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Synthesis and characterization of Gefitinib and Paclitaxel dual drug loaded Cockle shell (*Anadara granosa*) derived Calcium carbonate nanoparticles

Presented by

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nanomaterials



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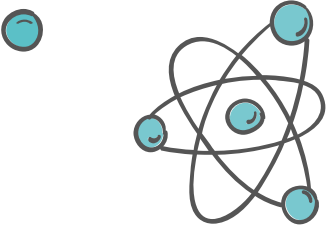
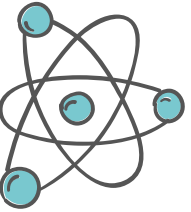
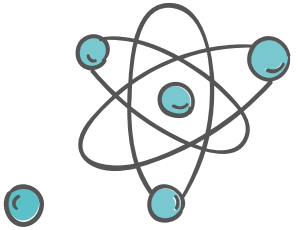
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Outline

Introduction
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Introduction



Nanomedicine –
future of
medicine

Nanoparticles – effective
drug delivery system as
they possess higher
surface area to volume
ratio (Din et al., 2017)

Cockle shells-
(*Anadara granosa*)-
source of Calcium
carbonate (**Aragonite**
polymorph)

Nano vectors
– Targeted
drug loaded
nano
materials

**Dual-drug loaded
system**

Distribution of blood cockle shells



Atlantic Ocean

Pacific Ocean

Indian Ocean

Indian Ocean

(FAO, n.d.)

Sustainable source of CaCO_3

Aragonite polymorph-
biocompatible, safe, pure (Kamba *et al.*, 2013; Hammadi *et al.*, 2017; Danmaigoro *et al.*, 2017)

pH dependent drug release
(Hammadi *et al.*, 2017; Danmaigoro *et al.*, 2017)

Cockle shell derived aragonite calcium carbonate nanoparticles (CSCaCO₃NP)

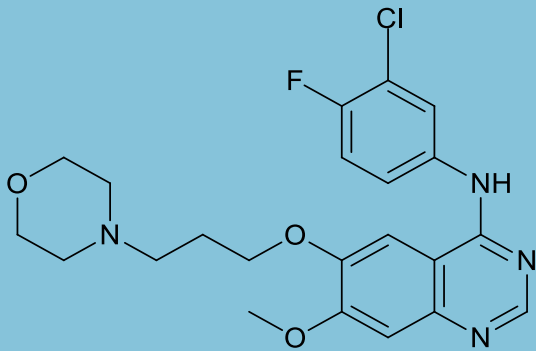


For delivering hormonal agents (Jaji *et al.*, 2017)

For delivering chemotherapeutic agents (Danmaigoro *et al.*, 2017; Ibiyeye *et al.*, 2020)

To deliver anti-bacterial agents (Saidykhani *et al.*, 2016; Idris *et al.*, 2019)

Iressa (Gefitinib, ZD 1839)



Small molecule EGFR-TKI
Reversible competitive inhibitor of EGFR tyrosine kinase (*Ward et al., 1994*)

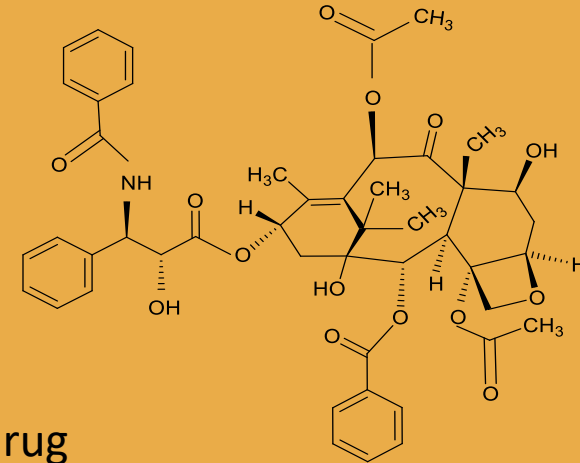
447 kD

FDA approved

-NSCL

NO approved
drugs

Paclitaxel



Cytotoxic drug

Promotor of tubulin polymerization and stabilizes microtubules to depolymerization (*Nikolic et al., 2011*)

853.89kD

FDA approved -* **Node positive breast cancer + adjuvant therapy, Metastatic BC**

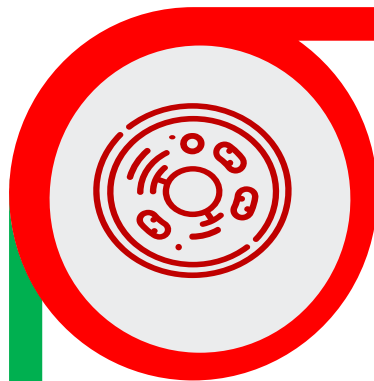
-Kaposi sarcoma

-NSCL

-Ovarian cancer

Abraxane, 2005

Size, PDI, shape, Surface chemistry,



Drug loading and encapsulation efficiency



**LONG TERM STABILITY/
BIOLOGICAL EFFECTS OF
NANOPARTICLES**

**Chemical composition,
bonding and in vitro drug
release kinetics**



Impurities present



(Hosokawa et al., 2007)

