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CUT Czestochowa University
of Technology

Hybrid oxidation of titanium substrates for biomedical applications

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Hybrid oxidation of titanium substrates for biomedical applications

Abstract

Titanium oxidation for biomedical applications is still a challenge in obtaining both good mechanical and physicochemical properties of thin oxide layers as well as the required good adhesion to titanium substrates and of course bioactivity. Interesting techniques for TiO_2 layers formation are electrochemical methods (anodizing), plasma methods (PVD) and diffusive methods (Fluidized Bed FB). Each method aims to create a thin homogenous oxide layer characterized by thermal stability and re-passivation in the presence of body fluid environment. However, an important aspect here is also phase composition of thin oxide layers, essential in the processes of osseointegration. Accordingly research carried out by the Author aims to produce such a titanium substrate, where surface zone is $\text{Ti}_\alpha(\text{O})$ solid solution formed with Fluidized Bed diffusion process (883K, 913K for 6h / 8h) and the outer layer is TiO_2 oxide produced by PVD magnetron sputtering. Effects of such hybrid oxidation on titanium physicochemical properties were investigated with TEM / EFTEM, SIMS, RS and Nanoindentation tests. Results showed that hybrid oxidation made it possible to generate favorable synergetic effect between Fluidized Bed and PVD oxide layers and to reduce the stresses at their interface. In turn, variable share of TiO_2 oxide phases (rutile + anatase mixture) obtained at the titanium surface allowed for the significant enhancement of hydroxyapatite growth which was confirmed by 7 / 14 days Kokubo tests. Hybrid oxidation processes also influenced the decrease in the surface roughness parameters, important for implant materials.

Functionalization of titanium substrates for biomedical applications – state of the art (1)

Thin layers formation: TiO_2 , TiN_xO_y
PVD, CVD, Sol-Gel, PLD (single stage treatments)

Investigation of layers:
Structure, Phase composition etc.



Sputtered titanium oxynitride coatings for endosseous applications:
 Physical and chemical evaluation and first bioactivity assays



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 Maria Cattani-Lorente^b, Rosendo Sanjines^c, Pierre Fontana^d, Anselm Wiskott^b,
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Bioactivity of the layers

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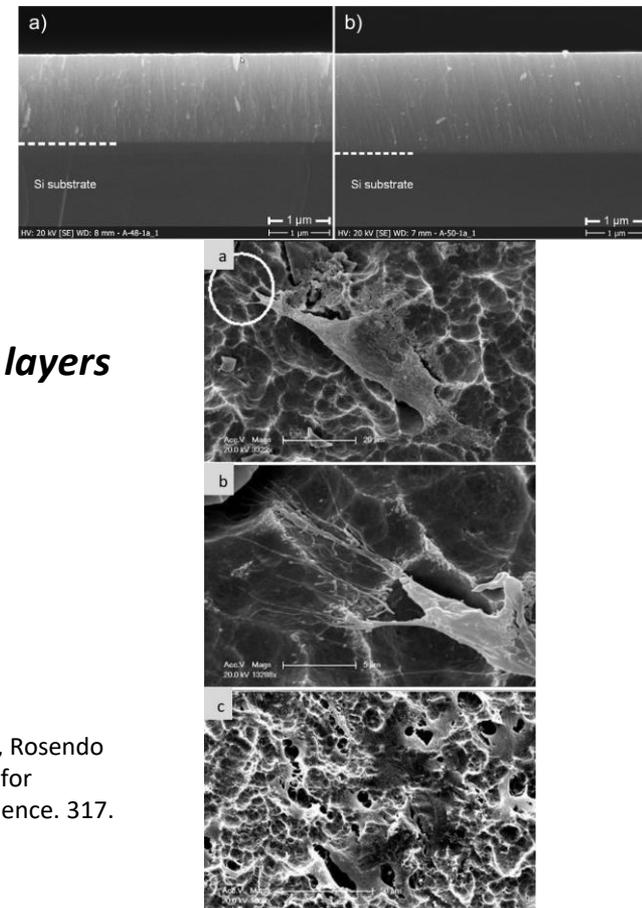
Keywords:
 Titanium oxynitride coating
 Reactive magnetron sputtering
 Bioactivity
 Dental implant

ABSTRACT

Titanium oxynitride coatings (TiN_xO_y) are considered a promising material for applications in dental implantology due to their high corrosion resistance, their biocompatibility and their superior hardness. Using the sputtering technique, TiN_xO_y films with variable chemical compositions can be deposited. These films may then be set to a desired value by varying the process parameters, that is, the oxygen and nitrogen gas flows. To improve the control of the sputtering process with two reactive gases and to achieve a variable and controllable coating composition, the plasma characteristics were monitored *in-situ* by optical emission spectroscopy.

TiN_xO_y films were deposited onto commercially pure (ASTM 67) microroughened titanium plates by reactive magnetron sputtering. The nitrogen gas flow was kept constant while the oxygen gas flow was adjusted for each deposition run to obtain films with different oxygen and nitrogen contents. The physical

Banakh, O & Moussa, Mira & Matthey, Joel & Pontearso, Alessandro & Cattani-Lorente, Maria & Sanjines, Rosendo & Fontana, Pierre & Wiskott, Anselm & Durual, Stéphane. (2014). Sputtered titanium oxynitride coatings for endosseous applications: Physical and chemical evaluation and first bioactivity assays. Applied Surface Science. 317. 986-993



Functionalization of titanium substrates for biomedical applications – state of the art

SBF, In vitro, Cell culture tests of TiO₂ thin layers Functionalization of TiO₂ scaffolds etc.



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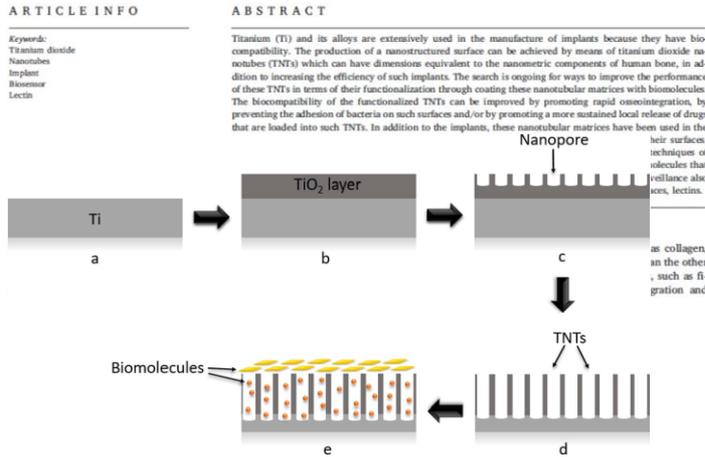
Review

Functionalization of titanium dioxide nanotubes with biomolecules for biomedical applications

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Bioactivation of titanium dioxide scaffolds by ALP-functionalization

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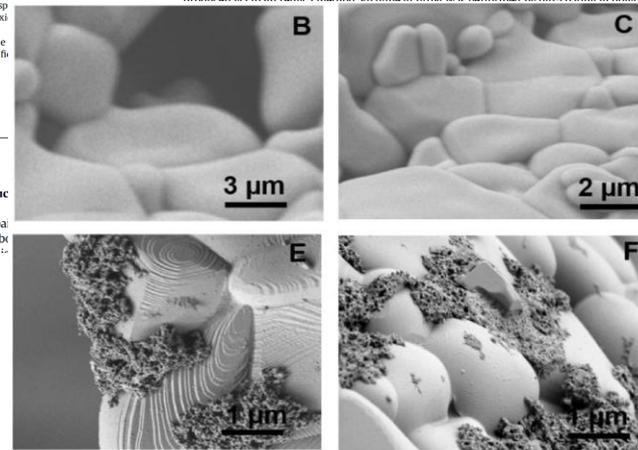
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ABSTRACT

Three dimensional TiO₂ scaffolds are receiving renewed attention for bone tissue engineering (TE) due to their biocompatibility and attractive mechanical properties. However the bioactivity of these scaffolds is comparatively lower than that of bioactive glass or hydroxyapatite (HA) scaffolds. One strategy to improve bioactivity is to functionalize the surface of the scaffolds using biomolecules. Alkaline phosphatase (ALP) was chosen in this study due to its important role in the bone mineralization process. The current study investigated the ALP functionalization of 3D titanium dioxide scaffolds using self-polymerization of dopamine. Robust titanium scaffolds (compressive strength=2.7 ± 0.3 MPa) were produced via a facile method. Enzyme activity was confirmed by histochemical staining in substrate



The SEM images show the morphology of the scaffolds at different magnifications: (B) 3 μm scale bar, (C) 2 μm scale bar, (E) 1 μm scale bar, and (F) 1 μm scale bar. Image (D) shows a cross-section of the scaffold.

1. Introduction

The repair of bone after trauma, fracture, or non-union is a complex process. The repair of bone after trauma, fracture, or non-union is a complex process. The repair of bone after trauma, fracture, or non-union is a complex process.

Sengottuvelan, Abirami & Balasubramanian, Preethi & Will, Julia & Boccaccini, Aldo. (2017). Bioactivation of titanium dioxide scaffolds by ALP-functionalization. Bioactive Materials. 2. 10.1016/j.bioactmat.2017.02.004.

