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In-Ear Energy Harvesting : Harvester Design and Validation (Part II)

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Aidin Delnavaz², Jérémie Voix²

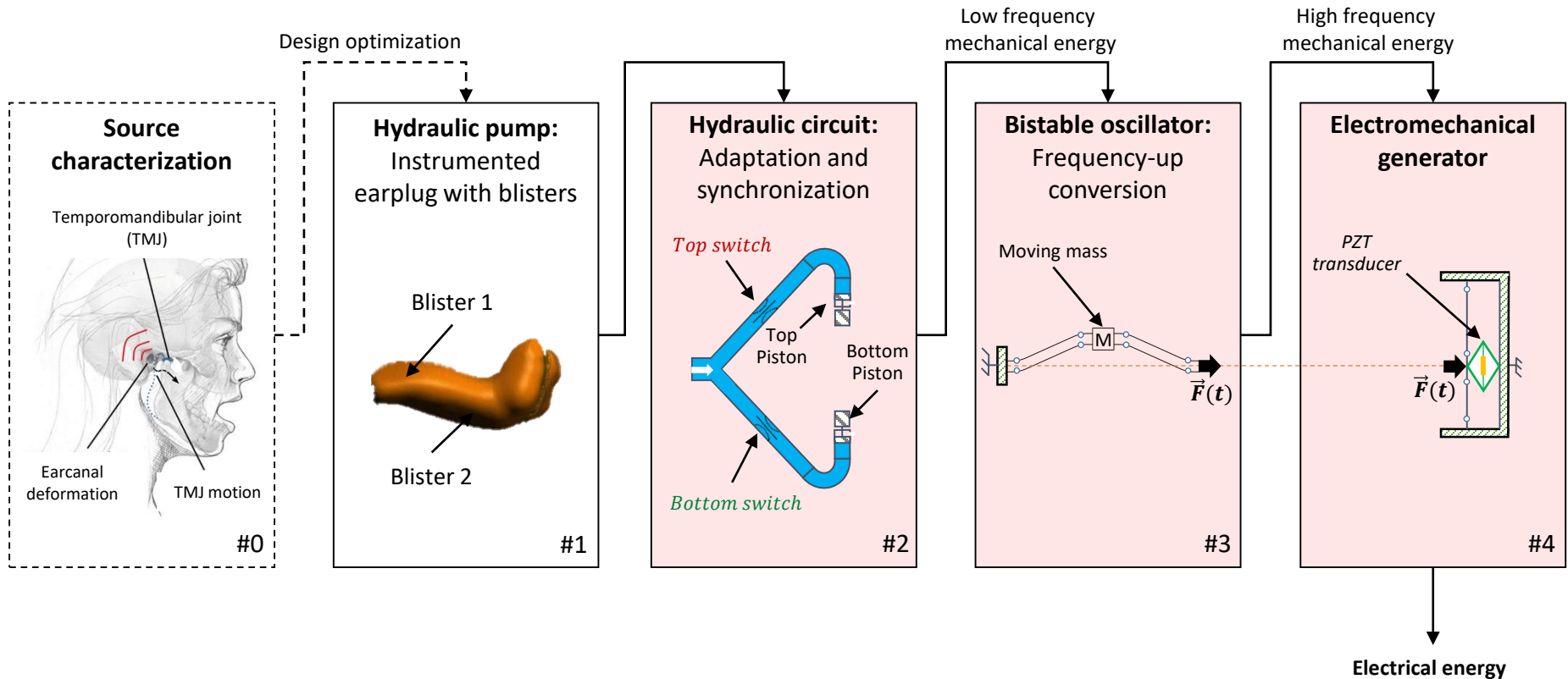


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Graphical abstract



Keywords: Ear; energy harvesting; generators; frequency-up; bistable oscillator; hydraulic transmission; passive hydraulic switches;

Abstract

The earcanal mechanical deformation induced by the temporomandibular joint movement constitutes a promising source of energy to power in-ear devices (hearing aids, communication earpieces, etc.). The large morphological variability of the human earcanal and its intrinsic dynamic characteristics - with displacement frequencies below 1.5 Hz with average volume variation of 60 mm^3 - motivate the development of non-conventional dedicated energy harvesting methods. This paper demonstrates the concept and design of a modular hydraulic-piezoelectric self-actuated frequency up conversion micromachine for energy harvesting. The mechanical energy is conveyed using a liquid-filled custom fitted earplug, which can be considered as a hydraulic pump. A dedicated hydraulic circuit drives two micro-pistons (MP) while ensuring the impedance matching between the earplug available pressure and swept volume and the MP required displacement and force. These MP actuate a mechanical oscillator associated to a piezoelectric transducer allowing the low frequency mechanical excitation to be efficiently converted into electric energy through frequency up-conversion. An innovative mechanical feedback selects the actuated MP depending on the mechanical oscillator position. By doing this, each jaw motion can be harvested. A complete theoretical multiphysics model of the machine has been established for the design and evaluation of the potential of the proposed approach. Global analytical and refined FEM approaches have been combined to integrate the fluid and mechanical behaviors. Based on simulation and preliminary experimental data, the harvested energy is expected to be $10 \text{ }\mu\text{J}$ for one jaw closing, with a theoretical 50 % end-to-end conversion efficiency.

Keywords: Ear; energy harvesting; generators; frequency-up; bistable oscillator; hydraulic transmission; passive hydraulic switches;

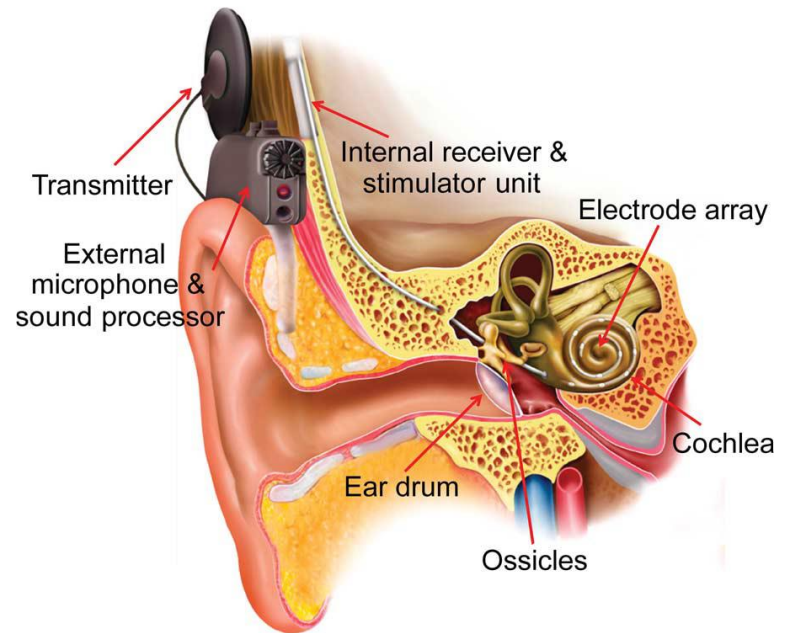
Need for energy supply around ears

Daily energy consumption ≈ 72 J



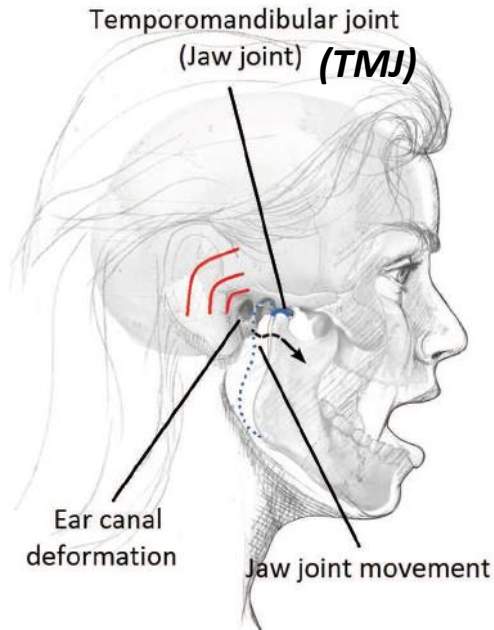
ReSound hearing aid
LYNX Quattro model [1]

Daily energy consumption ≈ 21 J

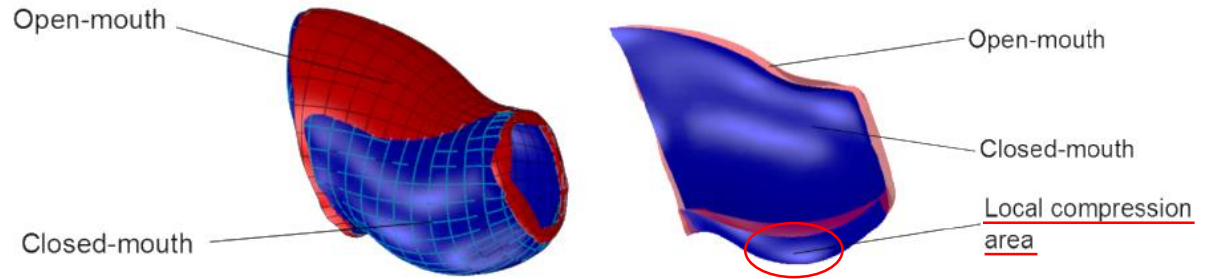


Block diagram of a conventional cochlear implant [M. Yip & al., 2015 [2]].

