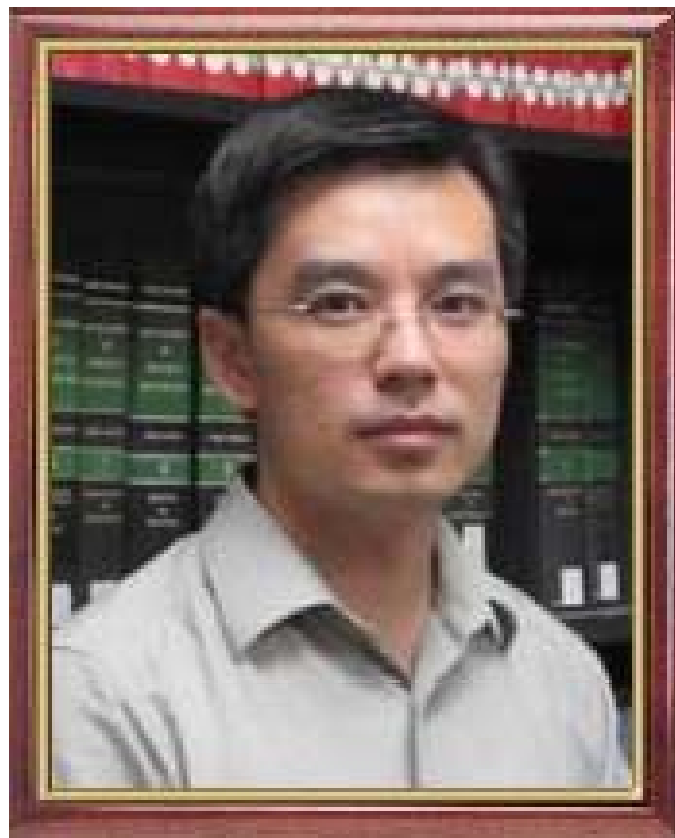


**Laminar Dispersive and Distributive Mixing  
with Dissolution and Applications to Hot Melt  
Extrusion (HME)**

**Costas G. Gogos and Huiju Liu**

**New Jersey Institute of Technology and the Polymer Processing Institute**



*Prof. Peng Wang 1975 – 2012*

*Sr. Polymer Scientist at NJIT and PPI 2007 - 2010*

# Oral drug delivery products

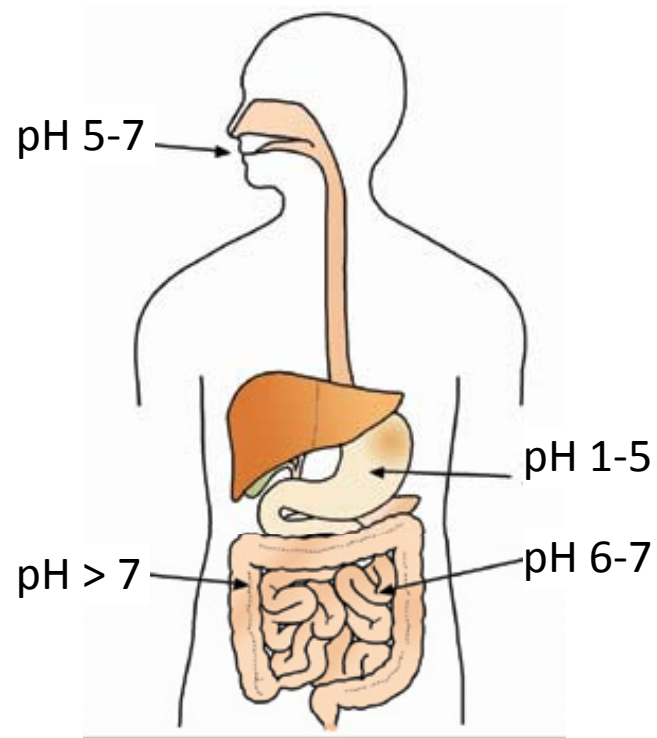


Figure adapted from: Rocca J. et al. (2004). *Drug Delivery Technology* 4

For the API to be **Bio-available** it must **necessarily dissolve in the GI tract** ( stomach or Small Intestines)

# API Solubility and Permeability

High Ionic and H-bonding capability



High Solubility in the GI Tract

High Lipophilicity (Hydrophobicity)



High permeability to get to the blood stream

**Bio-availability** (high API concentration in blood stream)



**Bio-availability = (Solubility) X (Permeability)**

# Oral Drug Delivery Products (tablets, capsules..)

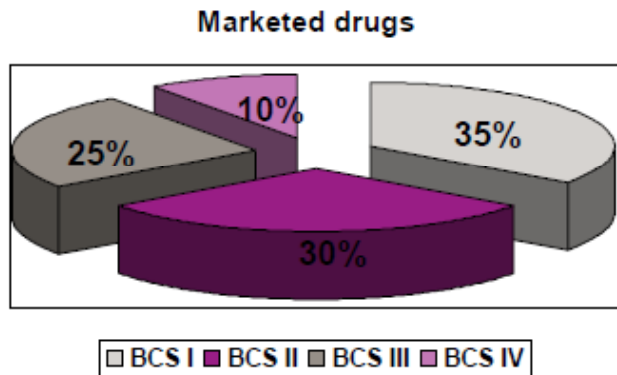
ACTIVE PHARMACEUTICAL INGREDIENT (API) = Ibuprophen  
(water soluble)



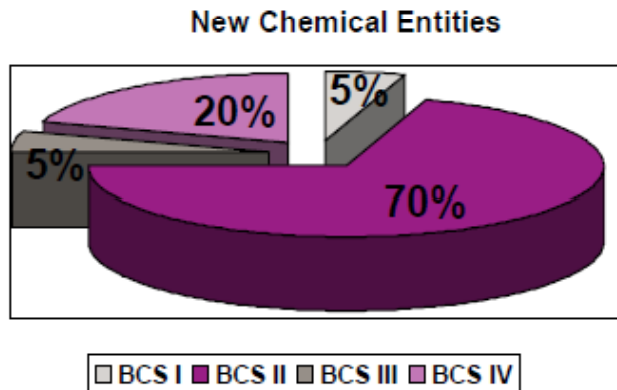
INACTIVE (EXCIPIENT) INGREDIENTS (binders/additives)

## What if the API were Very Poorly Water soluble?..

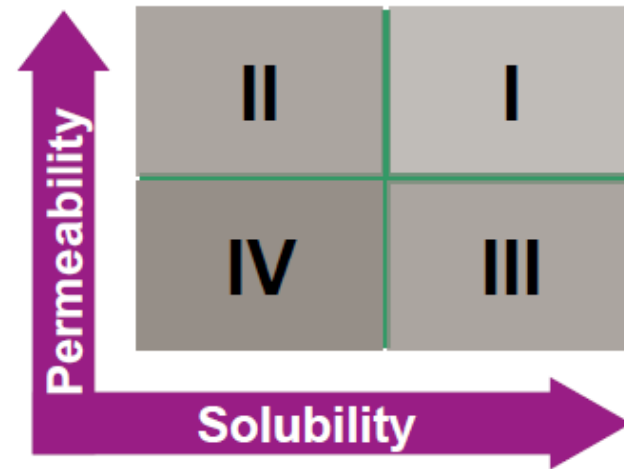
# Need for Solubility Enhancement



**Number of poorly soluble drugs is increasing!**



## Biopharmaceutical Classification System



- Class I: High solubility and high Permeability
- Class II: Low solubility and high Permeability**
- Class III: High solubility and low Permeability
- Class IV: Low solubility and low Permeability

From: Benet L. Wu C.-Y. et al 2006, Bulletin Technique Gattefosse 99:9-16

# Pharmaceutical Hot Melt Extrusion (HME) Holds the Potential of Dramatically Increasing API Solubility

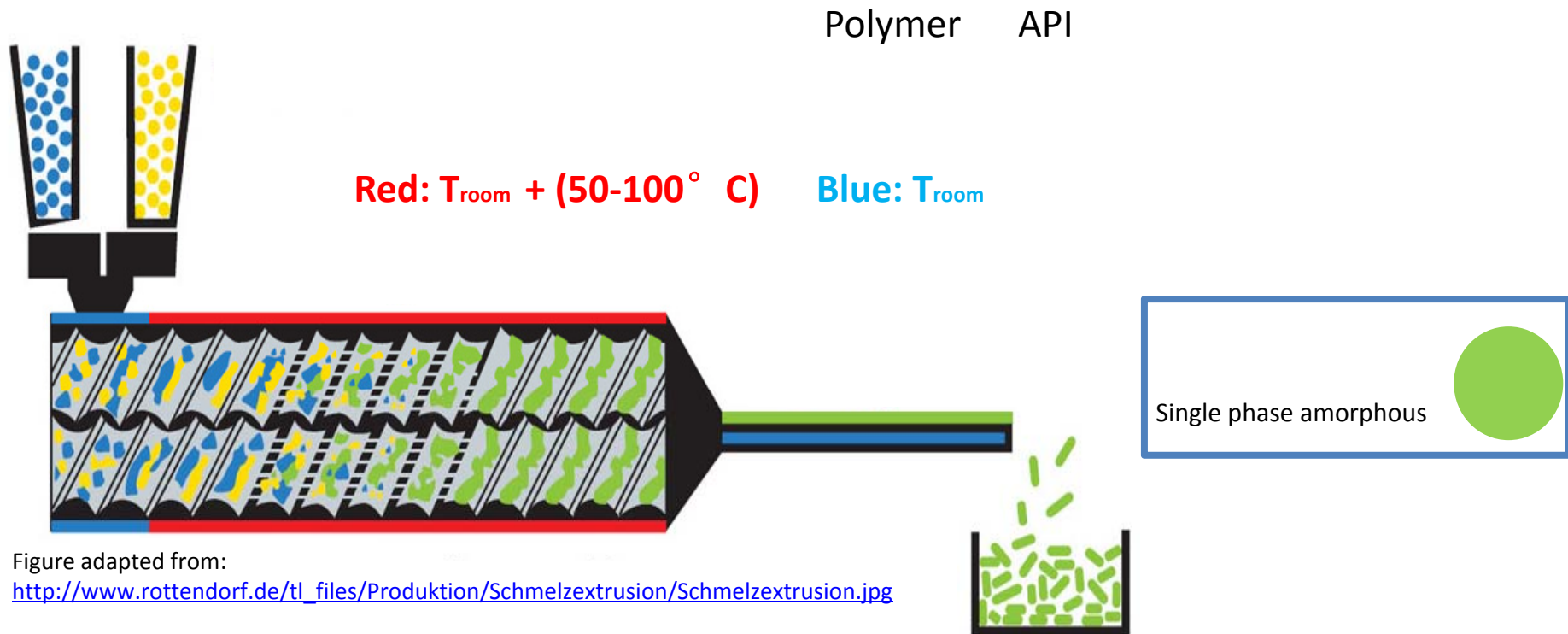


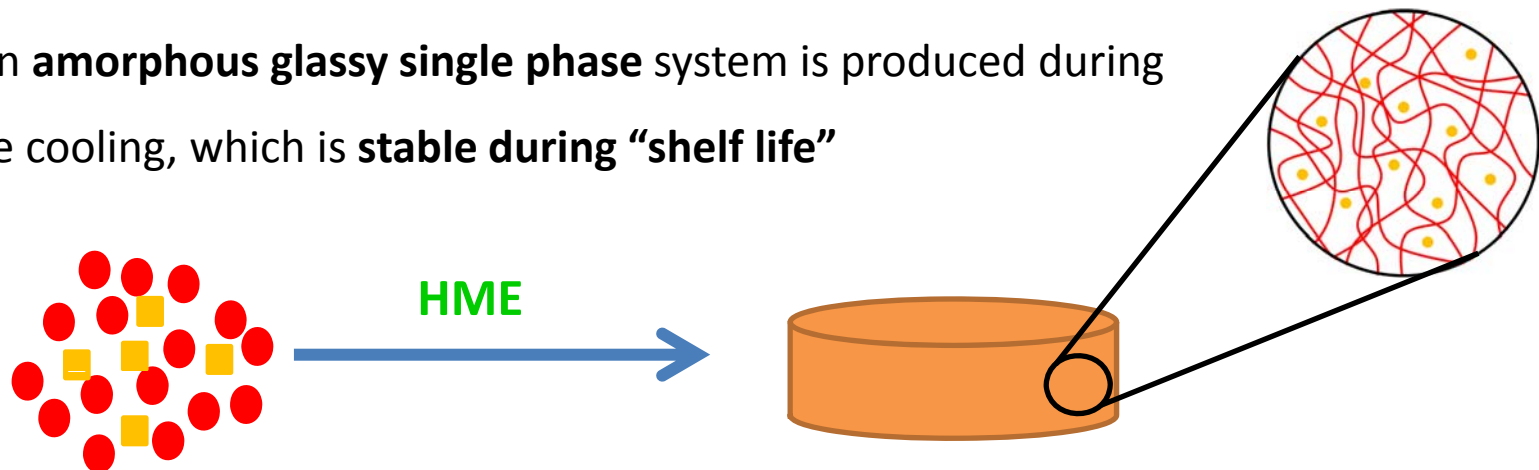
Figure adapted from:

