

Proceeding Paper

Simple Chromatographic Sensor with UV LED Optical Detection for Monitoring Patients Treated with Continuous Ambulatory Peritoneal Dialysis[†]

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Abstract: A novel simple optical sensor based on fast protein liquid chromatography was developed and tested for monitoring end stage renal disease (ESRD) patients treated with continuous ambulatory peritoneal dialysis (CAPD). The device provides direct determination of proteins and lower molecular weight metabolites in effluent peritoneal dialysate using ultraviolet (UV) photometric detection at the wavelengths 285 nm or 260 nm with deep ultraviolet light-emitting diodes. The sensor was calibrated with bovine serum albumin and nucleotides standard solutions. Chromatograms of peritoneal dialysate samples taken from a group of 28 ESRD patients were processed and approximated by a set of split-Gaussian functions. All chromatograms show three overlapping peaks: the first one represents proteins; the other two peaks probably correspond to mid- and low molecular weight metabolites. Strong correlation was revealed between the area of the first peak and total protein concentration determined by a standard biochemical assay, this makes possible estimation of peritoneal protein loss with a reasonable precision less than 15%. The area of the second peak correlated with dialysate optical density at a wavelength 355–365 nm, associated with the UV absorption of advanced glycation end (AGE) products. The third peak correlated with the optical density of the eluate at a wavelength 255–265 nm, associated with the UV absorption of purines and pyrimidines. Thus, we demonstrated the possibility of estimation of proteins and lower molecular weight metabolites in effluent peritoneal dialysate with the compact and affordable chromatographic optical sensor.

Keywords: optical chemical sensor; fast-protein liquid chromatography; UV LED; peritoneal dialysis; end stage renal disease; peritoneal protein loss.

1. Introduction

Chronic kidney disease (CKD) is a long-term and often slow-developing disease accompanied by a gradual deterioration of kidney function, which in some patients can progress to end-stage renal failure. CKD is one of the main causes of mortality among all non-communicable diseases in developed countries with relatively high life expectancy [1]. In the absence of renal replacement therapy (RRT), uremic intoxication occurs, which eventually leads to a fatal outcome. The methods of treatment include kidney transplantation, hemodialysis (HD), and peritoneal dialysis (PD). Currently about 10% of all patients, which require RRT, receive treatment with continuous ambulatory peritoneal dialysis (CAPD) at home for the following reasons: intolerance to HD, limited mobility, remoteness of the place of residence from the nearest dialysis center, hospital policy, or personal preferences [2,3].

CAPD is a method of RRT that does not require highly qualified medical staff and expensive equipment, so it can be performed at home by patients themselves or his/her caregivers. As any RRT modality PD has serious complications and side-effects, e.g., high peritoneal protein loss [4–7] and high risk of infection (dialysis peritonitis) [8,9]. Necessary measures to prevent or at least provide early treatment of these complications imply constant monitoring of CAPD outpatients, including assessment of peritoneal protein loss and other parameters of effluent dialysate. Conventional clinical laboratory methods are generally intended for analysis of blood and urine, not optimized for peroneal dialysate, and not suitable for at home testing [10]. As a possible alternative a novel simple optical sensor based on fast protein liquid chromatography with ultraviolet (UV) photometric detection was developed and tested for monitoring end stage renal disease patients treated with CAPD.

2. Materials and Methods

The sensor uses affordable PD-10 desalting columns (Code No. 17-0851-01) from GE Healthcare® Bio-Sciences AB (Uppsala, Sweden) with Sephadex G-25 Medium chromatographic gel to separate proteins from mid- and low molecular weight metabolites in effluent peritoneal dialysate according to the principles of fast protein liquid chromatography (FPLC) [11,12]. The instrument employs photometric detection at the wavelengths 285 nm (optimized for proteins) or 260 nm (optimized for nucleotides, nucleosides, purines and pyrimidines related substances) with deep UV light-emitting diodes (LED) as solid-state light source and a visible-blind UV photodiode as a photodetector. Chromatograms are recorded by direct measurement of the UV absorption of the eluate flowing from the PD-10 column passing through the quartz cuvette (Figure 1). More detailed description of the sensor was reported earlier [13–15].