Rahimi, Nazanin & A. Pax, Randolph & MacA. Gray, Evan. (2016). Review of functional titanium oxides. I: TiO₂ and its modifications. Progress in Solid State Chemistry. 44. 10.1016

Hybrid biomaterials – new approach in surface engineering

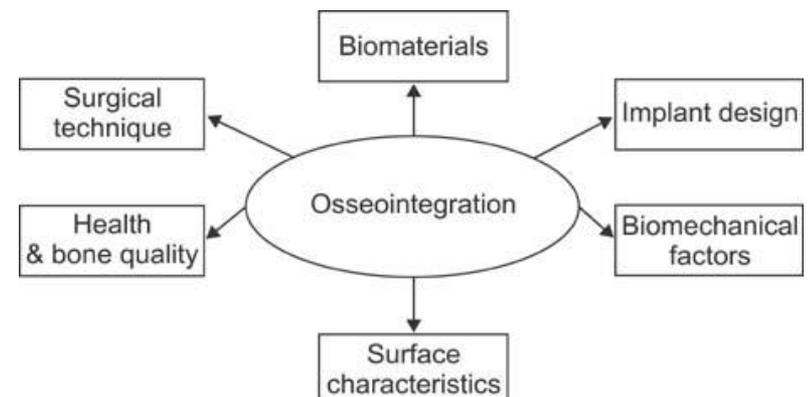
The new trend in biomaterials is to use materials that play an active role in tissue regeneration (bioactive and biodegradable materials) rather than passive and inert materials (biocompatible materials). Such class of hybrid materials has been described as the “Third Generation” biomaterials.

However in hybrid materials problem is more serious when thin layers are applied on surfaces. At the interface between the coating and the substrate considerable forces and stresses can appear that lead to inhomogeneities and cracks in the material.

Therefore to reduce this effect hybrid materials or nanocomposites are mostly formed by PVD, CVD, Sol-Gel methods

Crucial requirements for the biomaterials surfaces:

- ✓ Composition according to the desired end application.
- ✓ Favourable surface morphology
 - low roughness parameters ($R_a < 1$ micron)
- ✓ Low stresses at the substrate / layer interface
- ✓ High bioactivity (i.e. HAp growth at the Surface after 14 days Kokubo test)

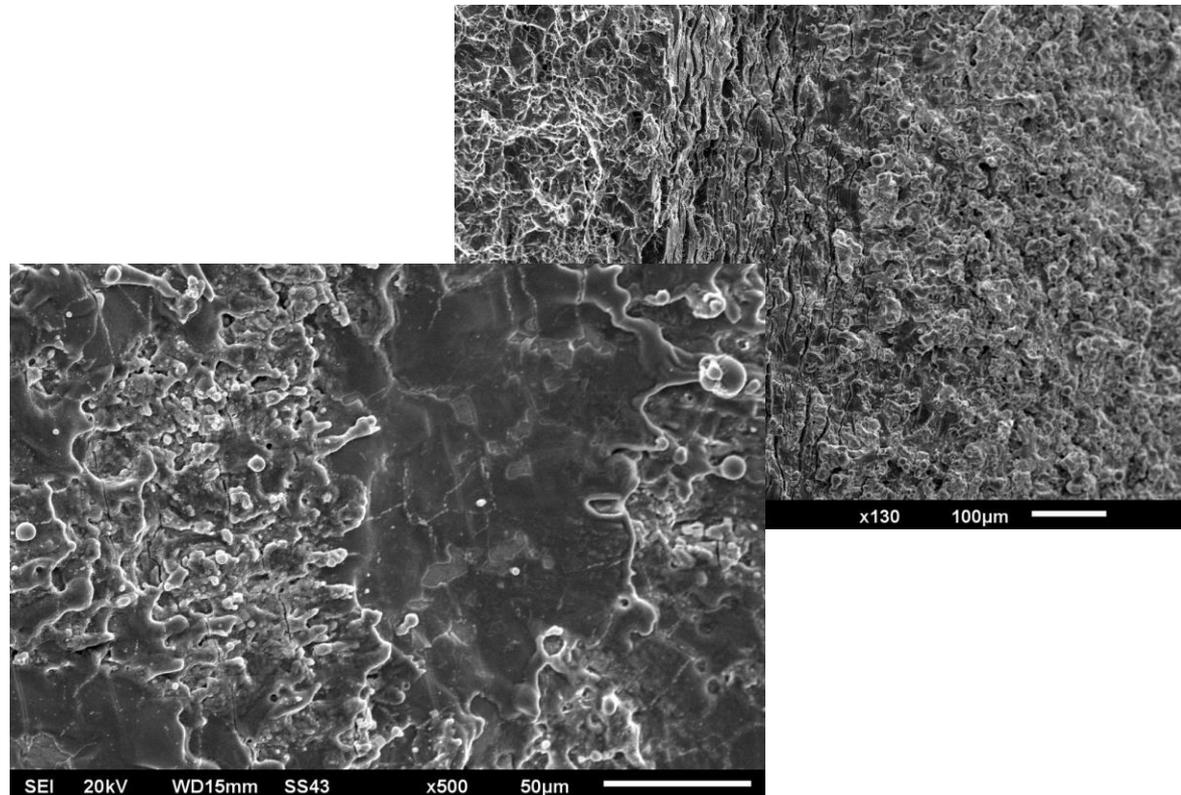
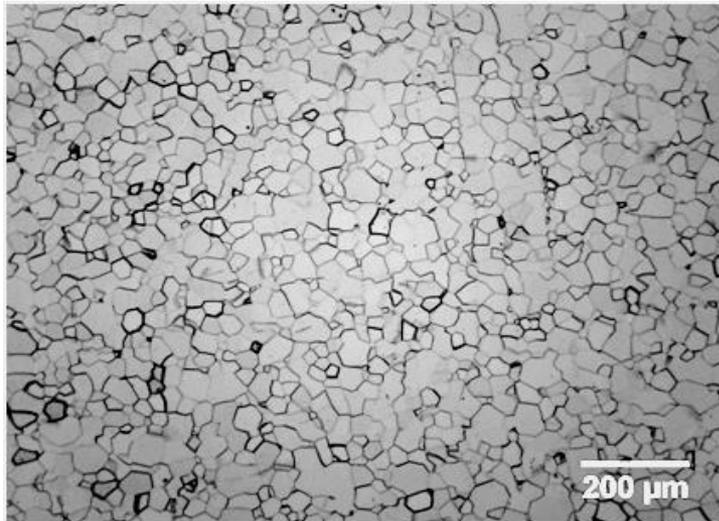


Substrate material analysis – titanium Grade 2

(LM / SEM)

Material	Chemical composition, mass %					
	O	N	C	H	Fe	Ti
Ti 99.2 / Grade 2 Certified by KOBE STEEL LTD	0,20	0,03	0,10	0,015	0,30	Rest

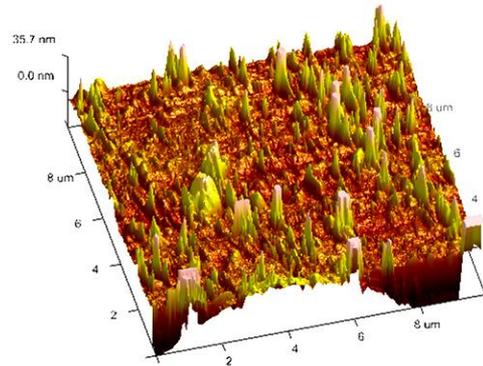
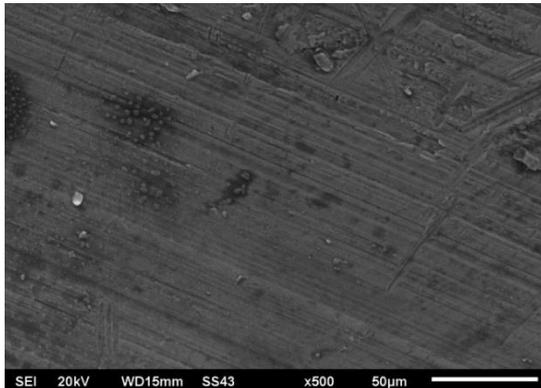
Microstructure: Ti_{α} – LM / SEM image, etched with 96% H_2O + 2% HNO_3 + 2% HF



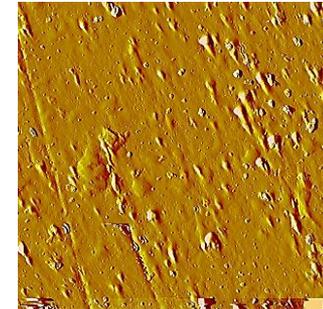
Titanium substrates preparation – SLA surface activation

(SEM / AFM)

