

# Silicon Carbide for advanced in-vivo medical devices

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**ICMA  
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# Nanomedicine (NIR-PIT)

MRI Compatible  
Implants



Neural Interfaces



Wearables



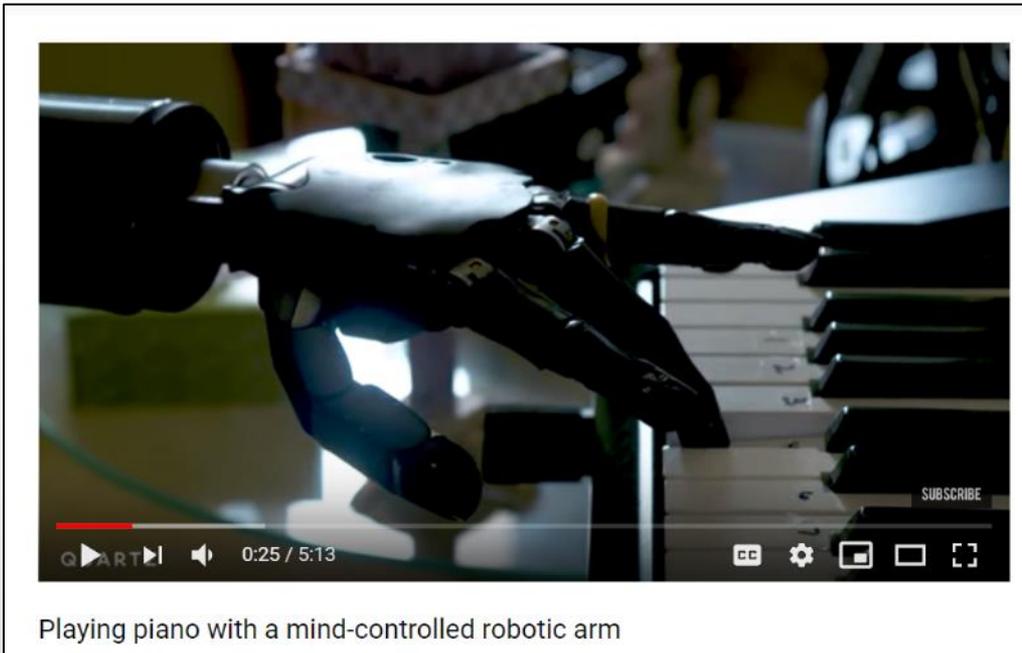
BME Outreach



Bio Sensors

# Bionics –restoring human functionality

- Prosthetics
- Spinal cord repair
- Neural bridge

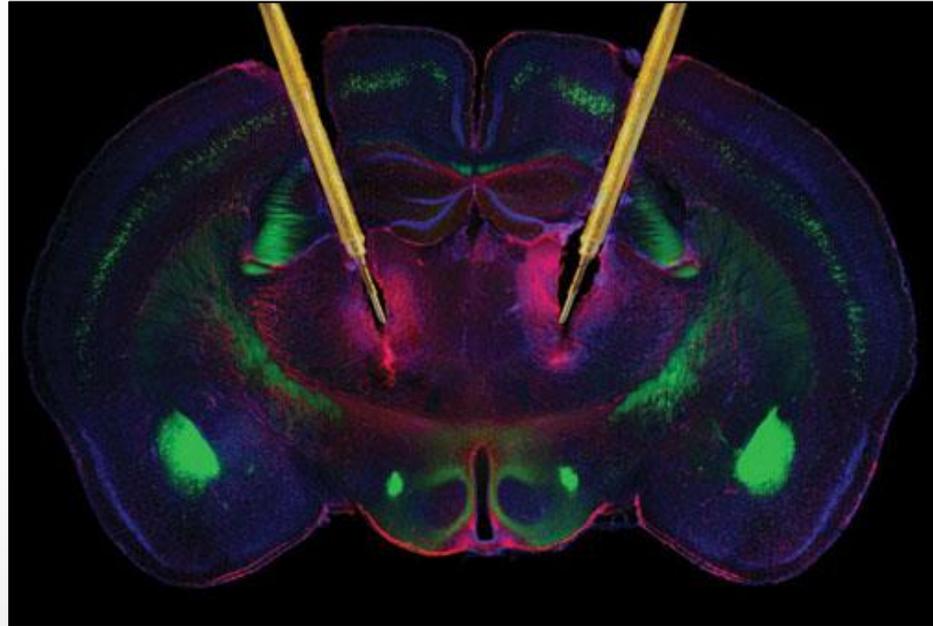


Johnny will tell you the movement is slow → neural interface would allow more natural movements

