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## In-Ear Energy Harvesting: Source Characterization and Mechanical Simulator (Part I)

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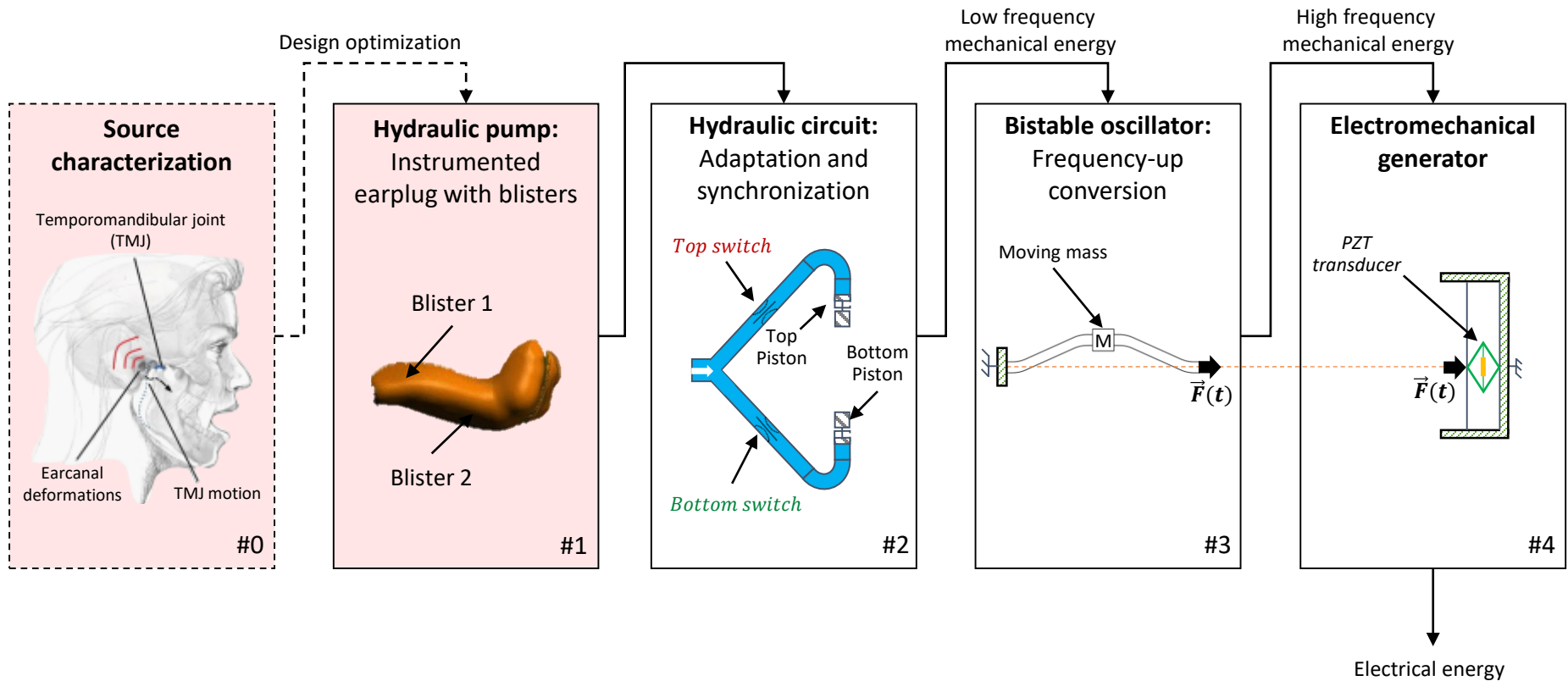


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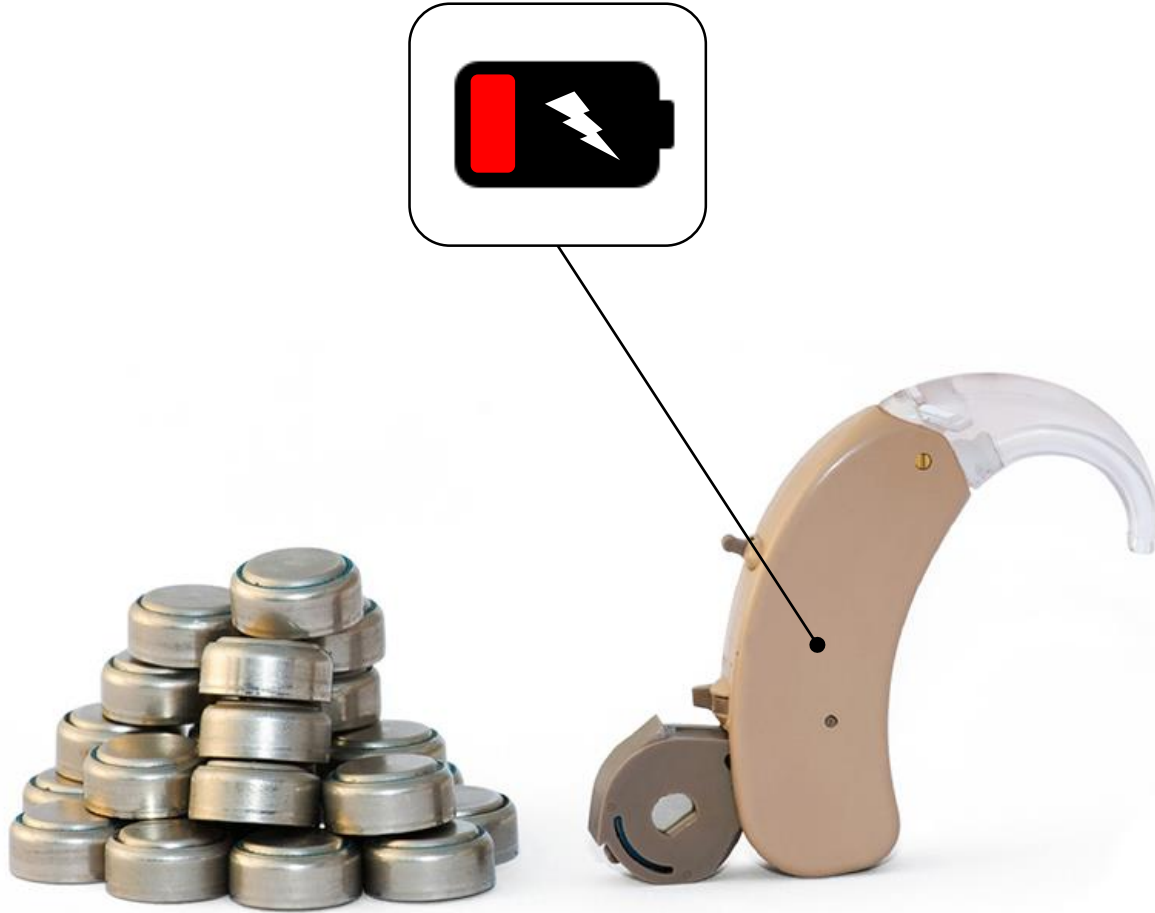
# Graphical abstract