1. Mechanical activation / metallographic paper (grit 600 to 2000)



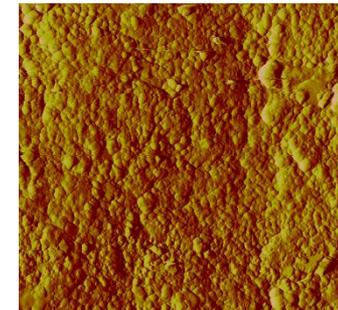
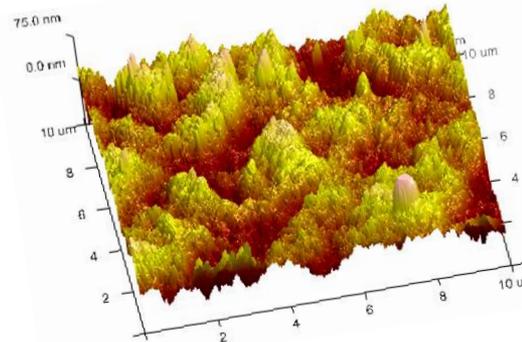
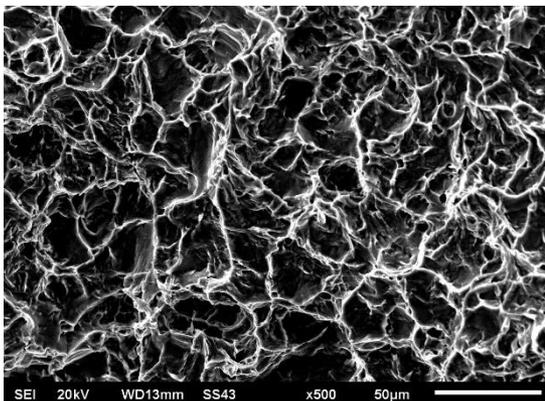
Scan area
AFM 10 x 10 µm



$$R_a = 0,463 \mu\text{m} ; R_q = 0,584 \mu\text{m} ; R_{max} = 0,874 \mu\text{m}$$

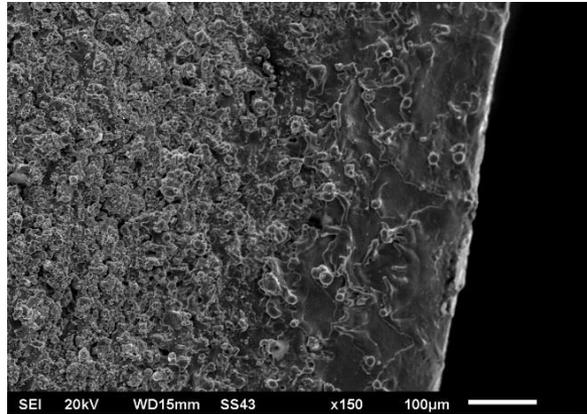
2. Mechano-chemical activation: $Al_2O_3 + NaAl + Si_3O_8 + ZrO_2 + TiO_2 + H_2SO_4$ 90°C / HCl 60°C

(Sand blasted, Large-grit, Acid etched – SLA)

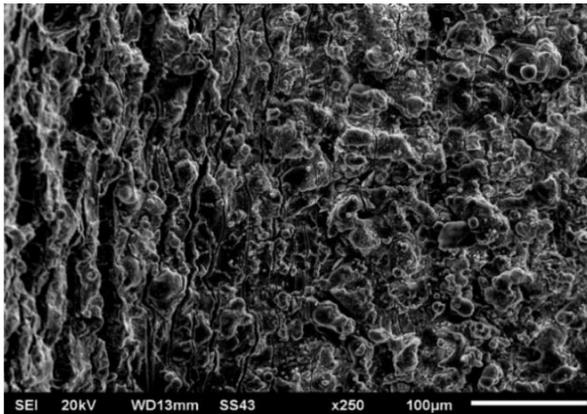
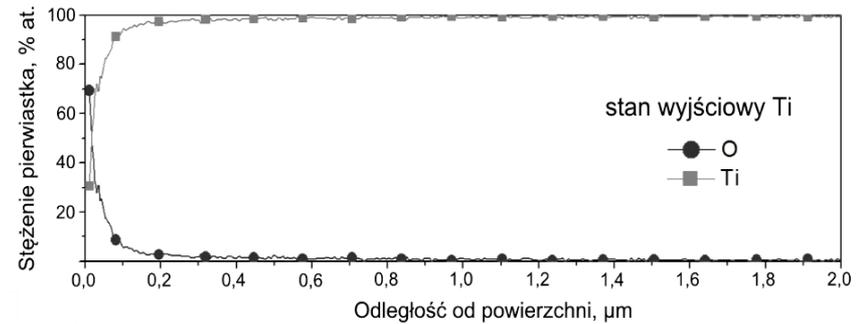


$$R_a = 0,937 \mu\text{m} ; R_q = 1,126 \mu\text{m} ; R_{max} = 1,386 \mu\text{m}$$

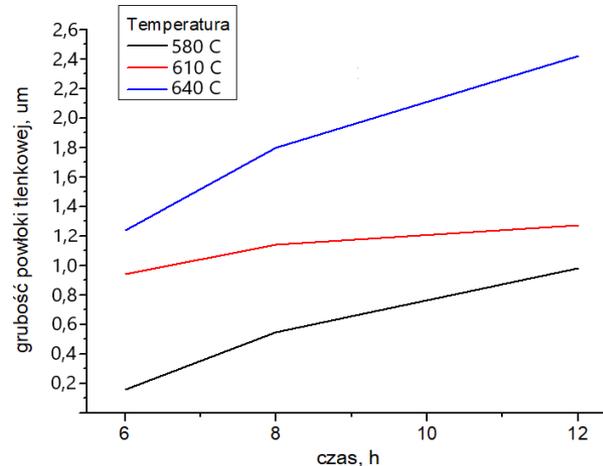
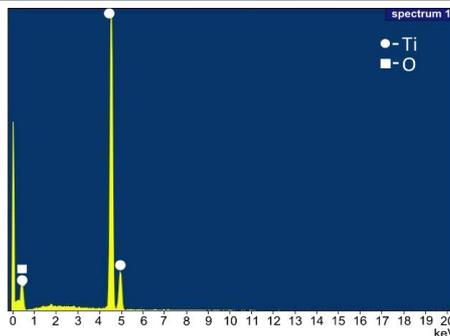
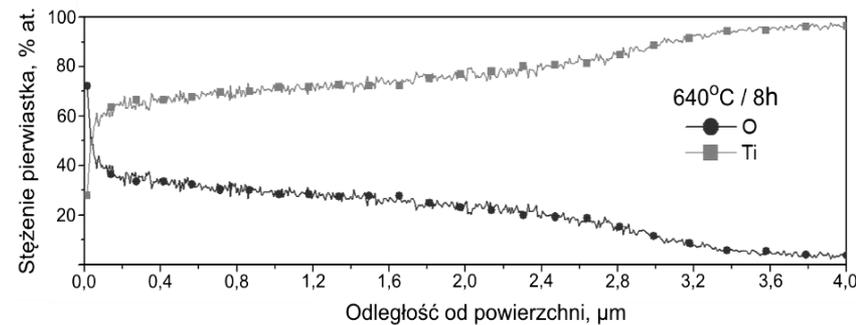
Diffusive oxidation (FADT) – surface layer analysis (SEM-EDX / GDEOS / HK)



Ti_α(O) diffusive layer
9.0 – 12.0 µm



nano-porous TiO₂ layer
1.6 – 1.9 µm

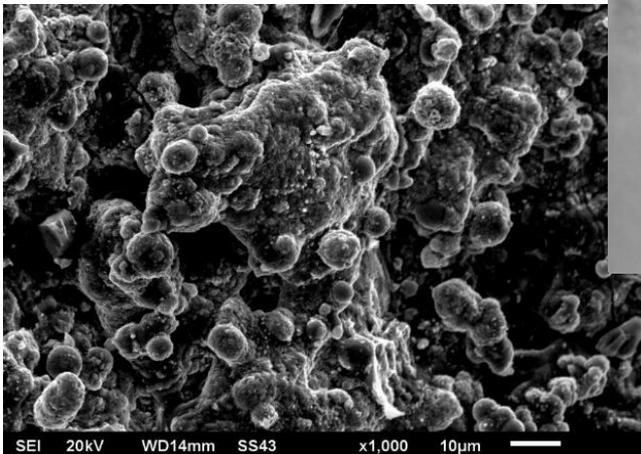
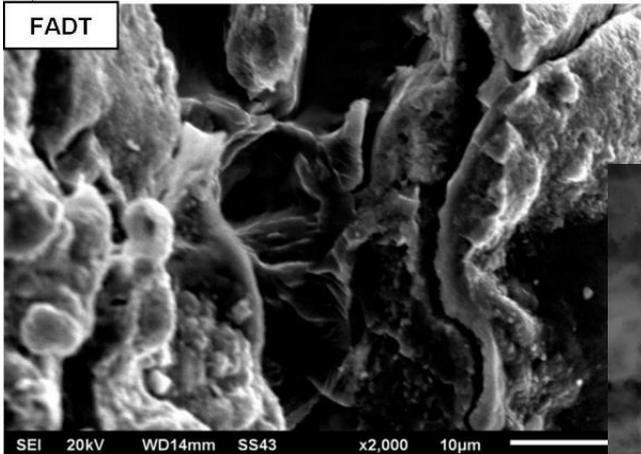


