

Chitosan/glycerol gel films for the accurate in vitro evaluation of the corrosion of biodegradable medical magnesium alloys

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INTRODUCTION

Medical magnesium-based metals are widely used in clinical applications, such as bone fixation devices, dental implants, and cardiovascular stents, thanks to their excellent biocompatibility and absorbability, as well as their ability to promote bone regeneration. However, when their degradation rate in the body exceeds expectations, excessive accumulation of magnesium ions may lead to hemolysis or osteolysis, while if the rate is too slow, there is a risk of inflammation from residual material. Therefore, it is essential to accurately quantify the degradation process in order to prevent these complications.

Biodegradable implants interact not only with bodily fluids and blood, but also with tissues and organs such as bones, muscles, and the extracellular matrix. Therefore, traditional electrochemical corrosion evaluation methods that rely on liquid electrolytes fail to accurately assess the degradation of these materials.

To address this issue, we used a chitosan hydrogel, which simulates the elemental composition and microstructure of biological tissues, as the background electrolyte. For example, the 3D porous network of the hydrogel mimics the extracellular matrix and intramuscular connective tissue, allowing for a more accurate assessment of the degradation process.

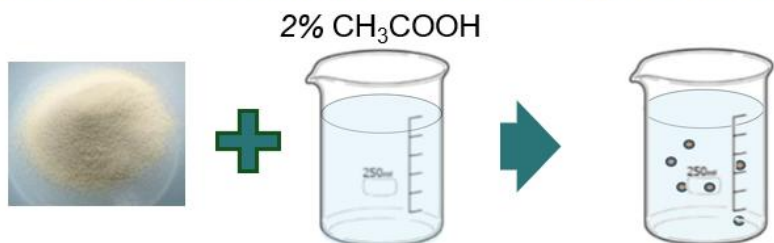
In this study, we compared the degradation of the magnesium alloy AZ91D in liquid and gel-based electrolytes through electrochemical analysis and observation of changes in the alloy's microstructure. Our results show that, unlike in solution, where the degradation is rapid and uniform, the alloy degrades more slowly when in contact with gel, accompanied by pitting corrosion on the surface and the formation of a mixed layer between the gel and alloy corrosion products.

We also investigated the influence of chitosan deacetylation degree, and electrolyte composition on the corrosion properties of the alloy. These findings can provide a basis for customizing corrosion tests to specific implant sites or individual patient variations in the future.

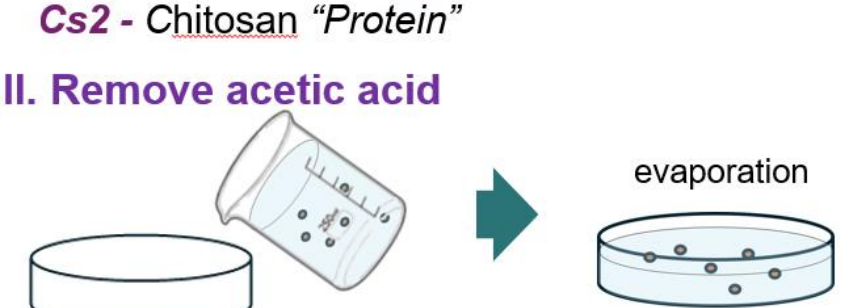
METHOD

Synthesis of gels

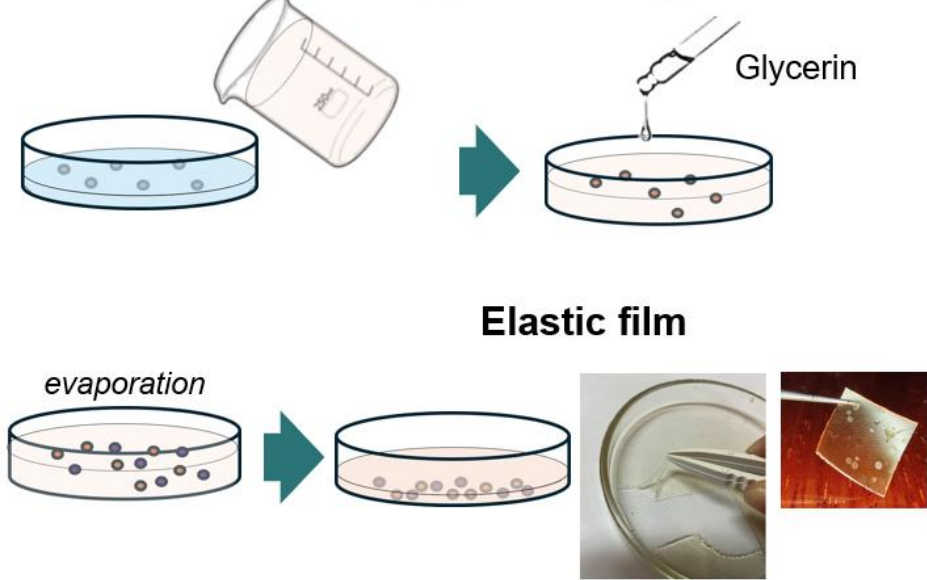
I. Dissolve chitosan powder using acetic acid