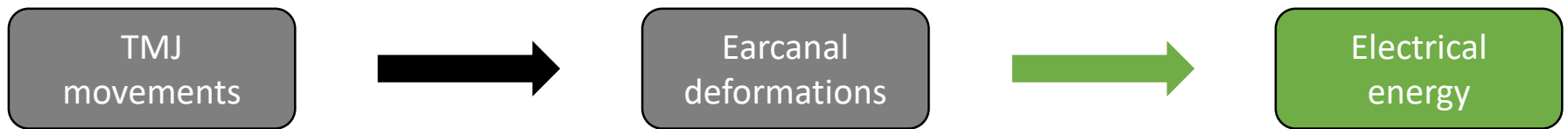
# Abstract

During the jaw's daily activities, the human ear canal is deformed by its anatomic neighbor called the Temporomandibular Joint (TMJ). Given the frequency of those activities, the ear canal dynamic movement is a promising source of energy within the ear, which can be harvested by using a mechanical-electrical transducer. Yet, the optimal design of such micromachine requires to characterize the TMJ's range of motion, its mechanical action on the ear canal and its capability. For that purpose, this research presents two methods to analyse the ear canal dynamic movements: 1) an in-situ approach based on measuring the pressure variation in a water-filled earplug fitted inside the ear canal; and 2) an anatomic-driven mechanism as a chewing test fixture with micrometric precision in reproducing the TMJ kinematics. The pressure earplug system provides the ear canal global dynamics which can be derived as an equivalent displaced volume; while the chewing test fixture gives the discrete displacement along the ear canal wall. Both approaches contribute to a better analysis of the interaction between TMJ and ear canal. Ultimately, the knowledge of the maximum displacement area and the derived generated power within the ear canal will lead to the design of a micromachine allowing to further investigate in-ear energy harvesting.

Keywords: Energy harvesting; ear canal dynamic motion; TMJ



# Introduction

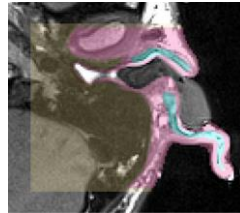


# Introduction

**In situ**  
(Willigen, 1976, Carioli et al., 2018)



**MR imaging**  
(Oliveira et al., 1992)



**Earmolds**  
(Willigen, 1976; Oliveira et al., 1992; Pirzanski, 1996;  
Grenness et al., 2002; Delnavaz et Voix, 2013)



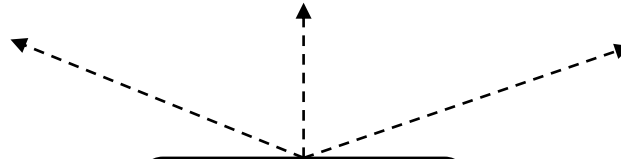
TMJ  
movements



Earcanal  
deformations



Electrical  
energy

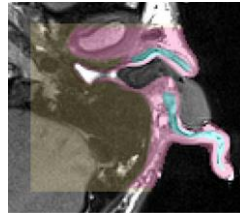


# Introduction

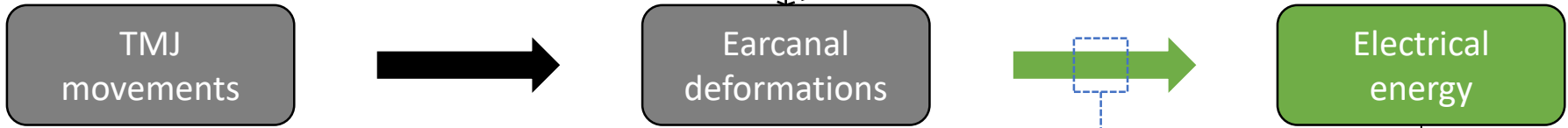
**In situ**  
(Willigen, 1976; Carioli et al., 2018)