Materials



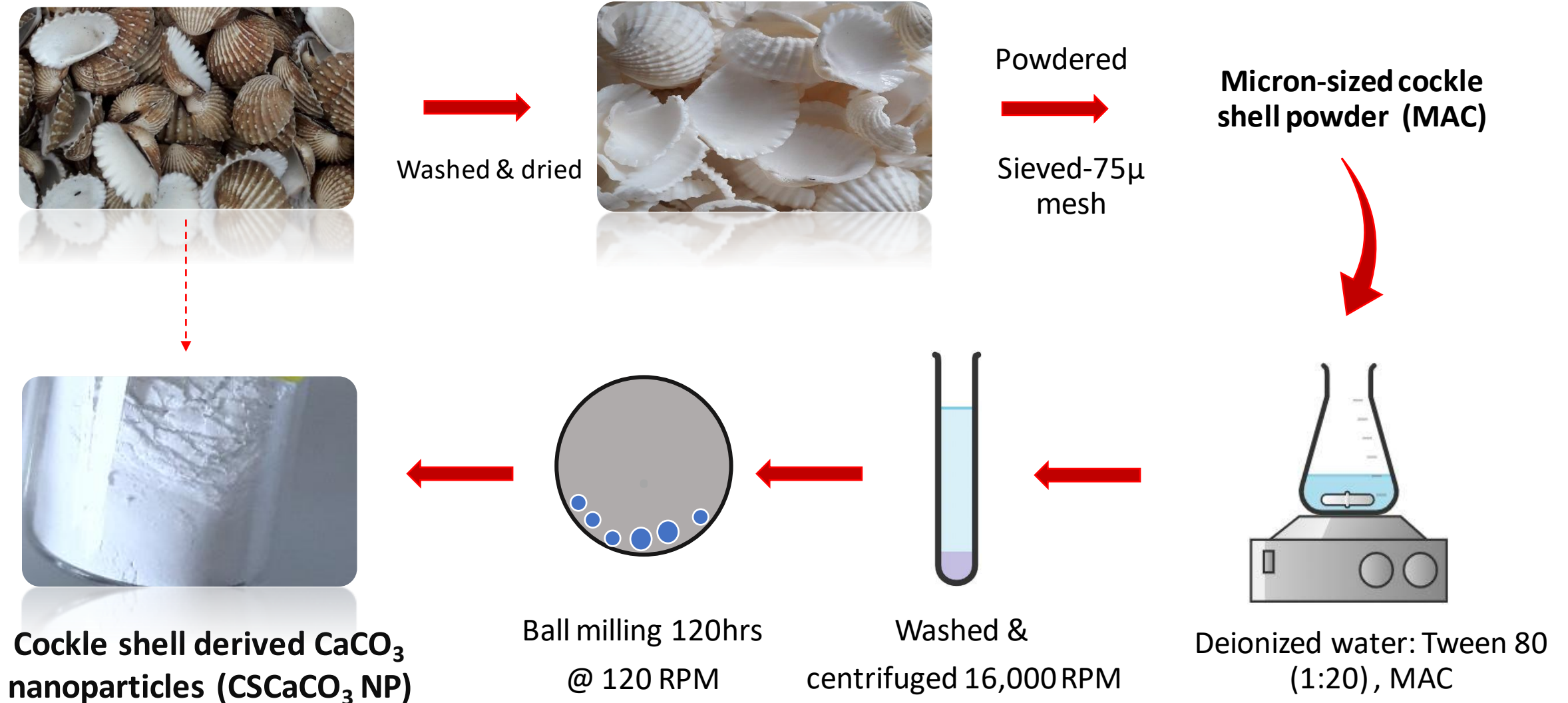
- **GEF and PTXL** (Gold Biotechnology, St. Louis, MO)
- **DMSO** (Fisher Scientific U.K)
- **Tween 80** (R & M marketing, U K)
- **Cockle shells** (local market in Serdang, Malaysia)
- **Deionized water** Milli-Q integral Water Purification System(Millipore Sigma, USA)
- **Double beam UV-VIS spectrophotometer** (Shimadzu 1650PC)
- **High speed centrifuge** (Optima XPN, Beckman Coulter instruments Inc., CA, USA)
- **Magnetic stirrer** (Dhaihan WiseStir® Systematic Multi-Hotplate Stirrer, South Korea)
- **Hot air oven** (Memmert UM500, GmbH Co, Germany)
- **Programmable ball miller** (BML-6", Diahan scientific®, Korea)
- **Transmission Electron Microscope**(HRTEM, JOEL JEM-2100F, Japan)
- **Field emission scanning electron microscope** (Nova Nanosem 230, Japan)
- **Carbon-coated copper grid** (Sigma- Aldrich, St. Louis, MO, USA)
- **Zetasizer Nano ZS** (Ver.7.2; Malvern Instruments Ltd., Malvern, UK)
- **XRD** (Shimadzu XRD- 6000 powder diffractometer)
- **FT-IR** (Model spectrum 100; Perkin Elmer, USA)
- **Micromeritics** (Tristar II Plus, USA).

