

# USING INTERDIGITATED ORGANIC ELECTROCHEMICAL TRANSISTORS AS ELECTROPHYSIOLOGICAL AND BIOCHEMICAL SENSORS

Dr. Dirk Mayer

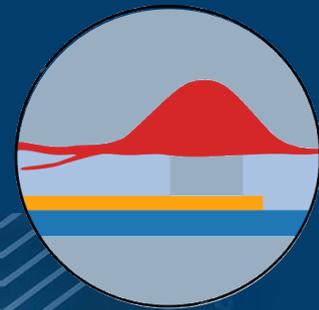


**How do we understand neuronal signaling in the brain?**

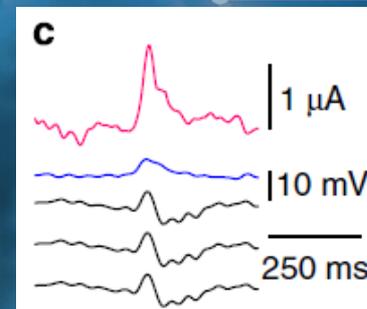
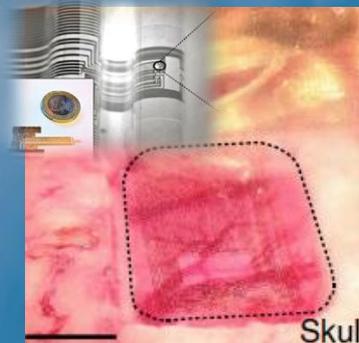
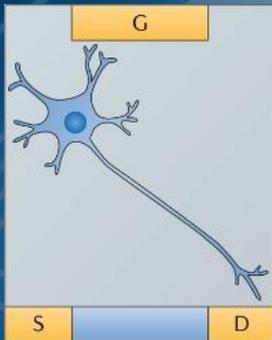
**How neurons control behavior?**

**How signaling malfunctions during disease?**

# Organic electrochemical transistors

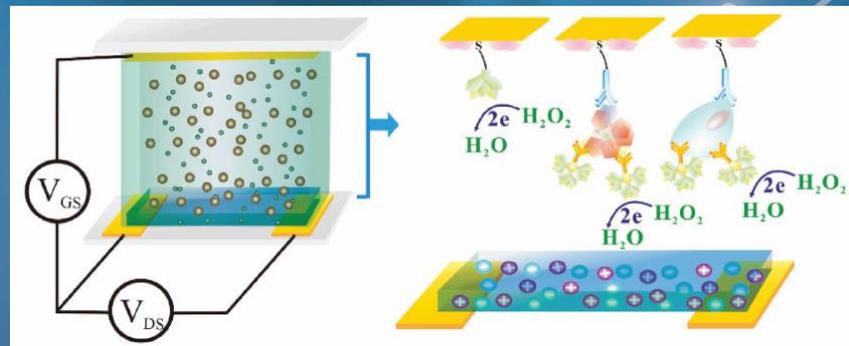
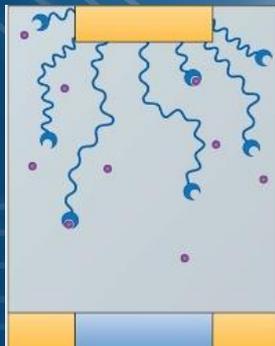


## Electrophysiological sensors

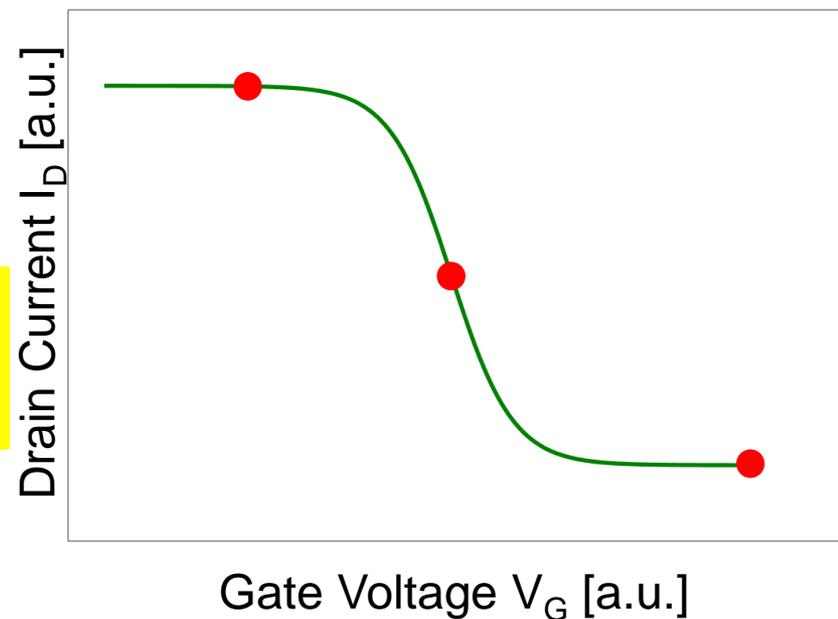
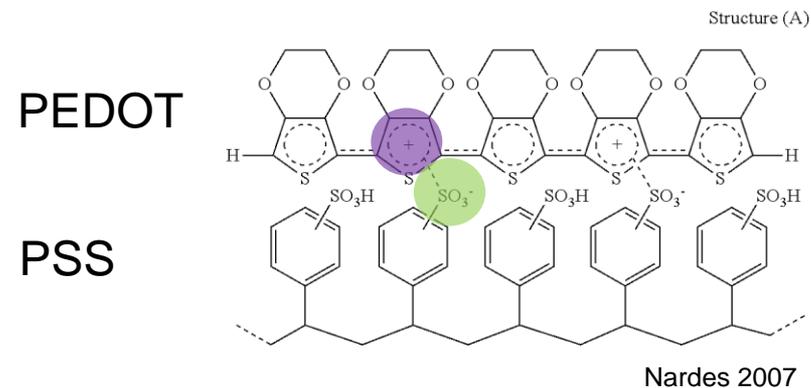
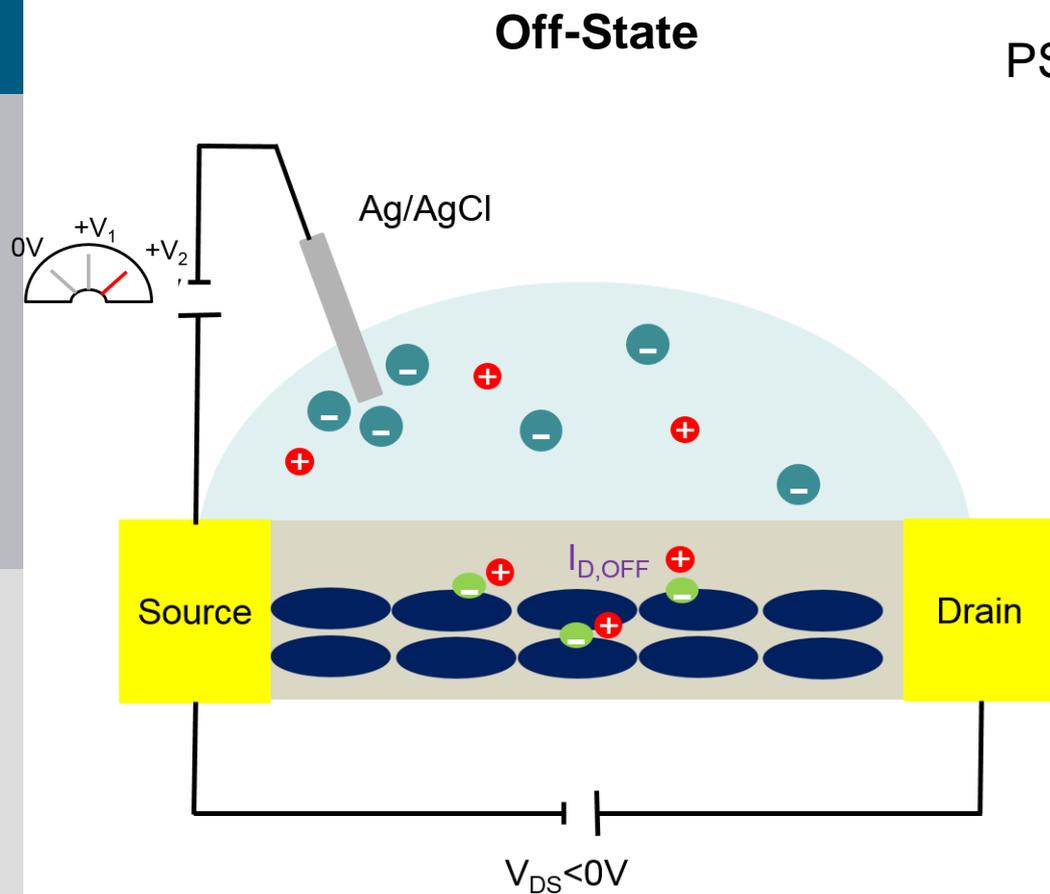