**MR imaging**  
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**Earmolds**  
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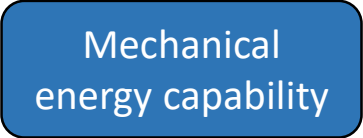


<b>Earmolds</b>	5.0 mW	Delnavaz et Voix (2014)
<b>Bending modeling</b>	15.0 mW	Carioli et al. (2016)
<b>Radial compression modeling</b>	3.9 mW	

<b>Hydro-electromagnetic</b>	0.3 $\mu$ W	Delnavaz et Voix (2014)
<b>Piezo-Ring</b>	0.2 $\mu$ W	
<b>Piezo-earpiece</b>	70.0 $\mu$ W	Delnavaz et Voix (2013)
<b>Earcanal bending sensor</b>	0.5 pW	Carioli et al. (2018)

# Introduction

Mechanical  
energy capability



## **Study #1: Global approach**

1. To improve previous results
2. To evaluate inter-subject variability
3. To test the feasibility of an all-in-one portable sensor

Earcanal  
deformations



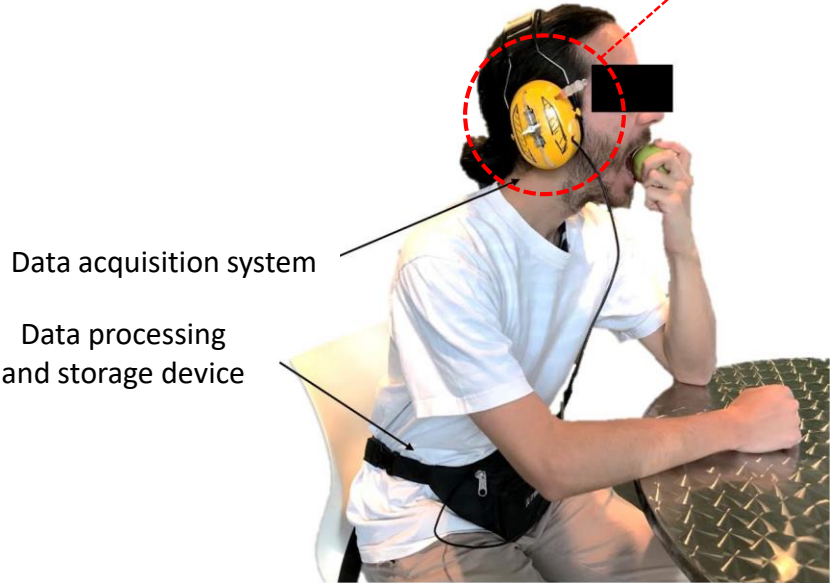
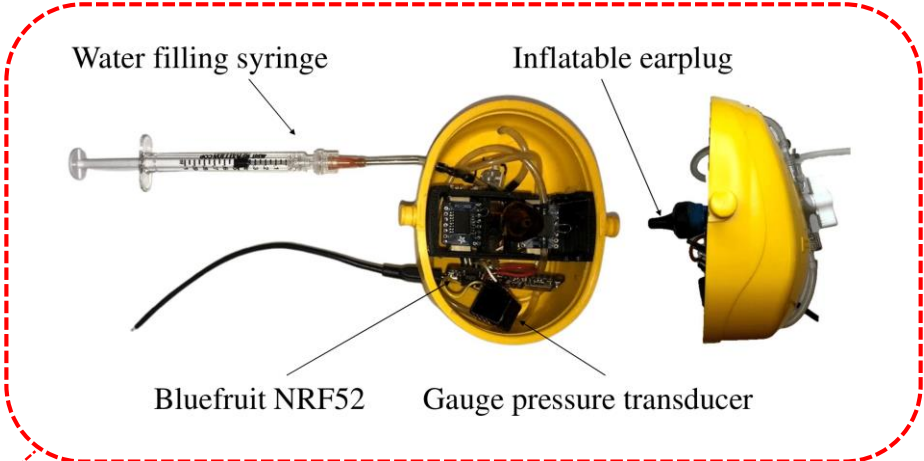
## **Study #2: Local approach**

1. To locate the maximal deformation areas
2. To characterize the deformation mode involved
3. To determine if they are antagonist displacements



# Global approach: Portable water-filled earplug

## Experimental set up

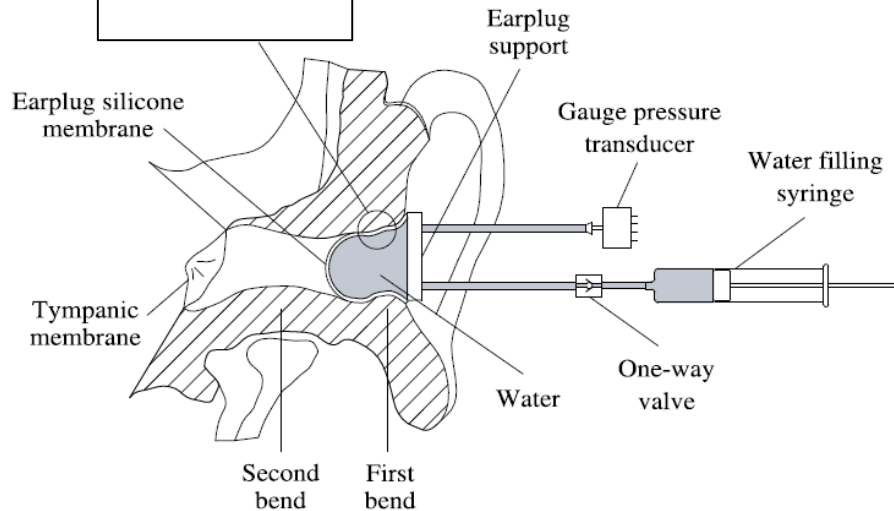
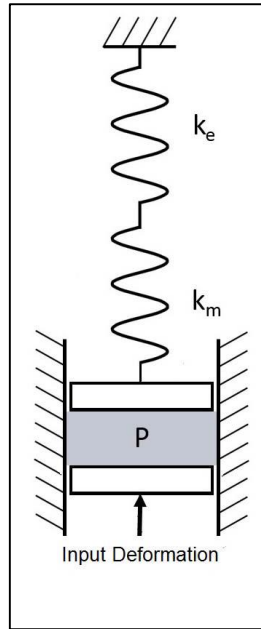