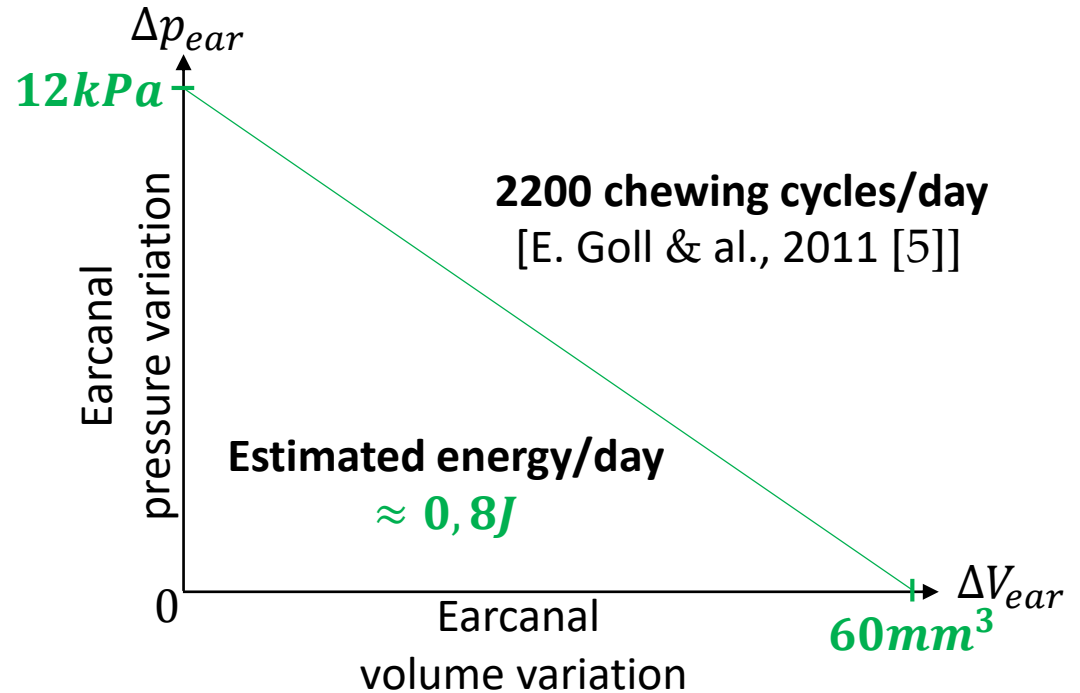
Earcanal = energy source



[A. Delnavaz & J. Voix, 2016 [3]]



[J. Carioli & al., 2016 [4]]



Introduction

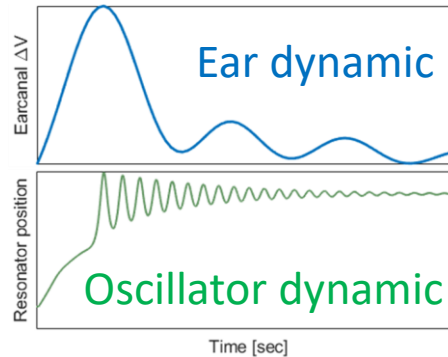
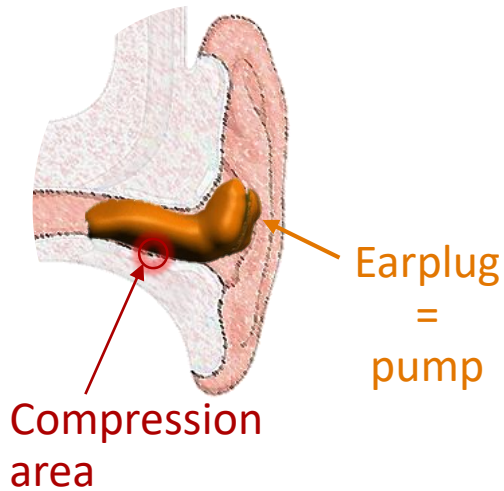
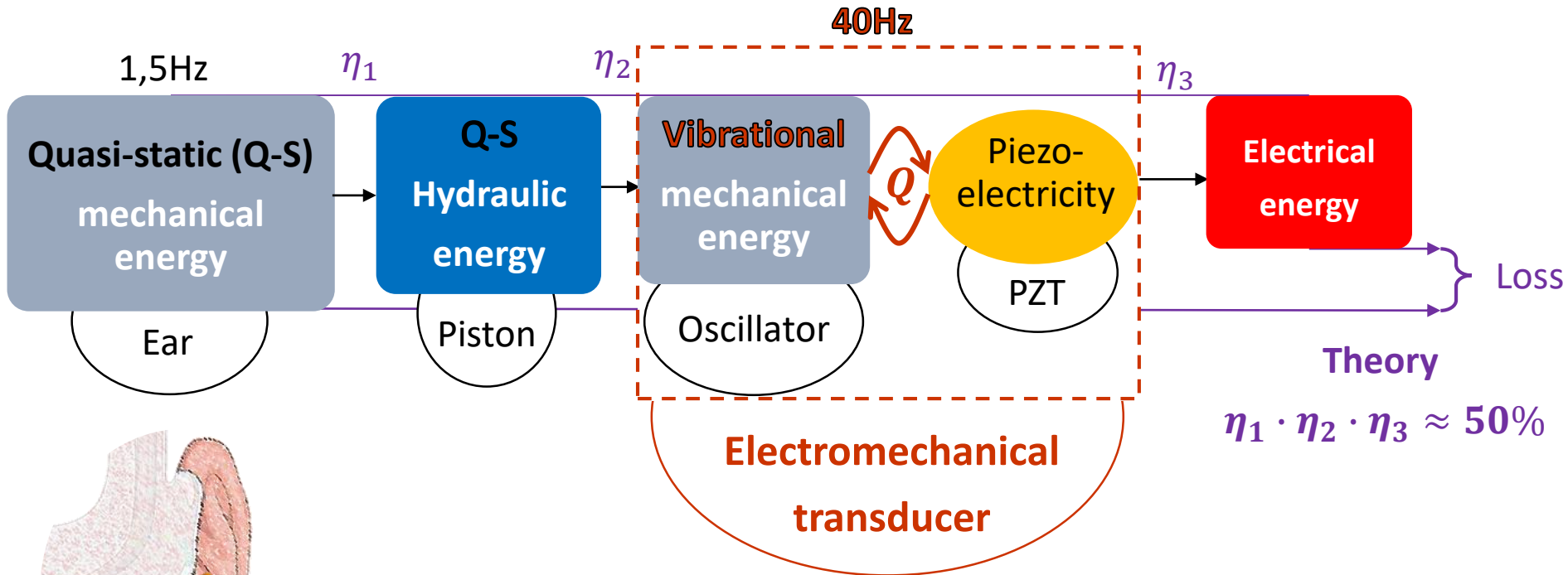
I. Harvesting strategy