[http://www.rottendorf.de/tl\\_files/Produktion/Schmelzextrusion/Schmelzextrusion.jpg](http://www.rottendorf.de/tl_files/Produktion/Schmelzextrusion/Schmelzextrusion.jpg)



# Why Does HME Result in a Dramatic Increase in API Solubility?

- A poorly soluble API and hydrophilic Polymer Excipient are extruded, much like in an extrusion **compounding** process
- Process Conditions:  $T_{m,API} > T_{process} > T_g + (50\sim 100^\circ\text{C})$   
and  $t_{res} = 60 - 200\text{s}$
- The API, with enhanced solubility at the elevated  $T_{process}$  dissolves in the molten polymer forming a homogenous solution
- Ideally, an **amorphous glassy single phase** system is produced during extrudate cooling, which is **stable during “shelf life”**



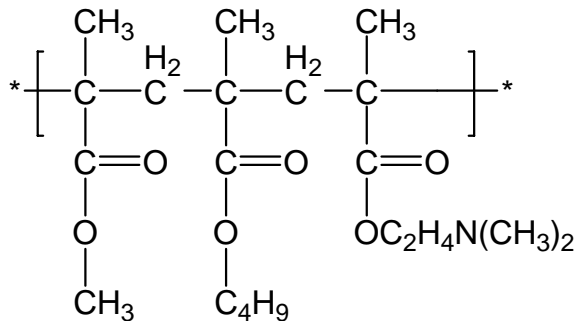


# Example: H M Batch Mixing

$$T_{m,API} > T_{process} > T_g + (50 \sim 100^\circ\text{C})$$

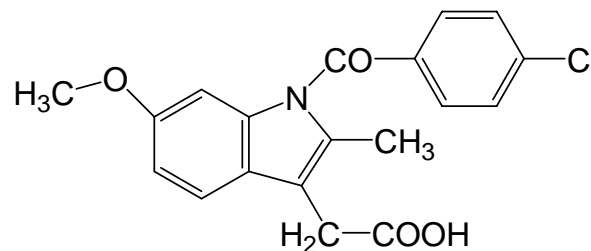
Eudragit™ E PO : Indomethacin  
(70 : 30 )

Run #	Process Temperature (°C)	rpm	Sampling Time
1	100	20	55, 100, 145 285 420
2	100	100	
3	110	20	
4	110	100	
5	140	20	



**Eudragit™ E PO (E PO)**

$T_g = 48^\circ\text{C}$



**Indomethacin (INM)**

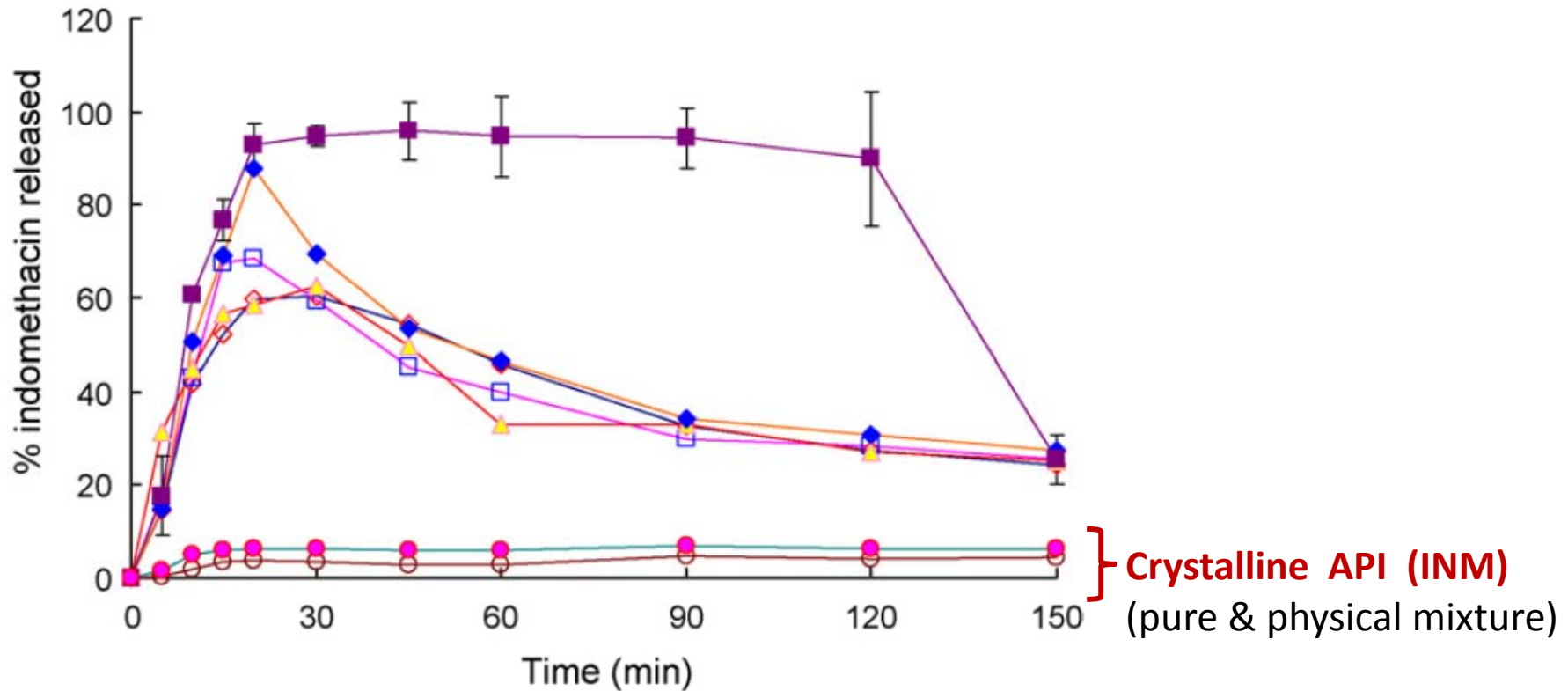
$T_m = 162^\circ\text{C}$



**Batch Mixer**

# Dramatic Increase of API solubility

H M Batch-mixed INM and Eudragit™ EPO.



**Fig. 9.** Dissolution profiles in pH 1.2 buffer solution of runs at: (○) 100% INM; (●) physical mixture; (◇) 100°C 20 rpm; (△) 110°C 20 rpm; (□) 100°C 100 rpm; (◆) 110°C 100 rpm; (■) 140°C 20 rpm.

From H. Liu et al. *Int. J. of Pharm.*, **383** 161 (2010).

# Polymer Excipients Used in Oral Drug Delivery

	Soluble in all pH	pH-dependent Soluble Polymers	Swellable
<b>LOW T<sub>g</sub></b> <b>Shelf life Stability?</b>	<ul style="list-style-type: none"> <li>• Polyethylene Glycol</li> <li>• Polaxamer</li> <li>• Soluplus</li> </ul>	<ul style="list-style-type: none"> <li>• Polymethacrylates                             <ul style="list-style-type: none"> <li>- Eudragit E</li> <li>- Eudragit L &amp; S</li> </ul> </li> <li>• Polyvinyl Acetate Phthalate</li> </ul>	<ul style="list-style-type: none"> <li>• Polymethacrylates                             <ul style="list-style-type: none"> <li>- Eudragit N</li> <li>- Eudragit RL &amp; RS</li> </ul> </li> </ul>
<b>High T<sub>g</sub></b> <b>API Degradation During HME?</b>	<ul style="list-style-type: none"> <li>• Povidone</li> <li>• Copovidone</li> <li>• Hydroxypropyl cellulose</li> <li>• Hypromellose</li> </ul>	<ul style="list-style-type: none"> <li>• Hypromellose Phthalate.</li> <li>• Hypromellose Succinyl Acetate</li> <li>• Cellulose Acetate Phthalate</li> </ul>	<ul style="list-style-type: none"> <li>• Ethycellulose</li> <li>• Cellulose acetate</li> </ul>

# Pharmaceutical HMR Process Objectives



API  
dissolved in  
hydrophilic  
polymer

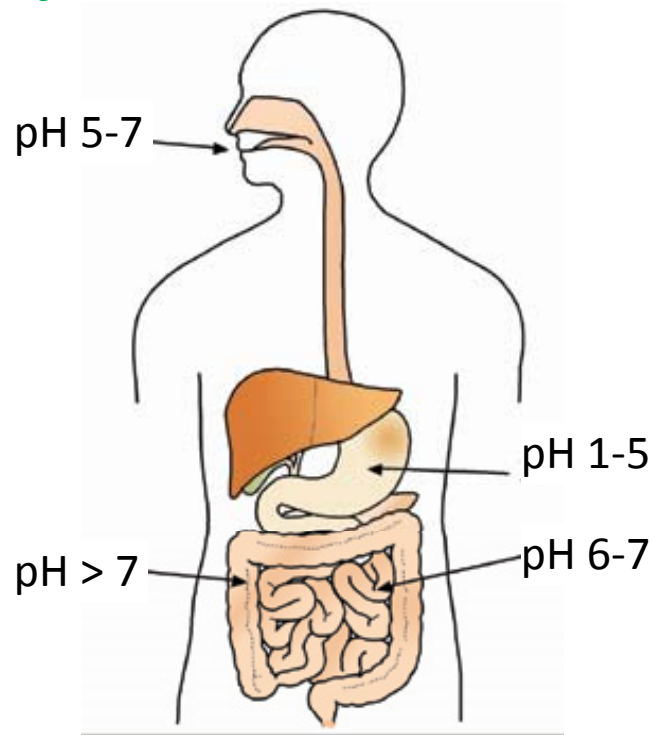
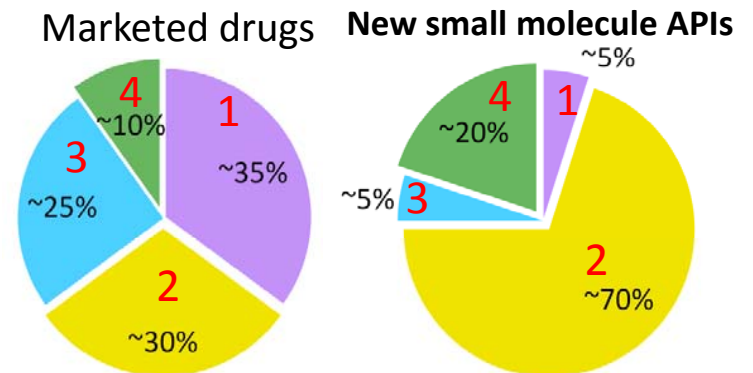


Figure adapted from: Rocca J. et al. (2004). *Drug Delivery Technology* 4

## Biopharmaceutical classification system (BCS) for APIs:

	High Solubility	Low Solubility
High Permeability	<b>Class 1</b> High Solubility High Permeability Rapid Dissolution	<b>Class 2</b> Low Solubility High Permeability
Low Permeability	<b>Class 3</b> High Solubility Low Permeability	<b>Class 4</b> Low Solubility Low Permeability

← **Result / objective of HME**



Figures adapted from: Benet, L. Z. et al. (2006). *Bulletin Technique Gattefassé* 99: 9-16.