Methods

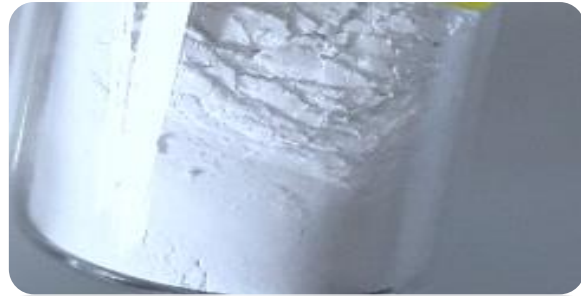


A. Synthesis of CSCaCO_3 NP and GEF-PTXL- CSCaCO_3 NP

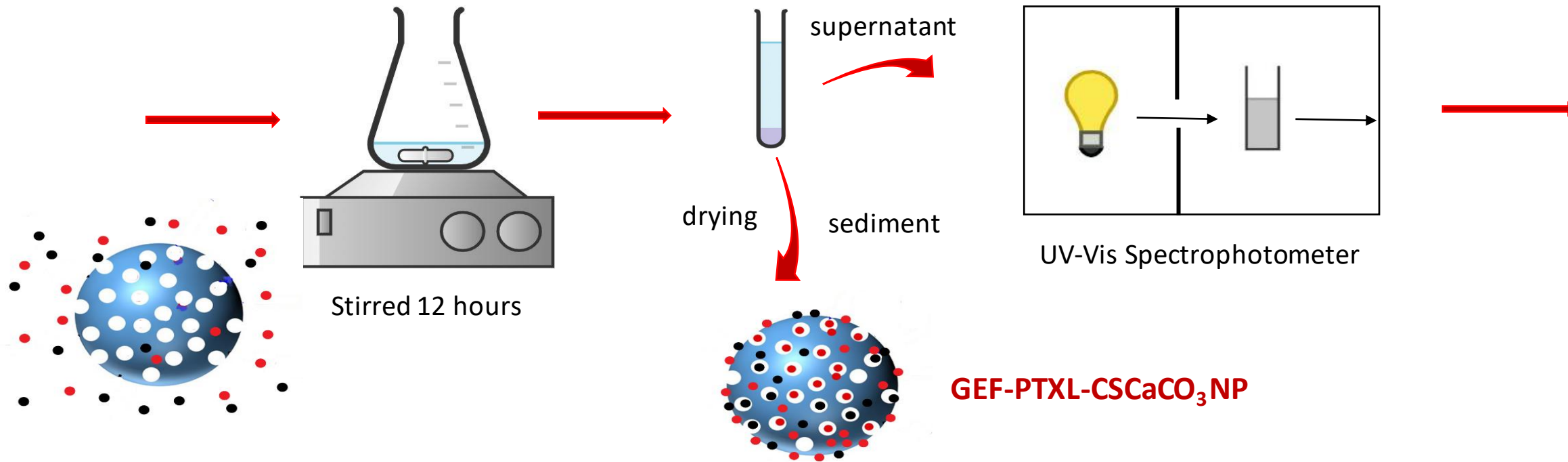
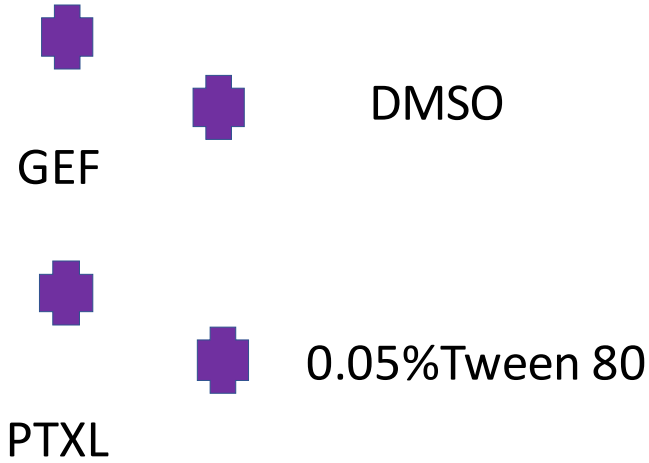
1. Top down synthesis of CSCaCO_3 nanoparticles from cockle shells (*Anadara granosa*)



2. Synthesis of GEF-CSCaCO₃, PTXL-CSCaCO₃ and GEF-PTXL-CSCaCO₃ nanoparticles



CSCaCO₃NP



3. Loading content and encapsulation efficiency of GEF-PTXL-CSCaCO₃ nanoparticles

The encapsulation efficiency (EE%) and loading content (LC%) was determined as the average measurement of 3 independent measurements (Fu *et al.*, 2017).

$$\text{Encapsulation efficiency (\%)} = \frac{W_t - W_f}{W_t} \times 100 \quad \text{--- (1)}$$

Where,

W_t is the total weight of drug fed

W_f is the weight of non-encapsulated free drug.

$$\text{Loading content (\%)} = \frac{W_t - W_f}{W_{np}} \times 100 \quad \text{--- (2)}$$

Where,

W_t is the total weight of drug fed

W_f is the weight of non-encapsulated free drug

W_{np} is the weight of the nanoparticles

B. Physicochemical characterization of CSCaCO_3 NP and GEF-PTXL- CSCaCO_3 NP

1. Transmission Electron Microscopy (TEM) and Field emission Scanning Electron Microscopy (FESEM) of CSCaCO_3 NP and GEF-PTXL- CSCaCO_3 NP
2. Electro-kinetic zeta potential, hydrodynamic diameter, and Poly-dispersity Index (PDI) of CSCaCO_3 NP and GEF-PTXL- CSCaCO_3 NP
3. Powder X- ray powder Diffraction (PXRD) of CSCaCO_3 NP and GEF-PTXL- CSCaCO_3 NP
4. Fourier-transform infrared spectroscopy (FT-IR) of CSCaCO_3 NP and GEF-PTXL- CSCaCO_3 NP
5. Specific Surface area and Pore Size of CSCaCO_3 NP and GEF-PTXL- CSCaCO_3 NP