II. System presentation : Specifications and design

III. Multiphysic system simulations

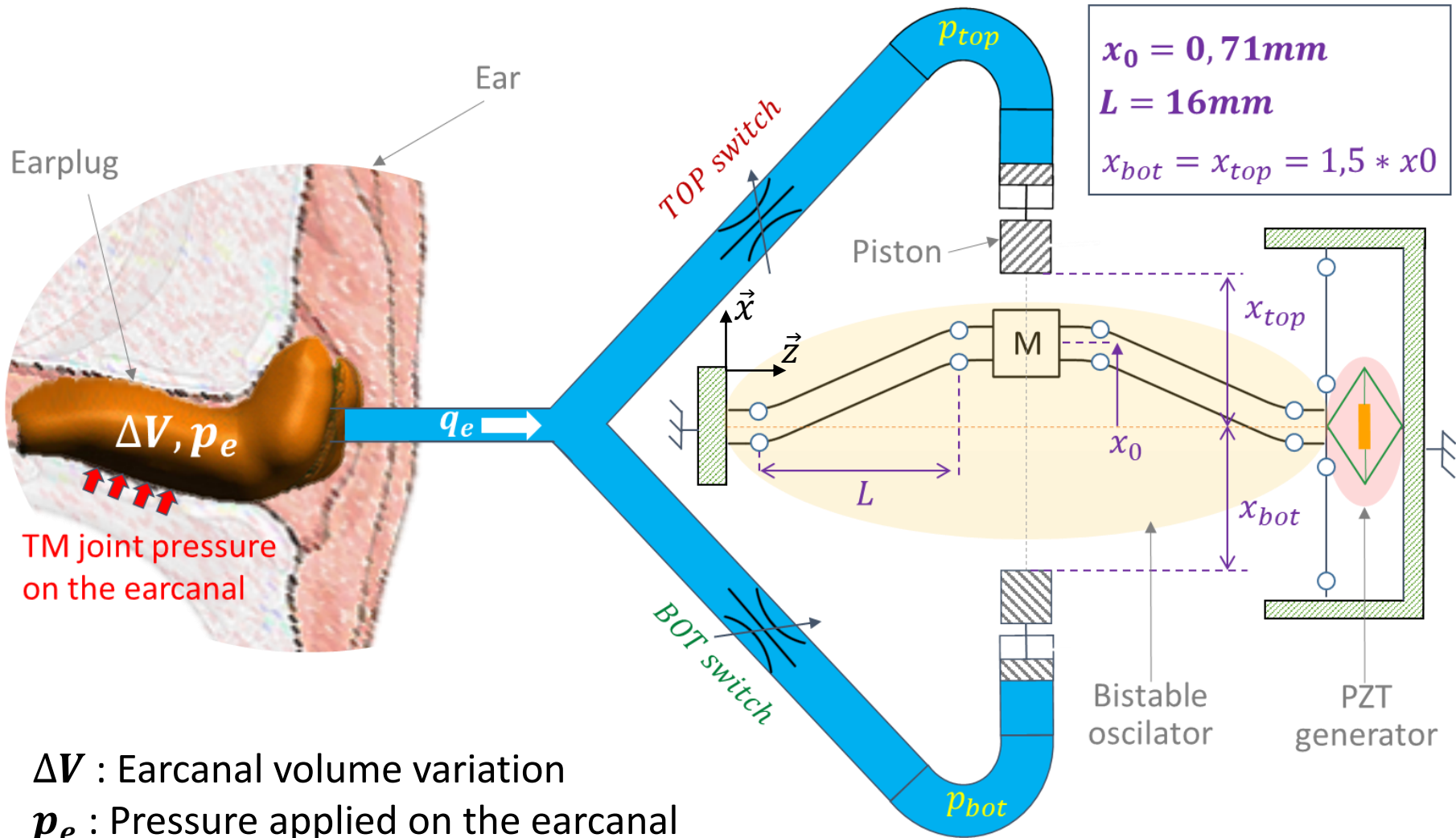
IV. Experimental characterizations

Energy harvesting strategy



$$\frac{k^2_{PZT}}{k^2_{PVDF}} > 10$$

Global system overview

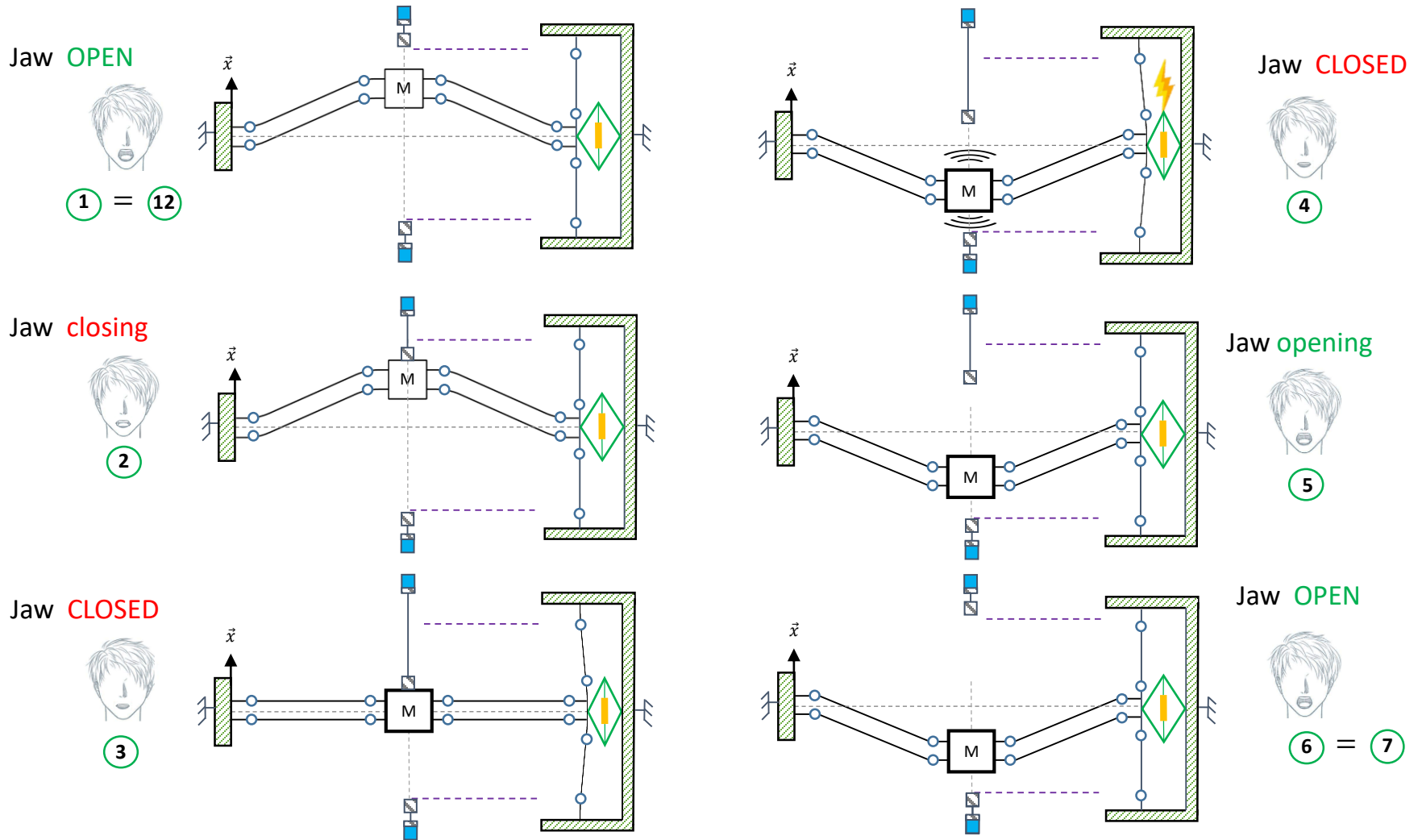


ΔV : Earcanal volume variation

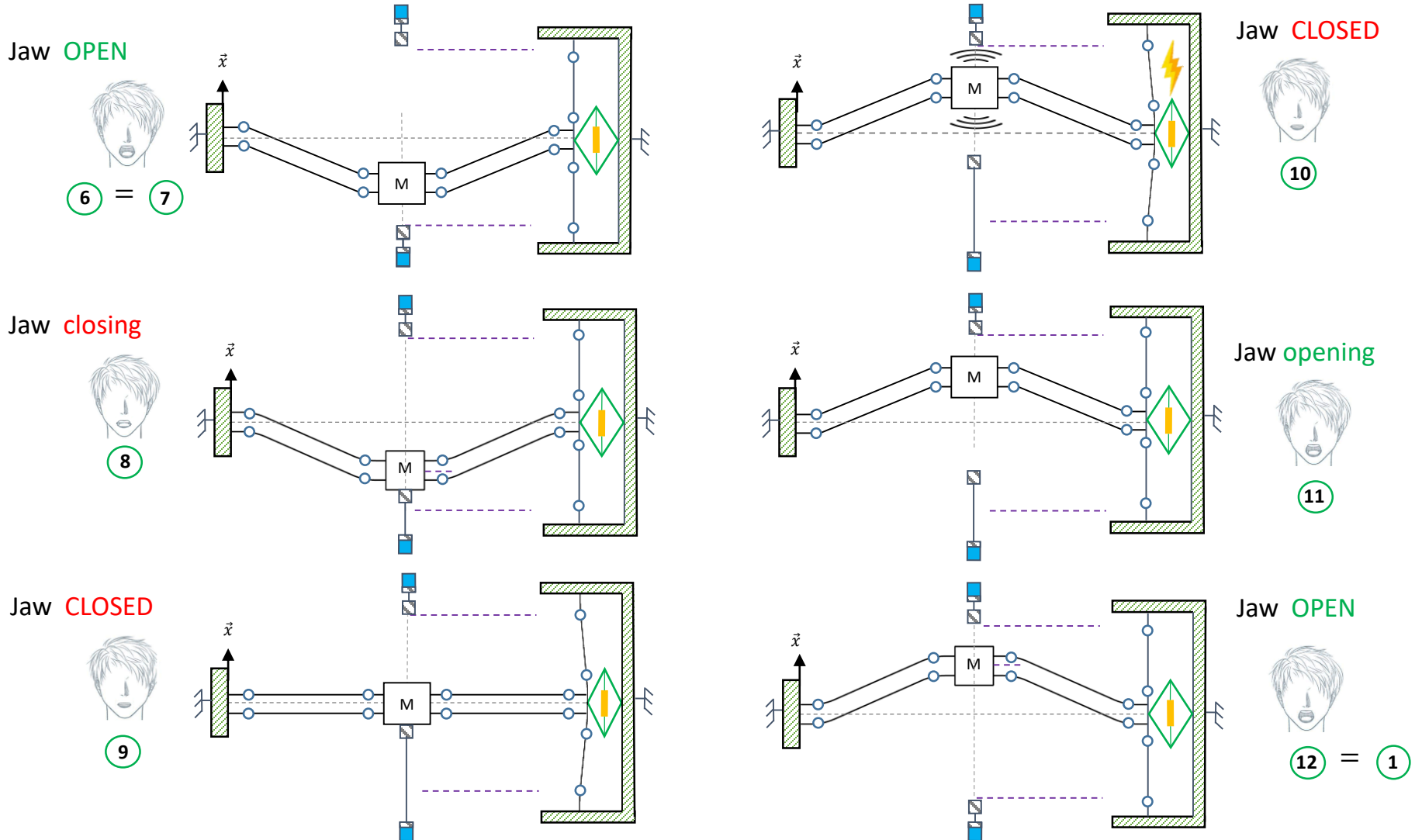
p_e : Pressure applied on the earcanal

q_e : Earplug fluid flow rate

System operation dynamics: Upward actuation

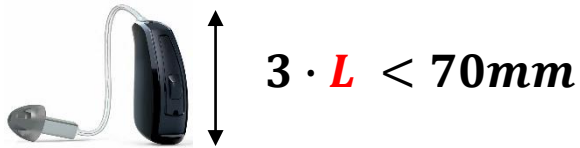


System operation dynamics : Downward actuation