# Drug delivery systems produced HME

Name	Polymer	Application	Indication
Dapivirine-Maraviroc	EVA	Implant	Anti-Viral (HIV)
Lacrisert®	HPMC	Implant	Dry eye syndrome
Nuvaring	EVA	Implant	Contraceptive
Zoladex	PLGA	Implant	Prostate cancer
Implanon	EVA	Implant	Contraceptive
Ozurdex®	PLGA	Implant	Macular Edema
Kaletra	PVP-VA	Tablet	Anti-Viral (HIV)
Norvir®	PVP-VA	Tablet	Anti-Viral (HIV)
Eucreas®	HPMC	Tablet	Diabetes
Zithromax®	HPMC	Tablet	Antibiotic
Gris-PEG®	PEG	Tablet	anti-fungal
Rezulin®	Povidone (PVP)	Tablet	Diabetes
PalladoneTM	EC + Eudragit® RS	Tablet	Pain
Cesamet®	Nabilone	Tablet	
Posaconazole			Anti-fungal
Anacetrapib			Cardiovascular disease

Withdraw from the market



Marketed

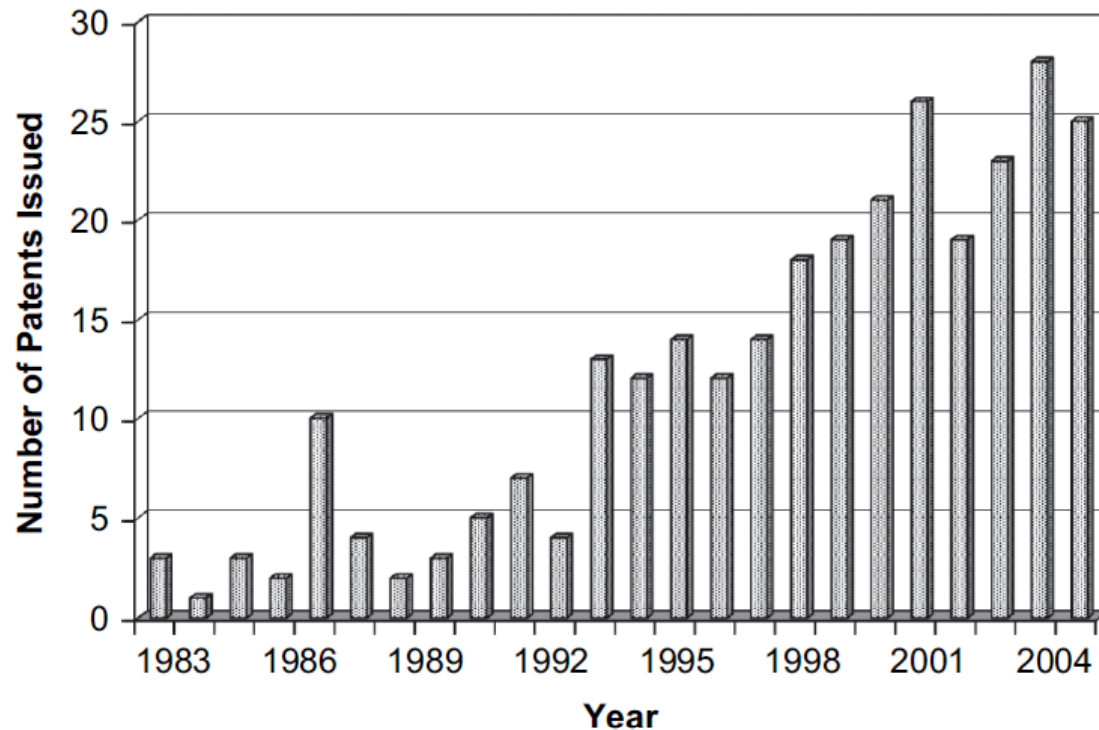


Under development

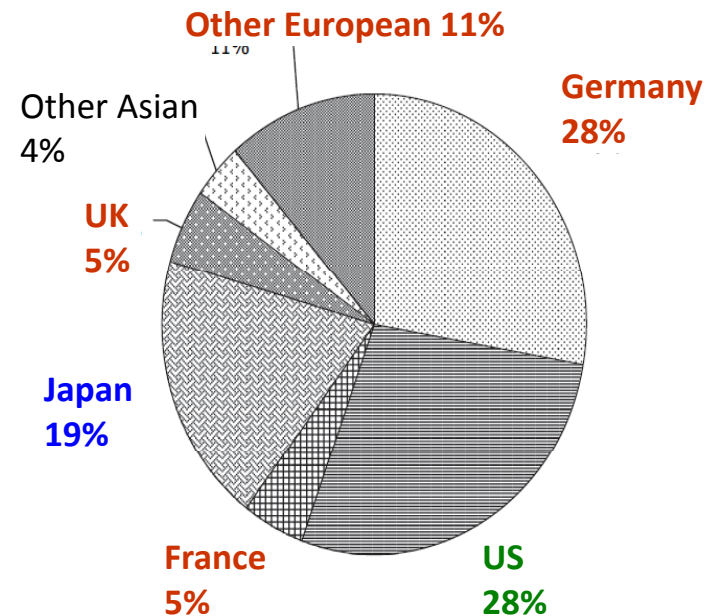


# HME patents from 1983 to 2006

## Number of HME patents issued for pharmaceutical applications



## World distribution of issued HME patents



Figures adapted from: Crowley, M.M. et. al. (2007).  
Drug Dev. Ind. Pharm. **33**, 909-926.

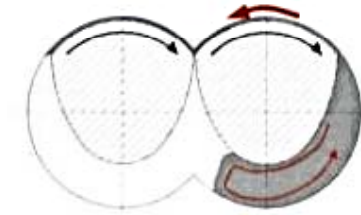


# The Leistritz Pharma Nano 16 at NJIT/PPI

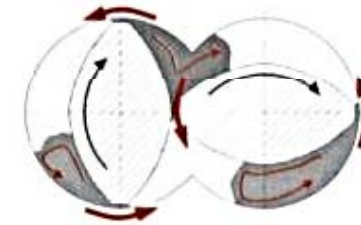


Figure taken from: <http://www.alec-usa.com/tsrpt0210.htm>

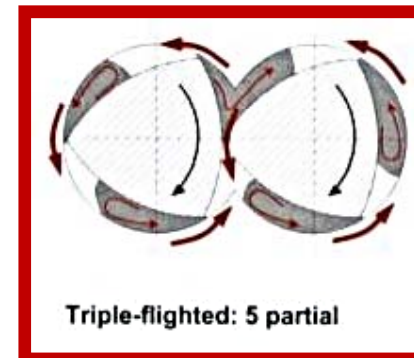
- **Co-rotating , Self-wiping TSE.**
- **Very small “Tri-lobal” free volume.**
- **Micro-plunger allows to work with small batches of 20-100g.**



**Single-flighted: 1 partial**



**Double-flighted: 3 partial**

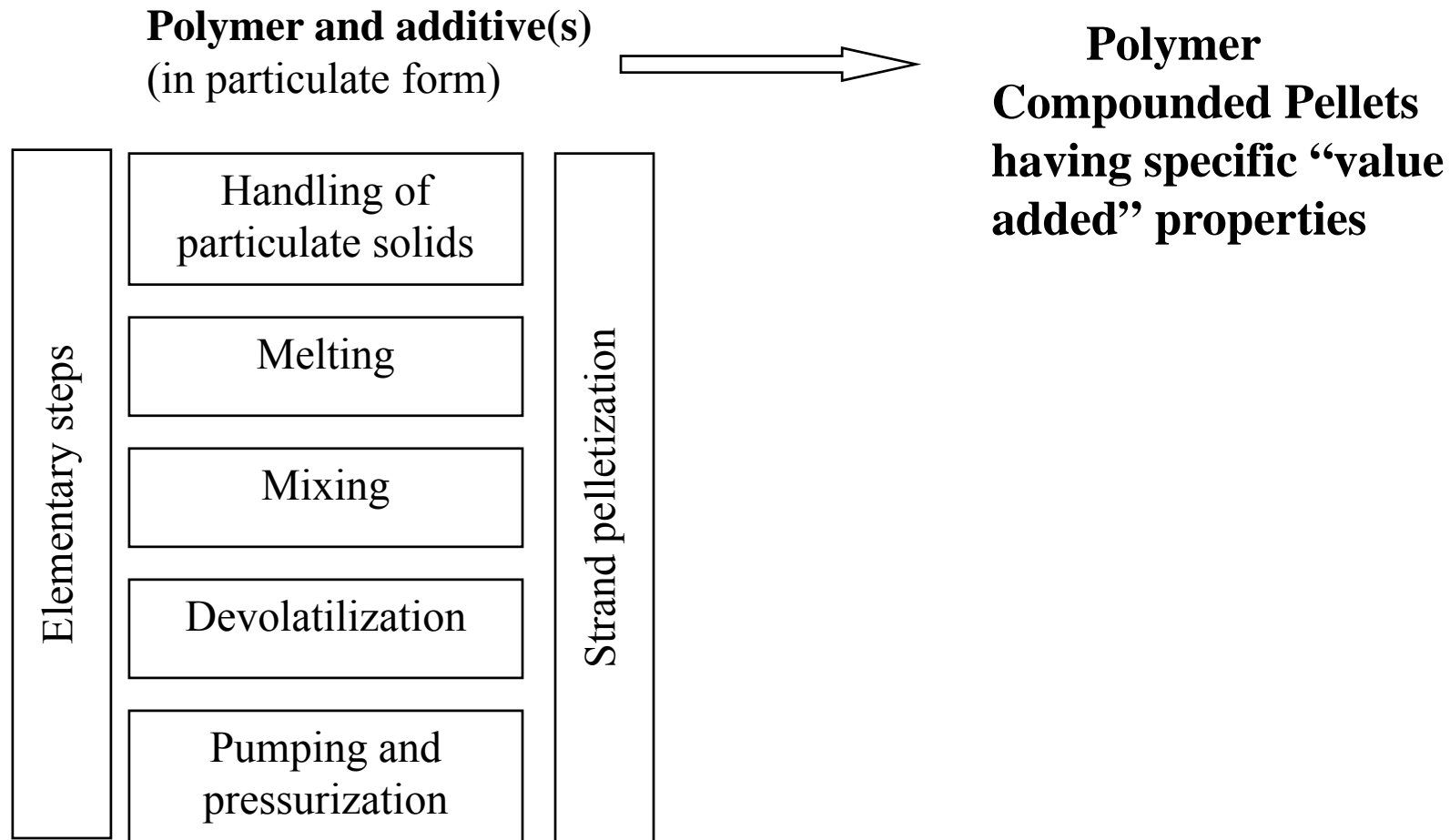


**Triple-flighted: 5 partial**

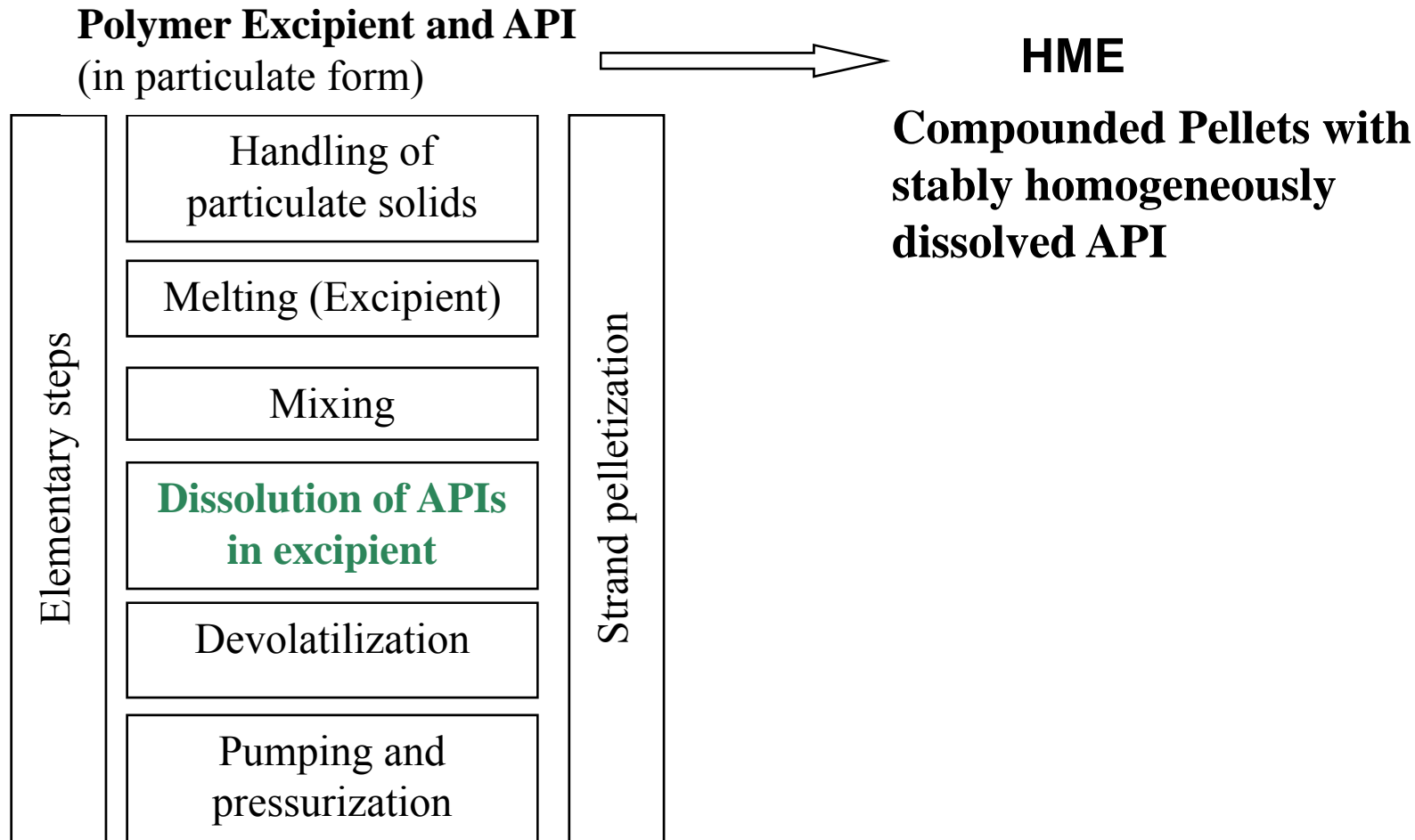
Figures adapted from K. Kohlgrüber (2008)