Results & Discussion



1. Loading content and encapsulation efficiency of GEF-PTXL-CSCaCO₃ nanoparticles

Table 1: Loading content (%) and Encapsulation efficiency (%) of various groups of GEF-PTXL- CSCaCO₃NP

Groups	Drugs	CSCaCO ₃ NP (μg)	Loading content (%)	Encapsulation efficiency (%)
GEF1-PTXL	GEF (400 μg)	10,000	1.98 ± 0.11	50.01 ± 2.18
	PTXL (200 μg)		0.92 ± 0.01	45.60 ± 0.32
GEF2-PTXL	GEF (400 μg)	15,000	1.14 ± 0.23	42.95 ± 8.98
	PTXL (200 μg)		0.50 ± 0.08	37.45 ± 5.73
GEF3-PTXL	GEF (400 μg)	20,000	1.12 ± 0.19	45.03 ± 10.37
	PTXL (200 μg)		0.44 ± 0.08	43.93 ± 7.25

The loading efficiency of drugs into the nanoparticles is also governed by the surface area availability on the CSCaCO₃ nanoparticles and water solubility of the drugs employed (Govender *et al.*, 2000).

The lower loading content of less than 10% is usually observed for inorganic carrier based nanoparticles. Similar result is reflected in the loading content obtained in the current experiment (Shen *et al.*, 2017).