**Ti substrates selected
for hybrid oxidation**

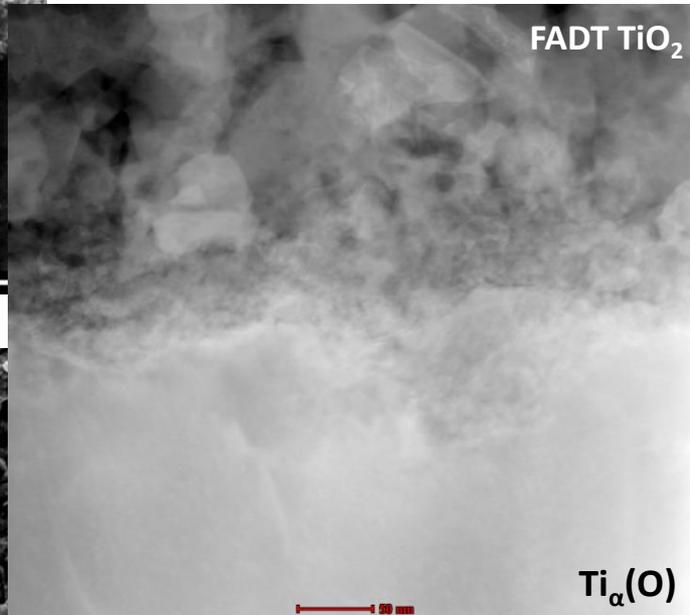
T = 640°C / 8 h
 $h_{\text{Ti}\alpha(\text{O})} = 9.0 - 11.0 \mu\text{m}$
 $h_{\text{TiO}_2} = 1.6 - 1.9 \mu\text{m}$
 H = 455 HK_{0.01}

Diffusive oxidation FADT – nano-porous TiO_2 layer analysis (SEM / STEM / RS)

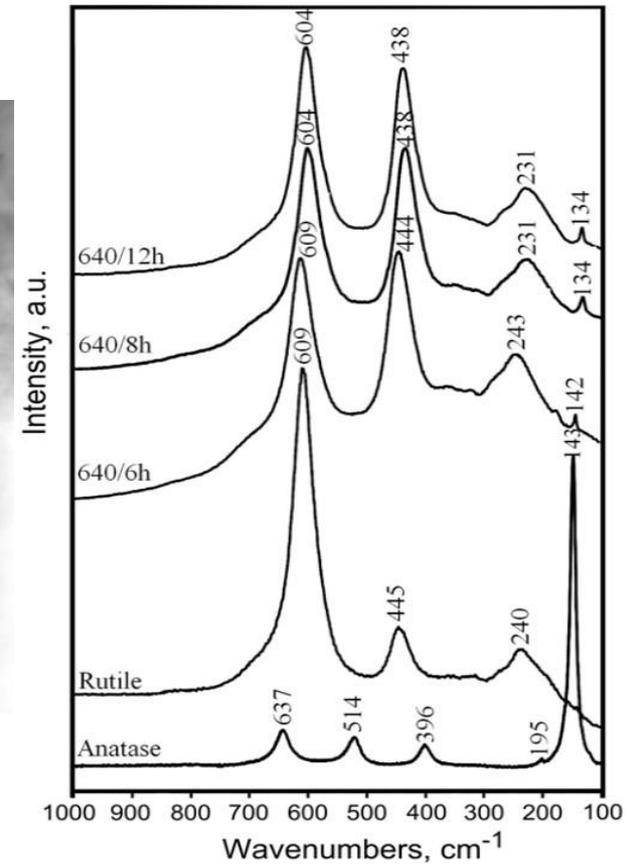
SEM



STEM



RS



Hybrid oxidation parameters

FADT+PVD TiO₂

PVD Magnetron sputtering

Process parameters

I. Stage: vacuum – 1×10^{-4} Pa

II. Stage: sputtering

Pressure: 3 Pa

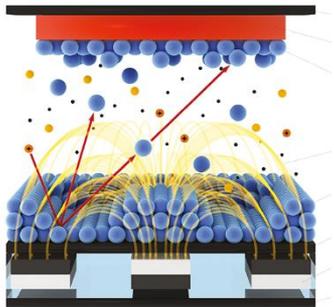
Power: 400 W

Atmosphere: 100% Ar

Target material: TiO₂

Sample – target distance: 55 mm

Process time: 20 min



visual-science.com

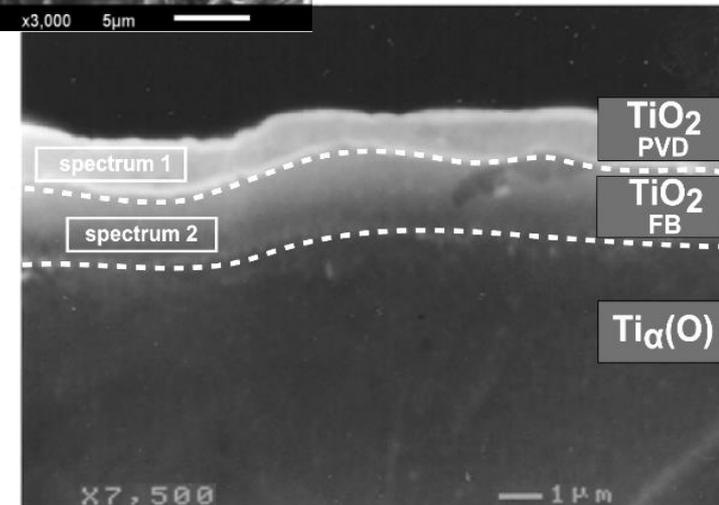
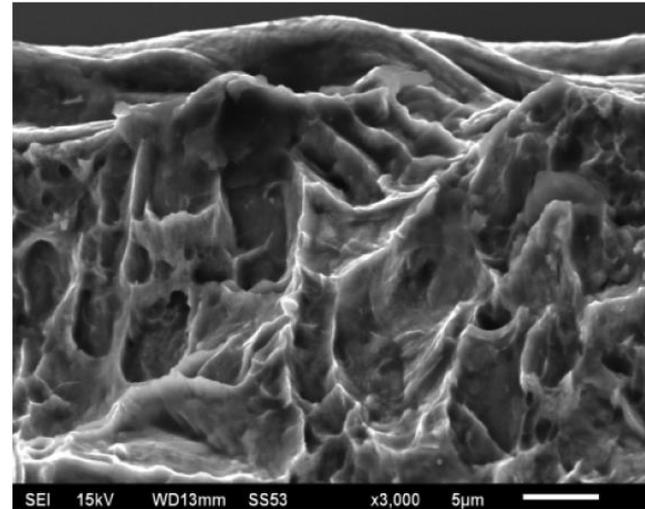


Patent application
no Pat-24/05/07/12,

Chemical heat treatment solution
of metallic alloys,

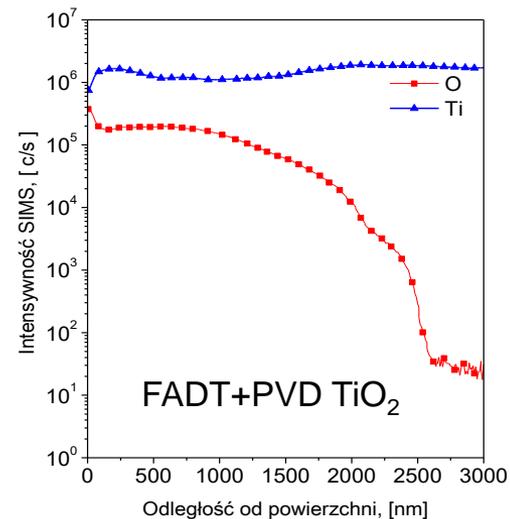
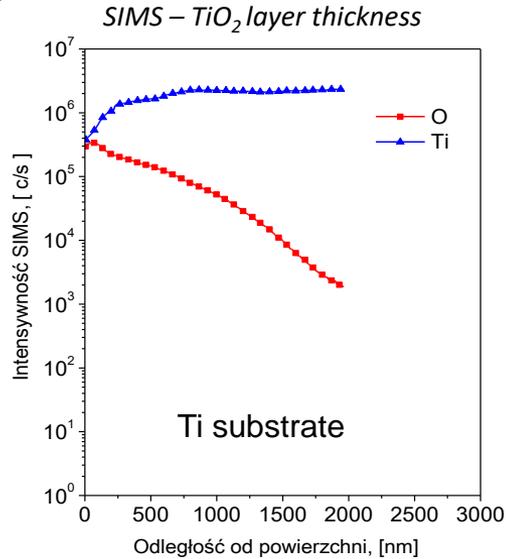
J.J.Jasiński P.Podsiad, J.Jasiński,

Microstructure FADT + PVD (SEM)