# Neural Interfaces face many challenges

## Long-term in-vivo results in:

- Device failure (50% device failure)
  - Tissue damage
  - Loss of functionality/performance
- 
- Si arrays (Michigan and Utah) ~ 1-6 months
  - Polymer arrays ~ 6-12 months
  - Novel coatings ~ 4 years MAX
  - A new strategy is clearly needed!
  - Cubic SiC → excellent neuro and hemacompatibility
  - In-vitro and In-vivo (1 month) data → solution?



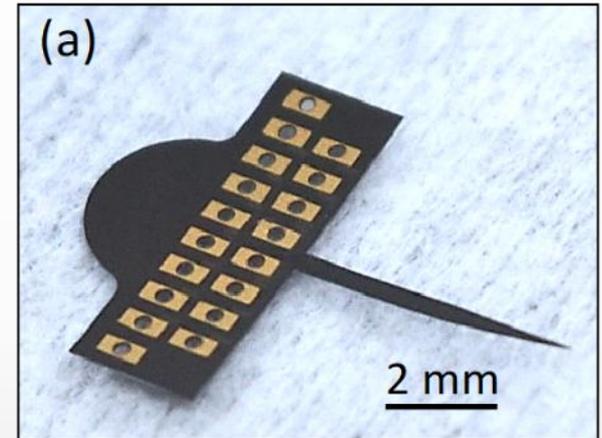
Severe tissue death with W probes

In-vivo challenge – suitable materials for 25+ year operation in the human body

# Monolithic 'All-SiC' INI a possible solution



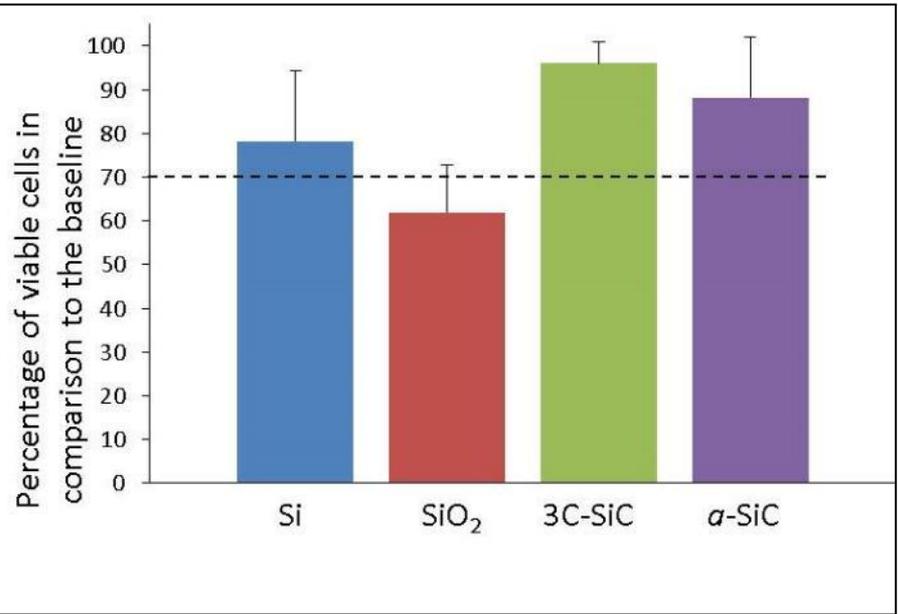
<http://www.jhuapl.edu/newscenter/pressreleases/2016/160112.asp>