B. Physicochemical Characterization

1. TEM and FESEM of CSCaCO₃NP and GEF-PTXL- CSCaCO₃NP

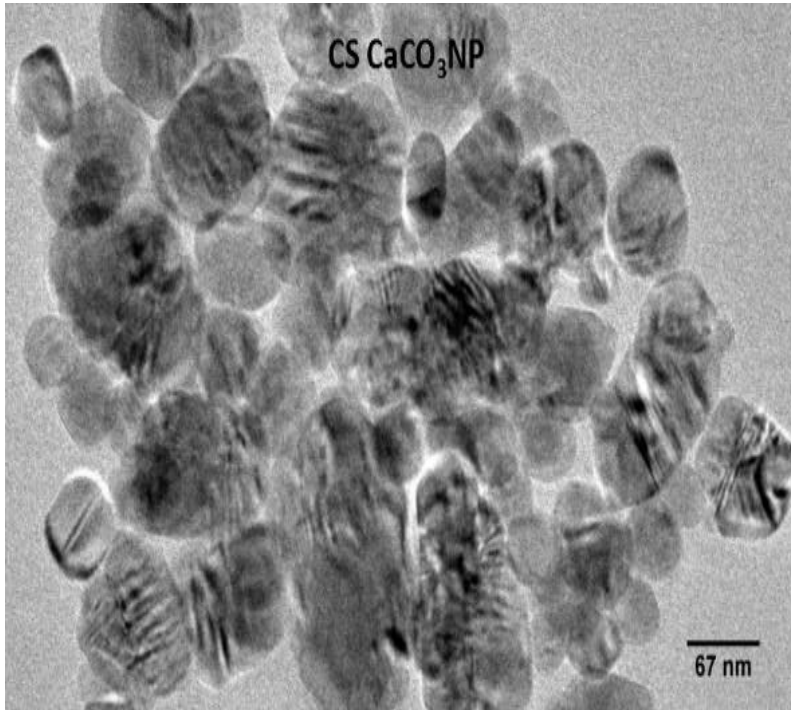


Figure 1: Transmission Electron micrograph of CSCaCO₃NP @50nm

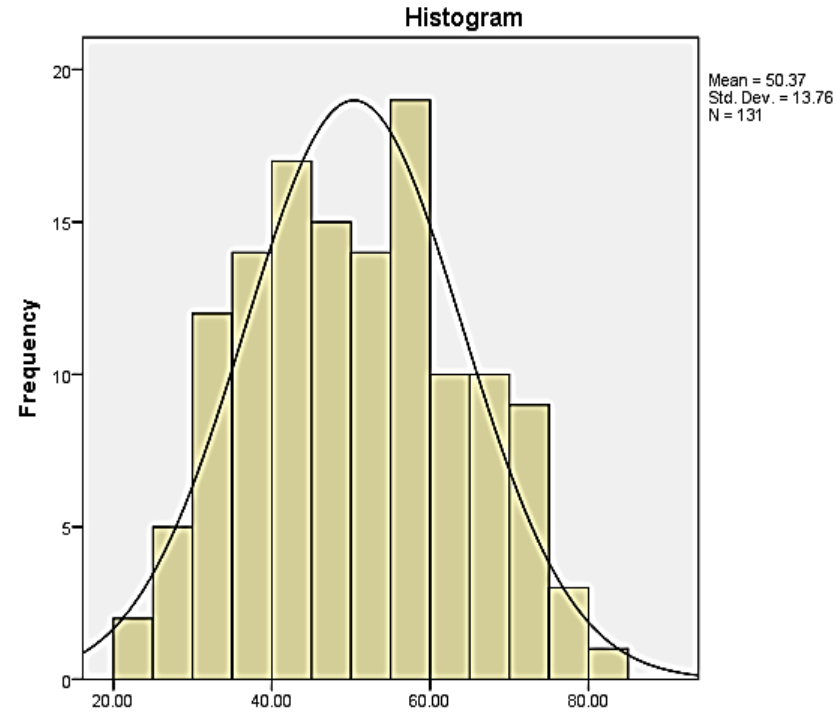


Figure 2: Size distribution chart of CSCaCO₃NP

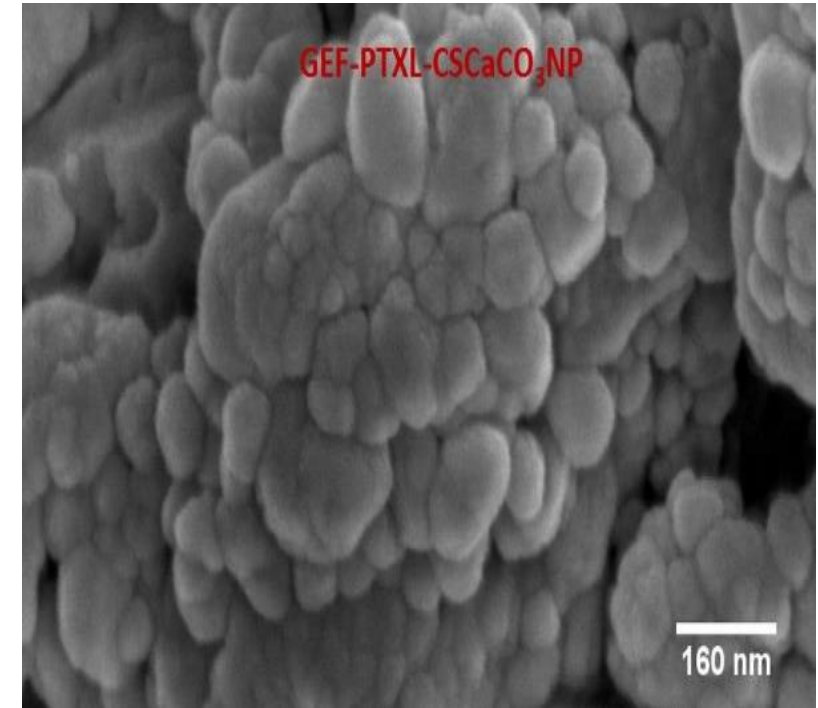


Figure 3: Scanning Electron micrograph of GEF-PTXL-CSCaCO₃NP @ 87nm

Similar results were obtained by [Ibiyeye et al.](#), where CSCaCO₃NP had similar average diameters of 53.65 ± 10.29 nm and CSCaCO₃NP loaded with Thymoquinone /Doxorubicin, had an average diameter of 60.49 ± 11.36 nm ([Ibiyeye et al., 2020](#)).