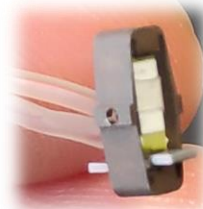


Design specifications

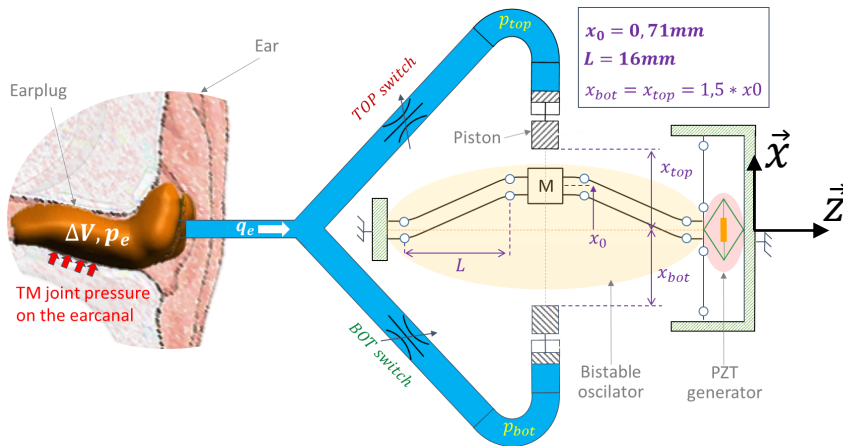
Space requirements



Transducer choice



K : Stiffness
 C_0 : Capacity
 k_e^2 : EM coupling



Buckling level

$$p_{ear(comfort)} = \frac{2 \cdot K \cdot x_{0(max)}^3}{3 \cdot \sqrt{3} \cdot L^2 S_{piston}}$$

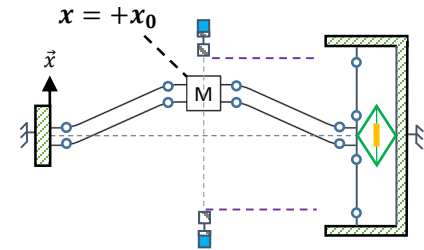
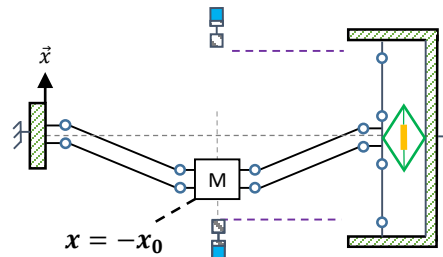
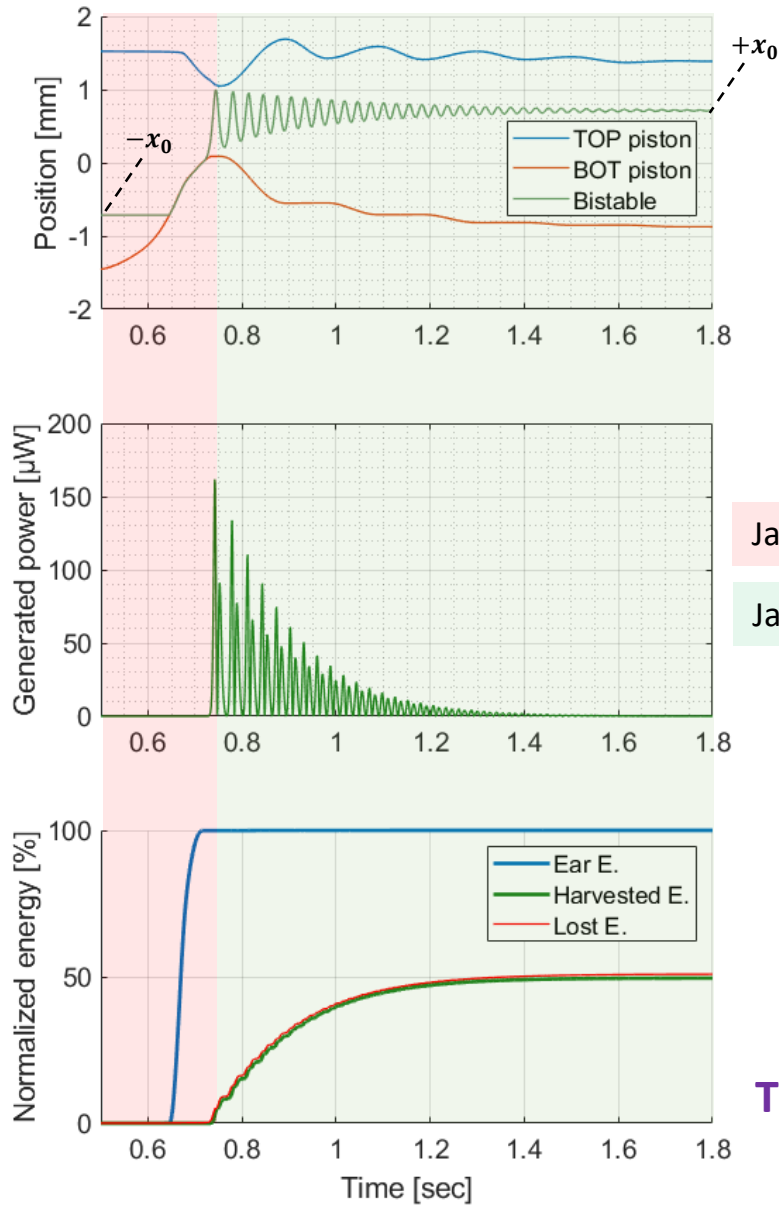
$$I = \left(\sqrt{k_e^2 \cdot K \cdot C_0} \right) \cdot \frac{x_M \cdot \dot{x}_M}{L} - C_0 \cdot U_p$$