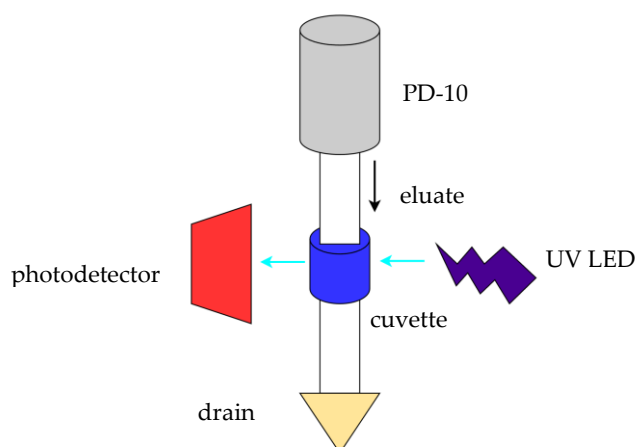


Figure 1. Schematic diagram of the sensor.

The instrument can be defined as a chemical sensor employing chromatographic separation and optical detection, which is capable of quantitative determination of biological molecules, i.e., proteins, nucleic acids, middle- and low molecular weight metabolic products. Such devices do not formally belong to the class of biosensors due to the fact that they do not incorporate a biointerface and cannot provide as high selectivity as real biosensors. Nevertheless, similar systems are often considered in the context of biosensors because they perform the same functions and can successively substitute or supplement biosensors in biomedical, environmental, or industrial applications.

The measurement procedure is as follows: after column regeneration with a small amount (25 ml) of TRIS buffer, a sample of effluent peritoneal dialysate is introduced into the column, held for 20-40 seconds (so that the dialysate is absorbed into the gel), another 25 ml of buffer is added. Over the next 10-15 minutes, the optical signal $I(t)$ is recorded by the photodetector at the wavelengths of 260 and 285 nm. In accordance with the Beer-Bouguer-Lambert law, optical absorption $a(t)$ is calculated as follows:

$$a(t) = \log \left(\frac{I_{max}}{I(t)} \right), \quad (1)$$

where I_{max} – reference signal, which is proportional to the intensity of UV light transmitted by the cuvette with the pure buffer recorded at the beginning of chromatogram processing.

The residual samples of effluent peritoneal dialysate taken from 28 CAPD patients during regular hospital visits were provided by the Mariinsky City Hospital (Saint Petersburg, Russia). The study was coordinated and approved by the Institute of Experimental Medicine (Saint Petersburg, Russia); the permission from the Institute Ethics Committee confirming that it meets ethical standards was obtained, and patients' personal information was not disclosed by the hospital. Total protein concentration in the samples was determined by the calorimetric photometric method using the Abbott Architect c8000 biochemical analyzer.

All PD chromatograms show three overlapping peaks: the first corresponds to proteins; the other two peaks probably correspond to medium and low molecular weight metabolites. Absorption $a(t)$ could be approximated by a series of split Gaussian functions:

$$a(t) = \sum_{n=1}^N f(t, t_{max_n}, A_n, \sigma_{left_n}, \sigma_{right_n}),$$

$$f(t, t_{max_n}, A_n, \sigma_{left_n}, \sigma_{right_n}) = \begin{cases} A_n \exp \left(-\frac{(t - t_{max_n})^2}{2(\sigma_{left_n})^2} \right), & t < t_{max_n} \\ A_n \exp \left(-\frac{(t - t_{max_n})^2}{2(\sigma_{right_n})^2} \right), & t \geq t_{max_n} \end{cases} \quad (2)$$

where A_n – the amplitude of the n^{th} peak, t_{max_n} – the elution time for the n^{th} peak, σ_{left_n} – the width of the left half of the n^{th} peak, σ_{right_n} – width of the right half of the n^{th} peak, N – number of peaks.

The coefficients $t_{max_n}, A_n, \sigma_{left_n}, \sigma_{right_n}$ are estimated using iterative least squares regression by built-in MATLAB `nlinfit()` function.

It was proven empirically that the area of right half-peak S_r found from the corresponding Bi-Gaussian function gives the most accurate information about protein concentration:

$$S_r = \int_{t_{max_n}}^{\infty} A_n \exp \left(-\frac{(t - t_{max_n})^2}{2(\sigma_{right_n})^2} \right) dt \quad (3)$$

Dialysate samples were also analyzed using AvaSpec-2048 fiberoptic UV spectrophotometer with a deuterium lamp as a UV source. UV spectra were recorded in the 200-400 nm spectral range with the spectral resolution about 1 nm.