D. Khodagholy, Nature Commun, 2013

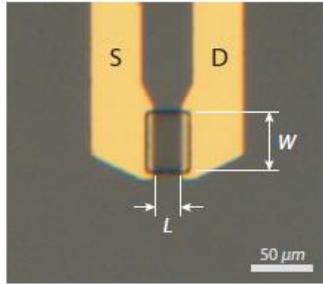
## Biochemical sensors



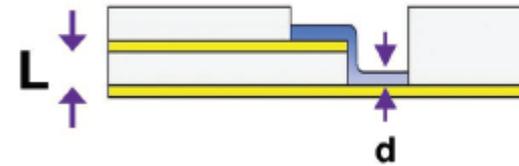
Fu et al Adv. Mater. 2017, 1703787



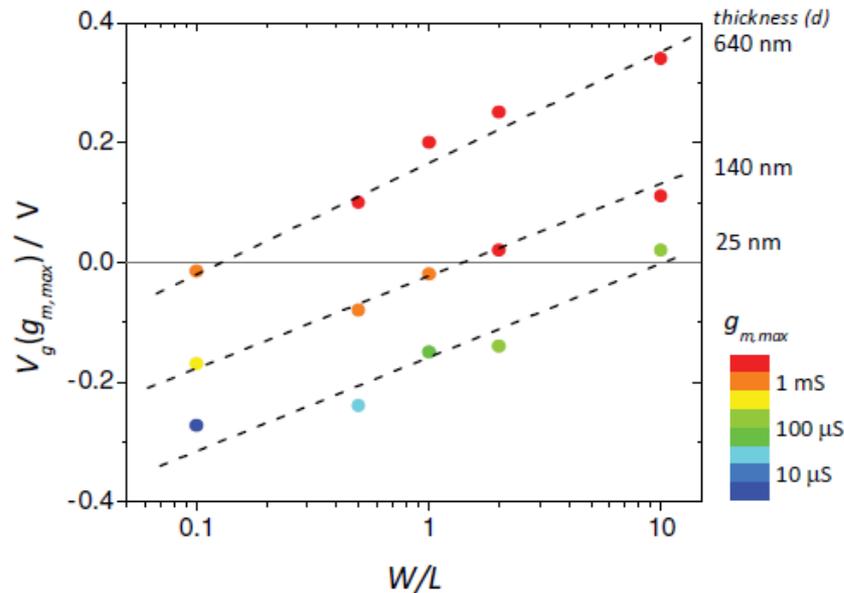
## Planar OECTs



## Vertical OECTs

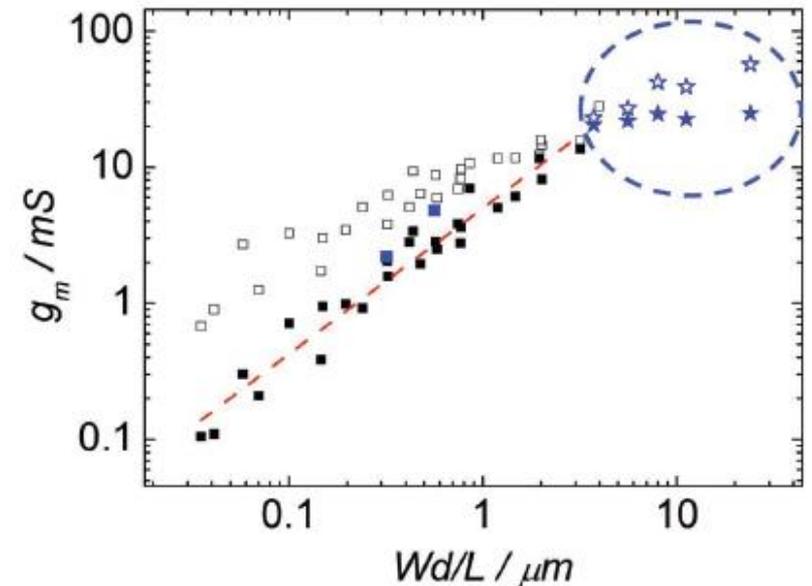


## Transconductance



Rivnay et al *Adv.Mater.* **2013**, 25, 7010–7014

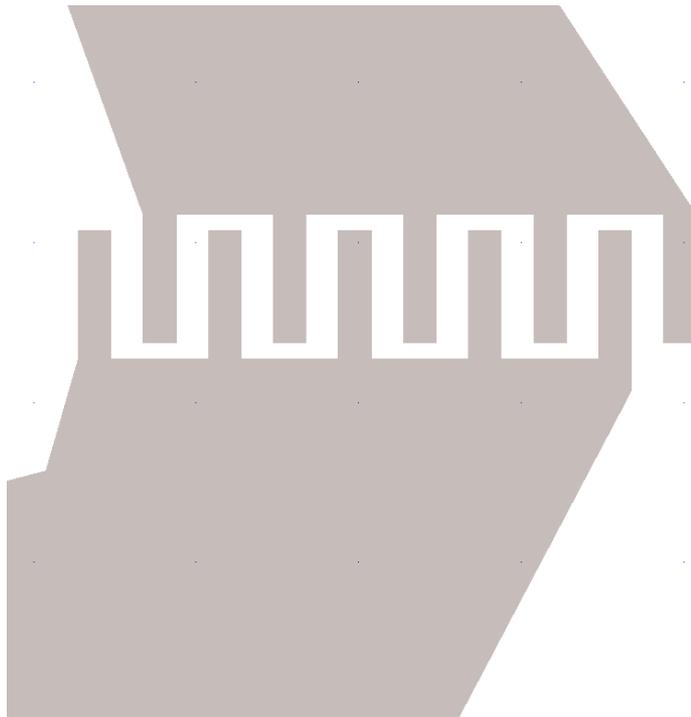
$$g_m = (W \cdot d / L) \cdot \mu \cdot C^* \cdot (V_T - V_G)$$



Donahue et al *Adv. Mater.* **2018**, 30, 1705031

**Low transistor density**

## Interdigitated Electrodes



### Advantage:

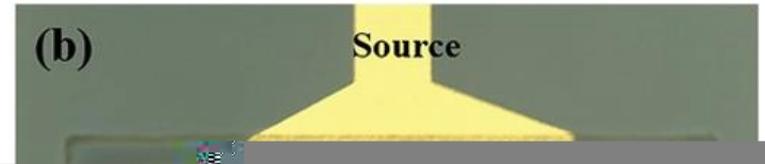
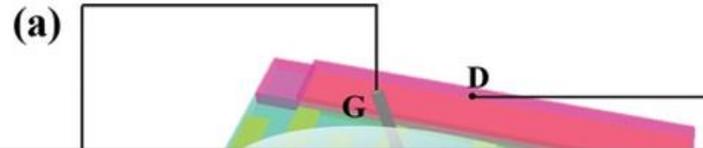
Large Channel Width  
Short Channel Length