Data acquisition system

Data processing and storage device

# Global approach: Portable water-filled earplug

## Energy modeling



$$E_T = \underbrace{E_{\text{int}}}_{=PV} + \underbrace{E_{\text{ext}}}_{=\frac{1}{2}k\Delta U^2}$$

fluid                      membrane

$$dE = VdP + kUdU$$

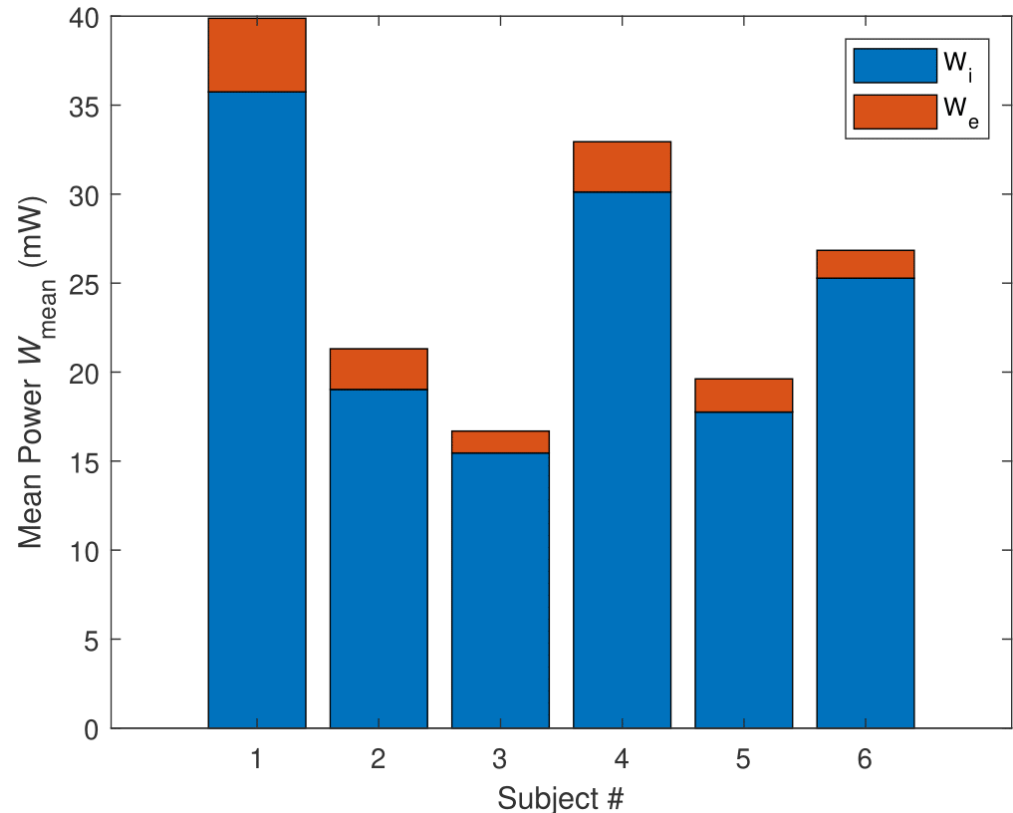
$$W = \frac{dE}{dt}$$

Determined experimentally

# Global approach: Portable water-filled earplug

## Experiment & Results

- **Participants:** 6
- **Process:**
  1. Earplug filled until  $P=14$  kPa
  2. Closing the one-way valve
  3. Recording during lunch time
- **Results:**
  - $W_{\text{average}} = 26.2 \text{ mW} \pm 1.9$
  - $r = \frac{E_{\text{int}}}{E_{\text{T}}} = 91\% \pm 1.7$