II. Remove acetic acid

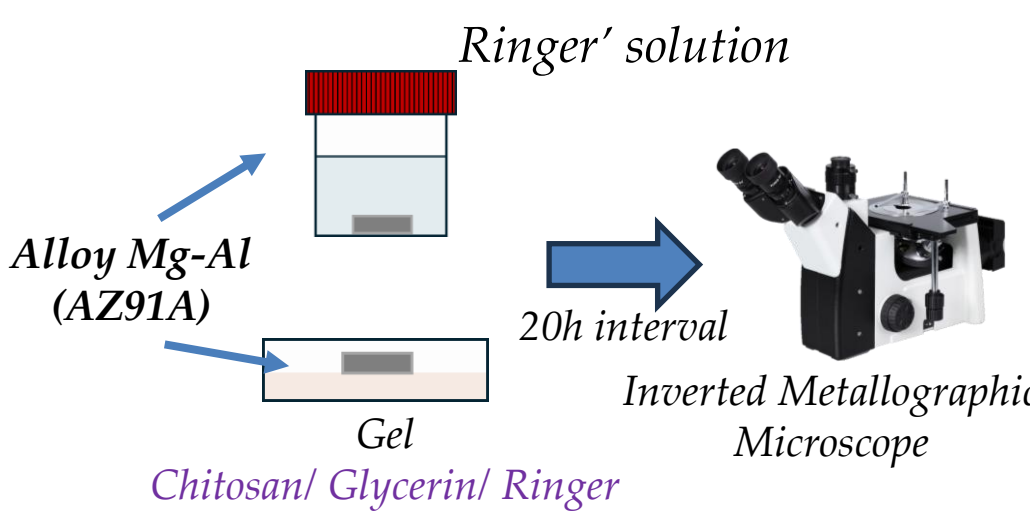


III. Introduction of 0.9% NaCl / Ringer's solution

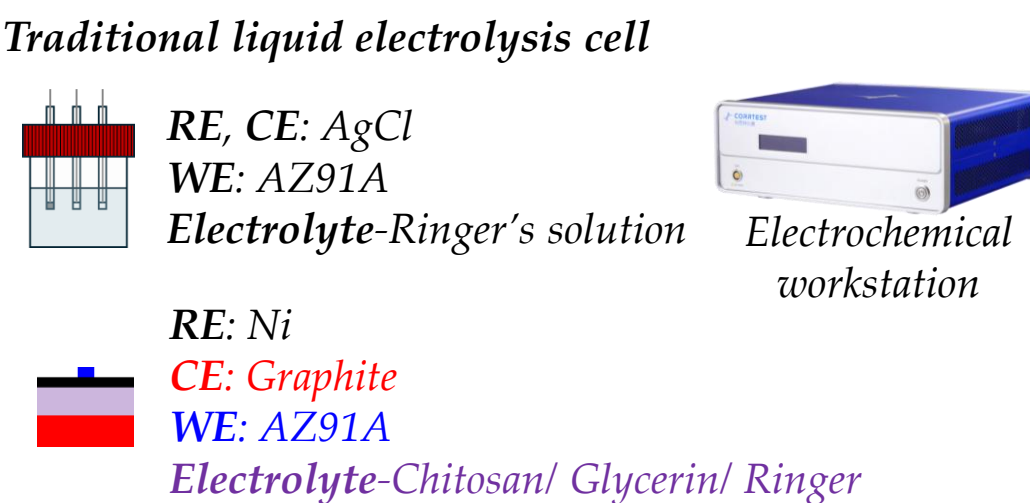


Experimental methods

Contact test

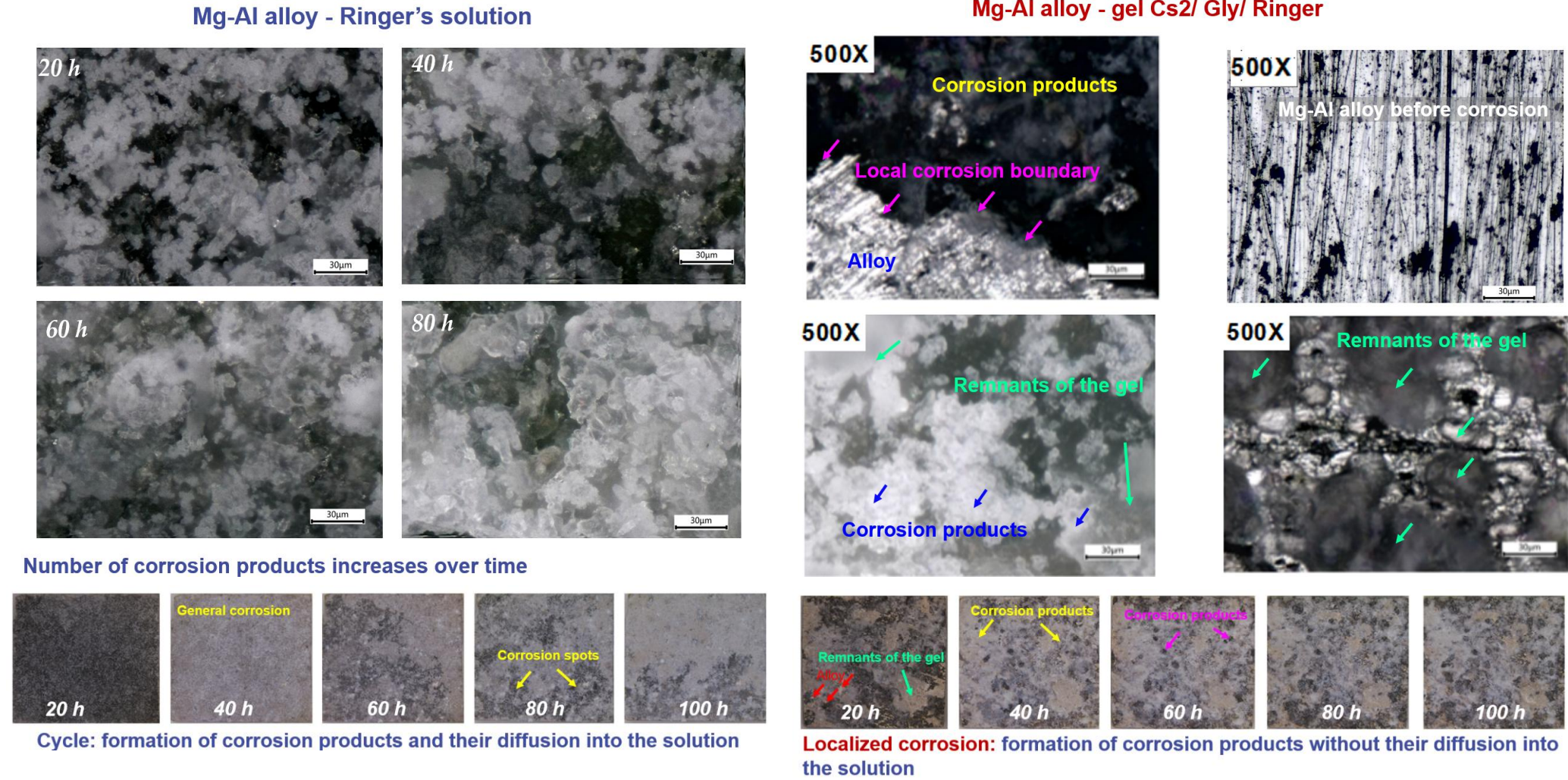


Electrochemical assessment

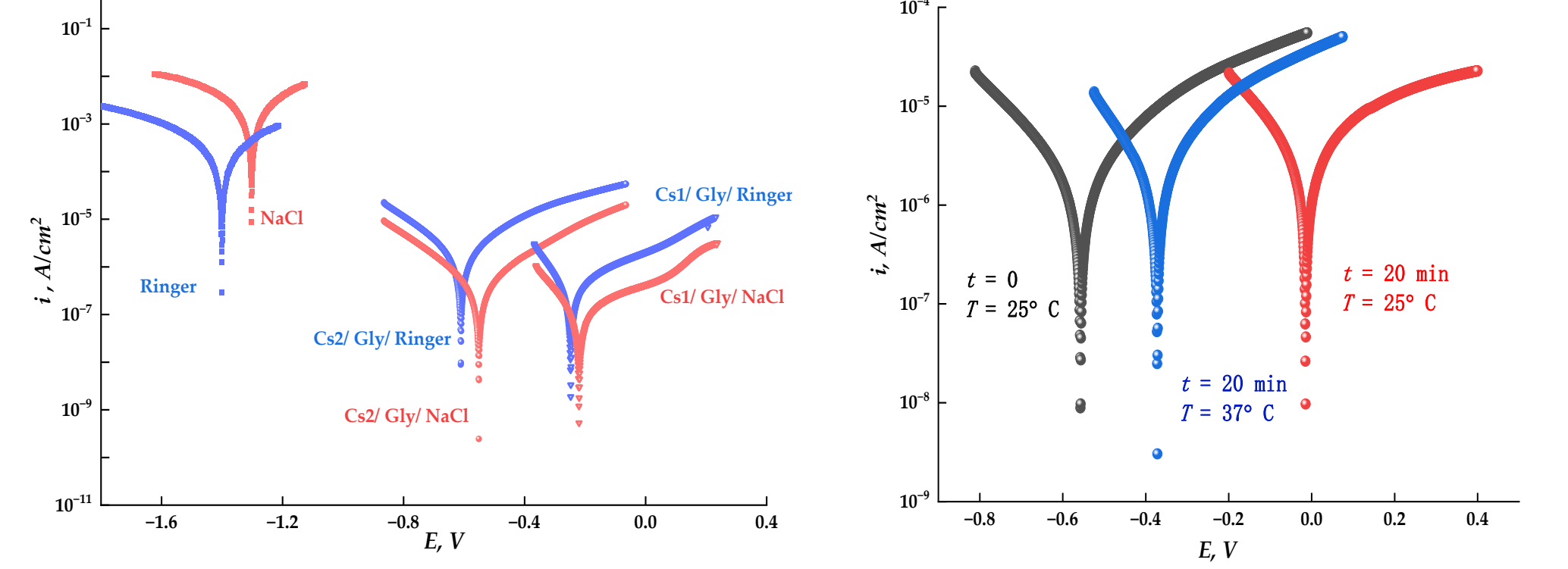


RESULTS & DISCUSSION

THE EVOLUTION OF THE ALLOY SURFACE DURING THE DEGRADATION PROCESS

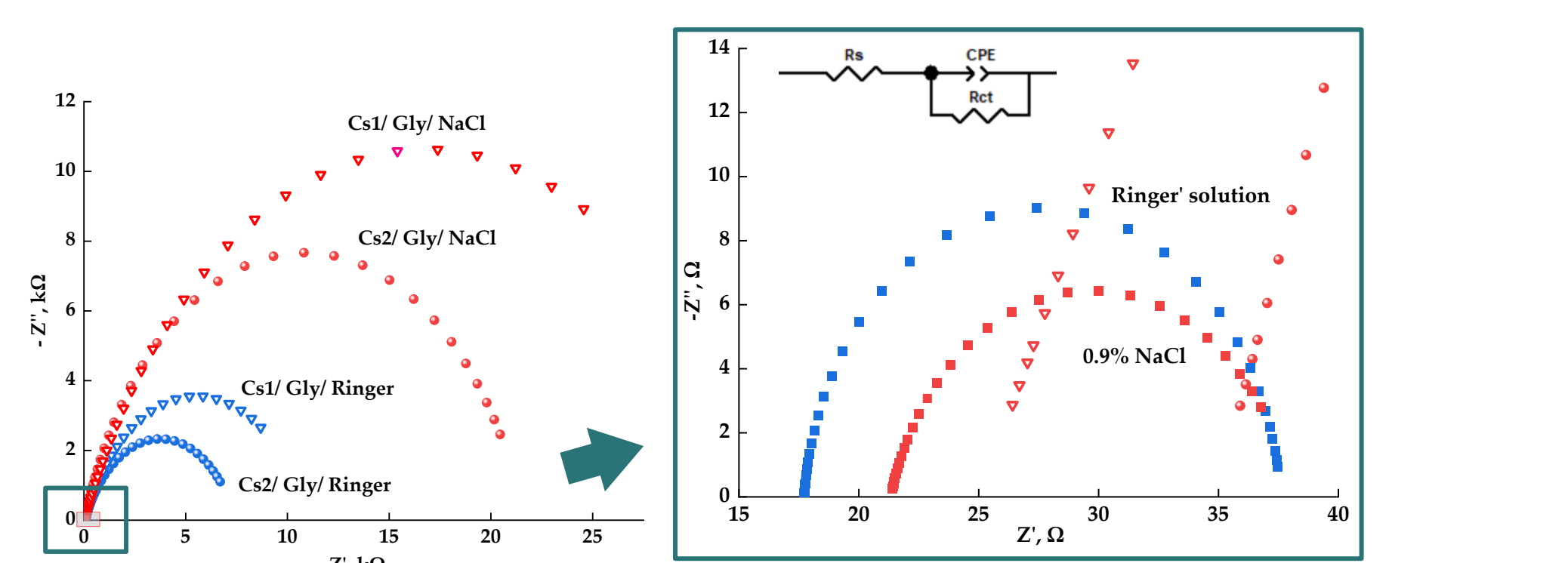


POTENTIODYNAMIC POLARIZATION CURVES



gel	Chitosan	i_{corr} $\mu A/cm^2$	E_{corr} V	v_{corr} mm/a
Chitosan/ glycerin/ Ringer	100stoing	0.455	-0.247	0.010
	protein	2.290	-0.557	0.048
Chitosan/ glycerin/ NaCl	100stoing	0.172	-0.220	0.004
	protein	0.518	-0.551	0.011
Ringer's solution		425.74	-1.401	9.009