3. Results

3.1. Sensor Calibration with BSA Solutions

The first stage of the study was to perform the sensor calibration using bovine serum albumin (BSA) aqueous solutions to determine the optimal sample volume and the working range of protein concentrations. Total protein concentration in effluent peritoneal dialysate varies from 0.5 g/l to 4.5 g/l according to [7], and the sensor has to provide reliable data in this range.

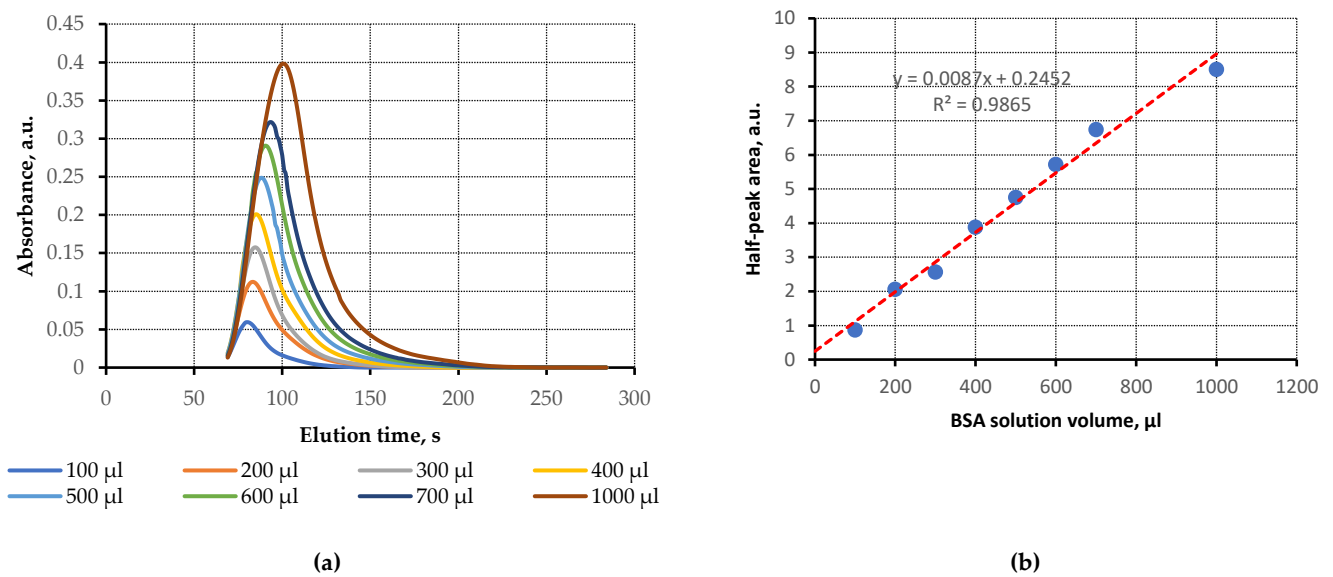


Figure 2. Calibration of the FPLC sensor with 2 g/l BSA solution with different sample volumes: (a) The chromatograms; (b) Dependence of the protein half-peak area on the sample volume.

