

Novel TNBC-targeted DOX-Arsonoliposomes

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Abstract: Arsonoliposomes (ARSL) constitute a particular class of liposomes that incorporate arsonolipids (ARS) in their membranes. ARSL realize selective toxicity to cancer cells, thus being an important tool in the treatment of cancer. Folic Acid (FA) is widely used in targeted drug delivery, due to its high affinity for the folate receptors that are overexpressed in cancer cell membranes. The aim of our studies was to develop novel TNBC-targeted ARSL, by incorporating folic acid-conjugated PEG-lipid in their membrane and loading them with anticancer drug doxorubicin (DOX). ARSL incorporating 0.1 mol% of FA-PEG-lipid (folate-PEG-DSPE) were prepared and loaded with DOX, using the active loading protocol. They were characterized for their size distribution, zeta potential and drug entrapment efficiency (%). Their cytotoxic activity towards TNBC cell lines, particularly MDA-MB-231 (epithelial human breast cancer cells) and MCF7 (Human breast cancer cells), was evaluated by the MTT-assay. The first results demonstrated enhanced toxicity of this novel type of ARSL towards cancer cells, which is particularly interesting and deserves further exploitation.

Keywords: arsonoliposomes; folic acid; doxorubicin; breast cancer; TNBC

1. Introduction

Arsonoliposomes (ARSL) are As(V)-containing vesicles that are composed of phospholipids, arsonolipids and cholesterol. Arsonolipids are analogues of phospholipids in which phosphorus has been replaced by arsenic in the lipid head group. It has been confirmed through in-vivo and in-vitro studies, that specific toxicity towards cancer is shown, and that ARSL are more toxic towards cancer cells, compared to normal cells. Recently, the loading of DOX into ARSL revealed that interesting synergistic effects may be demonstrated [1].

Folic acid receptor (FR)- α is a glycosylphosphatidylinositol-anchored membrane protein that is overexpressed in many human cancer cells, while it shows limited expression in normal cells. [2] Folic acid (FA) is used in drug delivery systems, as a tumor-targeting ligand, causing receptor-mediated endocytosis through binding of the folate conjugates to the folate receptor (FR) with high affinity, enabling nanoparticles to accumulate into cancer cells. [3]

Thus, based on all mentioned above we attempted to develop novel DOX-loaded ARSL that incorporate folic acid-conjugated PEG-lipid in their membrane in order to target the triple negative cancer cells (TNBC).

2. Experiments

Materials

1,2-Distearoyl-sn-glycerol-3-phosphatidyl-choline [DSPC] and 1,2-Distearoyl-sn-glycerol- 3-phosphatidyl-ethanolamine-N-[methoxy(polyethylene-glycol)-2000] [PEG2000] were purchased from Lipoid, Germany. Cholesterol (Chol) was purchased from Sigma-Aldrich (Darmstadt, Germany). The rac-2,3-dipalmitoyl-oxypropylarsonic acid [ARS] (C16), was synthesized as described [1]. 1,2-distearoyl-*sn*-glycero-3-phosphoethanolamine-N-[folate(polyethylene glycol)- 2000] [DSPE-PEG2000-FA] was synthesized in our laboratory. Doxorubicin, hydrochloric salt (DOX) was purchased by Tocris Bioscience, UK.

For the preparation of liposomes a bath sonicator (Branson) and a microtip-probe sonicator (Sonics and Materials, Leicestershire, UK) were used.

All other reagents and solvents used throughout the study were of analytical grade and were purchased from Sigma–Aldrich. All media used for cell growth and handling were purchased from Biochrom (Berlin, Germany).