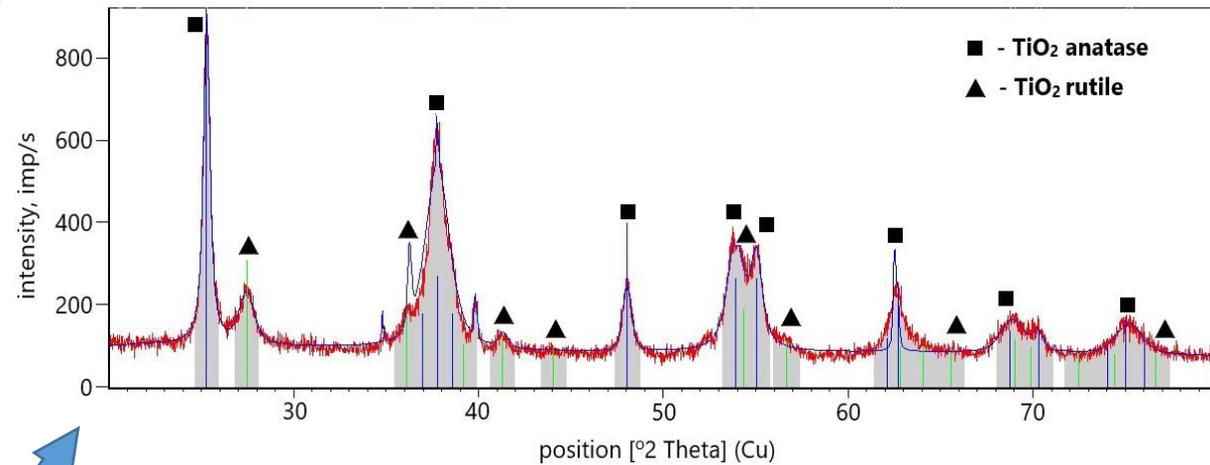


Hybrid oxidation – TiO₂ layers phase analysis

(SIMS / GID-XRD)



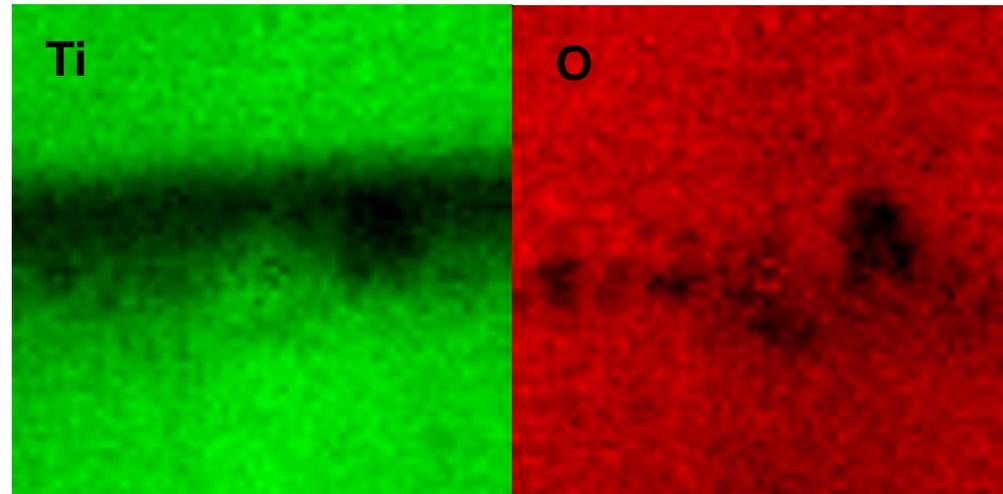
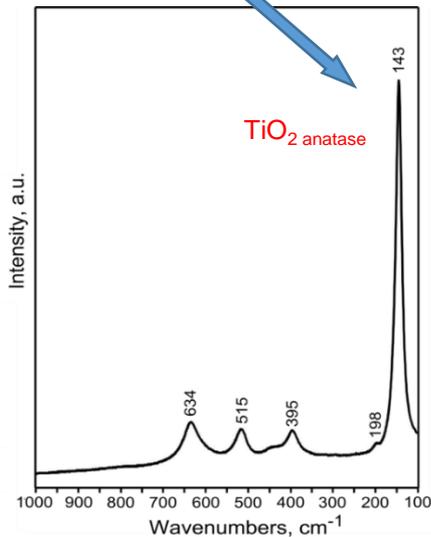
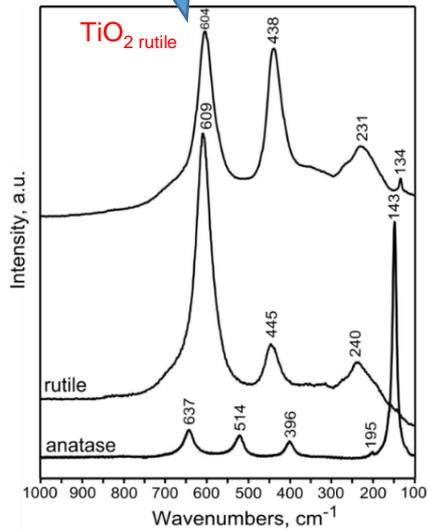
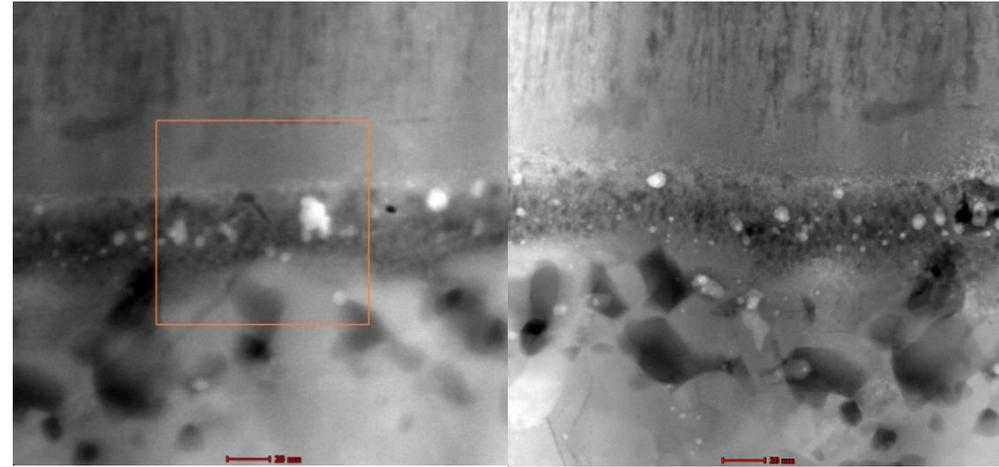
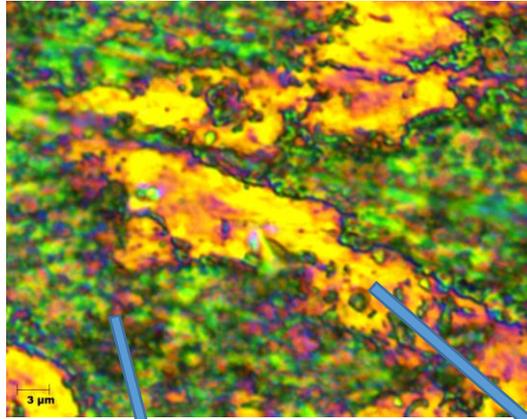
GID-XRD phase analysis of FADT + PVD TiO₂