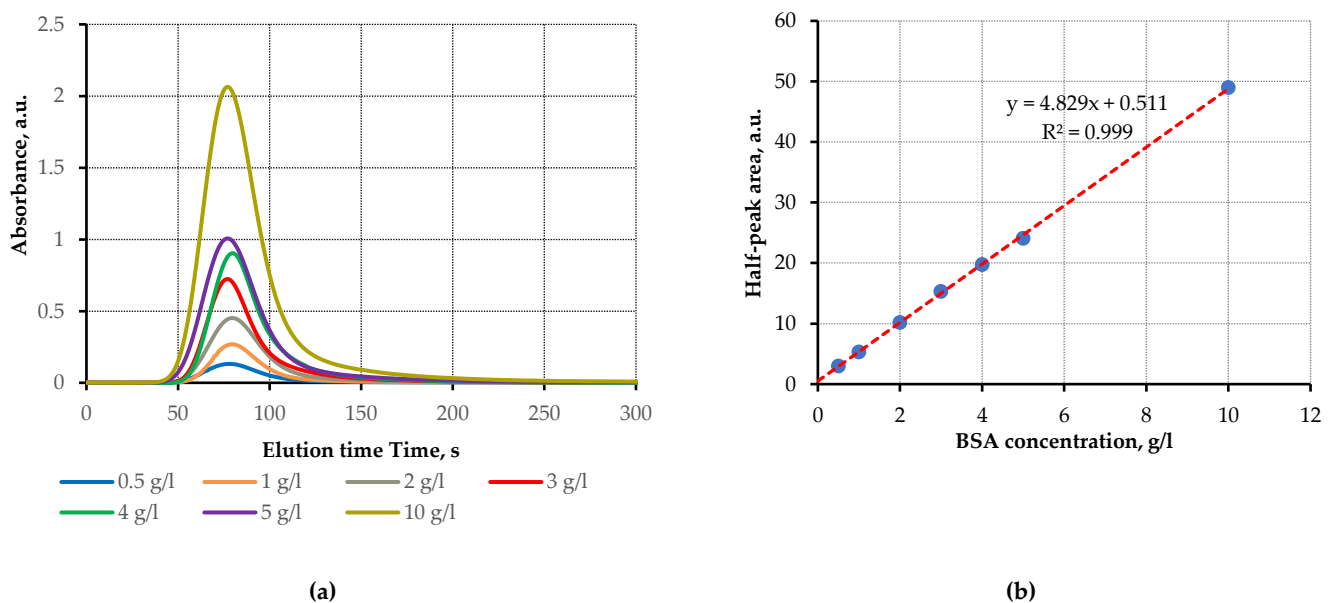


Figure 3. Calibration of the FPLC sensor with BSA solution with various concentrations: (a) The chromatograms; (b) Dependence of the protein half-peak area on the concentration.

The calibrating solutions with the concentrations 0.5, 1, 2, 3, 4, 5, 10 g/l were prepared from 99% pure BSA powder (Lot No. 60154016) purchased from DIA-M (Moscow, Russia). Initially, the chromatograms of the 2 g/l BSA solution with various sample volumes in the range of 100–1000 μ l were processed using the FPLS sensor; the elution time of BSA was approximately 50–100 s and slightly increasing with the concentration (Figure 2a).

The dependence of the area of the protein right half-peak in the chromatograms on the sample volume was almost linear in the whole range with Pearson's correlation coefficient $R^2=0.985$ (Figure 2b); only slight non-linearity started to emerge for the volumes more than 800 μ l.

For further experiments we chose an optimal sample volume of 500 μ l in such a way that the optical transmittance of the analyte in the sensor cuvette falls in the range 20–40% providing minimal instrumental errors. The chromatograms of the BSA solution (sample volume 500 μ l) with the various concentrations were processed afterwards (Figure 3a); the dependence of the area of the right protein half-peak on the BSA concentration was also linear in the whole range of 0.5–10 g/l with the Pearson correlation coefficient $R^2=0.999$ (Figure 3b).

3.2. Sensor Calibration with Nucleotides Solutions

The chromatograms of adenosine triphosphate (ATP), inosine monophosphate (IMP), inosine (Ino), and hypoxanthine (Hx) aqueous solutions were processed, the solutions were prepared from chemicals purchased from Sigma Aldrich (Darmstadt, Germany); the elution times for these nucleotides were obtained relative to the BSA peak. Experimental data are presented in Table 1 and Figure 4. As can be seen from the table and Figure 4b, the elution time is inversely proportional to the molecular weight.

Table 1. Elution times for nucleotides.

Substance	Molecular Weight, Da	Elution Time, s
ATP	507	94
IMP	348	124
Ino	268	202
Hx	136	267