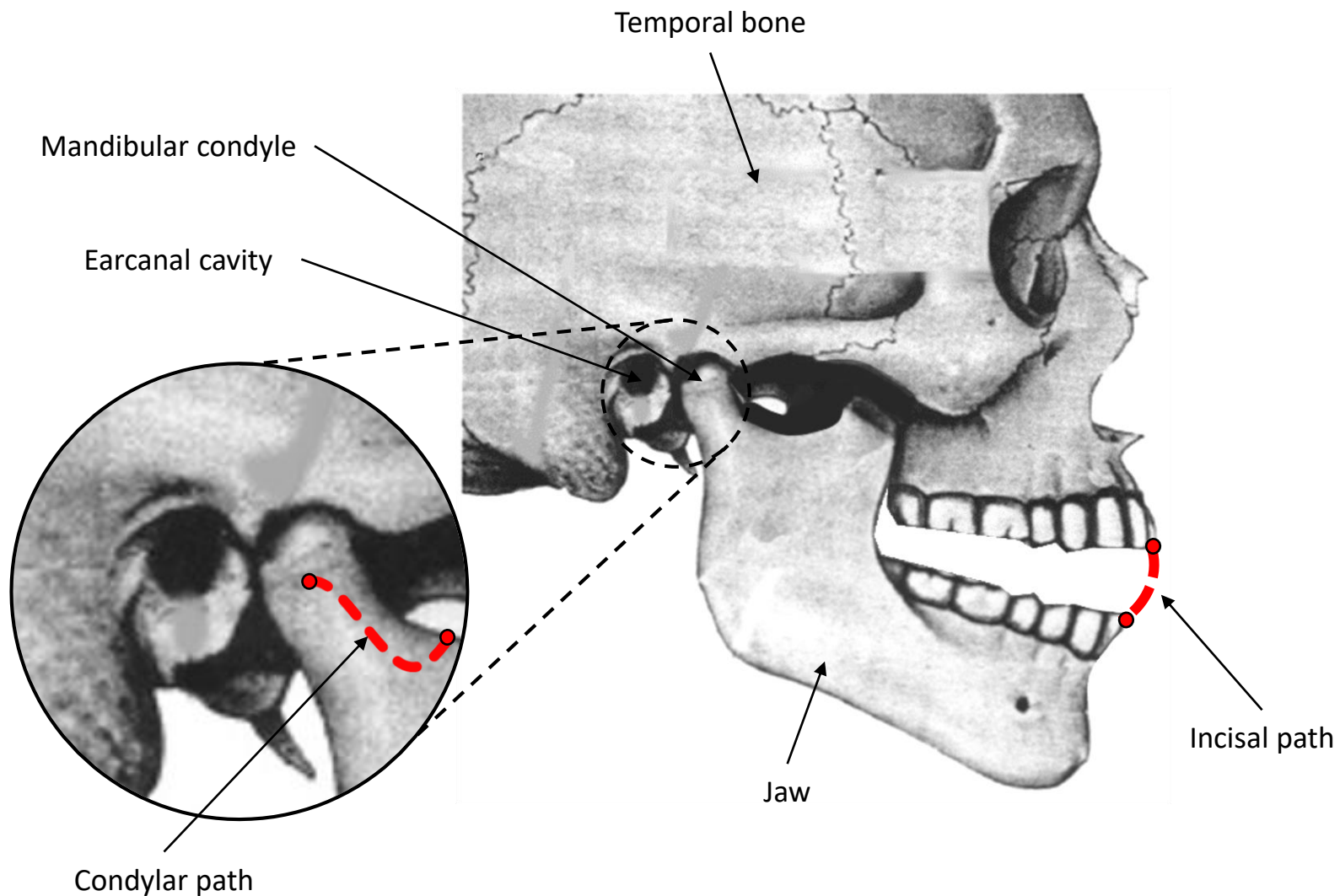
# Global approach: Portable water-filled earplug

## Limitations

- Portable design AND adapted to every human ear anatomy
  - **BUT** can be **uncomfortable** due to occlusion effect
- Measure performed where maximal of the earcanal deformations occur (between 1st and 2<sup>nd</sup> bend)
  - **BUT** only the **resulting dynamic motion** between open- and closed-mouth position is available

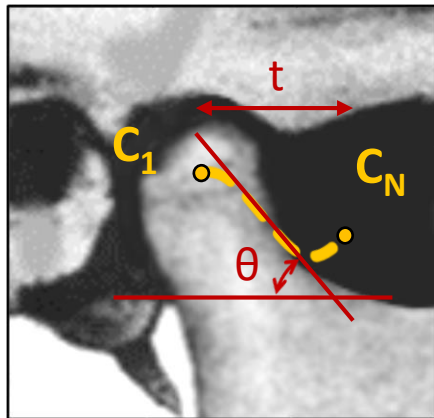
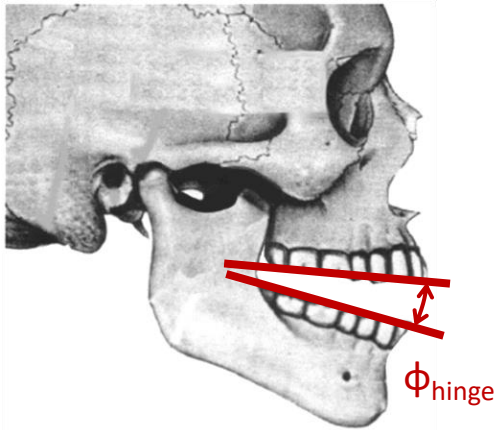
# Local approach: Chewing test fixture

## TMJ kinematics

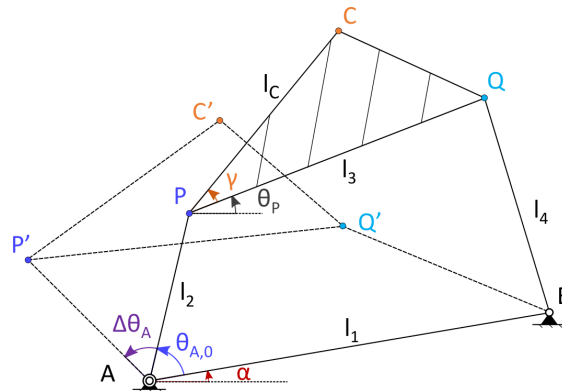
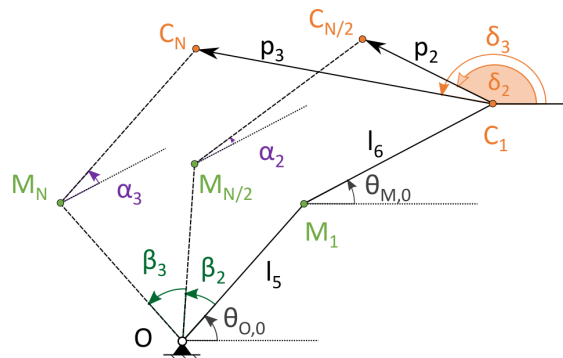