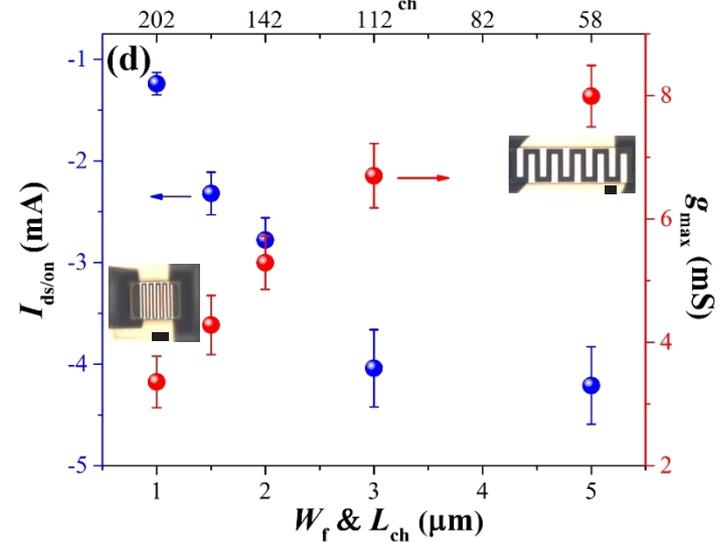
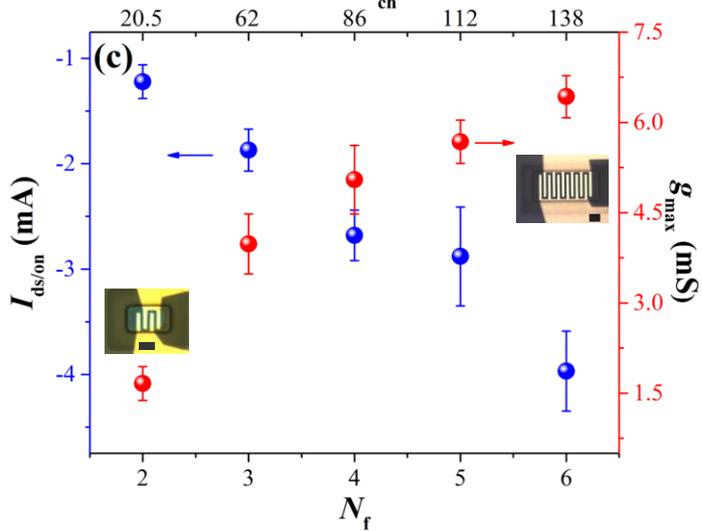
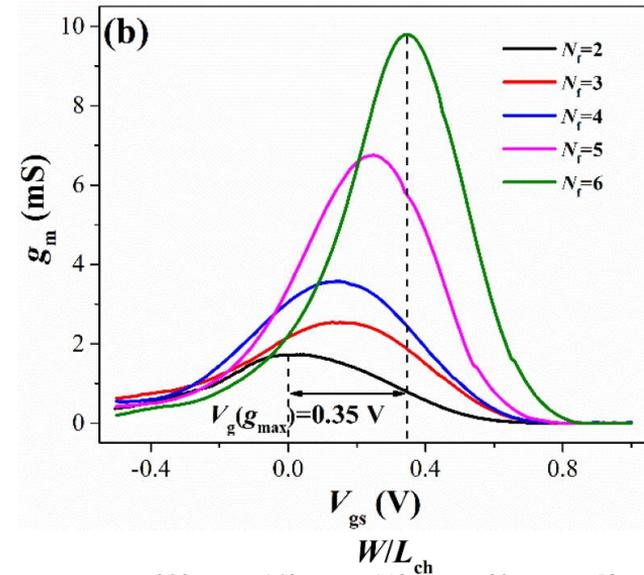
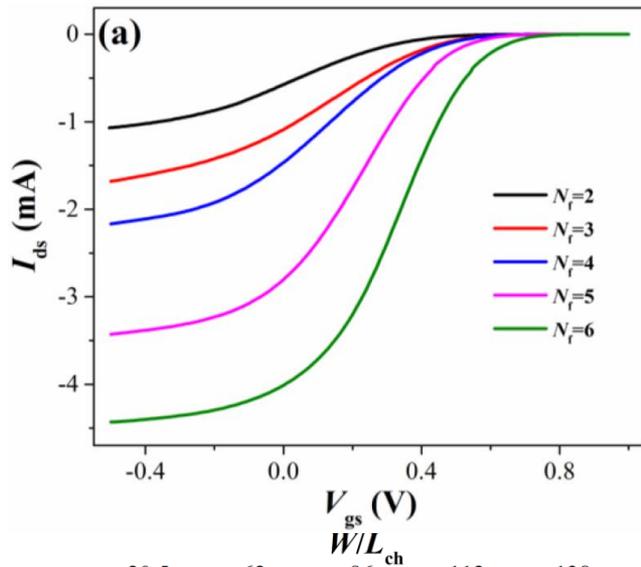
High Current +  
Low Voltage,  
High Sensitivity

Dimensions of  
Single Cells

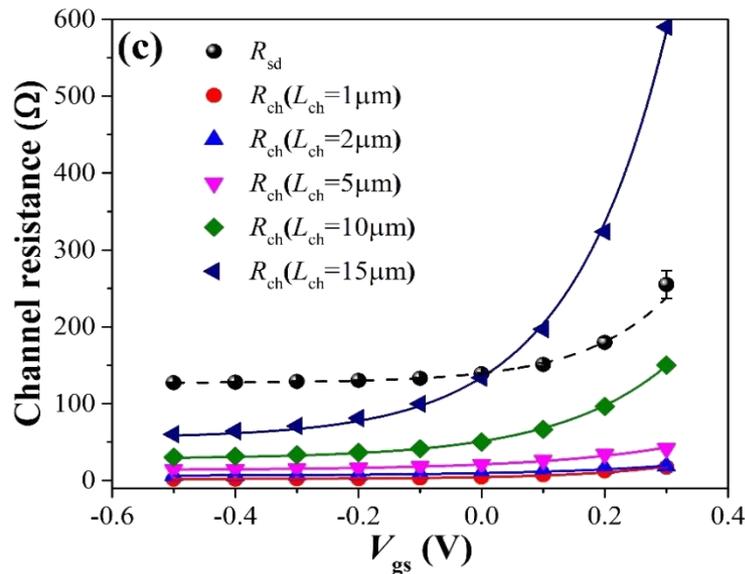
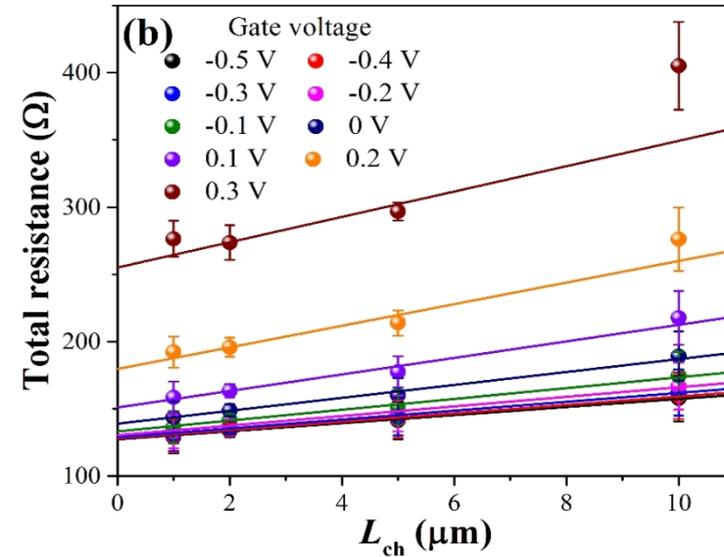
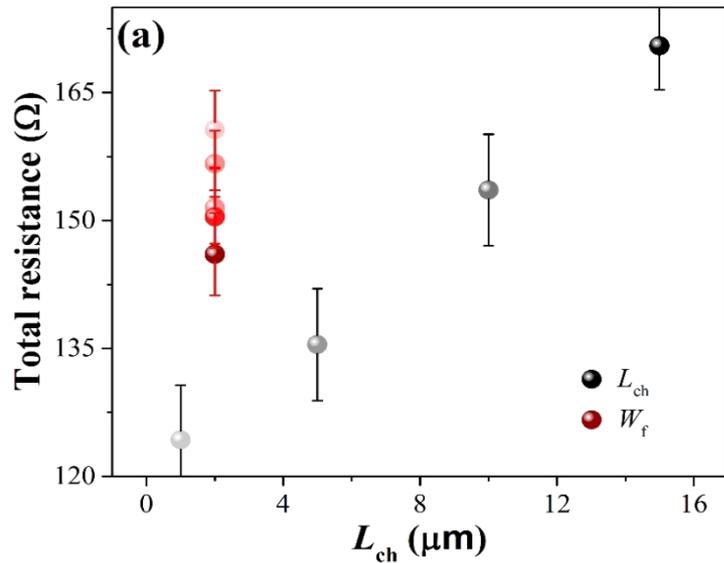
**Potentially improved  
performance**