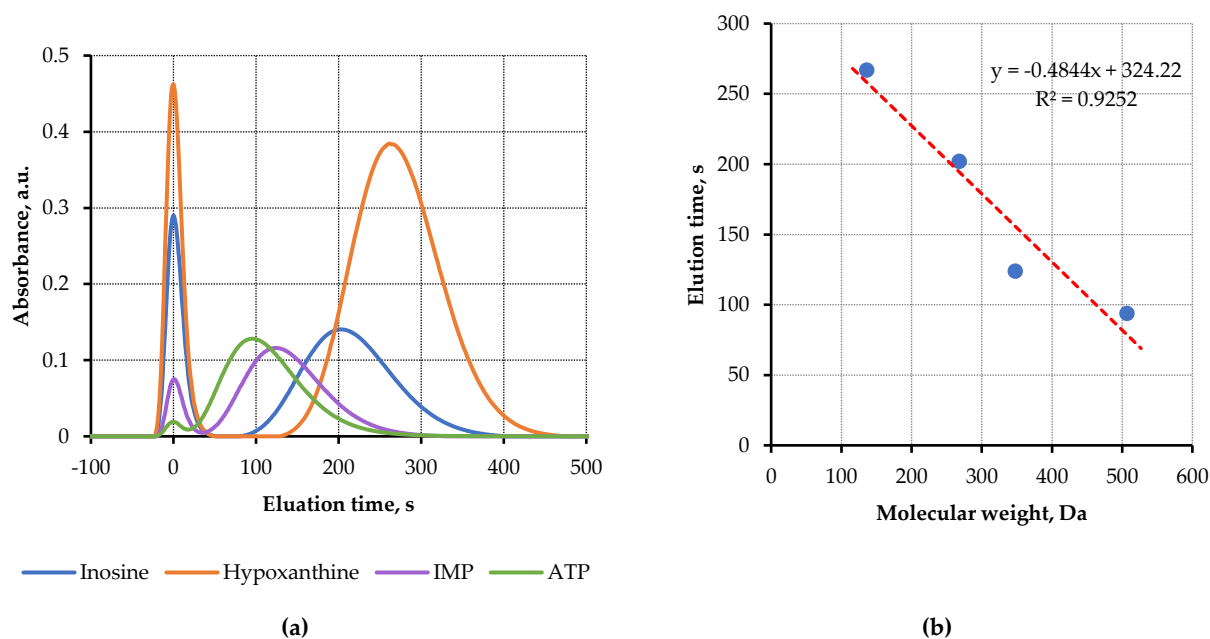


Figure 4. Calibration of the FPLC sensor with nucleotides solutions: (a) The chromatograms of the nucleotides with BSA peak as a time reference; (b) Dependence of the elution time on the molecular weight.

3.3. Chromatograms and UV Absorption Spectra of Effluent Peritoneal Dialysate

Chromatograms of effluent peritoneal dialysate taken from 28 patients with end-stage renal disease were processed. The UV absorption spectra of the samples were recorded in parallel; an example of a chromatogram is shown in the Figure 5a.

A strong correlation ($R^2 = 0.963$) was revealed between the area of the first half-peak and the concentration of total protein determined by the standard biochemical method (Figure 5b), which makes it possible to estimate the loss of peritoneal protein with an acceptable accuracy of less than 15%; more detailed data was reported earlier [6].