0.9% NaCl		11357	-1.303	240.341
Chitosan/ glycerin/ Ringer (protein)	Contact - 0min; 25°C.	2.290	-0.557	0.048
	Contact - 20min; 25°C.	7.337	-0.419	0.155
	Contact - 20min; 37°C.	3.063	-0.372	0.065
[1] AZ31; Subcutaneous area on the back of mice; 21d				0.223
[2] AZ91; Subcutaneous area on the back of mice; 60d				0.56

ELECTROCHEMICAL IMPEDANCE SPECTROSCOPY



gel	Chitosan	R_s Ω	R_{ct} Ω	C_{dl} $\Omega^{-1}S^n$	n
Chitosan/ glycerin/ Ringer	100stoing	66.71	10924	5.01E-5	0.7
	protein	50.49	7424	5.27E-7	0.7
Chitosan/ glycerin/ NaCl	100stoing	25.06	33517	2.01E-5	0.7
	protein	34.91	21632	8.84E-6	0.8
solution		R_s Ω	R_{ct} Ω	C_{dl} $\Omega^{-1}S^n$	n
Ringer's solution		17.71	19.89	70.80	0.9
0.9% NaCl		21.43	15.41	31.80	0.9

CONCLUSION

- The addition of glycerol enhances the elasticity of chitosan gel films, likely due to its molecules insert themselves into the chitosan structure, disrupting its rigid intermolecular hydrogen bonds to increase molecular mobility and thus make the chitosan film more flexible.
- In contact corrosion tests, the surface condition of the alloy after interaction with the gel more closely resembles the in vivo scenario.
- Compared to conventional simulated body fluids, test results using the gel as the background electrolyte align more closely with in vivo data; furthermore, after 20 minutes of contact at room temperature, the assessment results show improved agreement.
- Both the type of chitosan and the composition of the electrolyte solution influence the performance of the gel film in degradation evaluation.

FUTURE WORK / REFERENCES

FUTURE WORK

- The composition of corrosion products was analyzed using XRD and EDS.
- The degradation mechanism of magnesium alloy in gel medium was studied.
- KBr-Chitosan windows were prepared, and the degree of deacetylation of different brands of chitosan was determined using infrared spectroscopy.

REFERENCES

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- Sanchez, A. H. M.; Luthringer, B. J.; Feyerabend, F.; & Willumeit, R. Mg and Mg alloys: how comparable are in vitro and in vivo corrosion rates? A review. *Acta biomaterialia*, **2015**, 13, 16-31. <https://doi.org/10.1016/j.actbio.2014.11.048>