Feature Size  $\approx 2\mu\text{m}$   
Number of Unit Cells 2-6





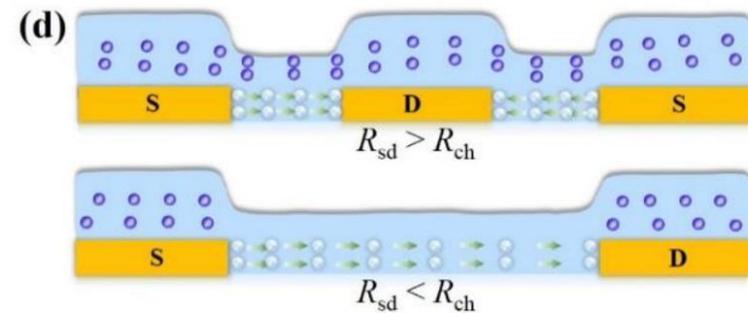
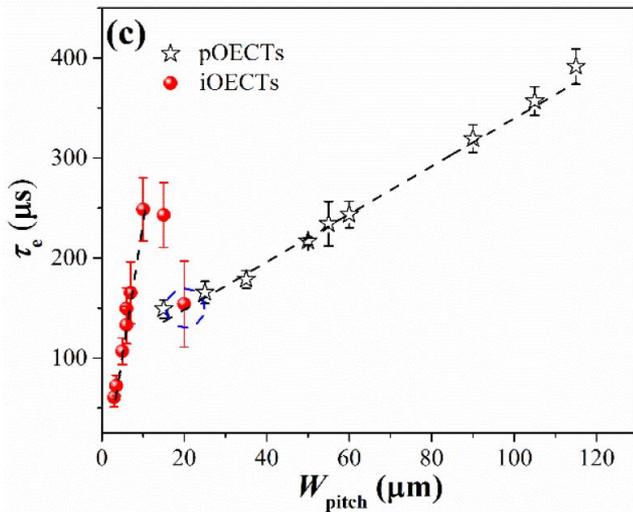
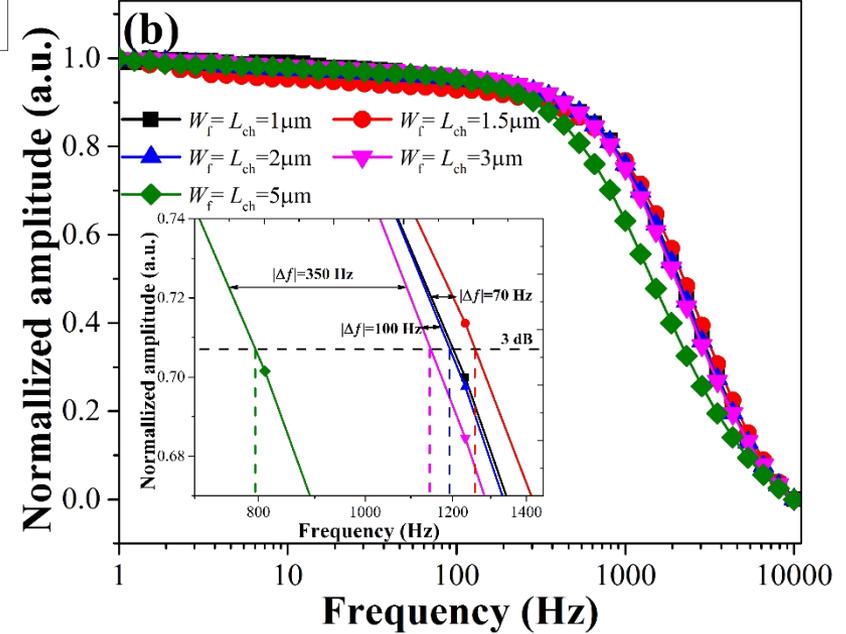
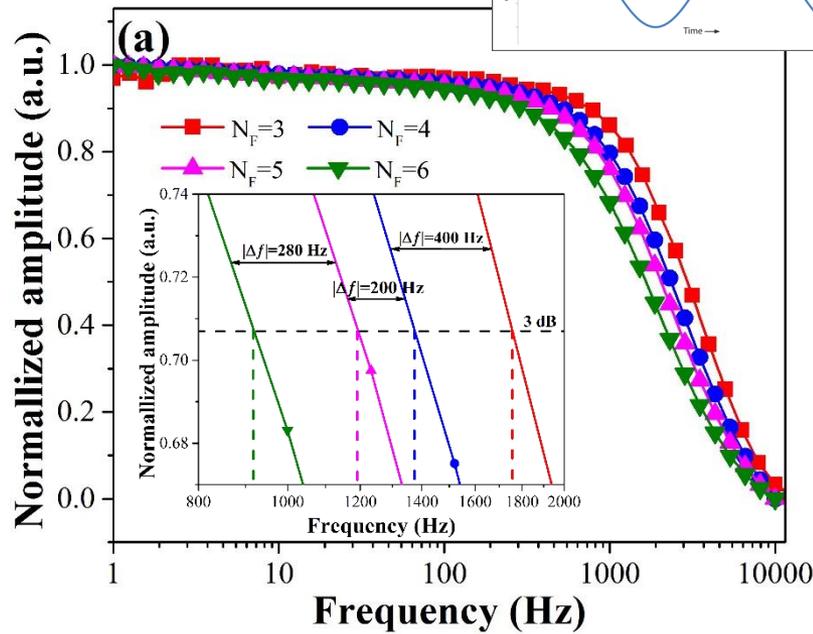
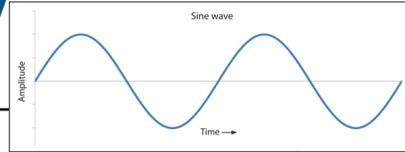
$N_f \uparrow$      $W_f \uparrow$      $L_{ch} \downarrow$      $g_m \uparrow$

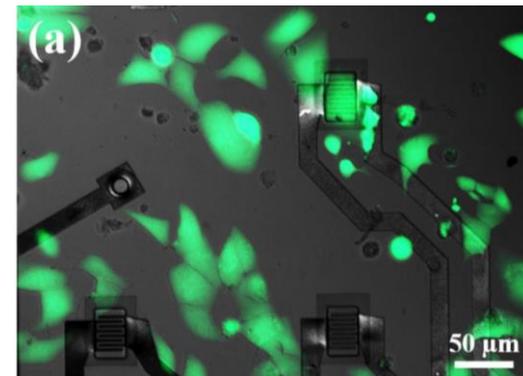
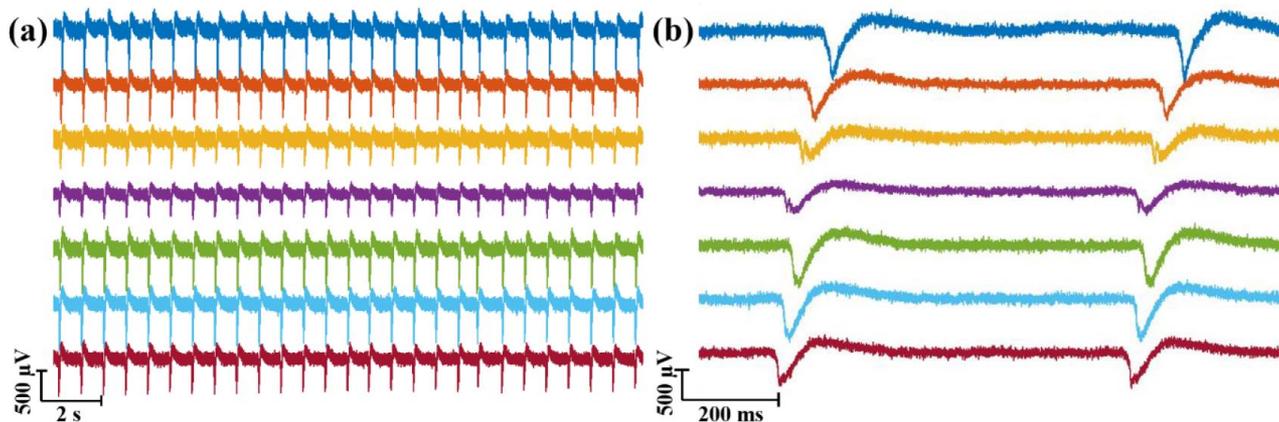