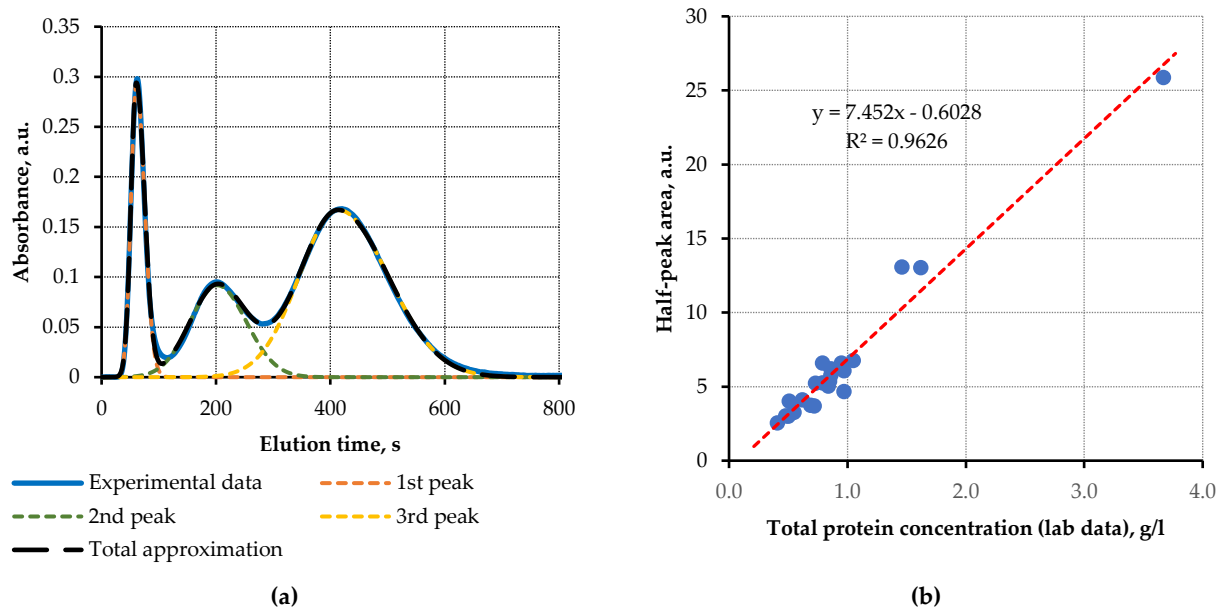


Figure 5. (a) An example of a effluent peritoneal dialysate chromatogram approximated with a set of split Gaussian fitting curves; (b) Dependence of right half-peak area on total protein concentration determined by a standard biochemical assay.

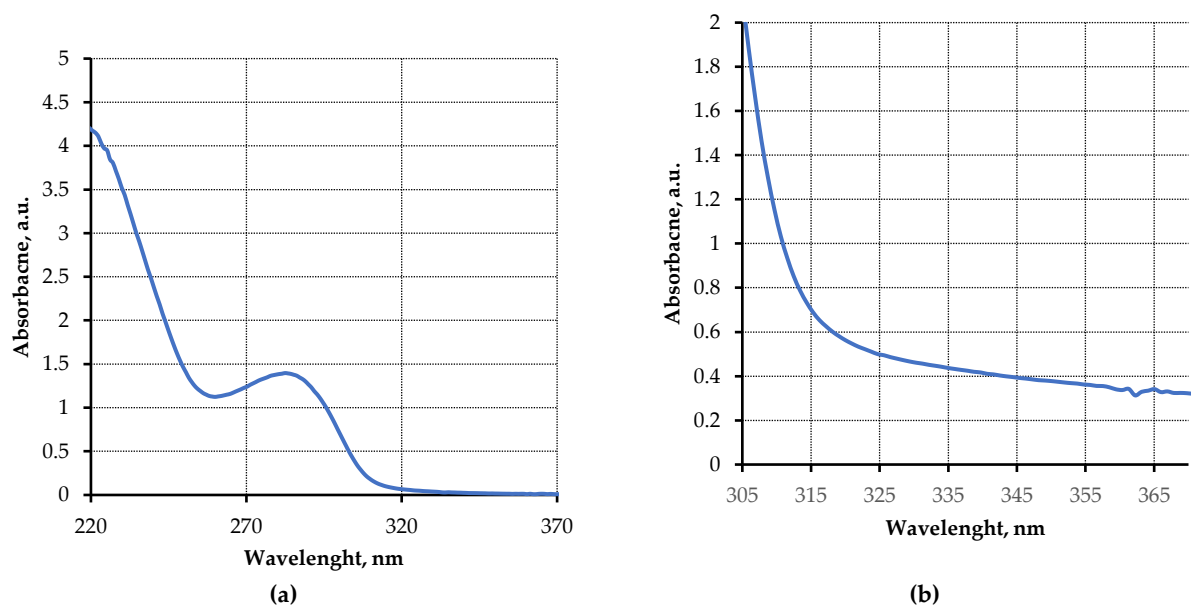


Figure 6. Examples of a dialysate UV absorption spectrum: (a) 5 mm cuvette; (b) 30 mm cuvette.

The origin of the second and the third peaks in the chromatograms still remains unclear, presumably, the second peak may be associated with the advanced glycation end products (AGE) and the third peak is related to purines and pyrimidines substances. To

prove this hypothesis UV absorption spectra of dialysate samples were recorded and compared with chromatograms. A cuvette with 30 mm optical path was used to record the weak absorption of AGE at 355–365 nm [16], the shorter wavelength part of the spectrum was recorded in a 5 mm cuvette (Figure 6).