2. Electro-kinetic zeta potential, hydrodynamic diameter, and Poly-dispersity Index (PDI)

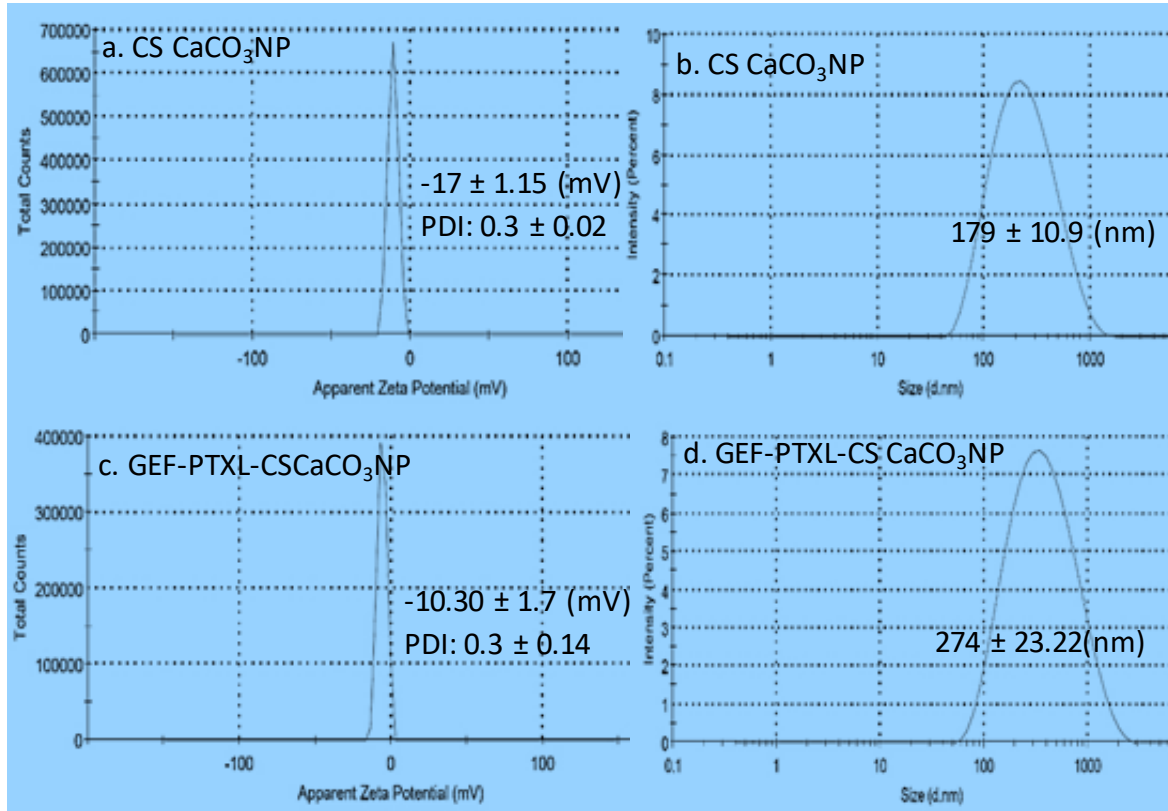
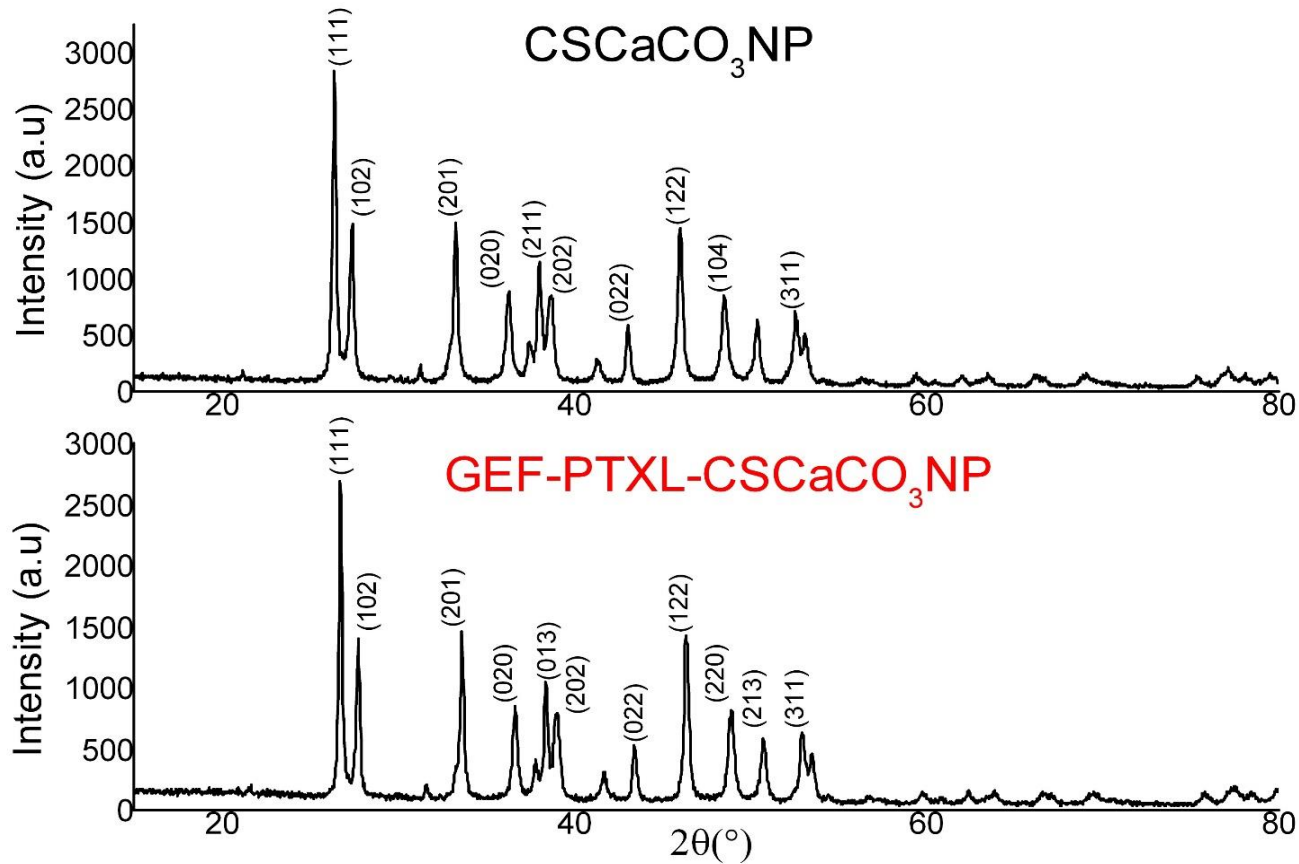


Figure 4: DLS results showing the apparent Zeta Potential and the Particle size distribution in deionized water and PBS with 0.2% Tween 80 for CSCaCO₃NP (a & b) and GEF-PTXL-CSCaCO₃NP (c & d), respectively.

The negative Zeta potential is in concurrence with the results from other researchers ([Danmaigoro et al., 2017](#); [Idris et al., 2019](#); [Ibiyeye et al., 2020](#)).

The hydrodynamic diameter of both of the nanoparticles was larger than the Doxorubicin loaded CSCaCO₃NP obtained by other researchers ([Danmaigoro et al., 2017](#) and [Hamidu et al., 2019](#)).

3. Powder X-ray Diffraction (PXRD)



Raw data of the PXRD, when analyzed in X'Pert High score Plus software, showed the highest score for aragonite phase of CaCO₃.

This result is in agreement with the results obtained by other researchers where various other drugs like Vancomycin ([Saidykhani et al., 2017](#)), Doxorubicin ([Danmaigoro et al., 2017](#)), Thymoquinone, and Doxorubicin ([Ibiyeye et al., 2020](#)) that have been loaded onto the CSCaCO₃NP.