>  $R_{sd}$  increases significantly at  $V_{gs}$  above 0V

> Critical channel length

# Cut-off frequency

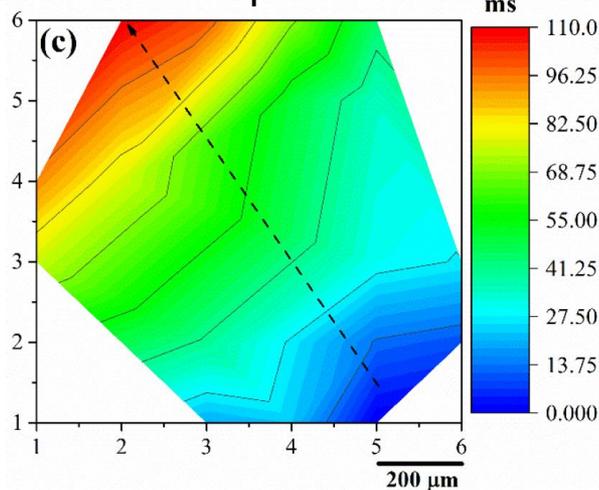




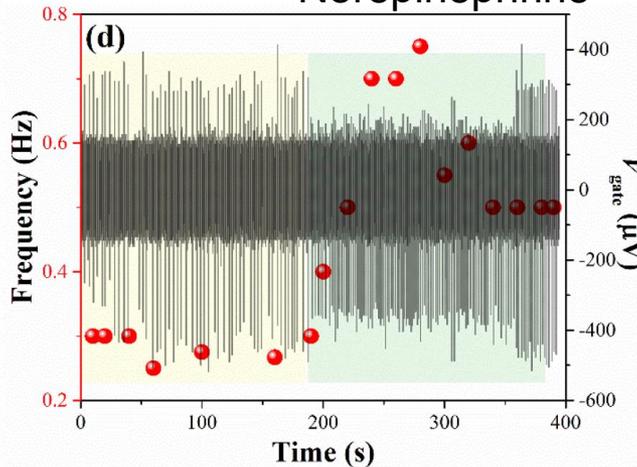
$N_f=5$ ,  $W_f=3 \mu\text{m}$ ,  $L_{ch}=3 \mu\text{m}$

Signal to noise ratio: 7~18

Isochronal map of time latencies



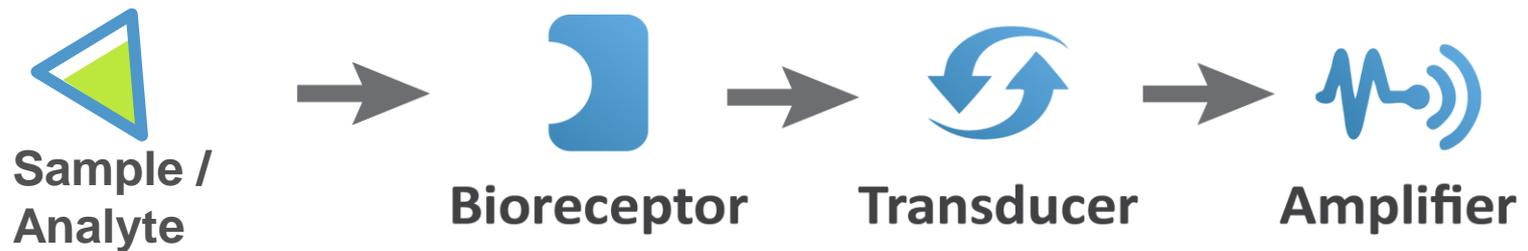
Norepinephrine



Smallest transistor area:  $30 \mu\text{m} \times 22 \mu\text{m}$

$N_f=4$ ,  $W_f=2 \mu\text{m}$ ,  $L_{ch}=2 \mu\text{m}$

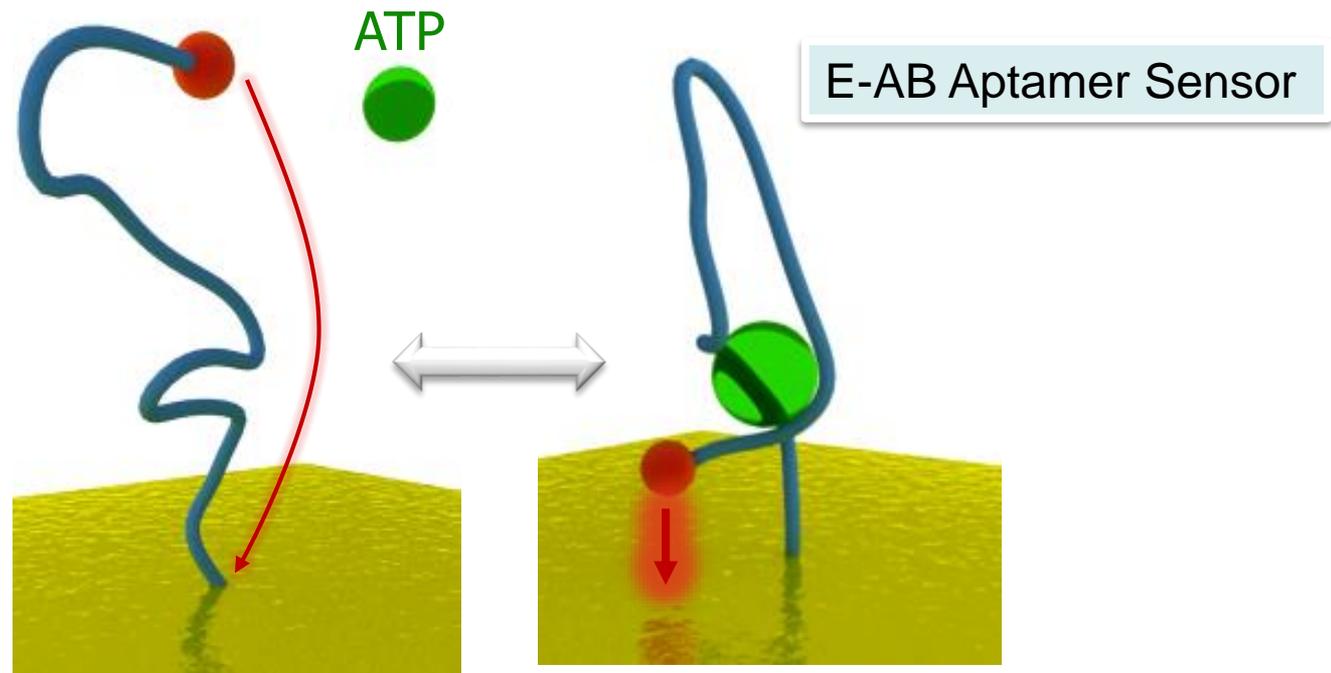
## *OEET as Biosensor*



## Electrochemical biosensors

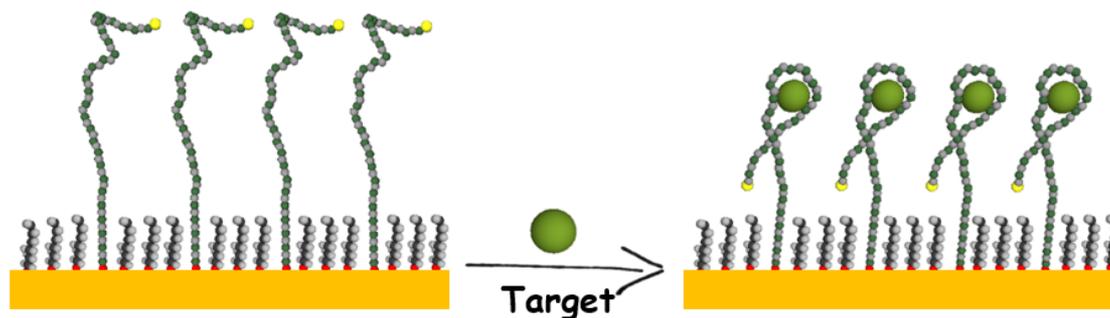
- Thermostable
- Easy modification
- Inexpensive

**Drawbacks:** The obtained electrochemical signals are usually limited by the surface probe density and high background signal