Methods

2.1. Preparation of liposomes and Loading of DOX

Liposomes of the following compositions were used in this study: (a) folate-PEG- arsonoliposomes composed of DSPC/ARS/Chol/ DSPE-PEG2000-MeO /folate-PEG-DSPE (12:8:10 mol/mol containing 8 mole% PEG2000 and 0.1 mole% folate-PEG-DSPE) and (b) control (non-targeted) ARSL composed of DSPC/ARS/Chol/DSPE-PEG2000-MeO (12:8:10 mol/mol containing 8 mole% PEG2000). Both liposomes were prepared by the thin-film-hydration method followed by probe sonication for size reduction. [1] The thin film is hydrated with 1 mL of ammonium sulfate solution (120 mM, pH 5.5, 300 mOsm) at 60°C, and the ARSL suspension was sonicated with probe sonicator (Sonics and Materials, Leicestershire, UK) for approximately 10 min, until the dispersion became completely clear. ARSL were purified from non-encapsulated ammonium sulfate by repeated ultracentrifugations for 1 h (each) at 60,000 rpm (Sorvall WX90 Ultra, Thermo Scientific, Waltham, MA, USA), and resuspended in PBS pH 7.4, for exchange of the dispersion media. At a lipid concentration of 1.4 mg/mL (in PBS) they were then incubated with 0.2 mg/mL DOX solution (in PBS) (corresponding to a lipid/DOX ratio equal to 7:1 [w/w]) for 60min at 60°C, for active loading of DOX. [1] Afterwards, the ARSL were purified from non-encapsulated drug by two repeated ultracentrifugation steps (60,000 rpm for 1 h, each) and both the supernatants containing non-encapsulated DOX. The lipid content of the samples was routinely determined using a colorimetric technique, which is widely applied for phospholipids, the Stewart assay. [4]

2.2. Physicochemical Properties of Liposomes

The ARSL prepared were characterized by measuring their size distribution, mean diameter and zeta-potential by DLS (dynamic light spectroscopy) with a Malvern Zetasizer 5000 (Malvern, UK). For measurement of their size, the ARSL dispersions were diluted with PBS pH 7.4 to a final concentration of 0.4 mg/mL. The electrophoretic mobility of the ARSL dispersions was measured at 25 °C, by the same instrument and zeta potential of the dispersions were calculated by application of the Helmholtz–Smolowkowski equation.

To estimate the drug concentration, DOX calibration curves in the concentration range between 5 and 40 µg/mL were prepared, and the final D/L ratio (w/w) was estimated and compared with the initial one, for calculation of the DOX encapsulation efficiency (%) of each liposome type, according to Equation (1):

$$EE (\%) = \frac{D/L_{final}}{D/L_{initial}} \cdot 100 \quad (1)$$

2.3. Cell Culture Studies

Two types of cells were used in this study: (i) MDA-MB-231 (epithelial human breast cancer cells), and (ii) MCF7 (Human breast cancer cells). The cancer cells were grown in RPMI 1640 medium supplemented with 10% FBS and 1% antibiotic-antimycotic solution (Invitrogen, Carlsbad, CA, USA). The cells were cultured at 37 °C, 5% CO₂/saturated humidity. Medium was changed every 2–3 days.

The toxicity of the various types of ARSL towards cancer cells was evaluated by the corresponding reduction of cell viability after 24 h incubation with ARSL or PBS by the MTT assay. For each experiment, cells were seeded overnight at 37 °C at a density of 5 × 10⁴ cells per well, in 24-well plates and then incubated for 24 h at 37 °C (5% CO₂/saturated humidity) with 0.4 mL growth medium and 0.1 mL of the formulation evaluated in each case. Viability (%) was calculated by the equation (2):

$$\text{Viability (\%)} = \frac{OD-570_{\text{sample}} - OD-570_{\text{background}}}{OD-570_{\text{control}} - OD-570_{\text{background}}} * 100 \quad (2)$$

where, OD-570_{control} corresponds to untreated cells (or PBS control) and OD-570_{background} to MTT without cells. All samples were diluted in order to achieve DOX concentrations of 1 μM and 3 μM.

For evaluation of DOX-uptake of ARSL (targeted or not) by cultured MDA-MB-231 and MCF7 cells, cells were seeded overnight at density of 12 × 10⁴ cells/mL per well in 12-well plates in RPMI at 37 °C (5% CO₂/saturated humidity), and then incubated with DOX liposomes for 1 h. DOX concentration was 10 μM (non toxic for 1h incubation). After treatment, the cells were washed twice with PBS, and then detached and lysed by the addition of 0,9 ml of PBS and 0,1 ml of Triton X-100 (20%). The samples were collected and their fluorescence intensity was measured (EX 490 and EM 520 nm). The protein concentration in every sample was measured by the Bradford microassay. Finally, DOX uptake by cells was expressed as % Uptake/Protein (by comparison of the DOX measured in the cells and the total amount of DOX incubated with the cells).