# Elementary Steps of Polymer Compounding

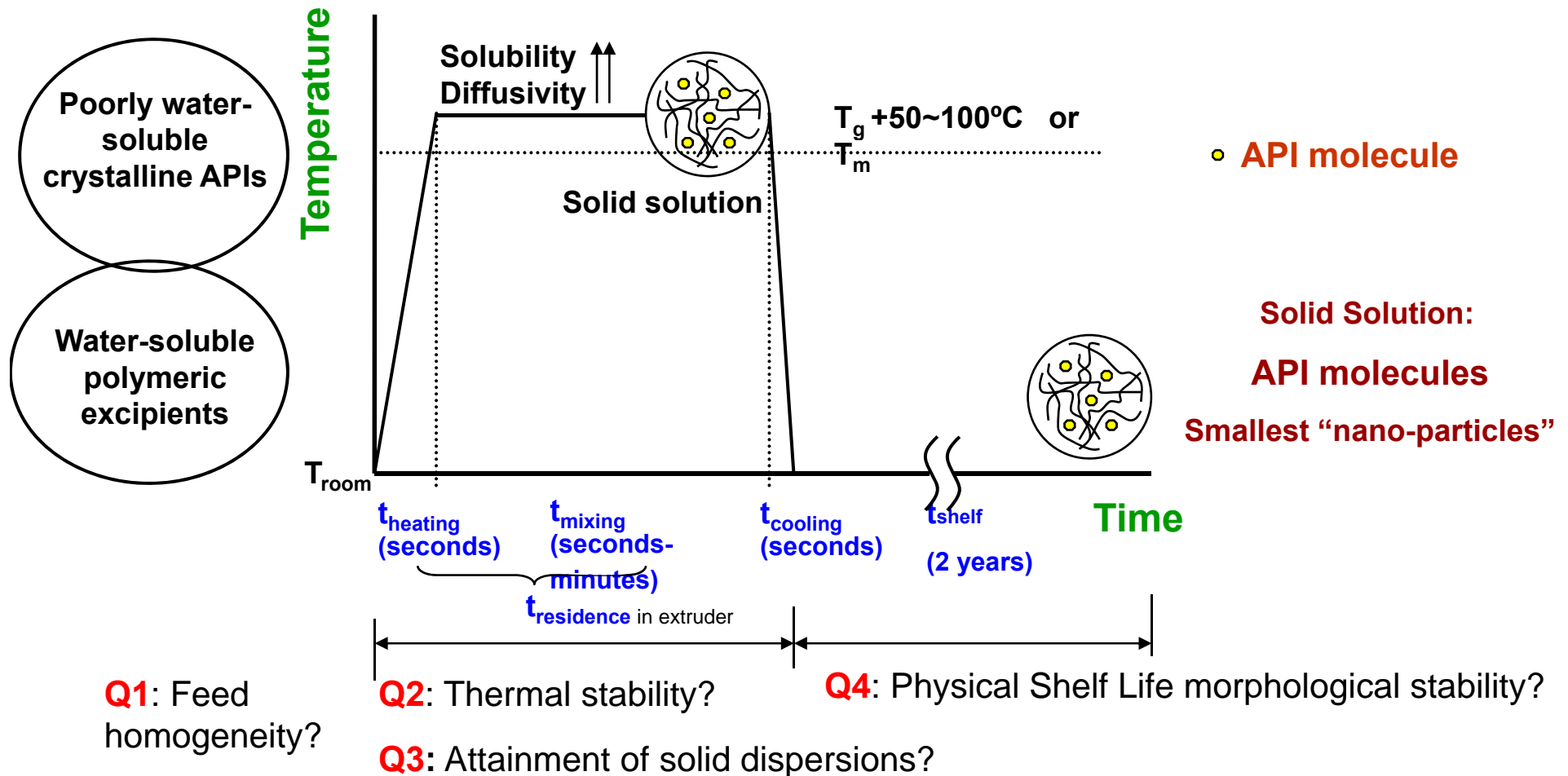


# Elementary Steps of Pharmaceutical Hot Melt Extrusion Processes

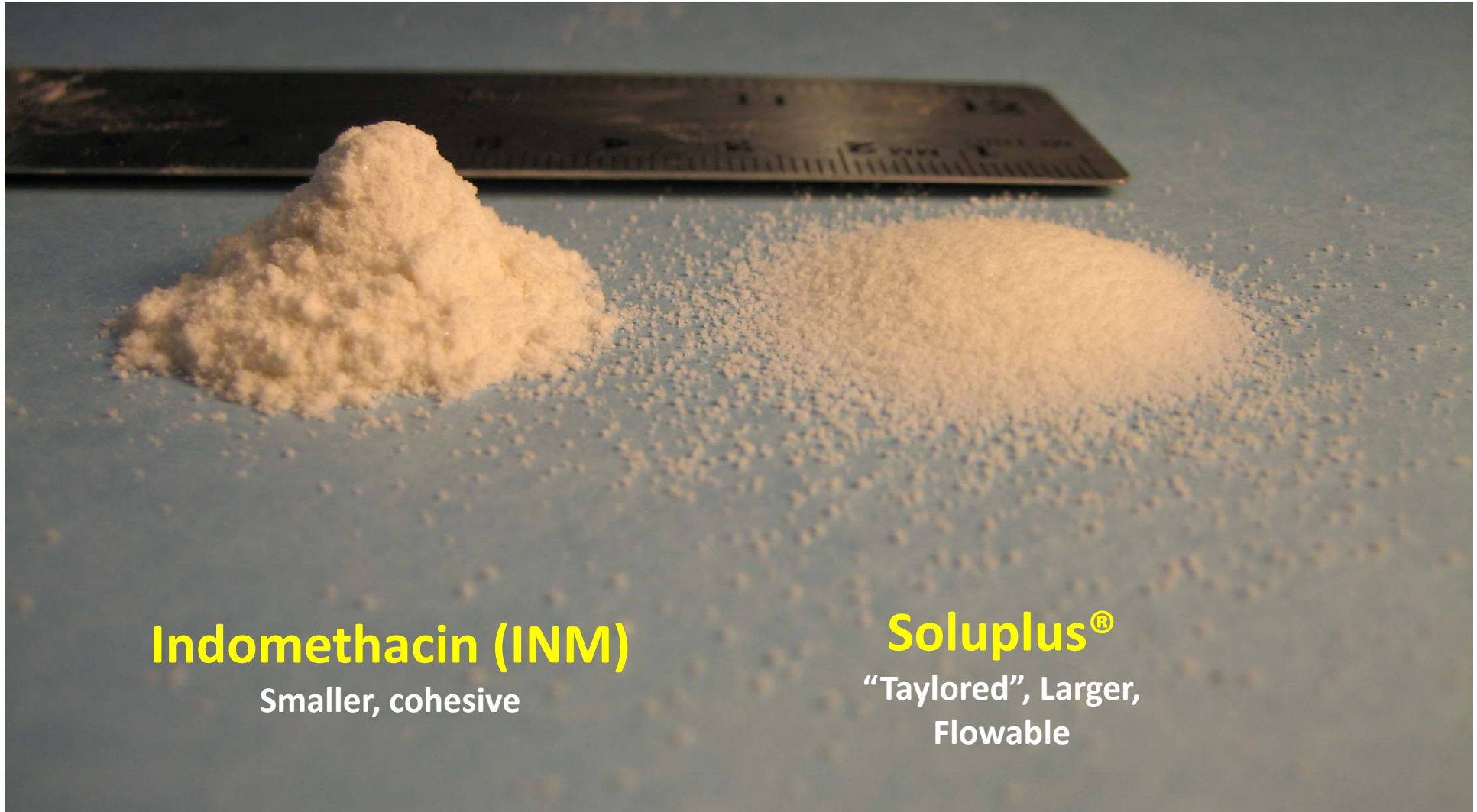


# The HME Process

## Thermo-mechanical History and Fundamental Process Issues



# Particulates Handling: Dissimilar Flowabilities of APIs and Polymer Excipients



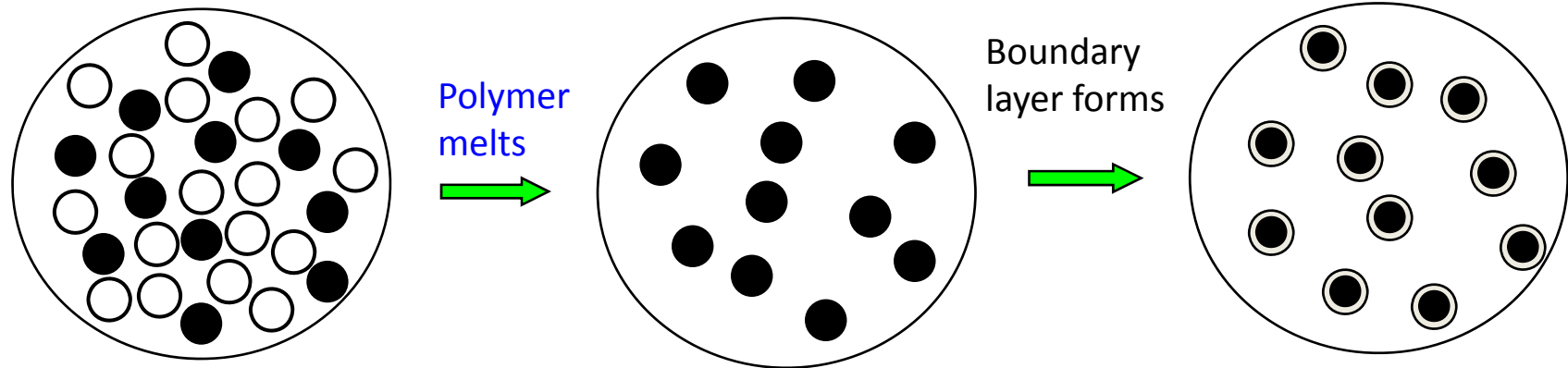
**Indomethacin (INM)**

Smaller, cohesive

**Soluplus®**

“Taylored”, Larger,  
Flowable

$$T_{\text{processing}} > T_g + (50 \sim 100 \text{ } ^\circ\text{C}) ; T_{\text{process}} < T_{m, \text{API}}$$



Premixed drug and polymer particles

Suspended drug particles

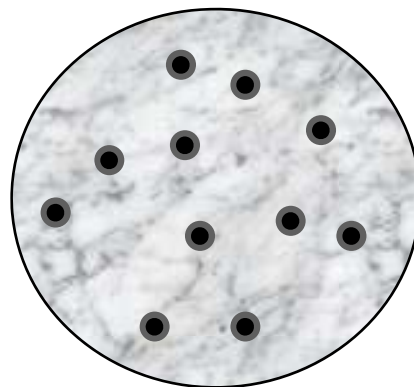
Suspended drug particles

Forced Diffusion

Mass Transfer



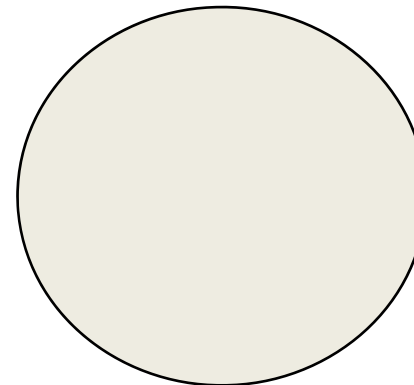
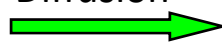
Distributive mixing