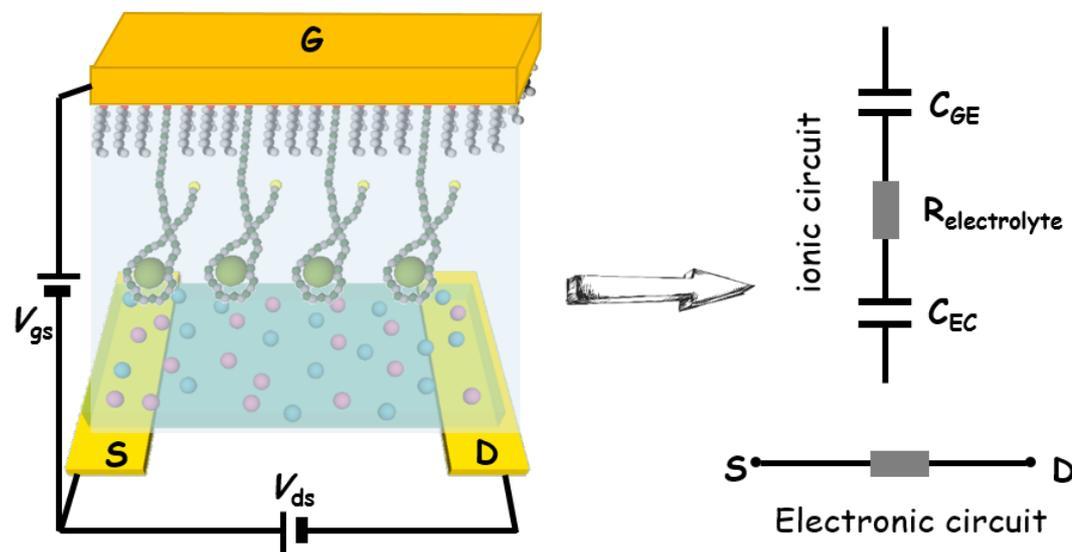


## Amperometric Transducer

Liang et al Bios. Bioelect. 2019 144, 111668



## Potentiometric Transducer



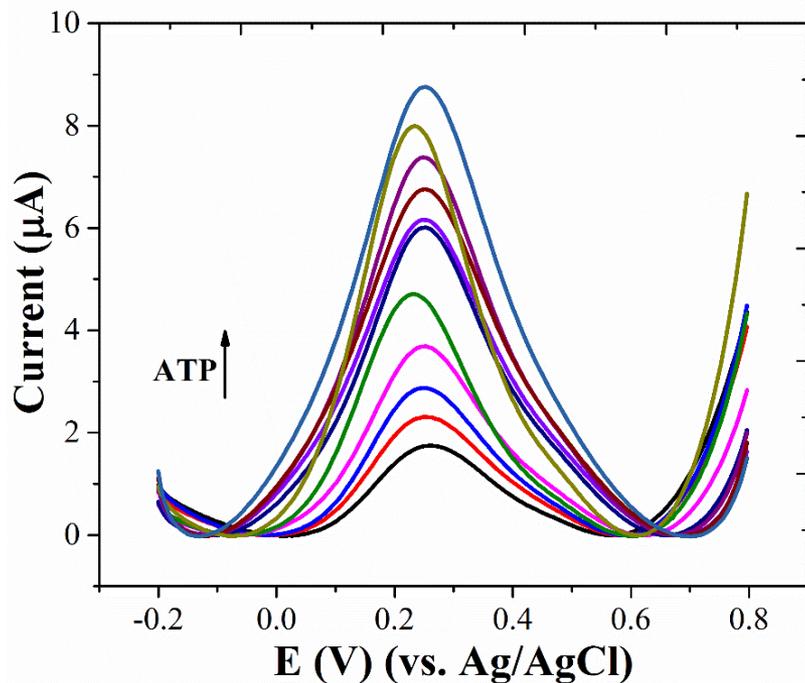
## Macroelectrode

Annealed with a hydrogen flame, then cooled down to room temperature

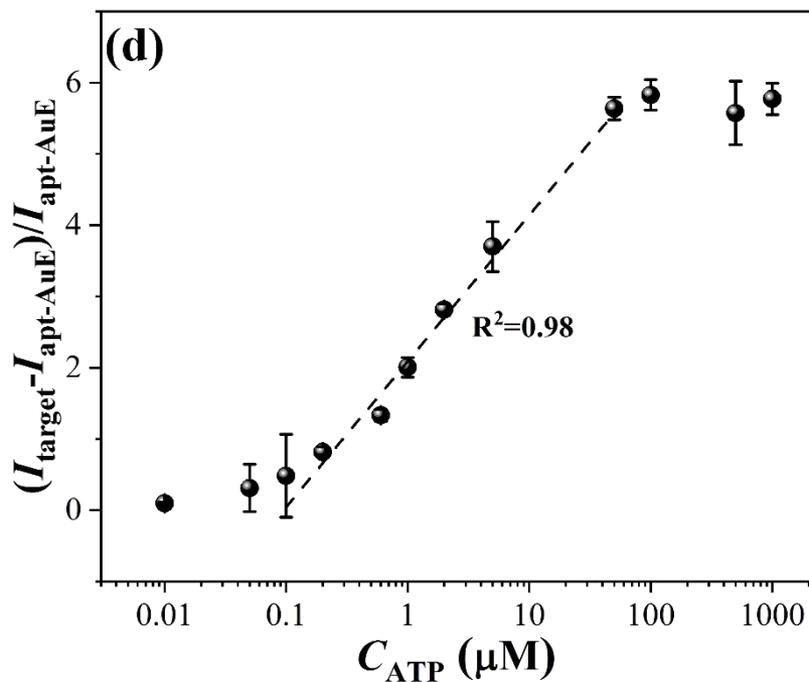
50 mM  $\text{H}_2\text{SO}_4$  to determine the surface area

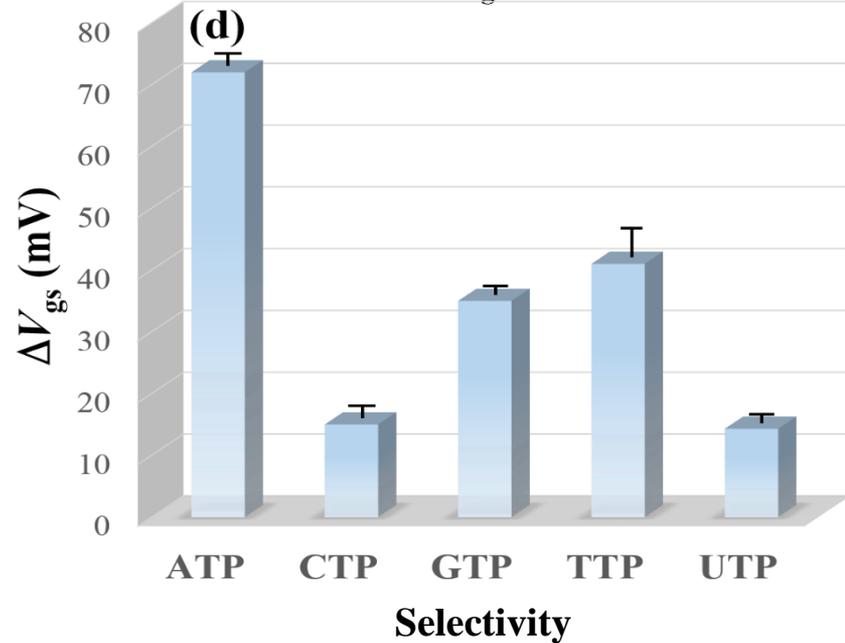
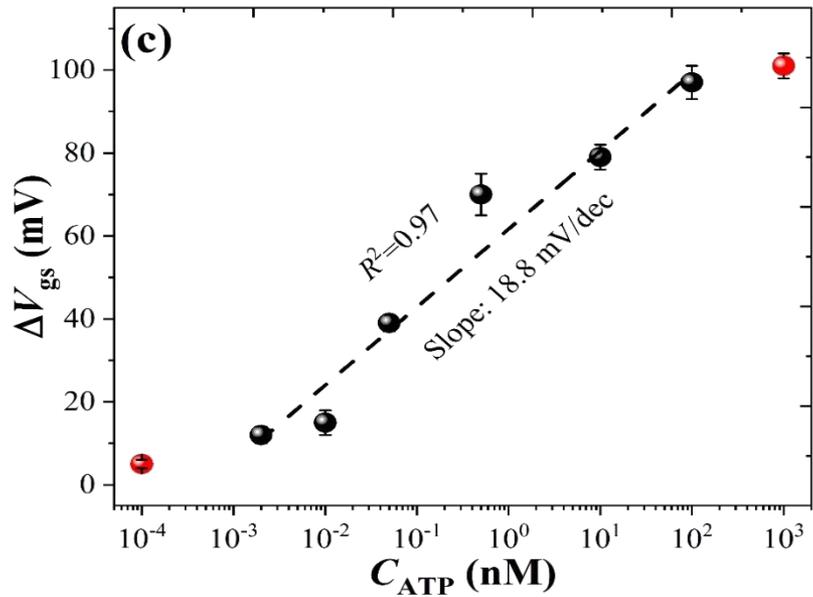
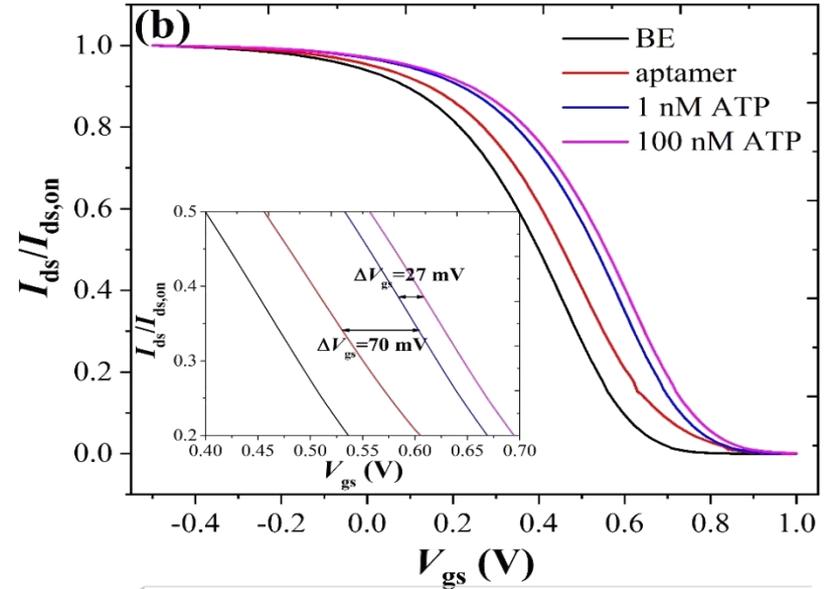
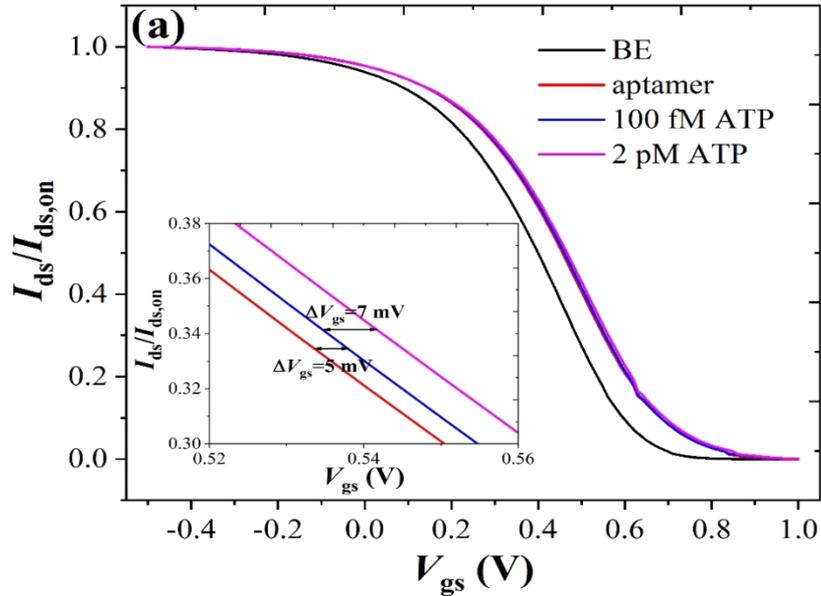
Incubation in DNA oligomer pretreated with TCEP for 16h