Generated power : $P = U_p \cdot I$


Pistons

$$S_{piston} \cdot 1,5 \cdot x_{0(max)} < \Delta V_{ear}$$

Multiphysics system simulation

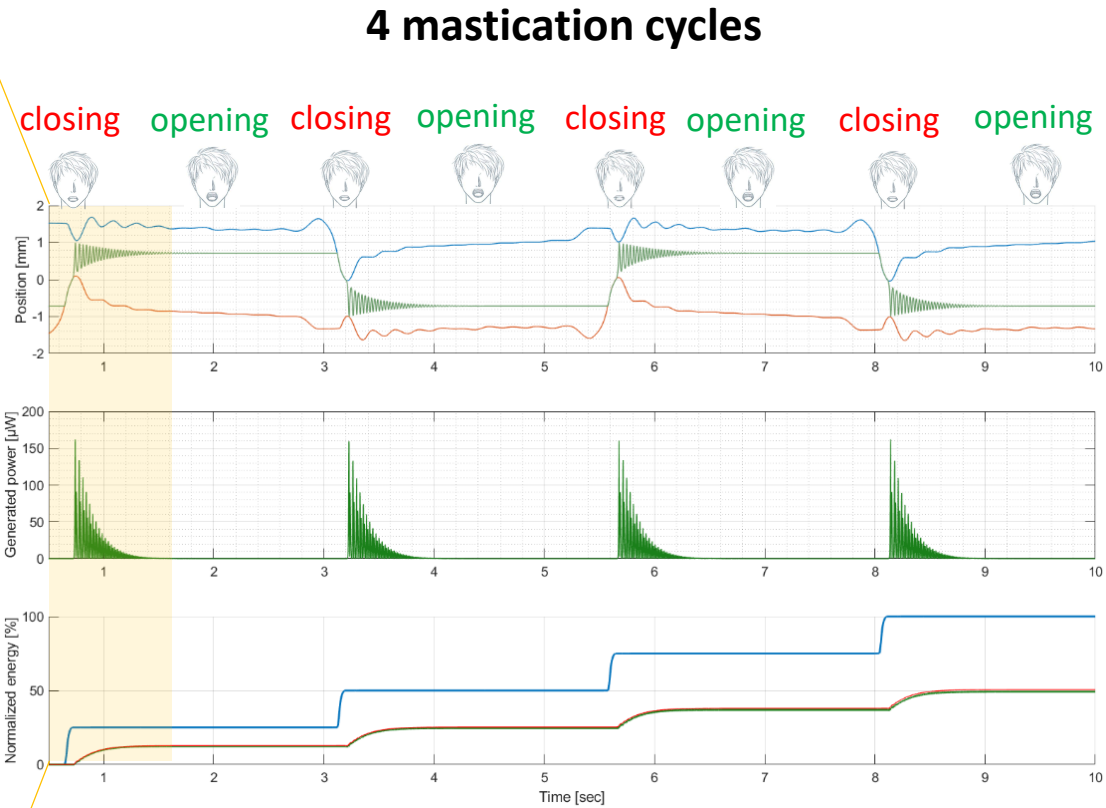
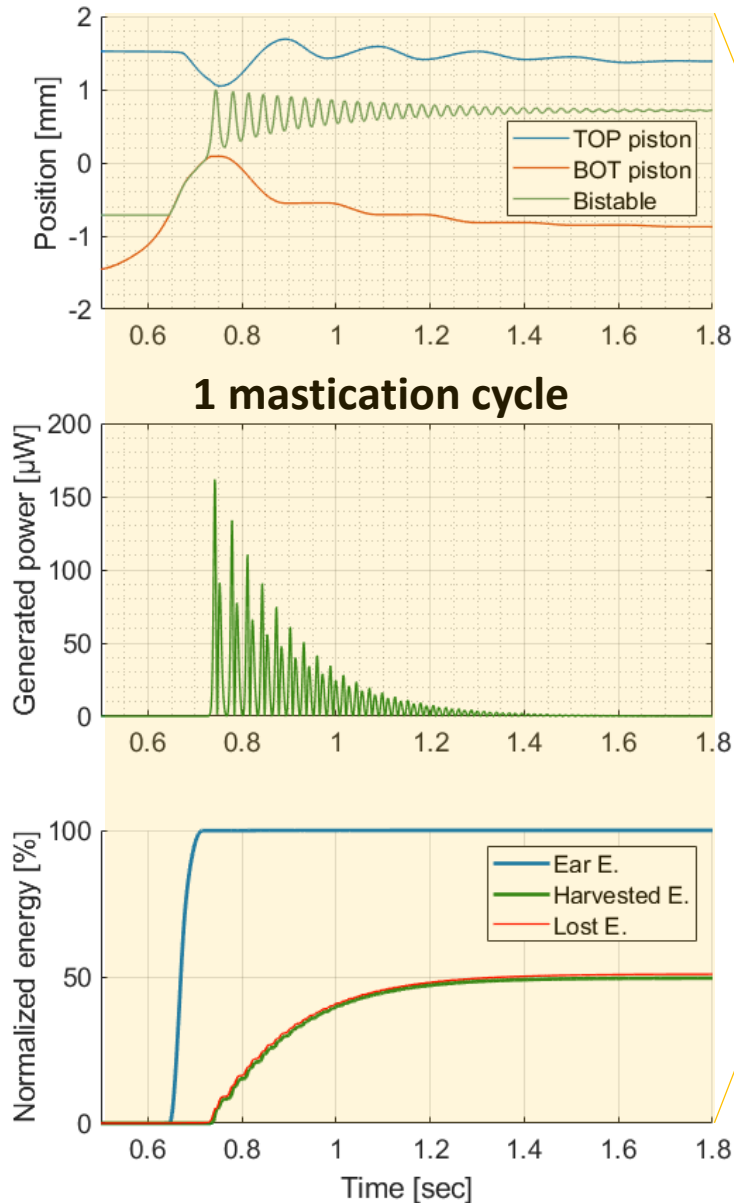