Figure 5: PXRD patterns demonstrate aragonite crystalline phase in both the nanoparticles and labeled are the Miller indices planes of the synthesized crystals

4. Fourier-transform infrared spectroscopy (FT-IR)

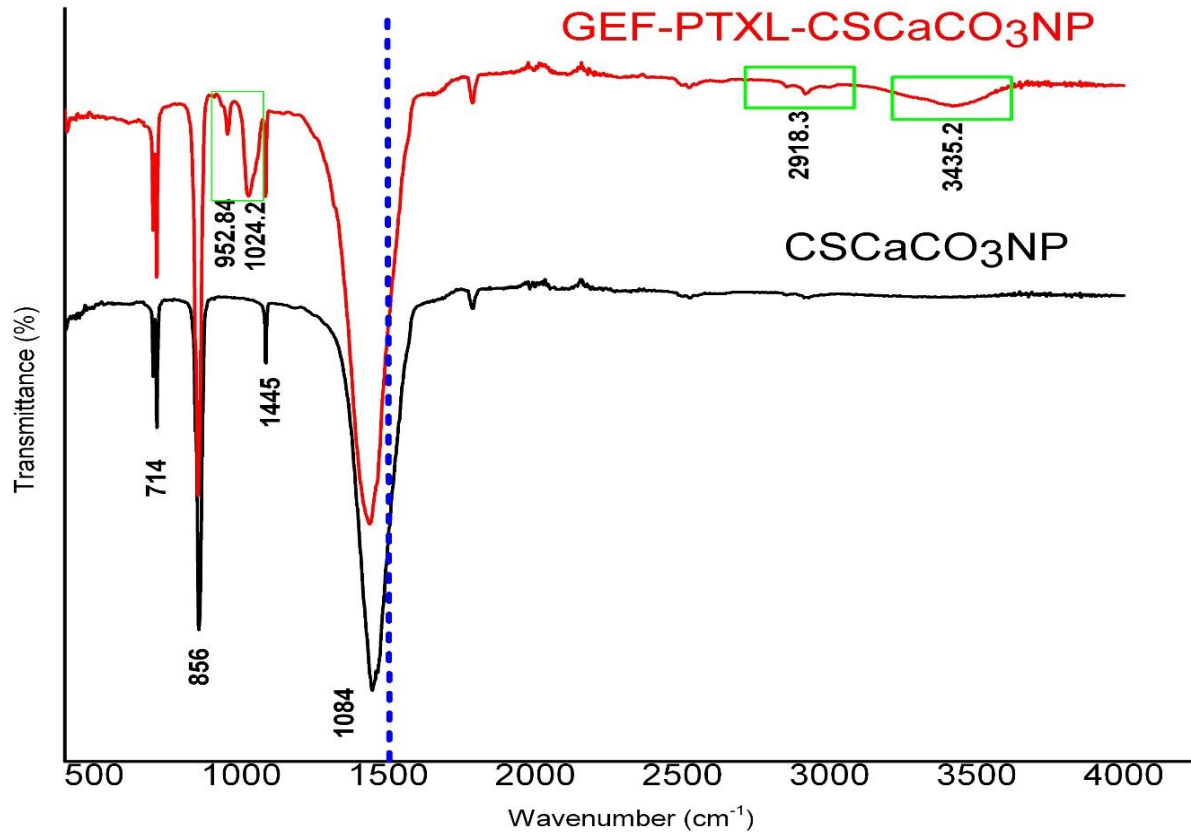


Figure 6: FT-IR pattern of CSCaCO₃NP and formation of new peaks (green box) in the spectra of GEF-PTXL-CSCaCO₃NP

CSCaCO₃NP :

1445, 1084, 856, and 714 cm^{-1} .

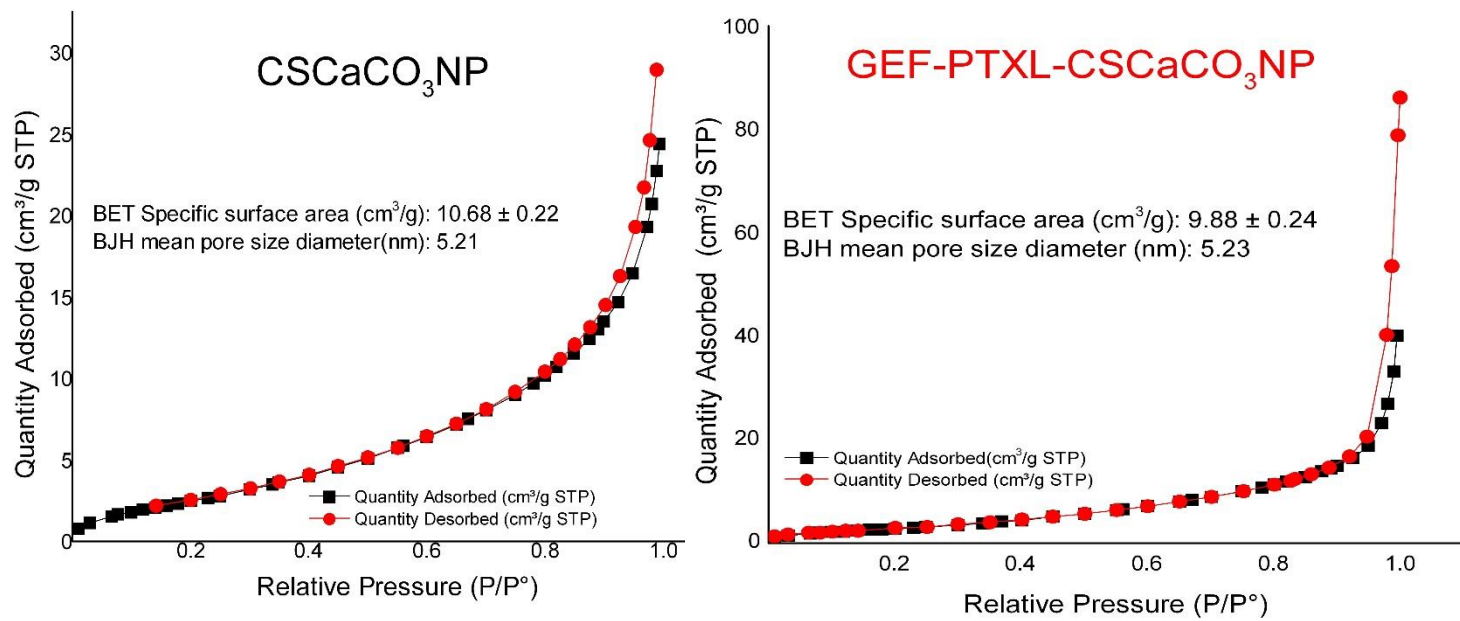
The largest and strongest band-1445 cm^{-1} C-O stretching band. The other peaks at 1084 and 856 cm^{-1} are attributed to CO₃²⁻ in the molecular structure of the calcium carbonate.