Blocked by MCH for 1h



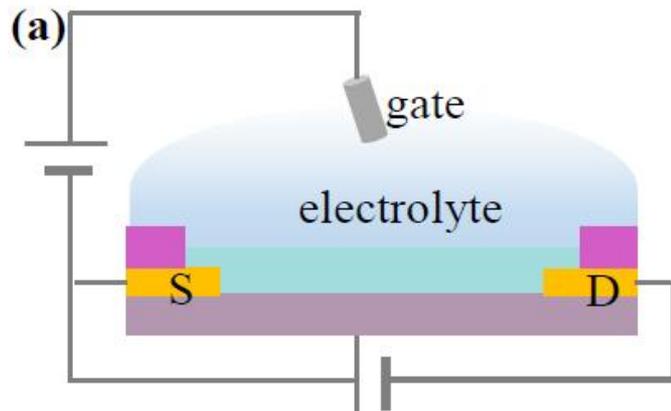
**Limit of detection: 100 nM**



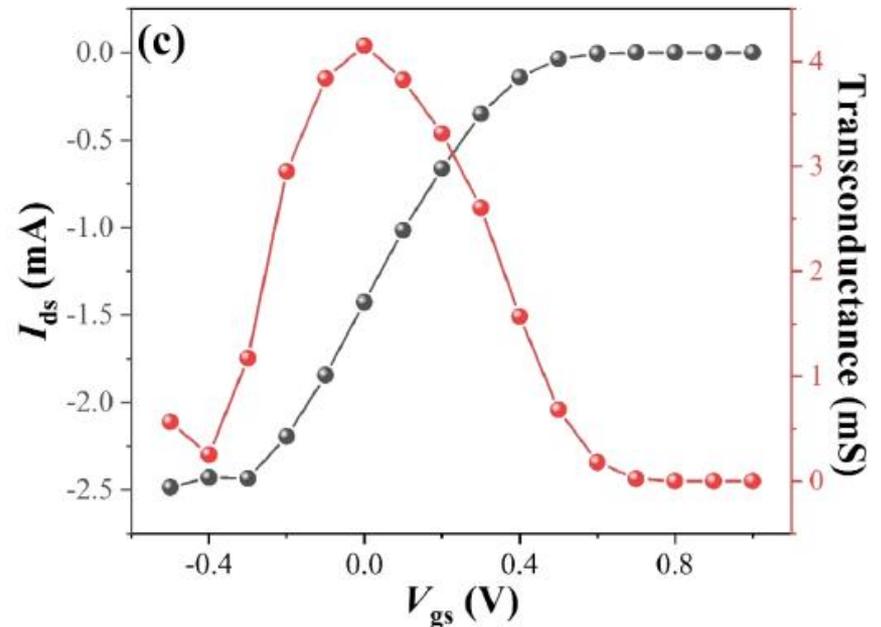
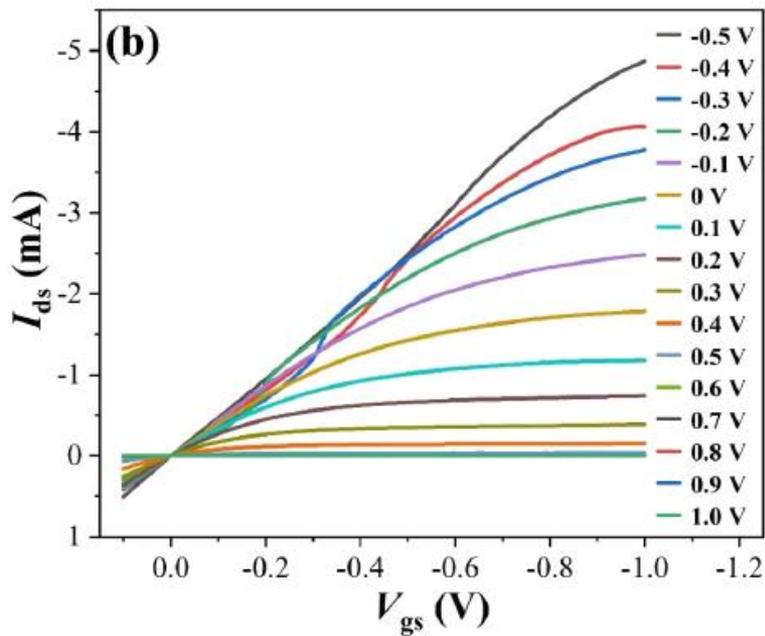