The area of the left side of the second peak in the chromatograms shows a relatively good ($R^2=0.705$) correlation with the absorption at the wavelengths of 355–365 nm, which are characteristic of AGE. This fact confirms that the second peak is at least partially associated with low molecular weight AGE [17,18], especially taking into account that the elution time for the second peak is close to the elution time of IMP (molecular weight 348 Da), but further research is needed to fully establish this association. The area of the third peak gives a weak correlation ($R^2 \approx 0.55$) with the absorption of samples at the wavelengths of 260–265 nm, which is associated with purines and pyrimidines. It could be suggested that this peak is possibly related to multiple substances.

4. Conclusion

Thus, the possibility of determining proteins and low molecular weight metabolites in the effluent peritoneal dialysate using a simple chromatographic optical sensor was demonstrated. The optimal sample volume and the working range of protein concentrations were determined by calibration with BSA aqueous solutions. The inverse relationship between the elution time and the molecular weight of analytical substances was established with nucleotides aqueous solutions.

The chromatograms and UV absorption spectra of peritoneal dialysate samples taken from a group of ESRD patients were processed and analyzed; a relatively good correlation ($R^2 = 0.705$) was established between the second peak area and the optical absorption at 355–365 nm. This fact confirms the earlier hypothesis that this peak is at least related to low-molecular weight AGE products and apart from the protein loss assessment the sensor could be used for AGE products determination, which were shown to be associated with cardiovascular risks for dialysis patients.

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Institutional Review Board Statement: The study was conducted according to the guidelines of the Declaration of Helsinki, and approved by the Ethics Committee of the Institute of Experimental Medicine (protocol #2/22 from 06.04.22).

Informed Consent Statement: Patient consent was waived according to the Decision of the Council of the Eurasian Economic Commission No. 29 of February 12, 2016 "On Rules for Clinical and Clinical Laboratory Trials (Studies) of Medical Products". The document states that written informed consent is not required when residual laboratory samples are used exclusively for in-vitro research and testing of clinical laboratory equipment. Patients' personal data or medical history were not disclosed by the hospital.

Data Availability Statement: Data available on request due to the Hospital ethical policy.

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Conflicts of Interest: The authors declare no conflicts of interest.