# Local approach: Chewing test fixture TMJ kinematics modeling

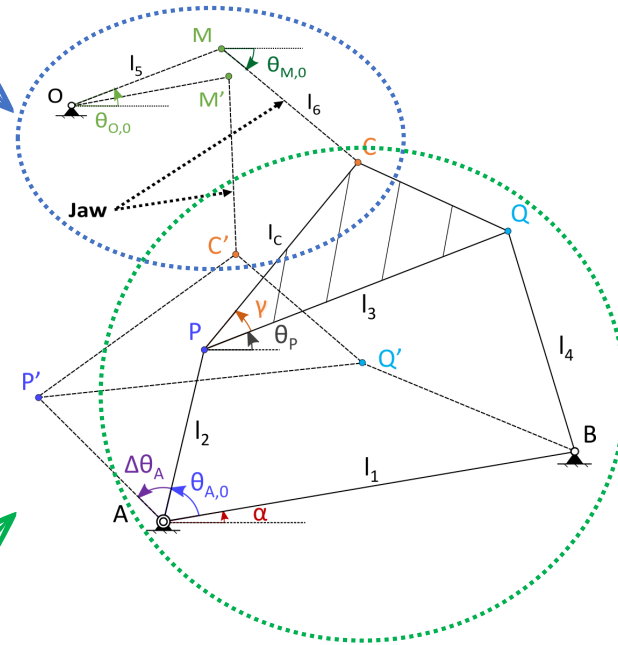
Biomechanical parameter identification



Bar-linkage sub-mechanism modeling

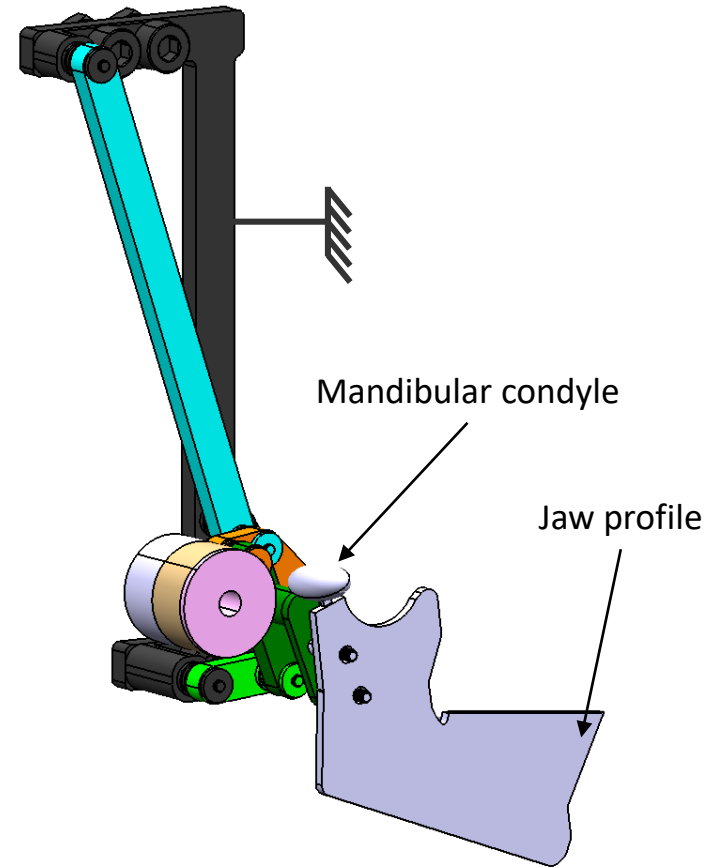
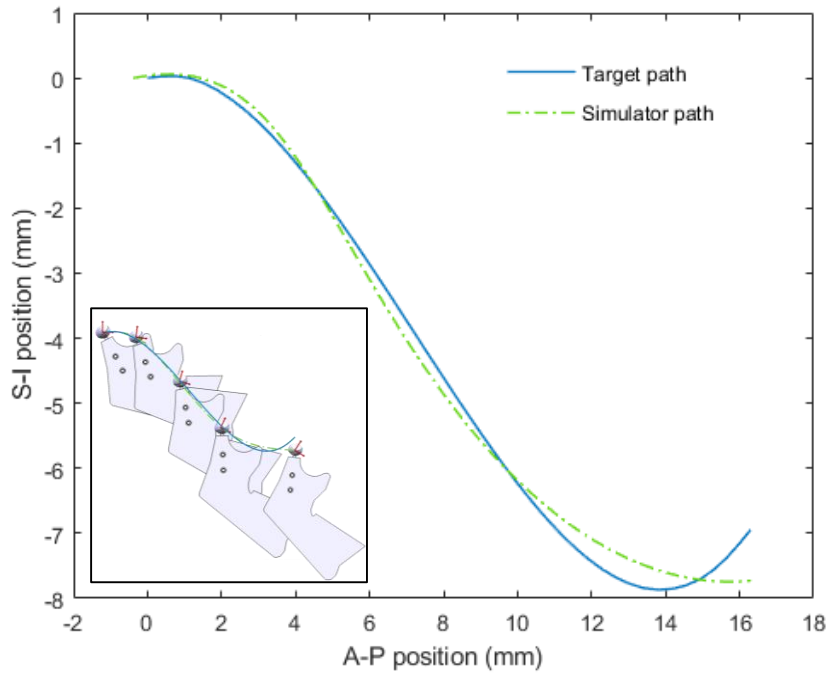