GID-XRD measurements: Cu anode / 2θ = 20°÷80° / Ω = 1° st. 0.02, time 2.4 s/step

Hybrid oxidation – TiO₂ layers phase analysis

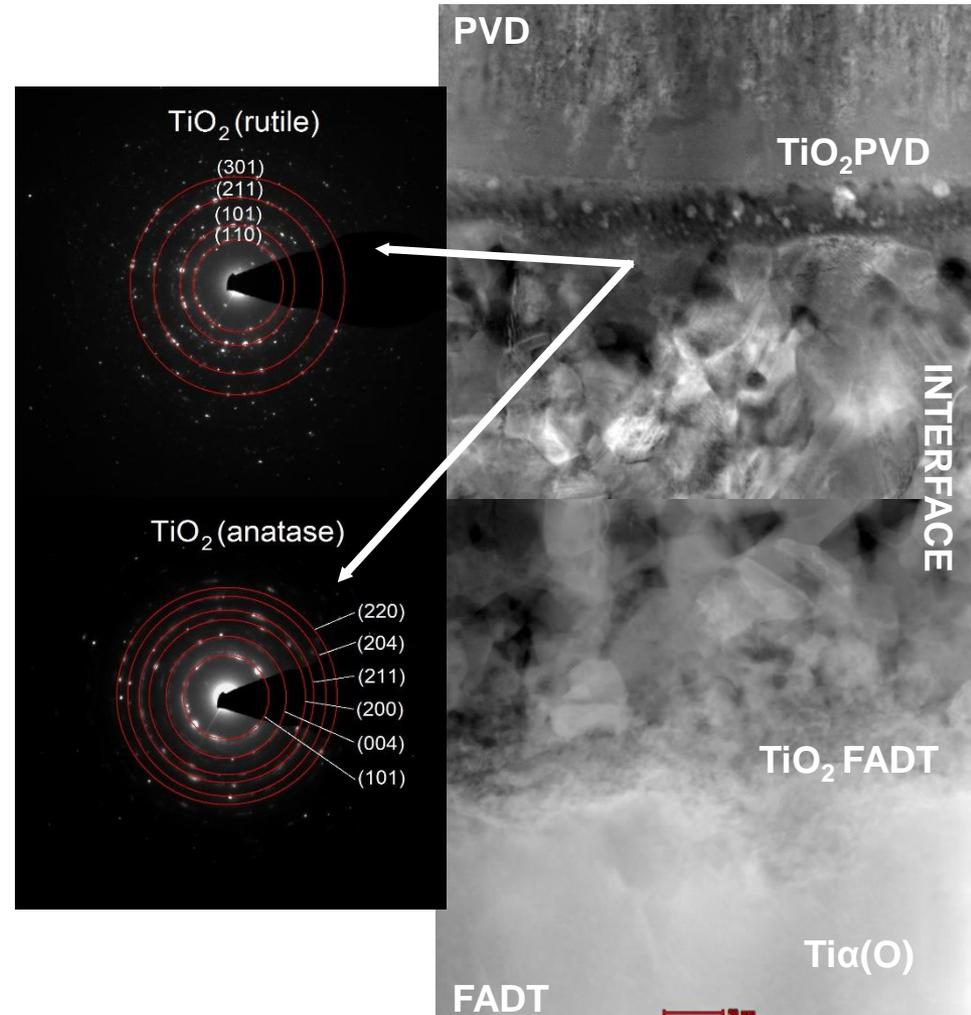
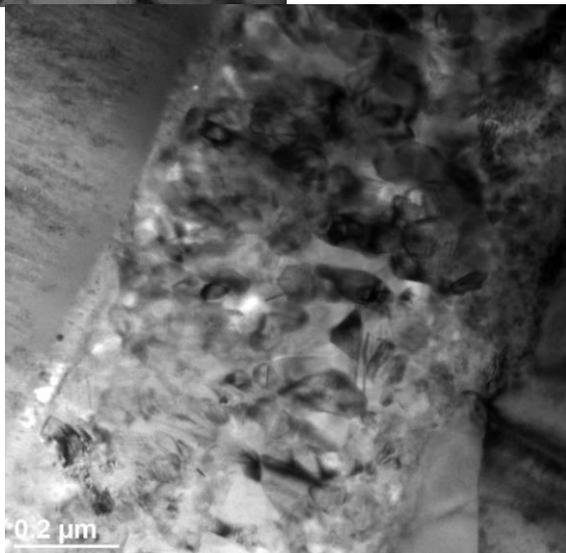
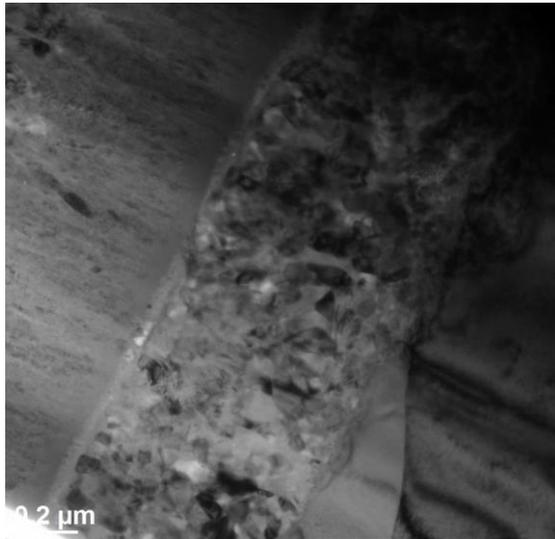
(CLSM / RS / EFTEM MAPS)



Hybrid oxidation – FADT TiO_2 / PVD TiO_2 interface analysis

(STEM)

TEM Microscope S/TEM FEI Titan 80-300

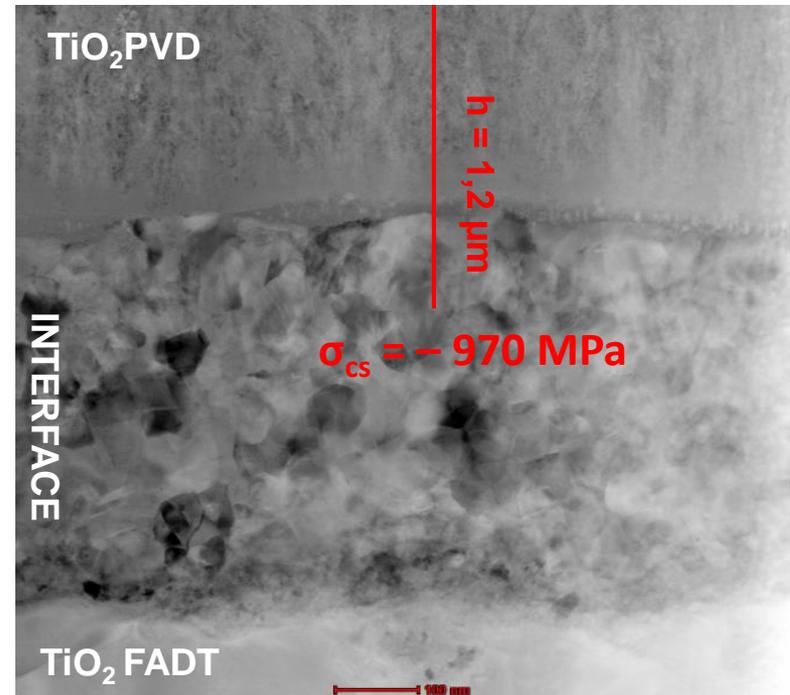
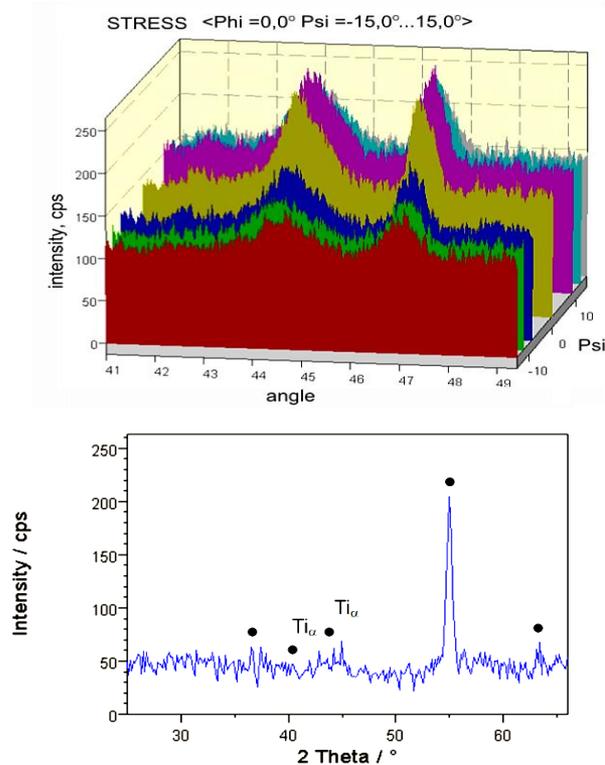


Hybrid oxidation – FADT TiO₂ / PVD TiO₂ interface analysis (Stresses, sin²Ψ)

Seifert 3003TT, Bragg-Brentano geometry, K_αCo=0,17902 nm. Database Rayflex i PDF4+
sin²Ψ method, (101) reflex, 2Θ = 46,99°.

3 symmetrical Ψ angle rotation.

E=112 GPa i v=0,33, reflex maximum analysis (Parabola Fit).

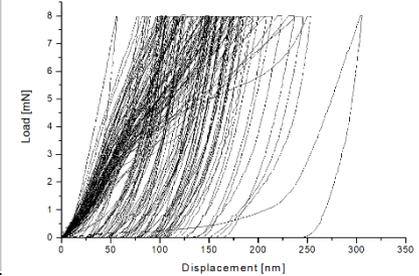
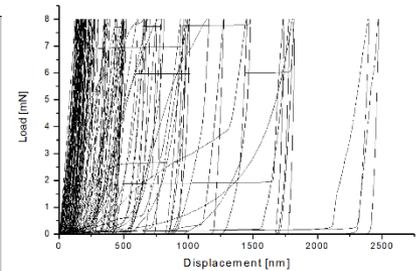
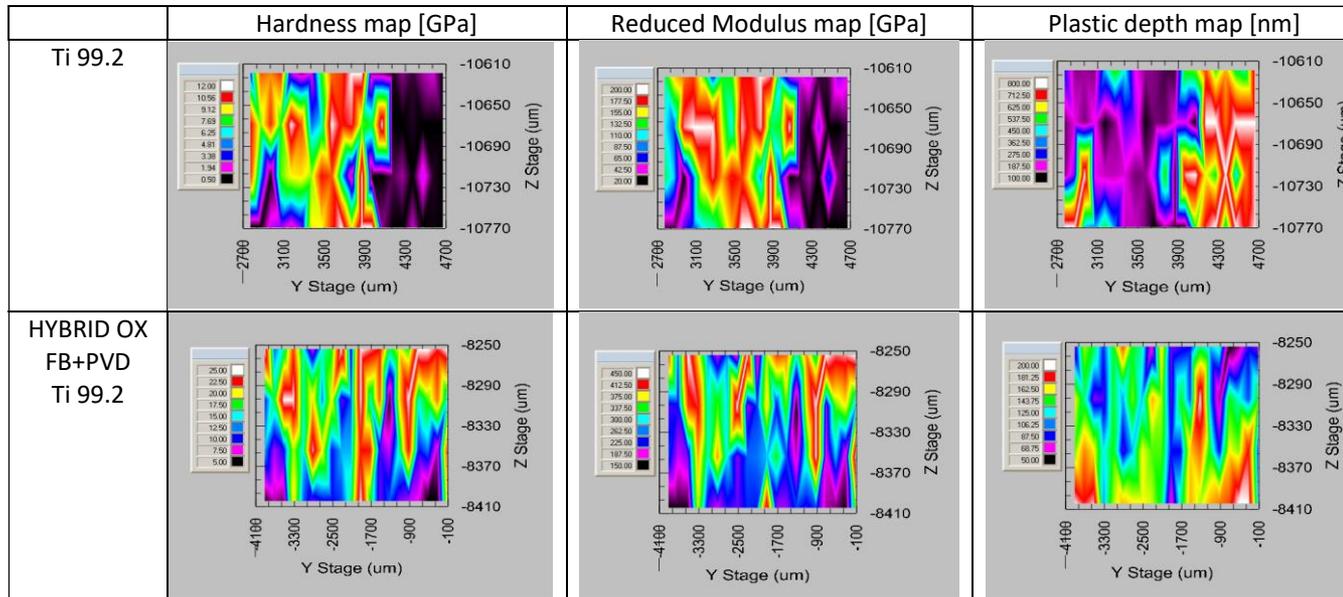