Jaw closing 

Jaw opening 

Theoretical efficiency $\approx 50\%$

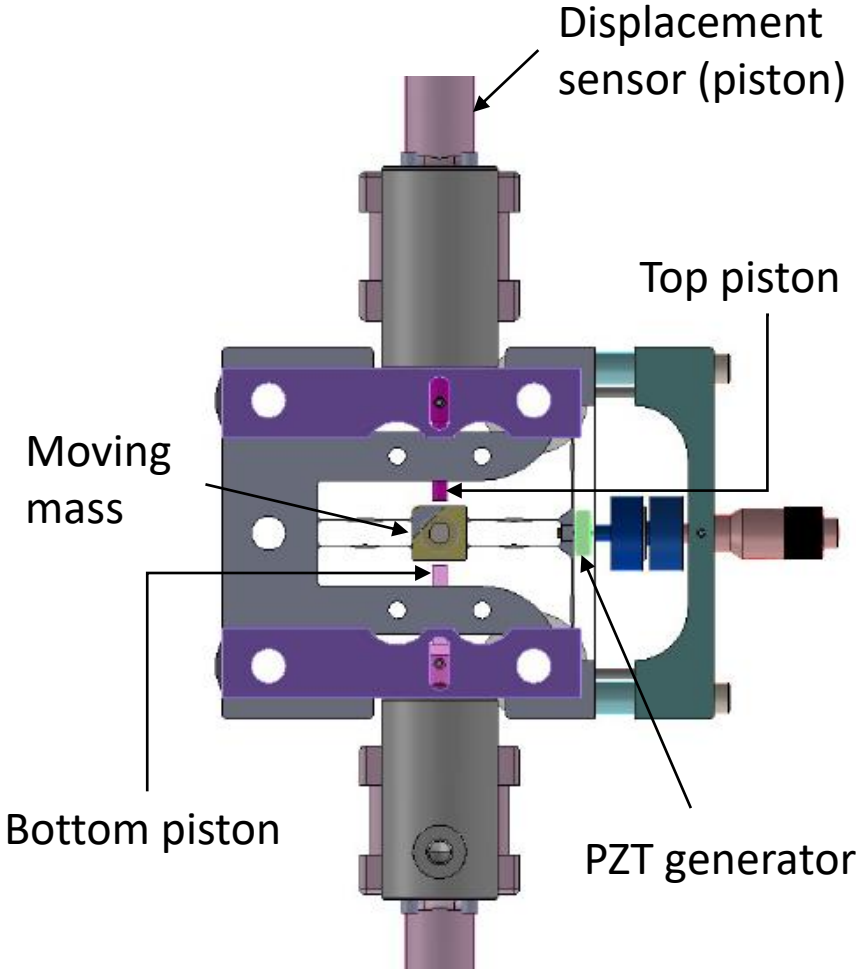
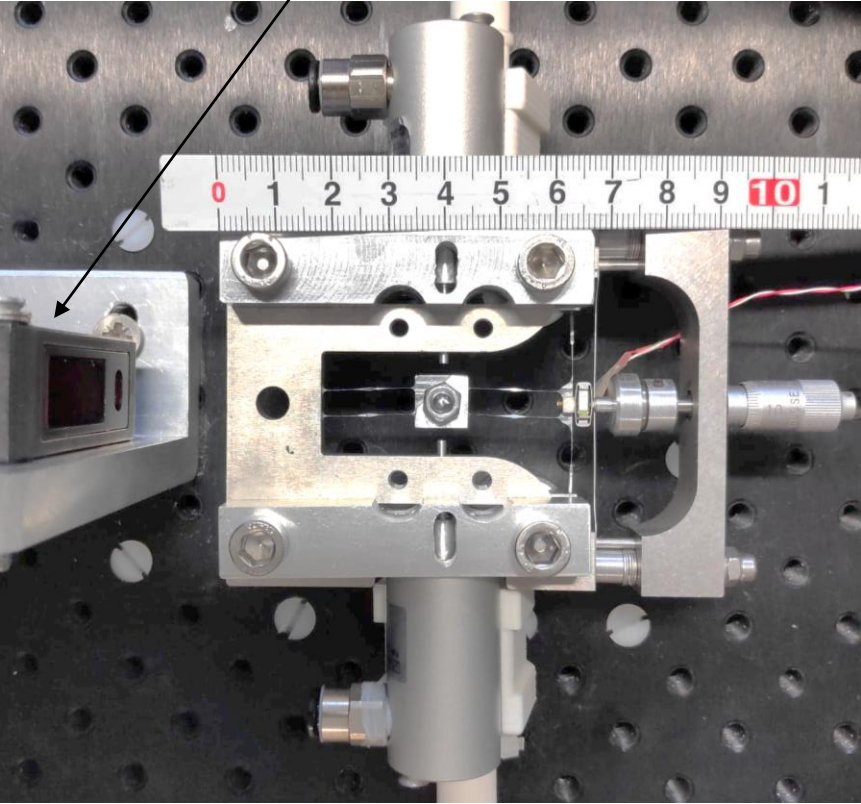
Multiphysics system simulation



Theoretical efficiency $\approx 50\%$

Oscillator with the generator

Displacement sensor (mass)

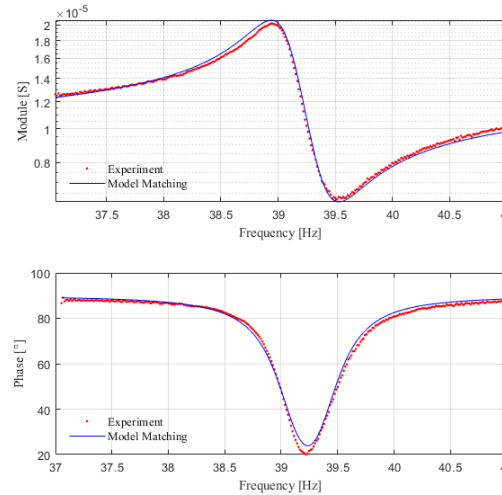


Experimental characterizations : Resonator behavior

Test conditions

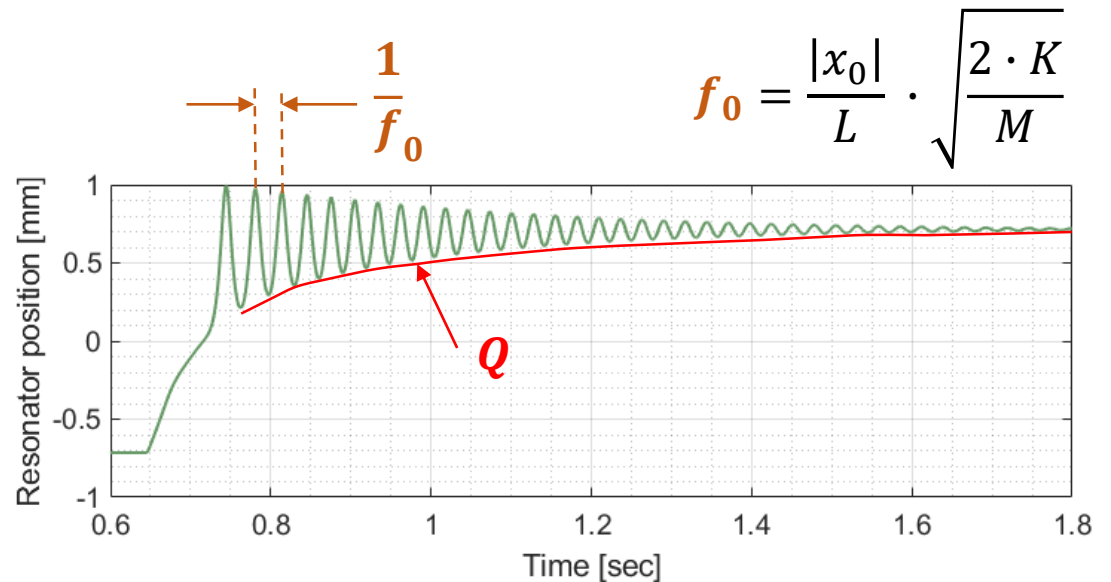
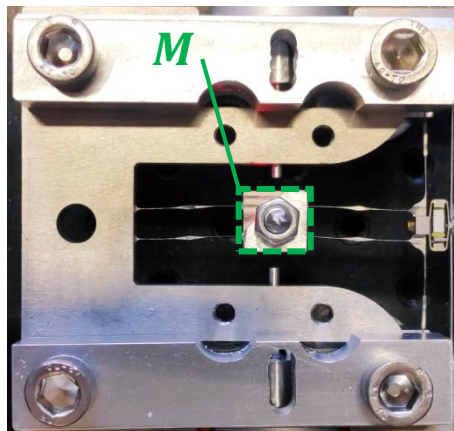
- Bistable buckled (x_0 unknown)
- Small displacements
- Initially at a stable position