Suspended drug particles dissolving at high rates

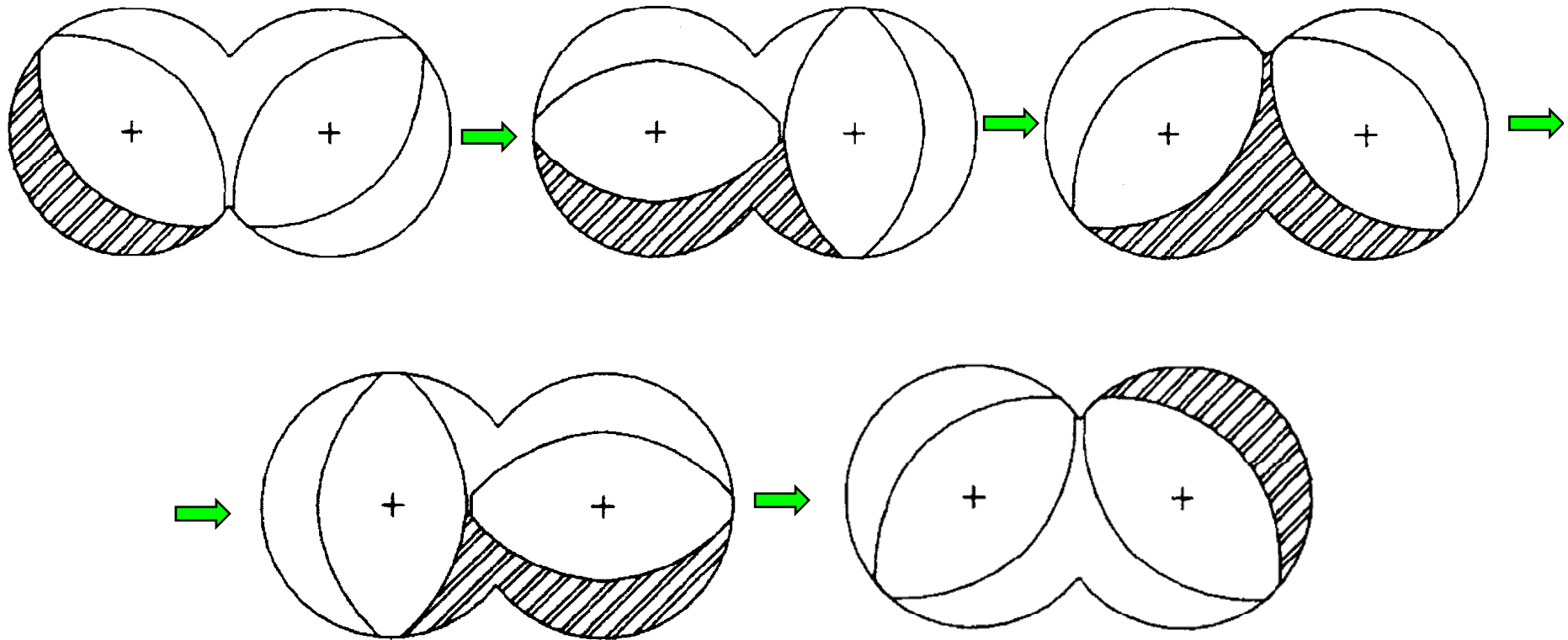
Diffusion

Distributive mixing



Final API/polymer solution

# Repeated Expansion/Contraction Deformations in FULL [F/R] Kneading Elements



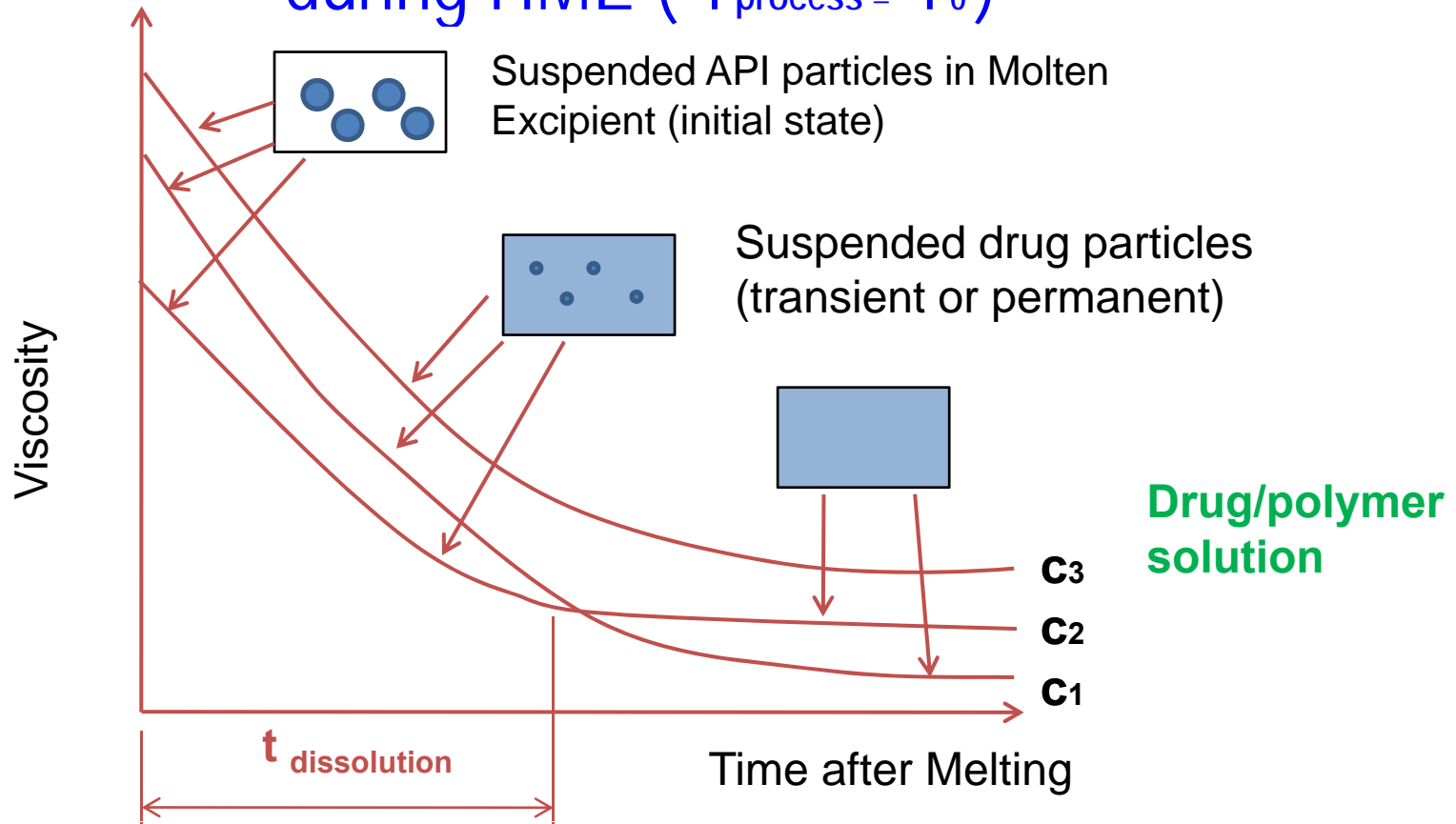
Result in Rapid and Space-wise Uniform Melting and Mixing

# Melting Mechanism in Co-rotating Twin Screw Extruders

					<p>“States” of the Stream</p> <p>Schematic Representation</p>
<p>Fully Filled Region in Melting Configuration      Partially Filled Region in Melting Configuration      Solids Conveying Configuration</p>					<p>Co-TSE Screw Configuration</p>
VED	PED VED (DMM)	PED	Conduction	Melting Mechanisms (Pellets)	
VED	PED VED (DMM)	PED	Conduction	Melting Mechanisms (Powder)	

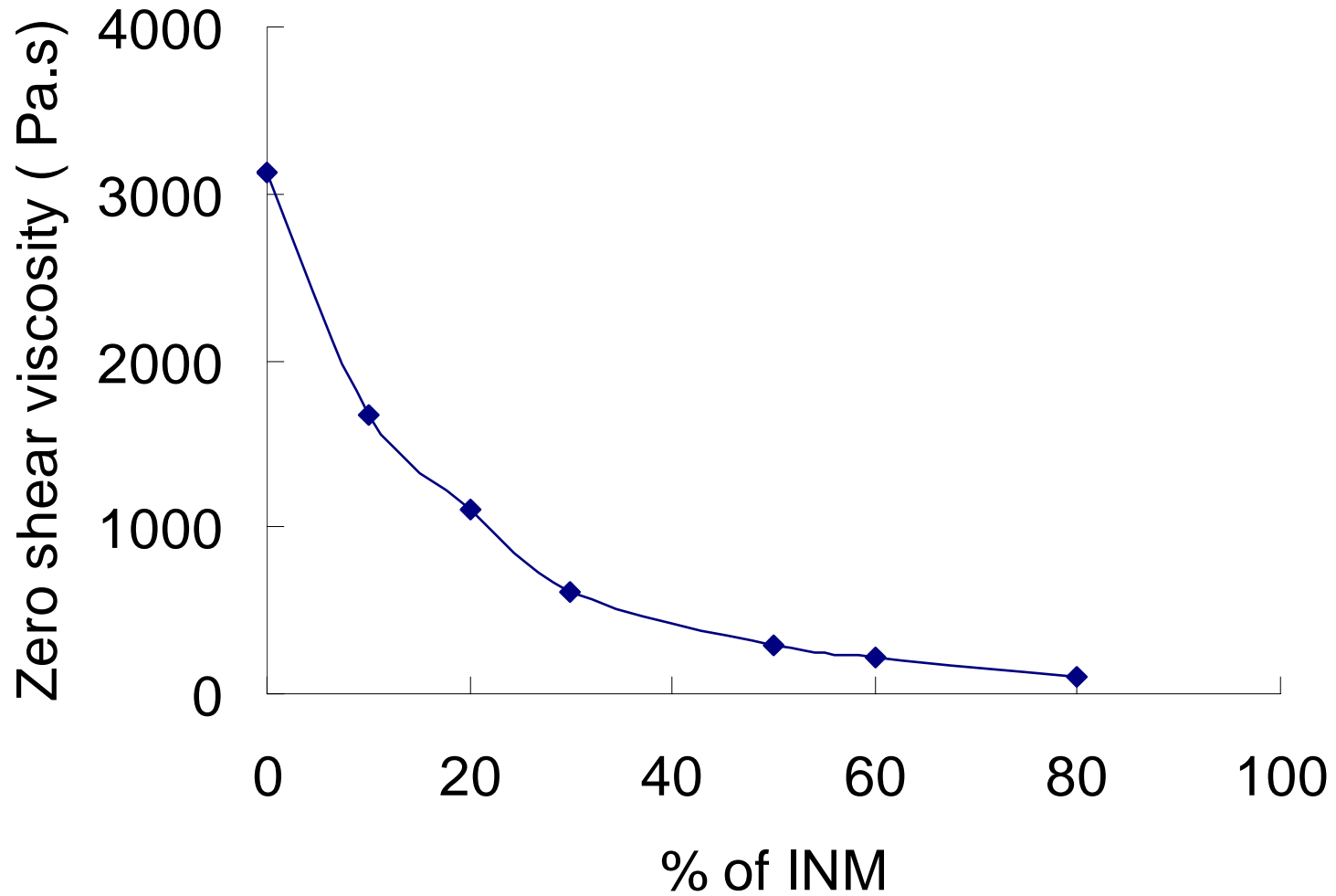


# Evolution of API Particulates Suspension and Dissolution during HME ( $T_{\text{process}} = T_0$ )



$$C_1 < C_2 < C_3$$
$$c_1 < \text{solubility @ } T_0 < c_3$$

**Zero shear viscosity vs. INM% in Eudragit™  
EPO at 145°C (Strong Intermolecular Forces)**



## Amorphous solid solutions

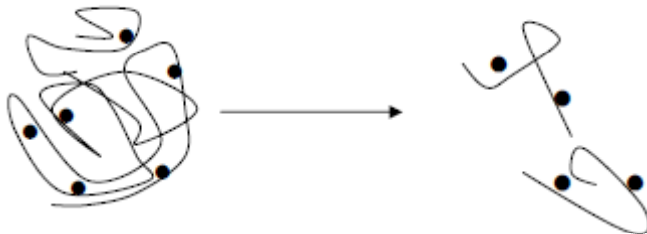


Figure adapted from: 2009 Evonik HME workshop

↑ API  
 Apparent solubility → Higher free energy  
 No lattice energy

## Stability of the amorphous state

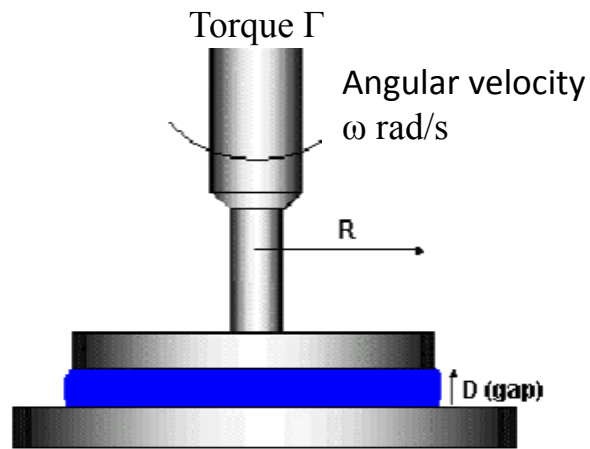
→ Reduce mobility  $T_g \gg T_{\text{storage}}$   
 → Polymer-API Specific interactions