TMJ simulator modeling



# Local approach: Chewing test fixture

## TMJ simulator design

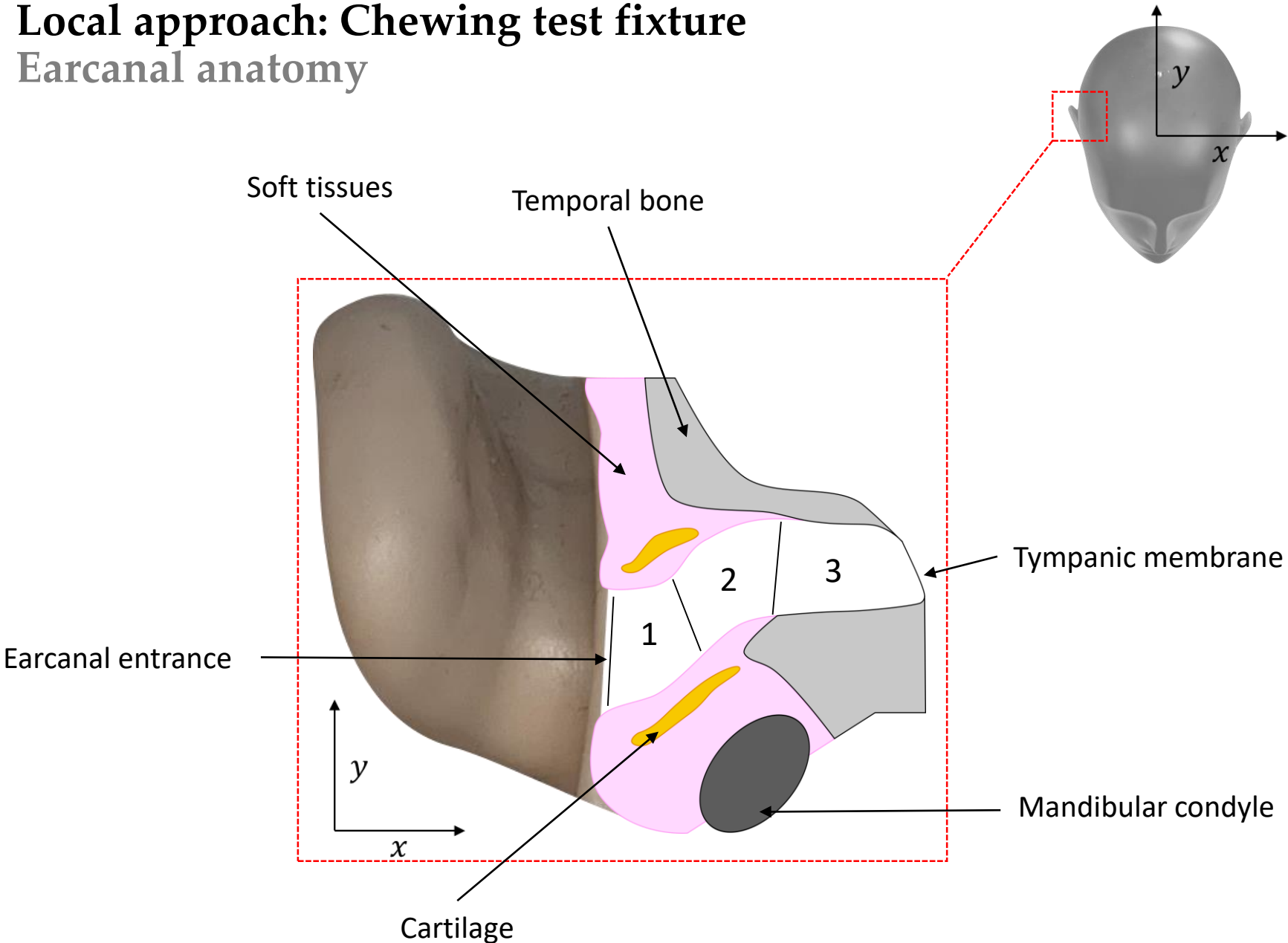


**Target VS optimal generated path**

Root mean square error	Horizontal translation	Slope	Opening angle	Roto-translation correlation
1.65%	1.9%	3.2%	0%	2.5%