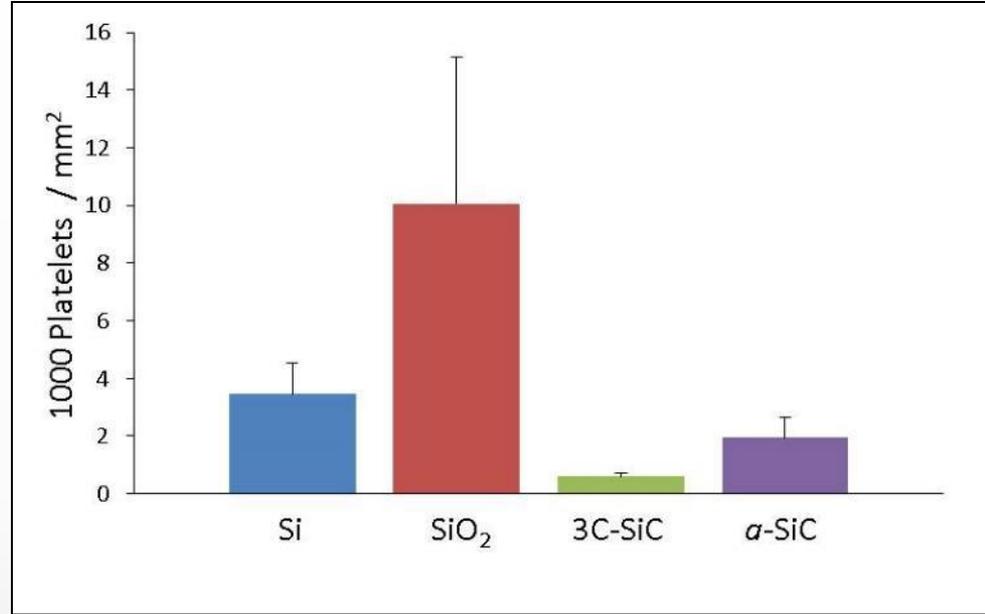
All-SiC neural probe to be packaged with an Omnetics 18 pin nanoconnector to a ZIF connector for animal testing

Osseo-integrated – lets integrate with a robust, long-term neural interface!

# In-vitro performance



Biocompatibility



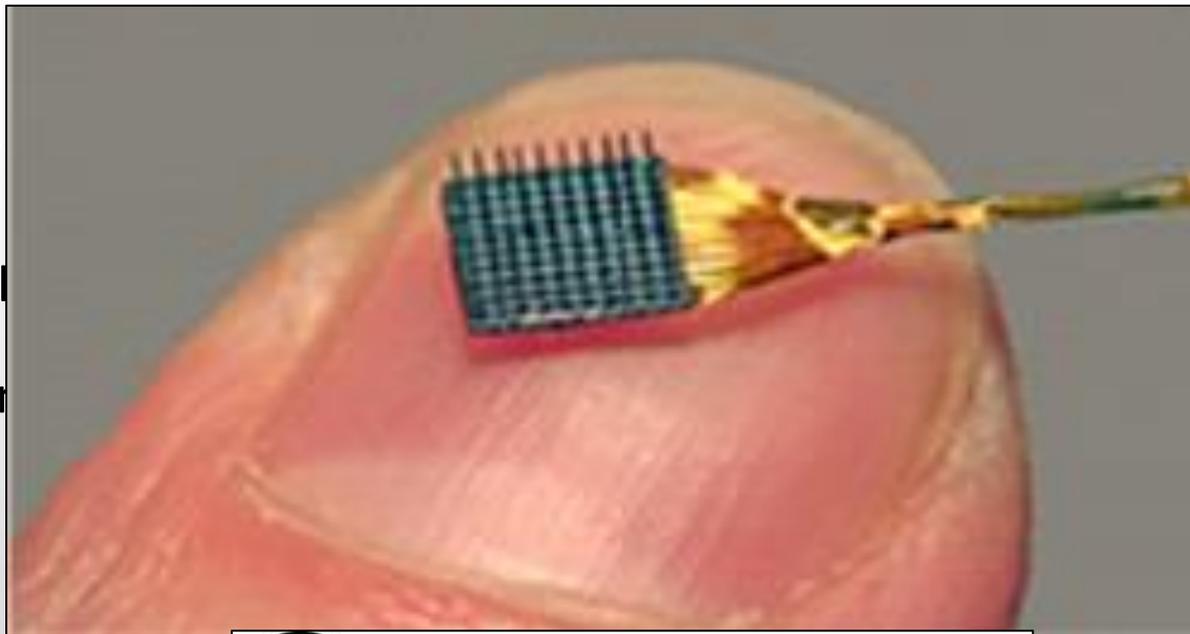
Hemocompatibility

**Only 3C-SiC** passed all ISO 10993 tests (chem stability, bio- and hemo-compat.)

# SiC Intracortical Neural Interfaces (INI)

3C-SiC has properties useful for many biomedical devices, such as neural interfaces:

- 3X harder than stainless steel, reducing surgical trauma
- Biocompatible
- Can be used for long-term implantation