Impedance Frequency Response



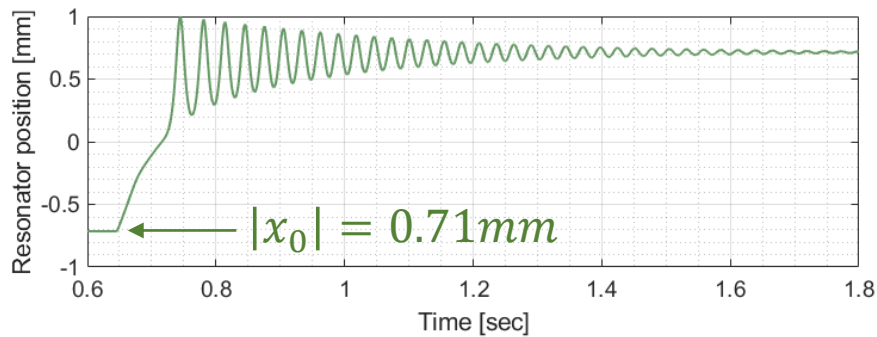
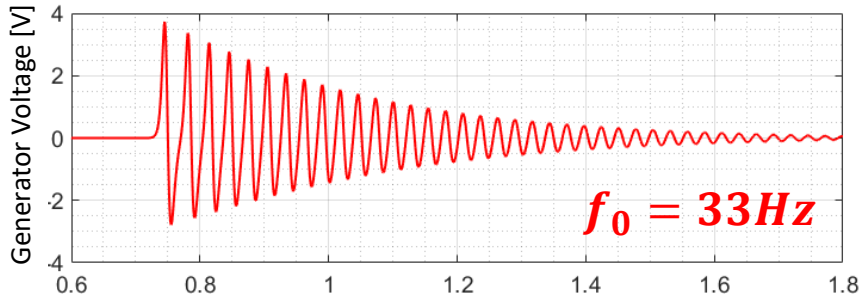
Experimental results

- EM coupling coefficient: $k_e^2 = 1,6\%$
- Quality factor: $Q = 78$
- Resonance frequency: $f_0 = 39\text{Hz}$
- Mass on the oscillator : $M = 5,88\text{g}$



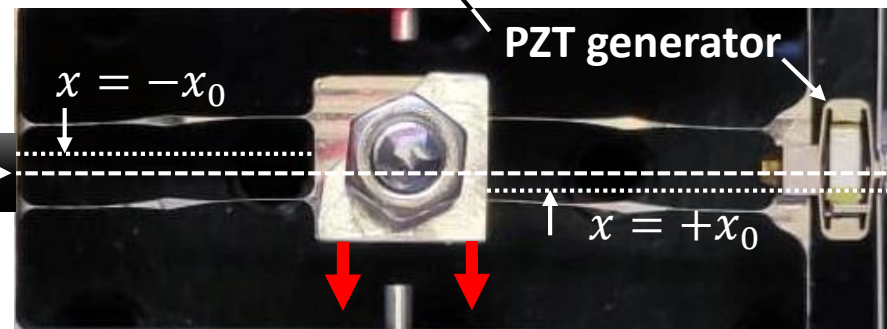
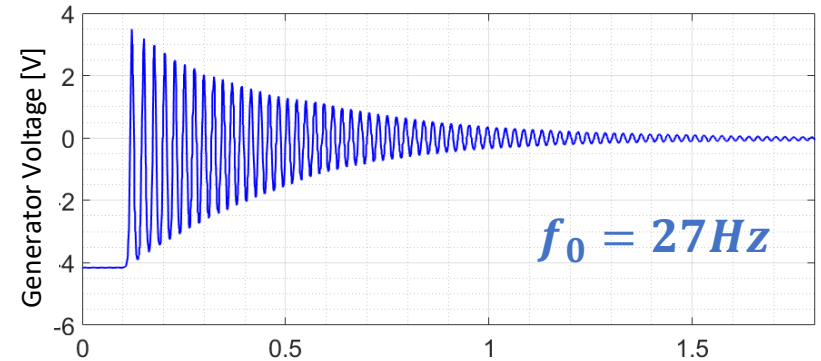
Experimental characterizations: Generator behavior

Theoretical model




$$f_0 = \frac{|x_0|}{L} \cdot \sqrt{\frac{2 \cdot K}{M}}$$

Expérimental $|x_0| \approx 0.58\text{mm}$

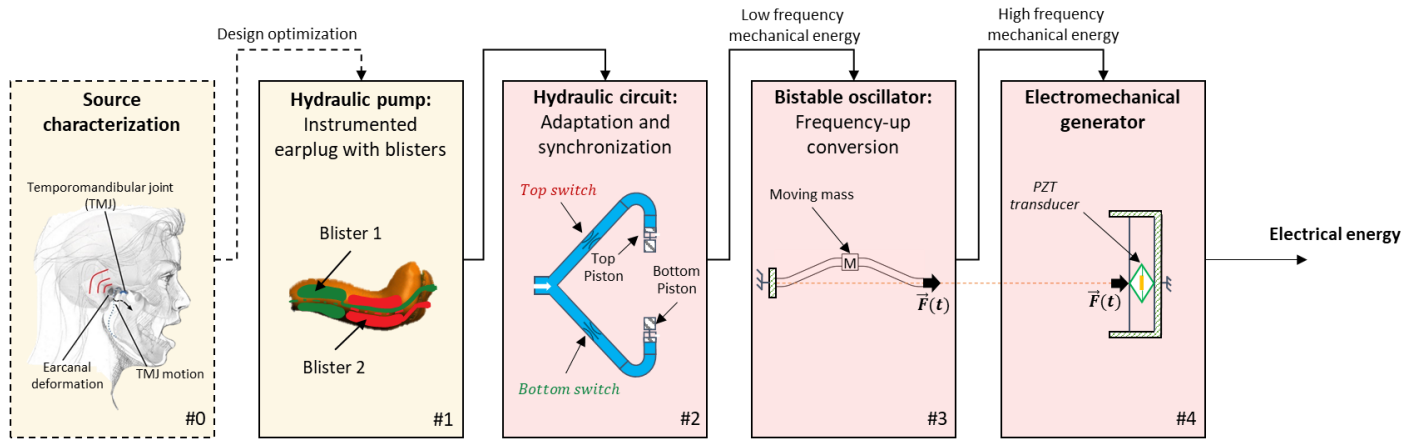


CONCLUSION

- Designed system : Hydraulics + Oscillator & generator ✓
- Experimental results in accordance with multiphysic model
 - Oscillator & generator ✓
 - Hydraulics 
- Application for patent [US Provisional Patent Application 63/173,463 (2021) [6]]

PERSPECTIVES

- Run the complete system : Self actuated experimental prototype
- Implement the **instrumented earplug** and the **harvesting prototype** together