Stresses at the FADT TiO₂ / PVD TiO₂ interface, h = 1.2 μm, σ = - 970 MPa

Hybrid oxidation – TiO₂ layer mechanical tests

(Nanoindentation)

MICROMATERIALS LTD. NANOTEST VANTAGE



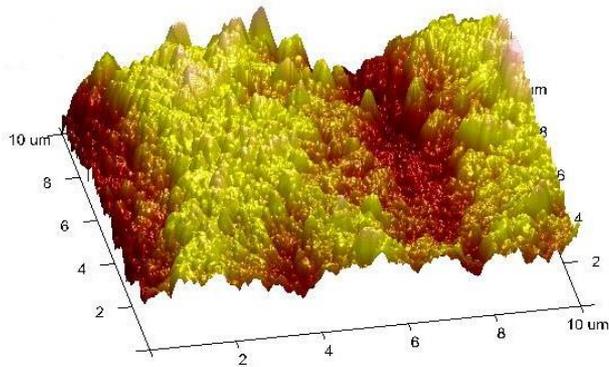
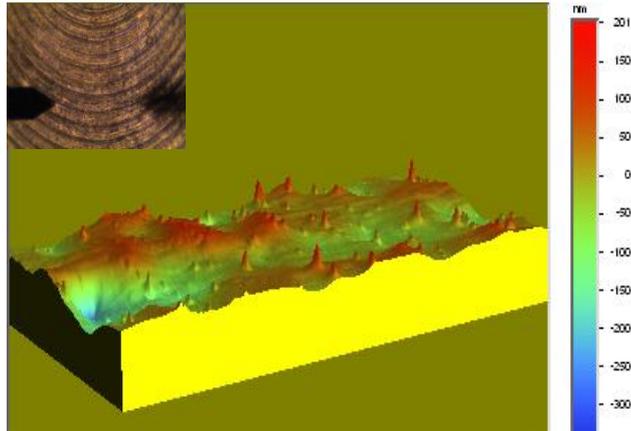
	Sample name	H, Hardness [GPa]	St. Deviation	E _R , Reduced Young modulus [GPa]	St. Deviation	E, Calculated Young Modulus [GPa]	St. Deviation	Maximum depth [nm]	St. Deviation	Plastic depth [nm]	St. Deviation
1.	Ti99.2 – TiO ₂	9.33	4.14	160.00	60.30	148.34	55.91	204.08	57.41	167.17	54.36
2.	Ti99.2 FADT+PVD TiO ₂	15.21	6.04	281.83	87.79	261.28	81.39	144.90	28.87	119.20	27.37

Poisson's ratio $\nu_{Ti} = 0.33$

Hybrid oxidation – surface morphology

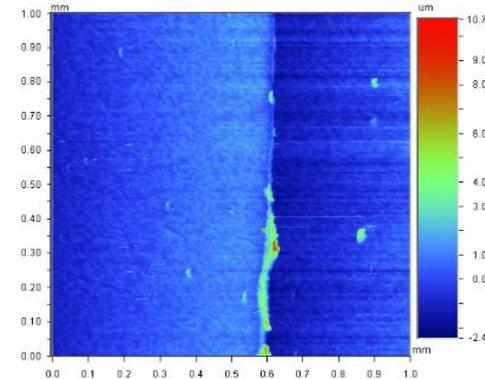
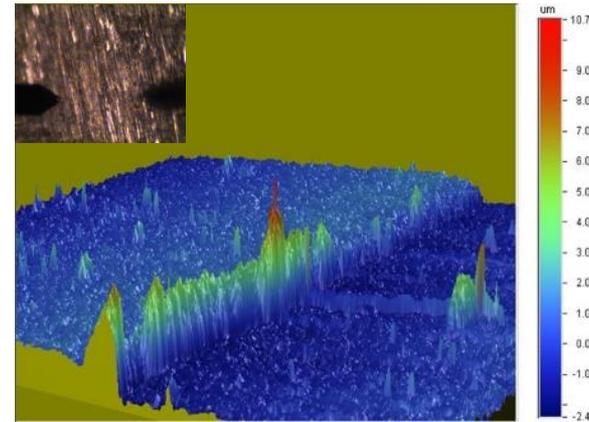
(AFM)

FADT



	Surface roughness [μm]
Ra	1.384
Rq	1.702

FADT+PVD TiO₂



	Surface roughness [μm]
Ra	0.741
Rq	0.922

Bioactivity tests of Ti substrates after hybrid treatment (Kokubo test, 14 days)

„A bioactive material is defined as a material on which bone-like hydroxyapatite (HAp) forms selectively when it is immersed in a serum-like solution SBF (i.e. a material that accelerates heterogeneous HAp crystallization on its surface in a solution supersaturated towards HAp)”.

Tadashi Kokubo, (2006)

Ion	Ion concentrations [mM]			
	c-SBF2	c-SBF3	SBF-JL1	SBF-JL2
Na ⁺	142.00	142.00	142.00	142.00
K ⁺	5.00	5.00		
Mg ²⁺	1.50	1.50		
Ca ²⁺	2.50	2.50	2.50	2.31
HCO ₃ ⁻	4.20	35.23	34.90	34.88
HPO ₄ ²⁻	1.00	1.00	1.00	1.39
SO ₄ ²⁻	0.50	0.50		
Cl ⁻	147.96	117.62	111.00	109.90

c-SBF2 bioactivity test parameters

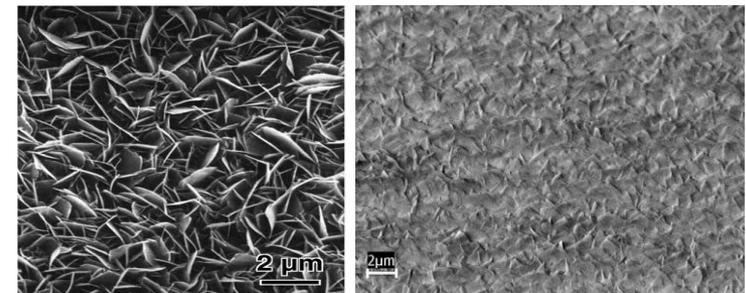
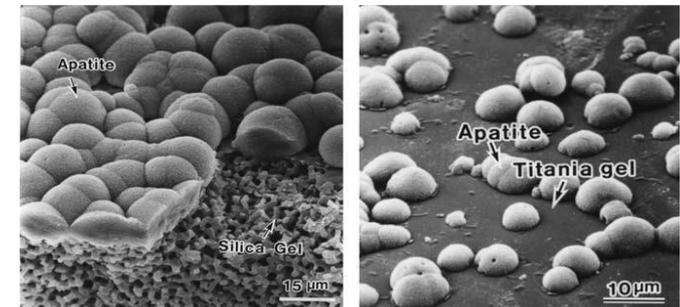
Ionic strength = 140 mM,

