml)	T _{max} (h)	AUC _{0-480 min} (ng min/ml)	$AUC_{0-\alpha \min}$ (ng min/ml)
	BUH(i.v.)	Brain	384.15 ± 13.42	2	1151.01 ± 54.78	1253.01 ± 10.32
	BUH (i.n.)	Brain	417.77 ± 19.24	2	2036.9 ± 51.62	3941.26 ± 26.99
BUH TCS-NPs (i.n.) Brain 797.46 \pm 35.76 2 4048.29 \pm 28.35 6057.21 \pm 52.3	BUH TCS-NPs (i.n.)	Brain	797.46 ± 35.76	2	4048.29 ± 28.35	6057.21 ± 52.3

BUH - Buspirone BUH TCS-NPs- Thiolated chitosan nanoparticles

- Thiolated chitosan- Polymer Cross-linker (alginate + TPP)

RILUZOL

Composition of the nanoparticles:

Chitosan- Polycation TPP- Polianion

Results

Particle size: 173,6 nm PDI: 0,264

Composition of the nanoparticles:

Chitosan- Polycation TPP- Polyanion Tf-ligand

Results

Particle size: 207,0 nm PDI: 0,406 DTE%: 1138,46% DTP%: 91,21%

In vivo pharmacodynamics Elevated plus maze test: • Confirmed the anxiolytic potential of riluzol



In vivo pharmacokinetics studies results:

- Suspension (i.v.)
- Suspension (i.n.)
- Chitosan Tf nanoparticles (i.n.)

Best results obtained after intranasal administration of nanoparticles with Tf.

CONCLUSIONS

Pharmacokinetics and pharmacodynamic results are very promising

- Polymeric nanoparticles were the preferred nanometric drug transport systems
 - Chitosan and alginate were the polymers most used due to their mucoadhesive properties

CONCLUSIONS

In the future it is important to compare these results with studies performed in humans in order to confirm the true potential of the intranasal administration of nanoparticles for the treatment of depression and anxiety

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