3. Results

3.1. Physicochemical Properties of Liposomes

All liposome dispersions were characterized for their size distribution (mean hydrodynamic diameter and polydispersity index), and their zeta-potential and the results are presented in Table 1.

Table 1. Physicochemical properties of ARSL and FA-ARSL before and after DOX loading, formulated in PBS buffer (pH 7.40).

Formulations	Mean Hydrodynamic Diameter (nm)	PI	ζ-Potential (mV)	DOX Loading (%)
ARSL	118.9 ± 0.8	0.231	-6.73 ± 0.29	-
DOX-ARSL	143.1 ± 1.8	0.421	-6.35 ± 0.59	94.9 ± 1.8
FA-ARSL	113.6 ± 1.4	0.265	-7.32 ± 0.64	-
DOX-FA-ARSL	126.9 ± 0.6	0.410	-8.78 ± 0.54	95.9 ± 2.4

The mean hydrodynamic diameter of all ARSL was in the nano-range, between 113 and 143 nm. The polydispersity index values were between 0.231 and 0.421 for all ARSL, the lowest for ARSL and

the highest for DOX- FA-ARSL. All samples were monodisperse as observed in DLS reports (non-shown). The addition of FA-lipid doesn't seem to alter the vesicle mean diameter and the PDI. However, DOX-ARSL appear to have increased mean diameter and PDI, compared to all other formulations. Results of zeta potential measurements were in the range between -6.35 and -8.78 mV, which are anticipated (low negative values) due to pegylation. The loading of DOX was achieved in all ARSL types and loading EE% ranged between 95% and 96% when the incubation of DOX with empty vesicles was carried out at 60°C . There is no significant difference in DOX-loading values between arsonoliposomes and FA-arsonoliposomes (Table 1), suggesting that the addition of FA-lipid doesn't affect the loading capacity of the vesicle.

3.2. *In vitro* Toxicity

The cytotoxicity of DOX-ARSL and DOX-FA-ARSL was carried out with two cancer cell lines, MDA-MB-231 and MCF7 cells. The appropriate D/L ratios were used for preparation of the DOX-loaded liposomes, specifically a 0.05 mole/mole ratio in order to have $1\mu\text{M}$ of DOX. As seen on Figure 1.A a higher anticancer effect of DOX-FA-ARSL is evident towards MDA-MB-231, compared to all other formulations, a result consistent with the fact that these cells are known to have high FR expression. On the contrary, DOX-FA-ARSL anticancer activity towards MCF7 cells, was not significantly different than that of the other formulations (non-targeted), which is logical since these cells do not overexpress the FR receptor (Fig. 1.B).