# Flexible OEET

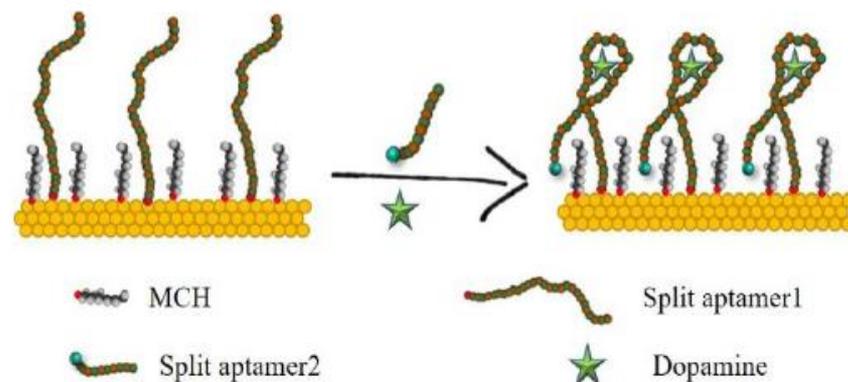
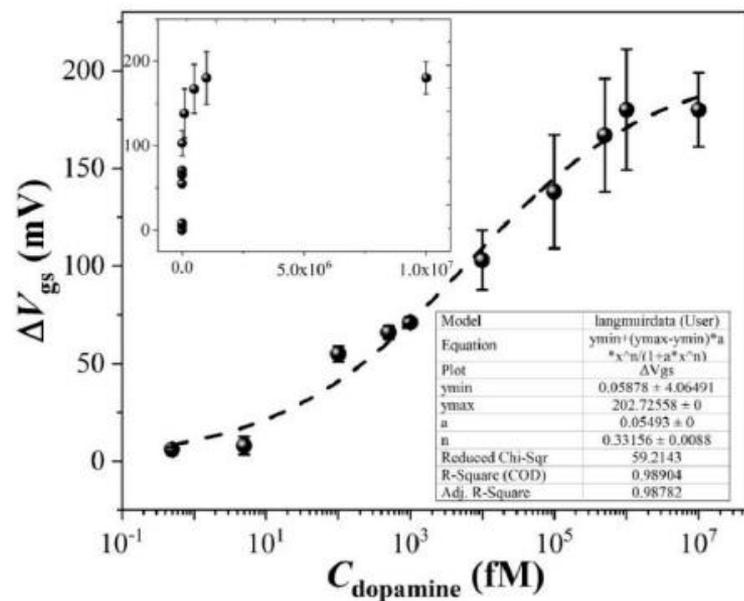
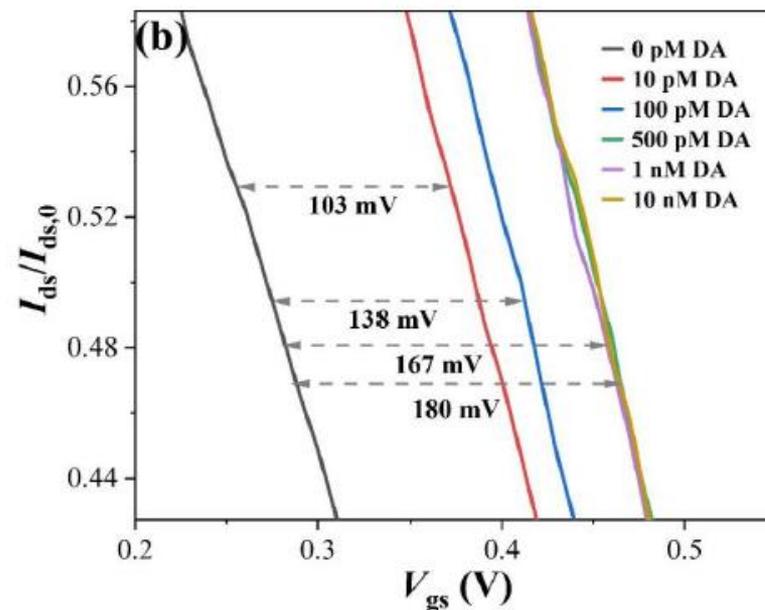
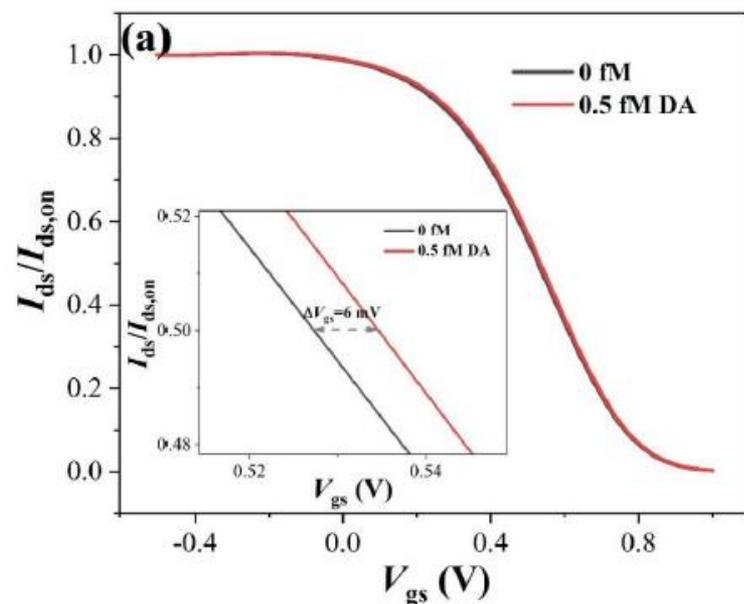
Liang et al. *Materials*13.11 (2020): 2577.



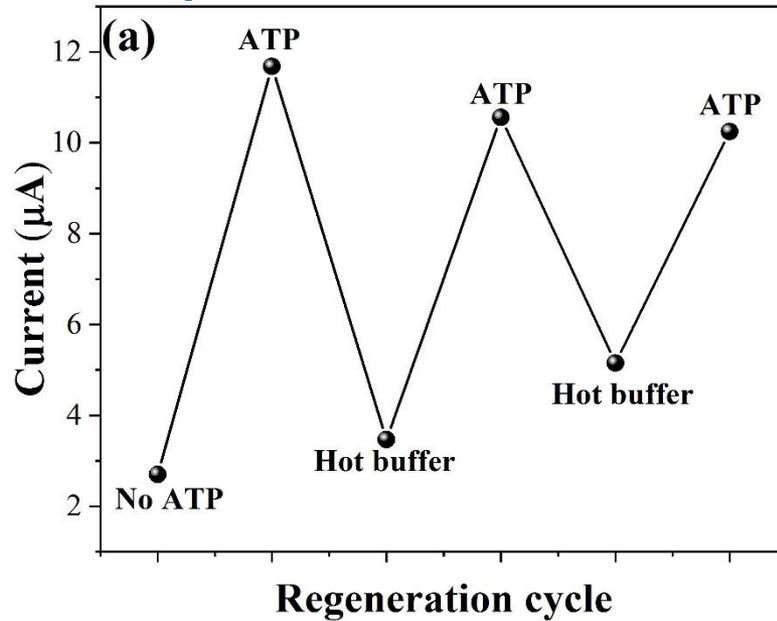
PI2611 Au  
HD8820 PEDOT:PSS



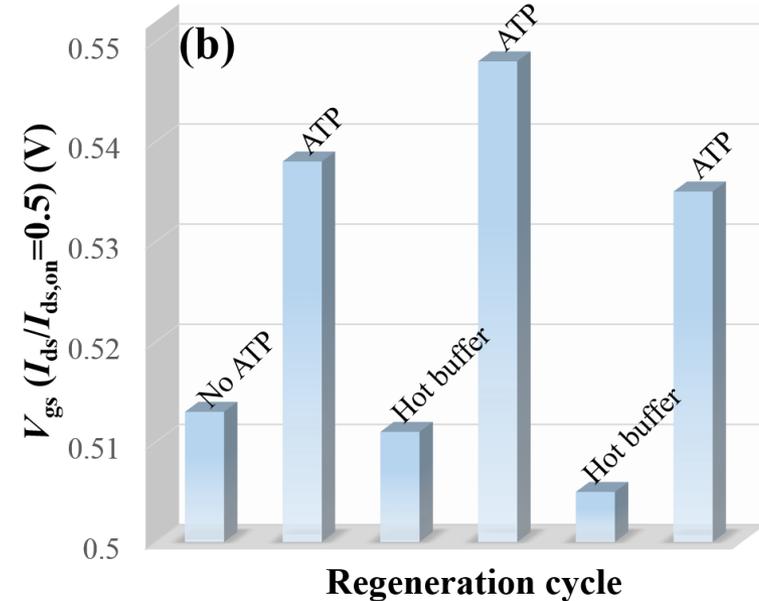
# Dopamine detection via OECT



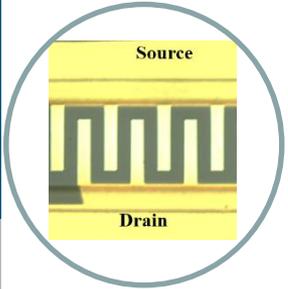
## Amperometric Transducer



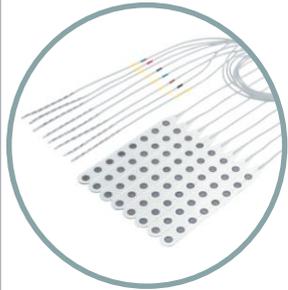
## Potentiometric Transducer



# Future directions



iOECT performance limited by source-drain series resistance  
3D source and drain electrodes, improve charge injection  
Improve channel stability



High density iOECTs potentially facilitate combination of  
electrochemistry with electrophysiology on chip but requires  
integration of gate electrode



Grand future challenge is to integrate different devices to better  
understand the coordinated changes of action potentials and  
different molecules on different time and length scales in the brain