REFERENCES

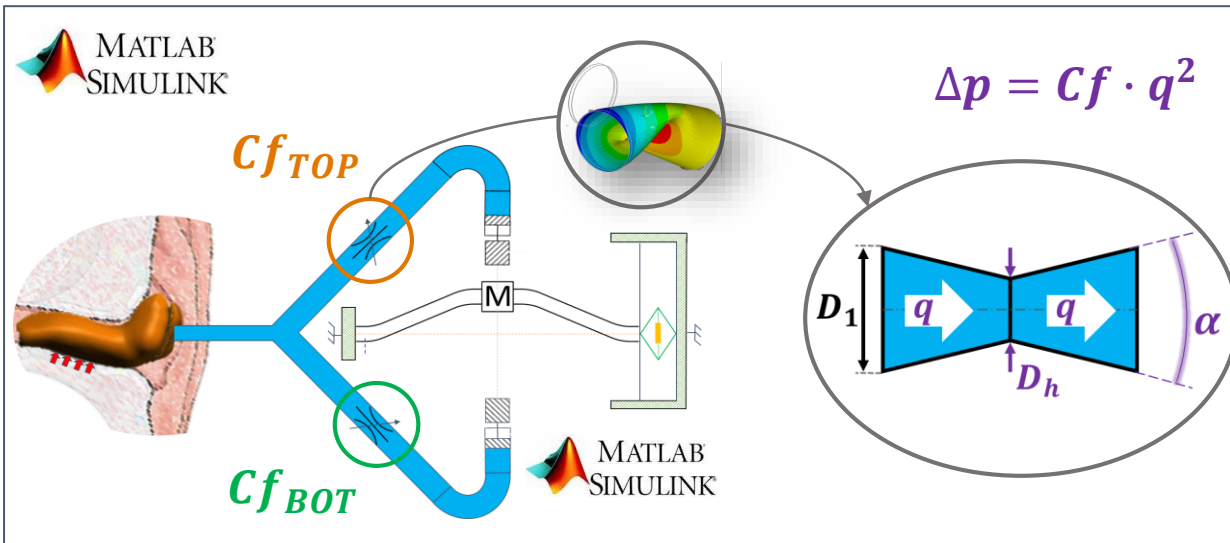
- [1] Resound hearing aid, model QUATTRO datasheet
<https://www.resound.com/enus/help/hearing-aids/linx-Quattro>.
- [2] Kumari, S., Sahu, S. S., Gupta, B., & Kumar Mishra, S.. Energy harvesting via human body activities. In *Smart Biosensors in Medical Care*, 2020.
- [3] Delnavaz, A., & Voix, J.. Micro-Power Energy Harvesting for In-Ear Devices. *PowerMEMS 2012*, 488–491, 2012.
- [4] Carioli, J., Delnavaz, A., Zednik, R. J., & Voix, J.. Power capacity from earcanal dynamic motion. *AIP Advances*, 6(12), 2016.
- [5] Goll, E., Zenner, H. P., & Dalhoff, E.. Upper bounds for energy harvesting in the region of the human head. *IEEE Transactions on Biomedical Engineering*, 58(11), 3097–3103, 2011

Patent application related to the present work :

- [6] **ENERGY HARVESTER DEVICE USING DYNAMIC MOTION AND METHOD THEREOF (Méthode et dispositif de grappillage énergétique à base de micro-pompe hydraulique : utilisation intra-auriculaire). US Provisional Patent Application 63/173,463 (2021)**

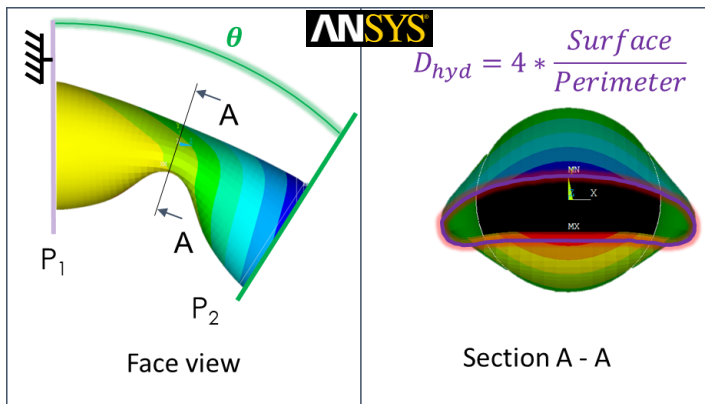
DESIGN OF THE HYDRAULIC SWITCHS

PHASE 1 : find Δp

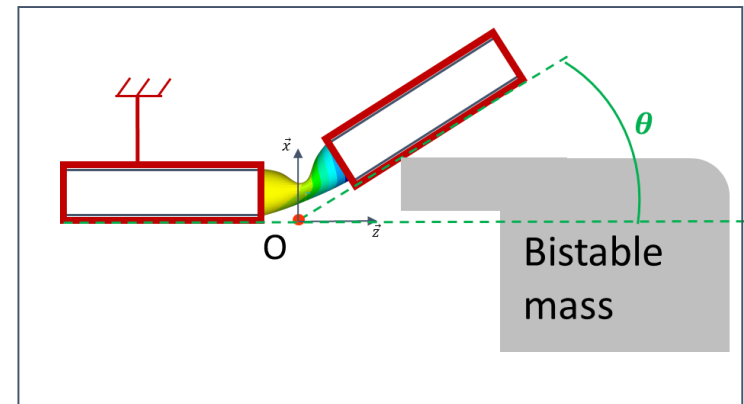


- Cf : Pressure loss coefficient
- D_h : Hydraulic diameter
- α : Enclosed angle
- q : Fluid mass flow
- x_{bis} : Bistable position

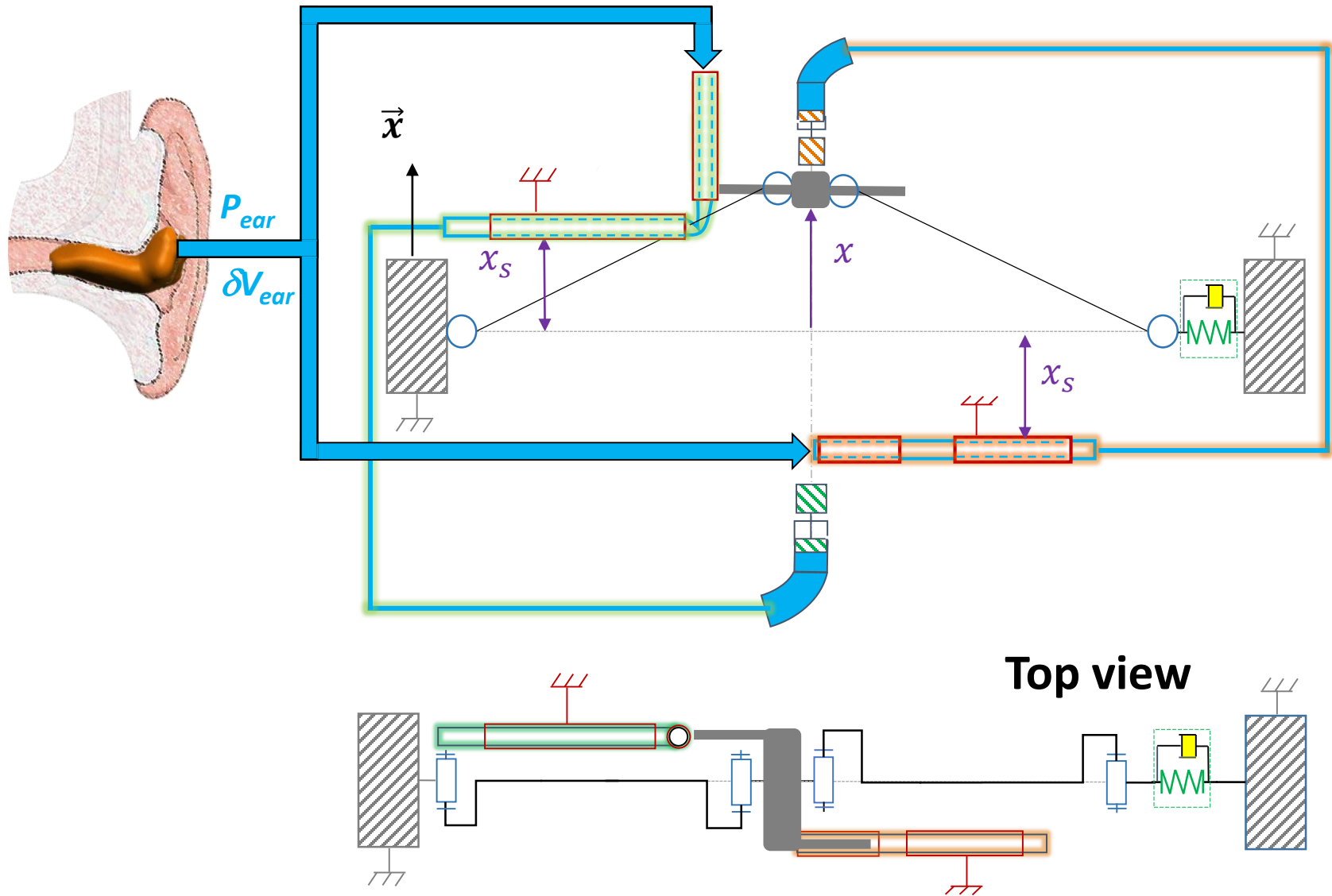
PHASE 2 : find θ



PHASE 3 : Integrate the switch



BISTABLE CYCLING MECHANISM



Top view