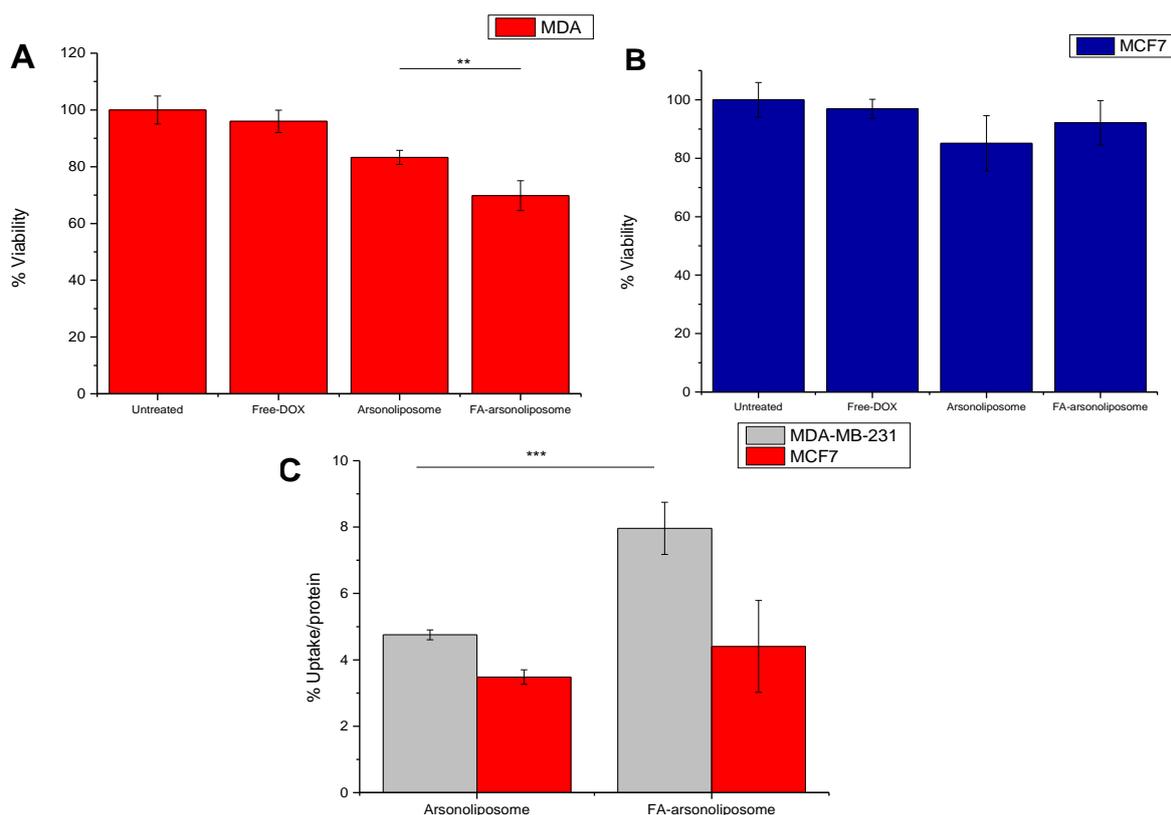


Figure 1. Viability of cells after incubation with DOX-ARSL, DOX-FA-ARSL and Free-DOX $1\mu\text{M}$ for 24 h. (A) MDA-MB-231 (B) MCF7. (C) Uptake of DOX by MDA-MB-231 and MCF7 cells, after 1 h of co-incubation of cells with DOX- ARSL (targeted and non-targeted). **corresponds to $p < 0.01$. *** corresponds to $p < 0.001$

The previous results are verified also by the DOX uptake results for the two cell types, which are in good agreement with the viability results. Indeed, as seen in Figure 1.C., the uptake of DOX by

MDA-MB-231 cells is substantially increased when DOX-FA-ARSL are used compared to non-targeted ARSL; while a similar effect was not observed in the case of the MCF7 cells.

4. Discussion

Herein, we investigated the potential of novel TNBC-targeted ARSL, by incorporating folic acid-conjugated PEG-lipid in their membrane and loading them with the anticancer drug DOX. Both, ARSL and FA-ARSL had mean diameters in the nano-range, between 120 and 143 nm (Table 1), polydispersity values below <0.4, and slightly negative zeta potential values, and could be efficiently loaded with DOX by an active-loading method.

The in vitro experiments on the cancer cells MDA-MB-231 and MCF7, two of the most commonly studied TNBC cell lines, presented hopeful results. The uptake of DOX by MDA-MB-231 cells, is significantly higher from targeted ARSL (with 0.1%FA) compared with non-targeted ones, suggesting that ARSL can be targeted using folic acid as a ligand. Moreover, the cytotoxic effect of DOX-FA-ARSL towards cancer cells was higher than that of free DOX and DOX-ARSL, indicating the importance of combining both compounds in the same vesicular structure.

5. Conclusions

The current results indicate the potential antitumor properties of the novel folic acid targeted ARSL that incorporate Doxorubicin towards Triple-negative breast cancer (TNBC), which merits further study in the future.

Acknowledgments: This research has been co-financed by the European Regional Development Fund of the European Union and Greek national funds through the Operational Program Competitiveness, Entrepreneurship and Innovation, under the call RESEARCH – CREATE – INNOVATE (project code: MIS5031802).

Author Contributions: S.G.A conceived the experiments and got the funding. S.M designed the synthesis of DSPE-PEG-FE lipid and the molar composition of each liposome. F.G. designed and helped with the execution of the cell experiments. P.Z conceived the experiments regarding the cells and the loading of drug into arsonoliposomes. M.M performed all the experiments needed together with E.L; M.M. wrote a first draft of the paper. M.M, F.G and E.L gathered and analyzed the data. S.A corrected the draft paper and wrote the final version.

Conflicts of Interest: The authors declare no conflict of interest. The funders had no role in the design of the study; in the collection, analyses, or interpretation of data; in the writing of the manuscript, and in the decision to publish the results.

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