# Local approach: Chewing test fixture

## Earcanal anatomy

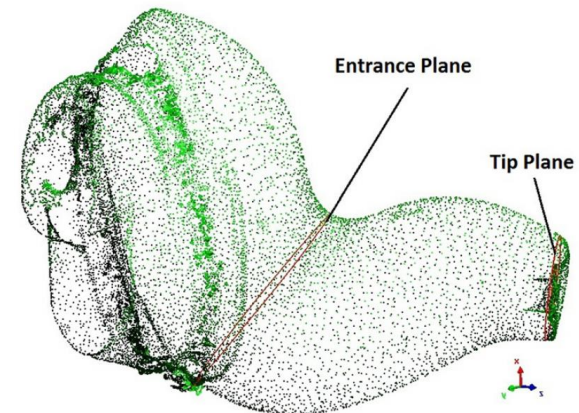
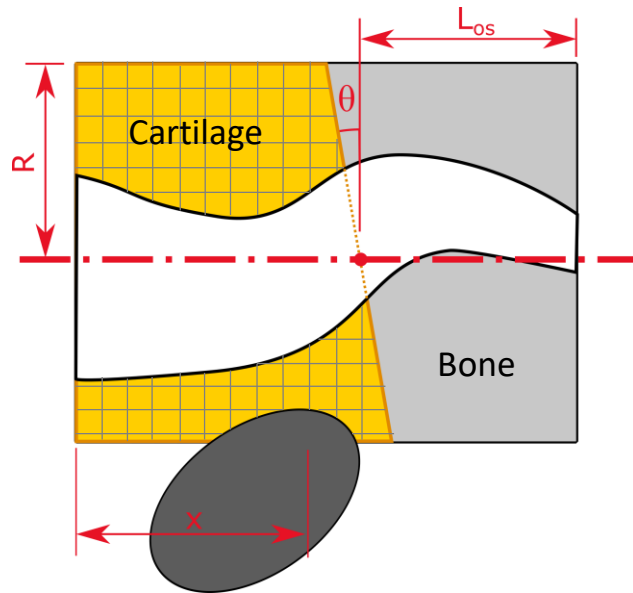




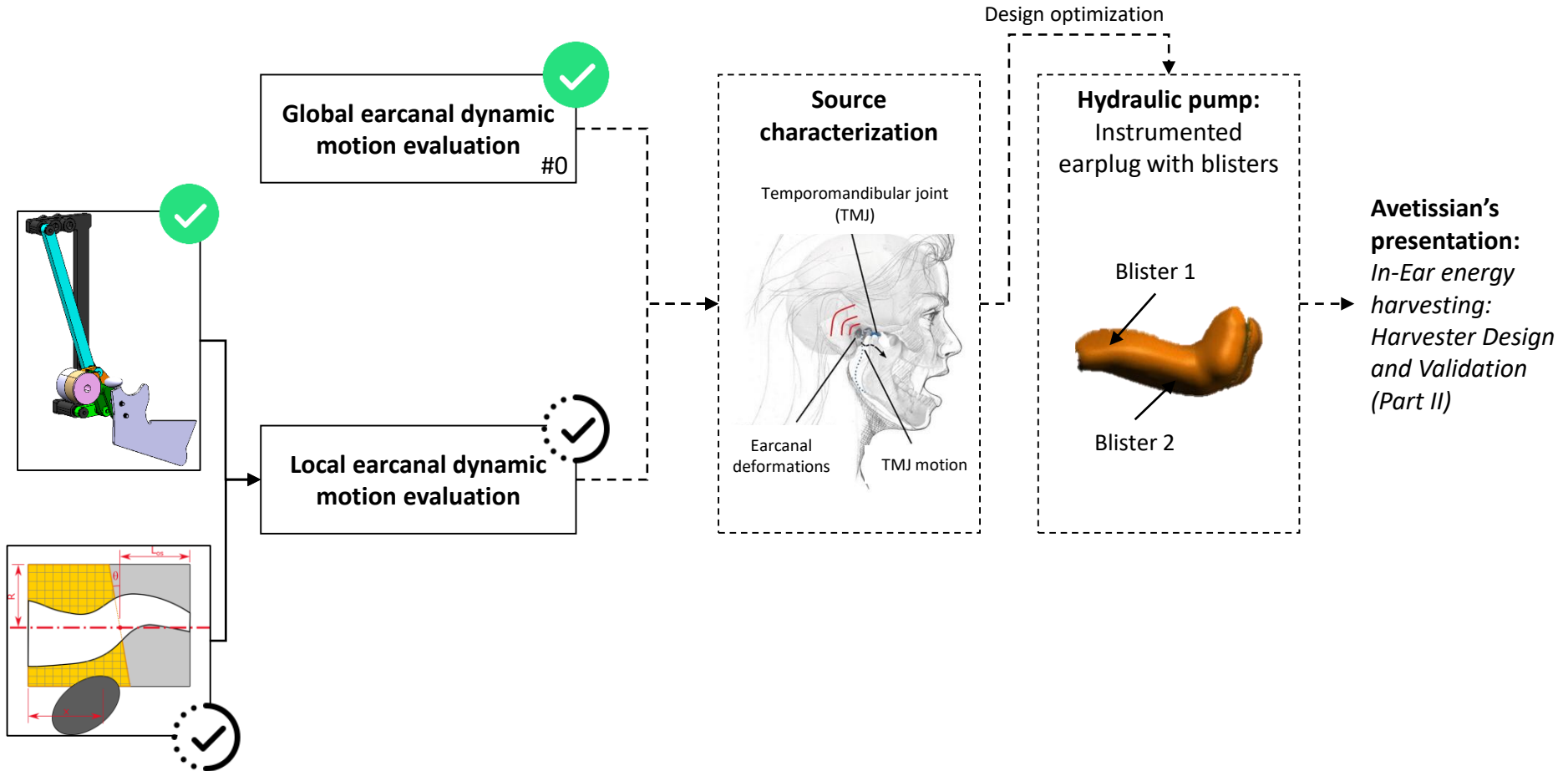
# Local approach: Chewing test fixture

## Earcanal modeling & anatomical coupling

- **3D finite element (FE) analysis** to find the optimal biomechanic setting:
  1. The surrounding tissues geometry reproducing the mechanical behavior of the earcanal cavity
  2. The anatomical coupling between earcanal and TMJ
- **Trial-and-error method** to compare FE earcanal cavity with earmold scatter plots in both open- and closed-mouth positions



# Conclusion & Expected outcomes



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