The derived spectra are similar to the spectra obtained by other researchers for cockle shell derived CaCO₃NP ([Hammadi et al., 2017](#); [Danmaigoro et al., 2017](#) and [Fu et al., 2017](#)).

GEF-PTXL- CSCaCO₃ NP;

New vibrational band assignments at 952.84 (cyclohexane), 1024.20 (C-F stretch), 2918.30 (C-H stretching) and 3435.22 (aromatic amine and OH⁻ stretch) cm^{-1} ([Renuga Devi and Gayathri, 2010](#) and [Talari et al., 2017](#))

5. Specific Surface area and Pore Size

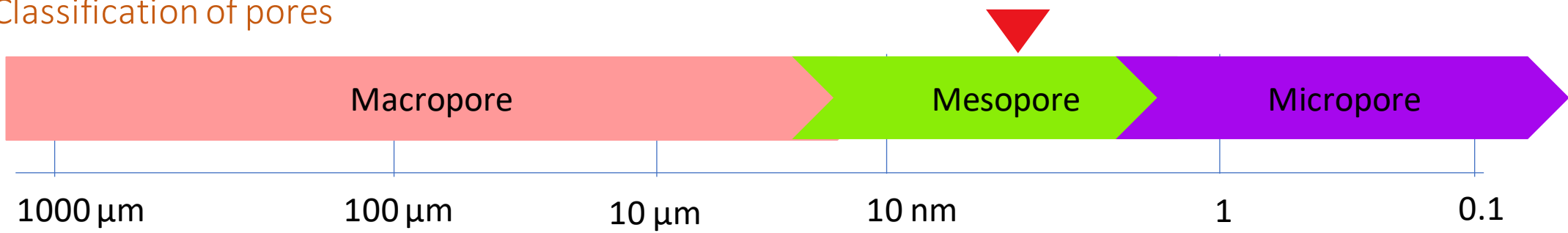


BET Brunauer-Emmett-Teller
 Type IV isotherm + “hysteresis loop H1”
 initial loop- mono-multi layer adsorption,
 2nd loop- desorption of gases
 (Sing, 1982; Thommes *et al.*, 2015)

According to Hammadi *et al.*, there is increase in surface area have been observed for the drug loaded Cockle shell derived CaCO₃NP.

Figure 7: BET nitrogen adsorption isotherms revealing the characteristic isotherms of plain CSCaCO₃NP and GEF-PTXL- CSCaCO₃NP

Classification of pores



(Sing, 1982)

Conclusions



CSCaCO₃NP

- The top down method of synthesis of Cockle shell derived (CSCaCO₃NP) resulted in nanoparticles of average size of 52.36 ± 15.82 nm and spherical shaped nanoparticles.
- -17 ± 1.15 (mV) of zeta potential, with PDI of 0.3 is indicating stability
- XRD data revealed that the CSCaCO₃NP is purely aragonite crystals
- FTIR analysis shows that the synthesized CSCaCO₃NP possessed the characteristic spectra of calcium carbonate compound.
- The BET pore size of 5.21 nm, with good surface area of $10.68 \text{ cm}^3/\text{g}$ makes it a good candidate as a drug carrier.

GEF-PTXL-CSCaCO₃NP

- The Loading content (%) and encapsulation efficiency (%) for GEF and PTXL in dual drug-loaded NP (GEF-PTXL-CSCaCO₃NP) was 1.98 ± 0.11 , 50.01 ± 2.18 and 0.92 ± 0.01 , 45.60 ± 0.32 .
- The synthesized GEF-PTXL-CSCaCO₃NP had an average size of 87.20 ± 26.66 nm.
- -10.30 ± 1.7 (mV) of zeta potential and PDI of 0.3 is indicating stability
- XRD data revealed that the GEF-PTXL-CSCaCO₃NP belong to the aragonite signature even after loading of the drugs
- FTIR analysis shows that the certain functional groups of the drugs are found in the loaded GEF-PTXL-CSCaCO₃NP.
- The BET pore size of 5.23 nm, with surface area of $9.88 \text{ cm}^3/\text{g}$, reduction in surface area could be due to the loaded drugs on the surface and pores of the CSCaCO₃NP

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Thank you.