Type of bond	Bond energy [kJ/mol]
Ionic bonds	600-1500
Hydrogen bonds	35- 51
Dipole-Dipole	up to 10

↑ strength

# HME Processing Temperature Solubility Determination Using RMS Rheometry

$$\eta = \tau / \dot{\gamma}$$



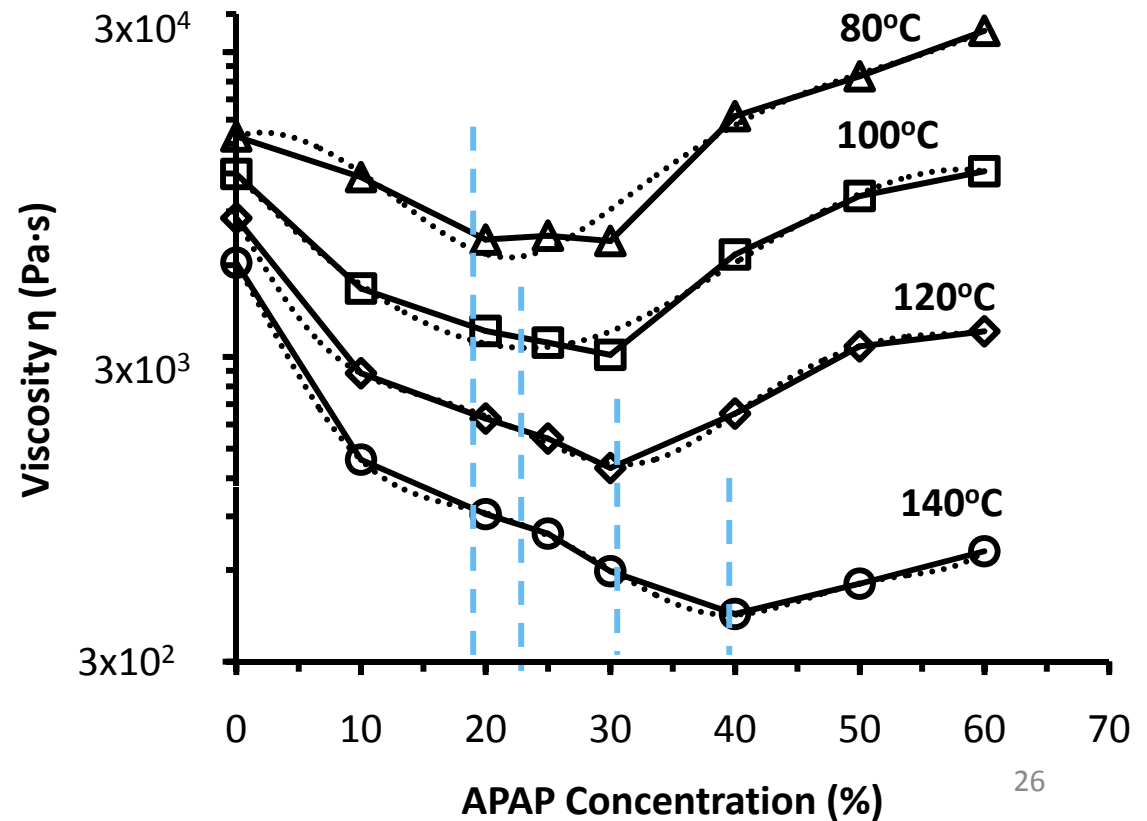
$$\dot{\gamma} = \frac{R}{D} \omega \quad \left| \quad \tau = \frac{2}{\pi R^3} \Gamma$$

Shear rate      Shear stress

$T_m$  (APAP) 170 °C

$T_m$  (PEO) 62 °C

- $\eta$  decreases indicating drug dissolution induced plasticization
- $\eta$  increases due to the formation of API particle /molten polymer “suspension” formation



## B. TSE: Effects of Screw Configuration on the Dissolution of Indomethacin in Eudragit® E PO (E PO:INM=70:30)

One Fully-filled F/R Kneading

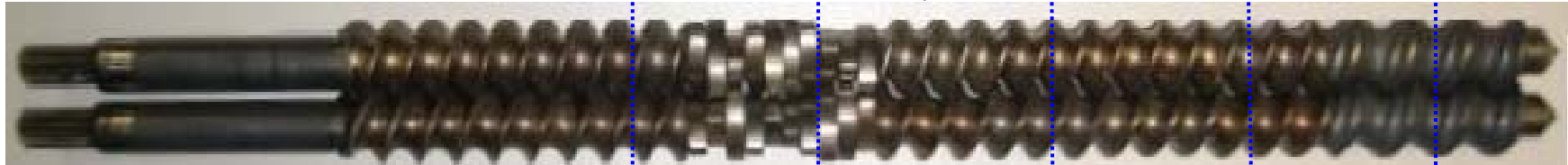
12 paddles (9 forward 30° plus 3 reversed 30°)

One kneading (10 paddles forward 30°)



One Strong Fully Filled F/R Kneading

10 paddles (5 forward 60° plus 5 reversed 30°)



One Fully Filled F/R Kneading

10 paddles (7 forward 30° plus 3 reversed 30°)



No Fully Filled F/R Kneading



8

13

19

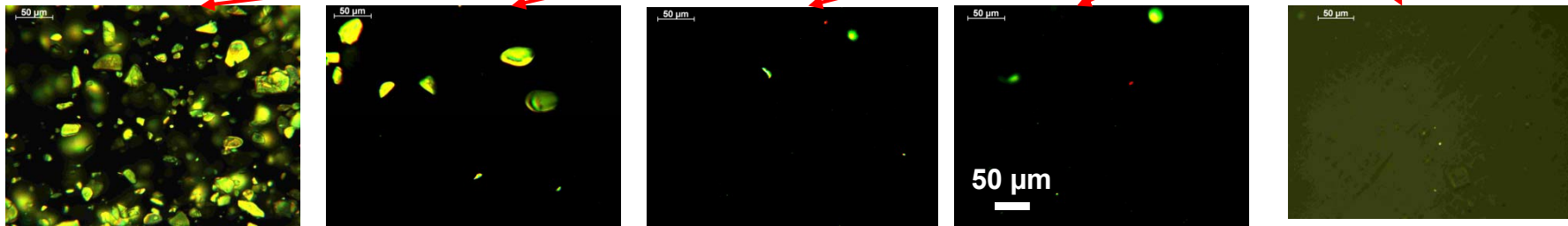
24

28

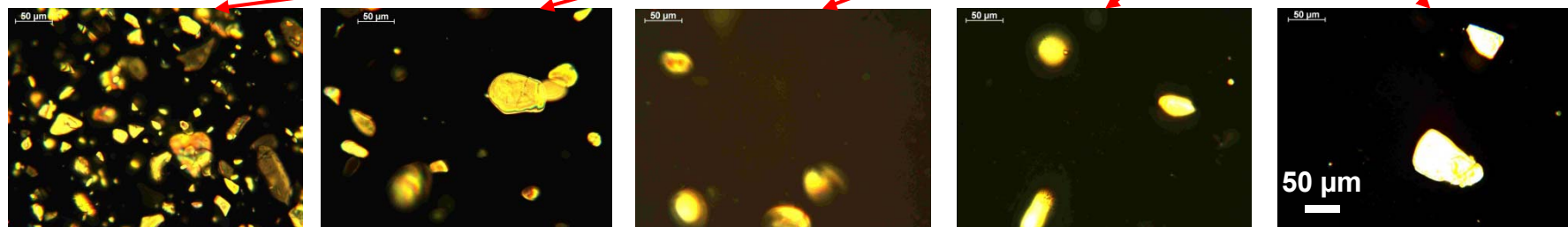
27

# Morphology Evolution (140 °C 50rpm 0.2kg/hr)

## One Strong Fully Filled F/R Kneading



## No Fully Filled F/R Kneading



Lobe  
no.