C₀ Ca²⁺ = 2.5 mM,

pH = 7.4,

Temperature = 37°C,

CO₂ partial pressure = 0.05 atm

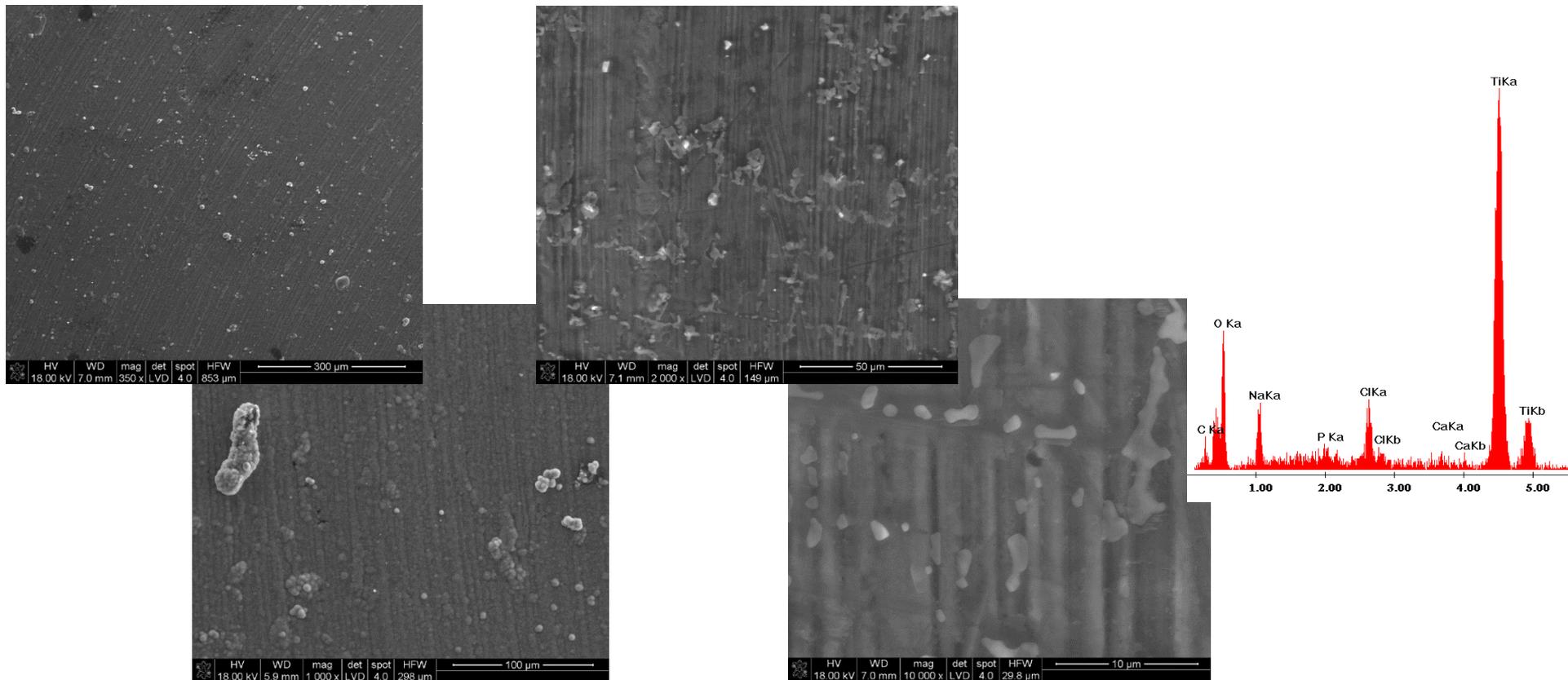


T. Kokubo et al.: How useful is SBF in predicting in vivo bone bioactivity, *Biomaterials* vol. 27, 2006, pg. 2907–15

T. Kokubo, H.M. Kim, M. Kawashita, T. Nakamura, *Bioactive metals: preparation and properties*, *Journal of Materials Science: Materials in Medicine* Vol. 15, 2004, pg. 99-107

Bioactivity tests of Ti substrates after FADT treatment (Kokubo test, 14 days)

Ti substrates after FADT – nano-porous TiO_2 rutile

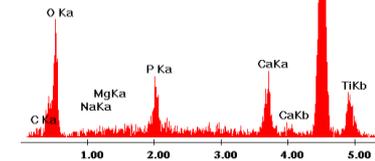
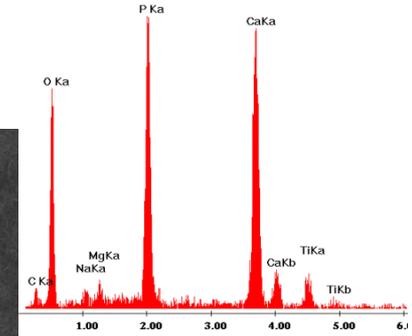
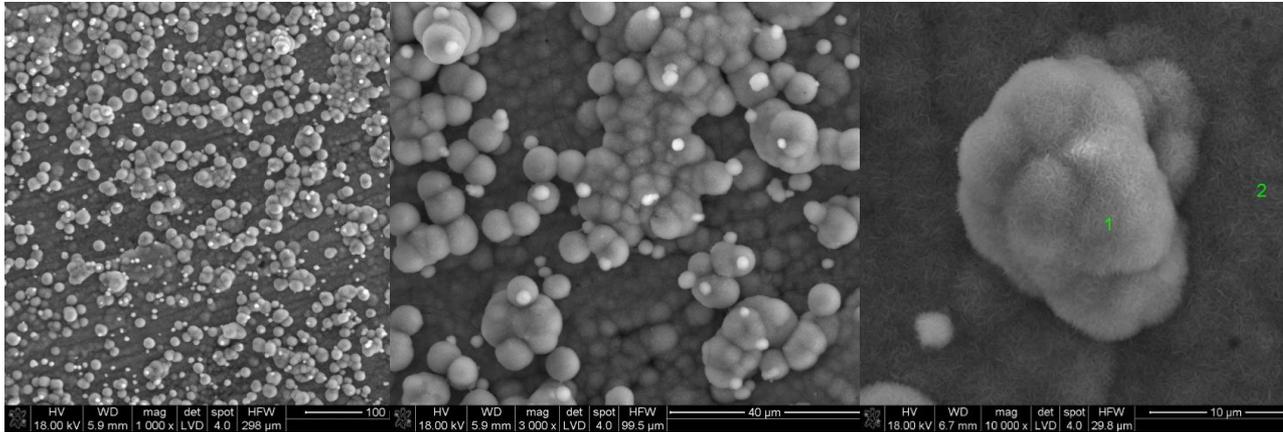


„On the microscopic level, the heterogeneous crystallization of HAp on existing surfaces is a process that involves electrostatic interactions of the surface with the calcium and the phosphate ions in SBF via sequential formation of metastable intermediates (i.e. Ca-rich and Ca-deficient phases of amorphous calcium phosphate, ACP)”

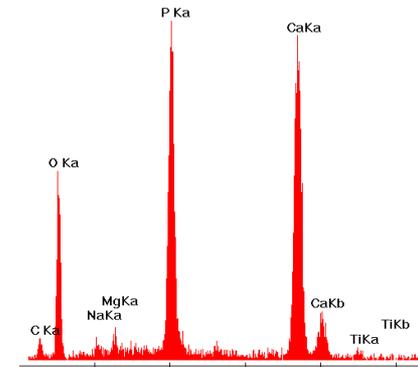
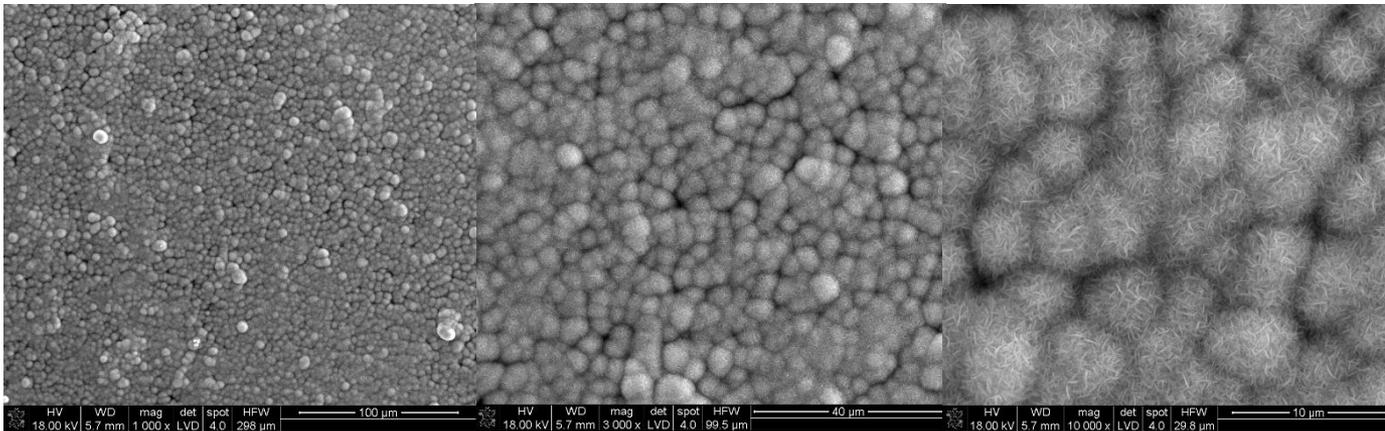
Bioactivity tests of Ti substrates after hybrid treatment (Kokubo test, 14 days)

Ti substrates after hybrid oxidation FADT+PVD TiO₂ rutile/anatase

7 days



14 days



Conclusions

- 1. The modification of titanium substrates by oxidation in a fluidized bed (FADT) leads to formation of a highly defected diffusion zone ($Ti_{\alpha}(O)$ solid solution) and the nanoporous TiO_2 which plays a role of foundation for a subsequent deposition of TiO_2 thin oxide layer by PVD magnetron sputtering.*
- 2. Titanium hybrid oxidation leads to smoothing the surface as a result of the formation of a homogeneous TiO_2 PVD top layer. This is especially important in the subsequent intensified growth of globular form hydroxyapatite compounds.*
- 3. In hybrid oxidation, the interface between porous TiO_2 and PVD TiO_2 with a favorable state of stress has an influence on the formation of a highly bioactive top surface oxide layer with a phase composition of rutile and anatase mixture.*
- 4. Hybrid oxidation process has a significant impact on HAp growth in the first stage of vascularization of the tissues at the bioactive implant surface and finally improves the rate of osseointegration.*

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THANK YOU FOR YOUR ATTENTION

Questions ?

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