References

1. Bikbov, B.; Purcell, C.A.; Levey, A.S.; Smith, M.; Abdoli, A.; Abebe, M.; Adebayo, O.M.; Afarideh, M.; Agarwal, S.A.; Agudelo-Botero, M.; et al. Global, regional, and national burden of chronic kidney disease, 1990–2017: A systematic analysis for the Global Burden of Disease Study 2017. *Lancet* **2020**, *395*, 709–733, doi:10.1016/S0140-6736(20)30045-3.
2. Li, P.K.-T.; Chow, K.M.; Van de Luijngaarden, M.W.M.; Johnson, D.W.; Jager, K.J.; Mehrotra, R.; Naicker, S.; Pecoits-Filho, R.; Yu, X.Q.; Lameire, N. Changes in the worldwide epidemiology of peritoneal dialysis. *Nat. Rev. Nephrol.* **2017**, *13*, 90–103, doi:10.1038/nrneph.2016.181
3. Mehrotra, R.; Devuyst, O.; Davies, S.J.; Johnson, D.W. The Current State of Peritoneal Dialysis. *J. Am. Soc. Nephrol.* **2016**, *27*, 3238–3252, doi:10.1681/ASN.2016010112.
4. Blumenkrantz, M.J.; Gahl, G.M.; Kopple, J.D.; Kamdar, A.V.; Jones, M.R.; Kessel, M.; Coburn, J.W. Protein losses during peritoneal dialysis. *Kidney Int.* **1981**, *19*, 593–602, doi:10.1038/ki.1981.57.
5. Fan, J.; Ye, H.; Zhang, X.; Cao, P.; Guo, Q.; Mao, H.; Yu, X.; Yang, X. Association of Lean Body Mass Index and Peritoneal Protein Clearance in Peritoneal Dialysis Patients. *Kidney Blood Press. Res.* **2019**, *44*, 94–102, doi:10.1159/000498841.
6. Chang, T.I.; Kang, E.W.; Lee, Y.K.; Shin, S.K. Higher Peritoneal Protein Clearance as a Risk Factor for Cardiovascular Disease in Peritoneal Dialysis Patient. *PLoS ONE* **2013**, *8*, e56223, doi:10.1371/journal.pone.0056223.
7. Lu, W.; Pang, W.-F.; Jin, L.; Li, H.; Chow, K.M.; Kwan, B.C.-H.; Leung, C.B.; Li, P.K.-T.; Szeto, C.C. Peritoneal protein clearance predicts mortality in peritoneal dialysis patients. *Clin. Exp. Nephrol.* **2018**, *23*, 551–560, doi:10.1007/s10157-018-1677-9.
8. Dong, J.; Chen, Y.; Luo, S.; Xu, R.; Xu, Y. Peritoneal Protein Leakage, Systemic Inflammation, and Peritonitis Risk in Patients on Peritoneal Dialysis. *Perit. Dial. Int.* **2013**, *33*, 273–279, doi:10.3747/pdi.2011.00326.
9. Fung, W.W.-S.; Li, P.K.-T. Recent advances in novel diagnostic testing for peritoneal dialysis-related peritonitis. *Kidney Res. Clin. Pract.* **2022**, *41*, 156–164, doi:10.23876/j.krcp.21.204.
10. Lingervelder, D.; Koffijberg, H.; Kusters, R.; IJzerman, M.J. Point-of-care testing in primary care: A systematic review on implementation aspects addressed in test evaluations. *Int. J. Clin. Pract.* **2019**, *73*, e13392, doi:10.1111/ijcp.13392.
11. Walls, D.; Loughran, S.T. *Protein Chromatography: Methods and Protocols*, 2011th ed.; Humana Press: Totowa, NJ, USA, 2011; p. 681, ISBN 9781607619123.
12. Determann, H. *Gel Chromatography, Gel Filtration, Gel Permeation, Molecular Sieves: A Laboratory Hand Book*, 2nd ed.; Springer: New York, NY, USA, 1969; p. 208, ISBN 978-3642950841.
13. Sünter, A.; Frorip, A.; Korsakov, V.; Kurruk, R.; Kuznetsov, A.; Ots-Rosenberg, M. Optical method for screening and a new proteinuria focus group. *J. Biomed. Photonics Eng.* **2015**, 236–247, doi:10.18287/JBPE-2015-1-4-236.
14. Kuznetsov, A.; Frorip, A.; Sünter, A.; Kasvand, N.; Korsakov, V.; Konoplev, G.; Stepanova, O.; Rusalepp, L.; Anton, D.; Püssa, T.; et al. Fast Protein and Metabolites (Nucleotides and Nucleosides) Liquid Chromatography Technique and Chemical Sensor for the Assessment of Fish and Meat Freshness. *Chemosensors* **2023**, *11*, 69, doi:10.3390/chemosensors11010069.
15. Kuznetsov, A.; Frorip, A.; Sünter, A.; Korsakov, V.; Konoplev, G.; Stepanova, O.; Roschina, N.; Ovsyannikov, N.; Lialin, D.; Gerasimchuk, R.; et al. Optical Chemical Sensor Based on Fast-Protein Liquid Chromatography for Regular Peritoneal Protein Loss Assessment in End-Stage Renal Disease Patients on Continuous Ambulatory Peritoneal Dialysis. *Chemosensors* **2022**, *10*, 232, doi:10.3390/chemosensors10060232.
16. Kuznetsov, A.; Frorip, A.; Gerasimchuk, R.P.; Konoplev, G.A.; Rosenberg, M.; Sinijärvi, H.; Sünter, A.; Vasilevsky, A.M.; Zemenchikov, A.Y. MP479 Multimode monitoring of age excretion in hemodialysis. *Nephrol. Dial. Transplant.* **2016**, *31*, i500-i501, doi:10.1093/ndt/gfw194.34.
17. Stingham, A.E.M.; Massy, Z.A.; Vlassara, H.; Striker, G.E.; Boullier, A. Uremic Toxicity of Advanced Glycation End Products in CKD. *J. Am. Soc. Nephrol.* **2016**, *27*, 354–370, doi:10.1681/ASN.2014101047.
18. Jiang, J.; Zhang, Y.; Chen, J.; Yang, X.; Mei, C.; Xiong, F.; Shi, W.; Zhou, W.; Liu, X.; Sun, S.; et al. Serum and Tissue Levels of Advanced Glycation End Products and Risk of Mortality in Patients on Maintenance Hemodialysis. *Am. J. Nephrol.* **2021**, *52*, 8–16, doi:10.1159/000512385.

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