8

13

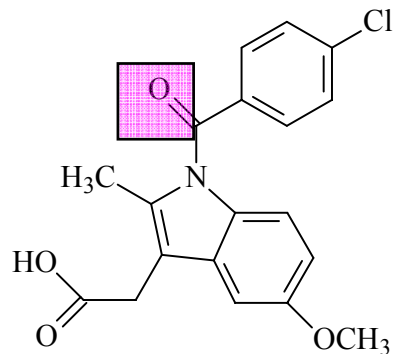
19

24

28

28

# Shift of the INM Benzoyl C=O Stretch Peak along the screw axial position

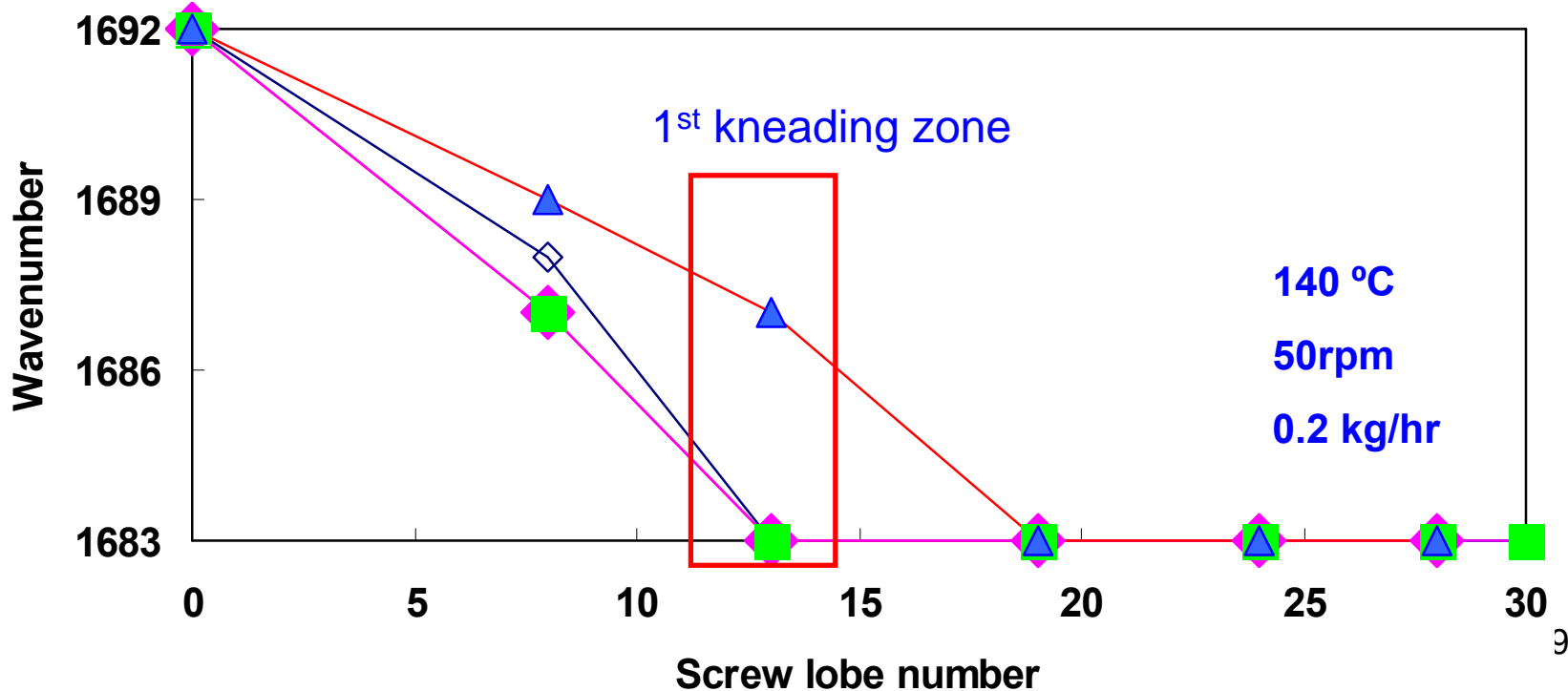


Benzoyl  $\nu$  C=O

1692  $\text{cm}^{-1}$  for  $\gamma$ - INM

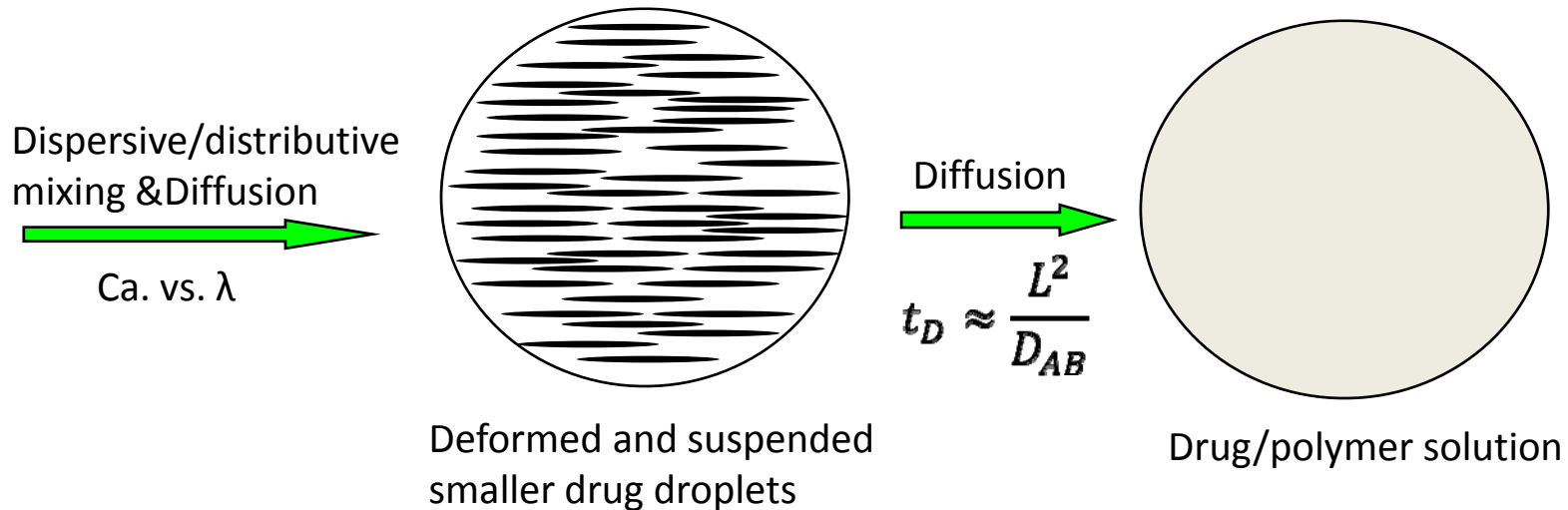
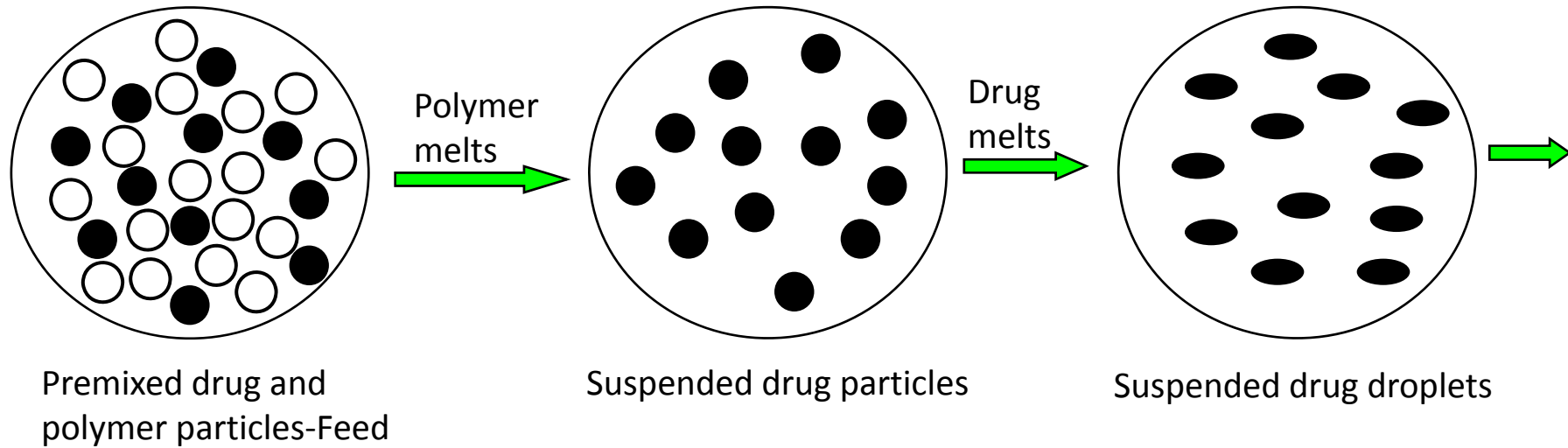
1683  $\text{cm}^{-1}$  for amorphous INM

(Taylor and Zografis, 1997)





$$T_{\text{processing}} > MT_{\text{polymer}} / T_g + 50 \sim 100 \text{ } ^\circ\text{C} \text{ and } T_{\text{processing}} > MT_{\text{drug}}$$



# Foam extrusion in drug delivery

## 1. Physical Blowing Agents as fugitive plasticizers:

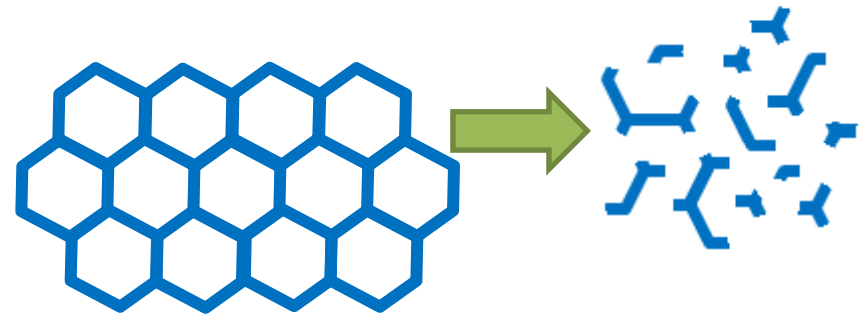
Processing temperature can be decreased without adding “dead weight” to the formulation and without affecting the long term stability and performance of the product.

## 2. Floating oral dosages:

Some APIs must be absorbed in the stomach due to therapeutic reasons or API's instability at higher pHs.

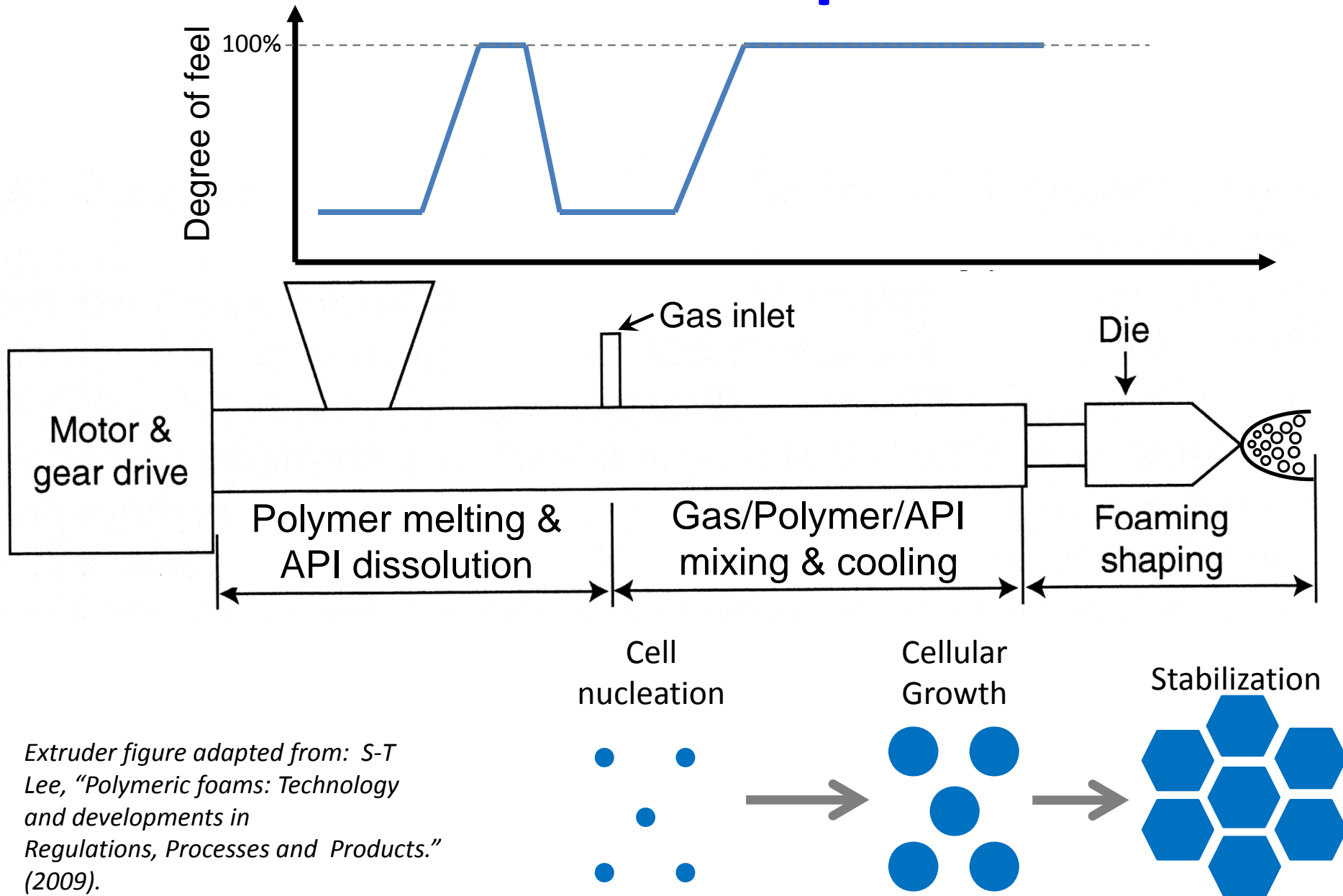
## 3. Foams to improve milling efficiency of HME products

By milling foamed structures it is possible to obtain **smaller particles** with **narrow** particle size **distribution** and **higher surface area**.



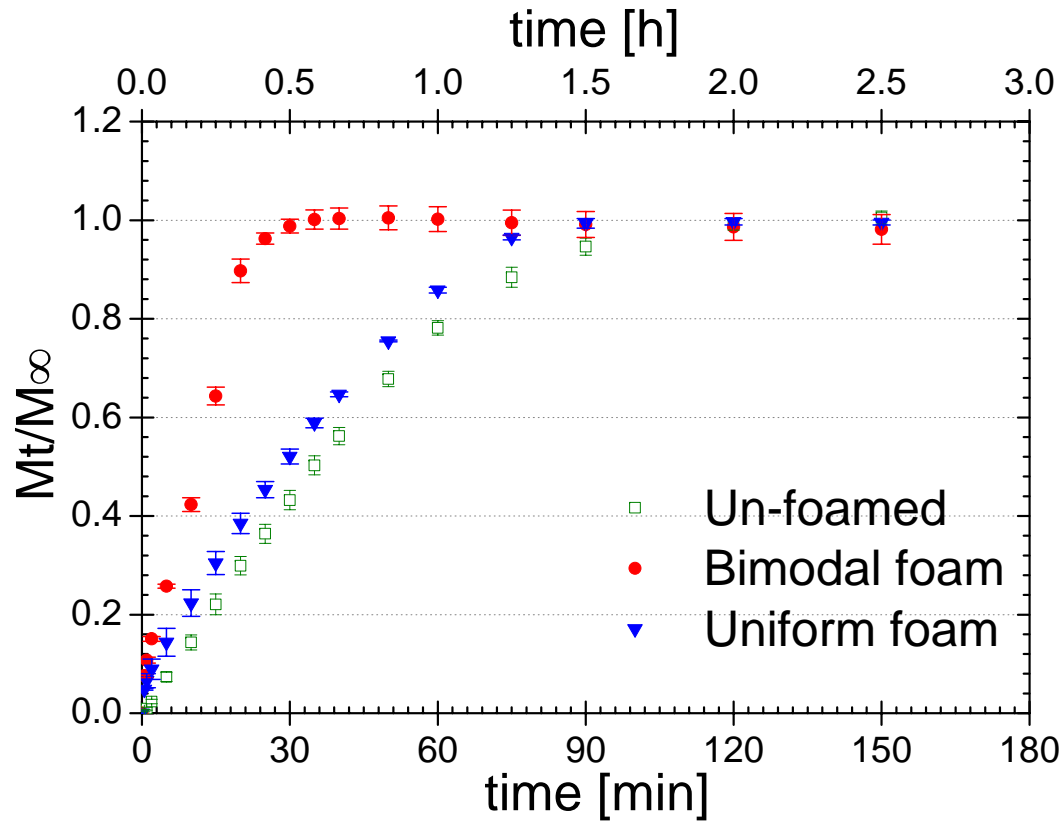
## 4. Increasing dissolution/release rate

# Foam extrusion process



Extruder figure adapted from: S-T Lee, "Polymeric foams: Technology and developments in Regulations, Processes and Products." (2009).

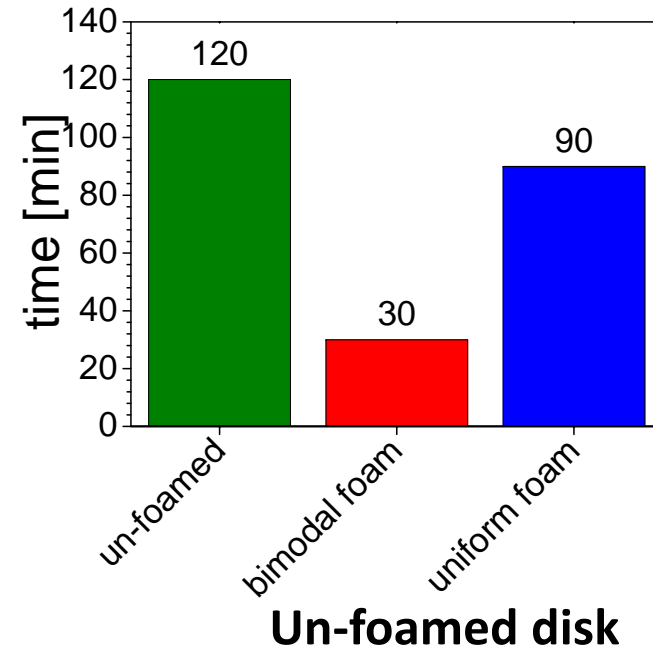
# INM's release Foam vs. Un-Foamed



Higher surface area & shorter diffusional lengths accelerate solvent absorption.

Random collapse and breakdown of cellular structure is key for an overall increase in release rate. This behavior is favored by non-uniform cellular structures

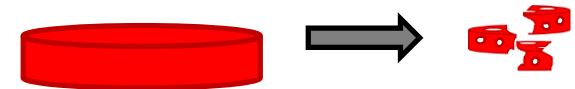
## TIME FOR COMPLETE INM'S RELEASE



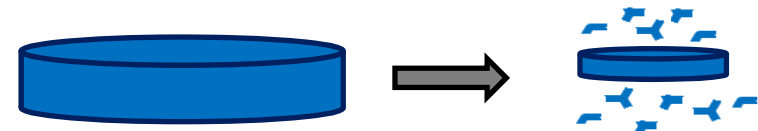
Un-foamed disk



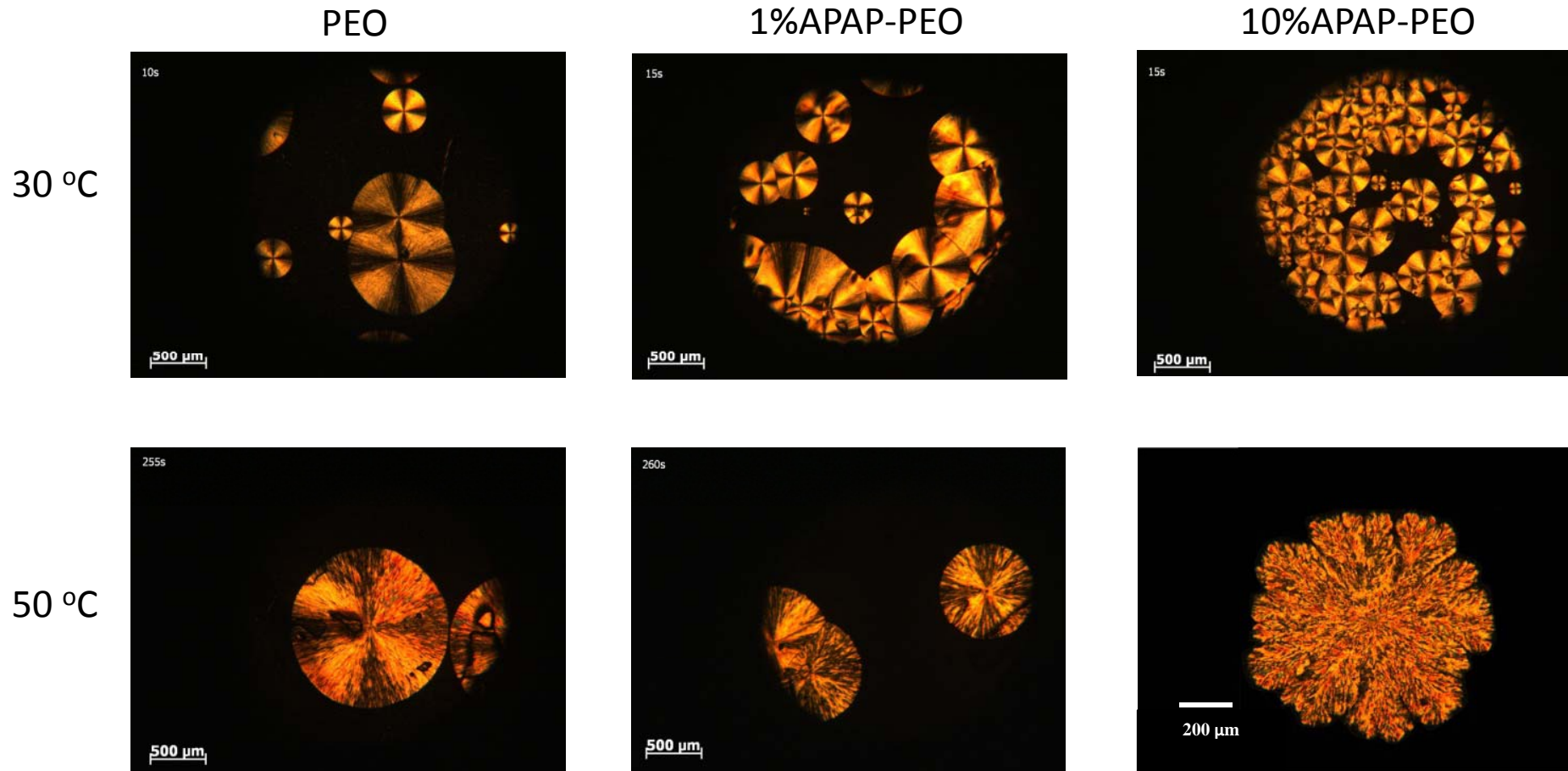
Bimodal foamed disk



Uniform foamed disk

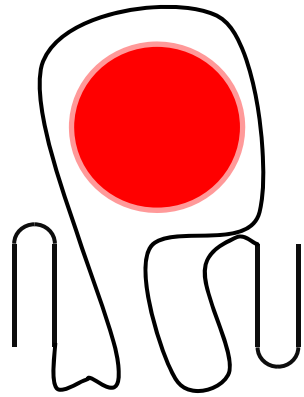


Determination of ambient temperature solubility for shelf life stability  
- spherulitic morphology and growth rate, number of spherulitic nuclei

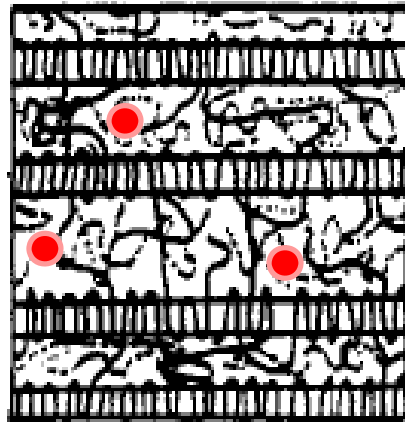


- @30 °C, # of spherulitic nuclei of 10%APAP-PEO >> PEO
- @50 °C, Maltese cross patterns and spherulite structure of 10%APAP-PEO was destroyed

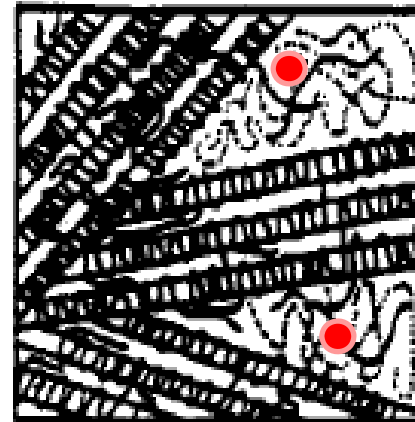
Possible modes of segregation in a binary blend that is miscible in the amorphous state and contains one crystallizing component



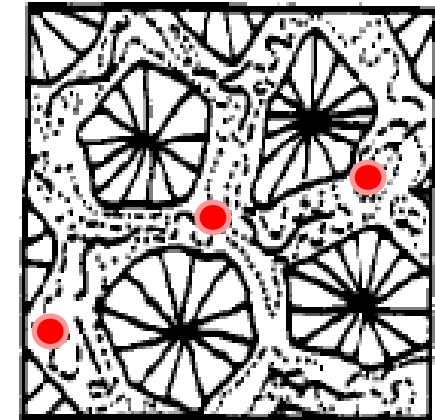
a. Intralamellar



b. Interlamellar



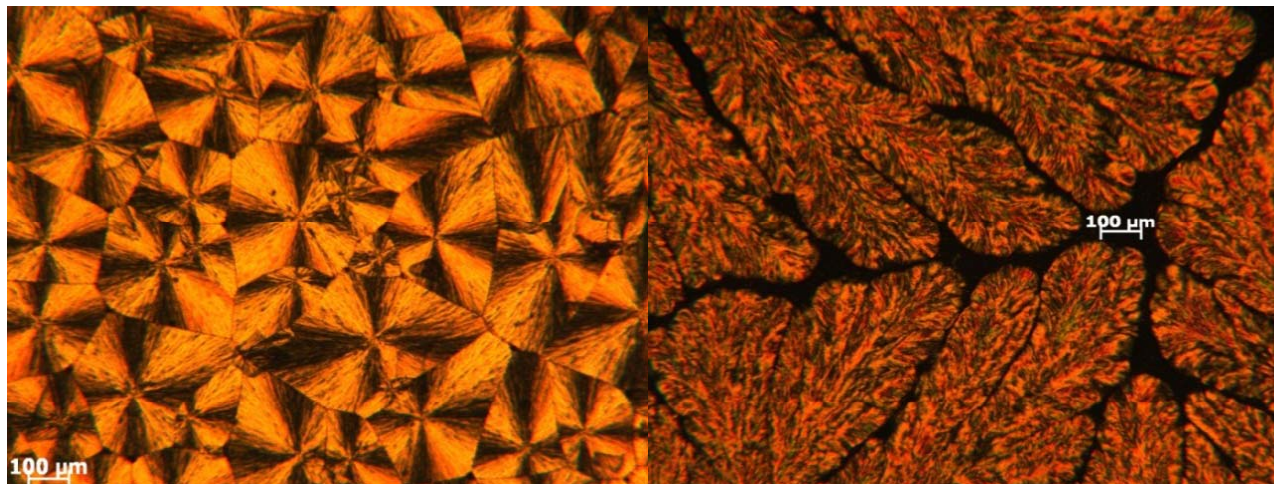
c. Interfibrillar



d. Interspherulitic

**APAP might locate between PEO spherulites (interspherulitic)@50 °C**

10%APAP-PEO  
@30 °C



10%APAP-PEO  
@50 °C

- Crevecoeur G, Groeninckx G. Binary blends of poly(ether ether ketone) and poly(ether imide): miscibility, crystallization behavior and semicrystalline morphology. *Macromolecules*. 1991; 24 (5): 1190-5.

# NJIT/PPI Center for Fundamental HME Studies

## NJIT

*Prof. Marino Xanthos*

*Dr. Huiju Liu Polymer – now at Honeywell*

*Dr. Nicolas Ioannidis*

*Prof. Costas Gogos*

- **PhD Students:**

*Dr. Min Yang – now at Evonik*

*Ms. Graciela Terife – studying HME foaming*

*Mr. Nonjaros Chomcharn – Studying the use of nanoclays*

## PPI

*Dr. Niloufar Faridi*

*Dr. Linjie Zhu*

*Dr. Herman Suwardie*