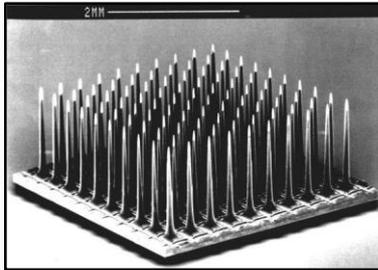
*surgical*

polyimide

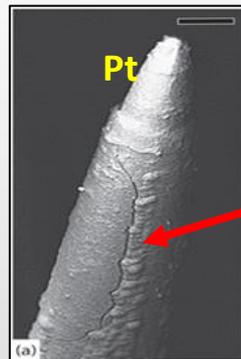
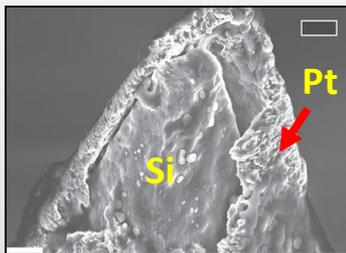
SiC

# Implantable Microelectrode Challenges

Utah  
Array



Single unit recordings not advantageous due to reliability challenges

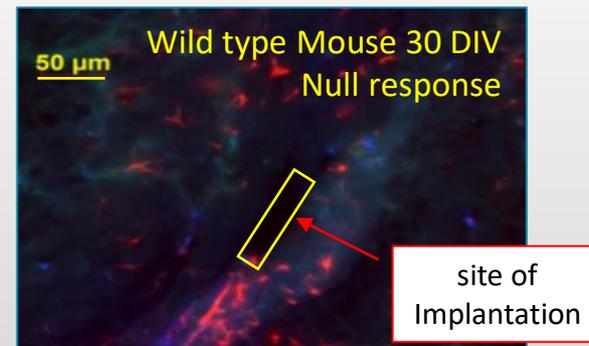
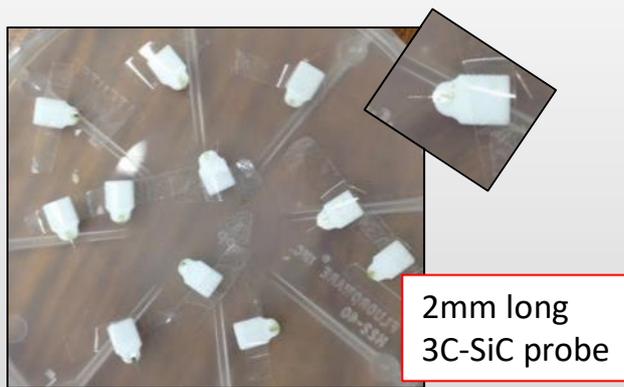


- Parylene C, Pt-Ir used for device insulation and conductors.
- Parylene C cracking/delamination Pt-Ir for micro-scaled devices has Limited current density

\* [1] J. C. Barrese, J. Aceros, and J. P. Donoghue, "Scanning electron microscopy of chronically implanted intracortical microelectrode arrays in non-human primates," *J Neural Eng.*, vol. 13, p. 026003, Jan 29 2016.

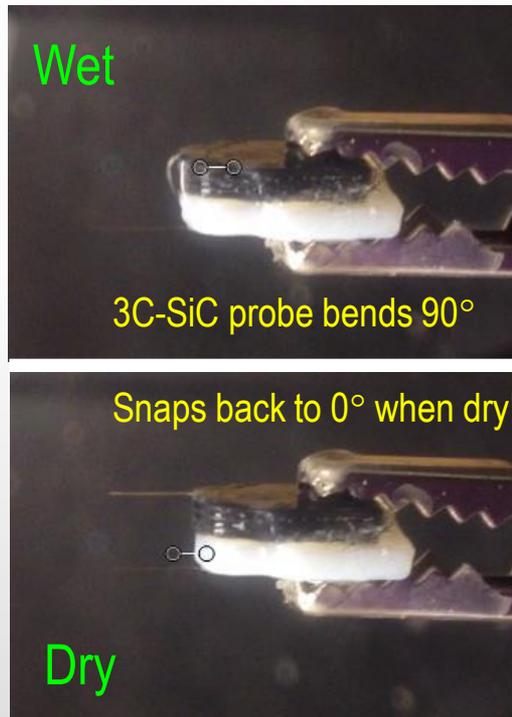
# Cubic SiC – Robust Microelectrode?

- SiC is a well-known chemically inert semiconductor:
  - Processed like Silicon (Neuronexus, etc.) → Microelectrode array (MEA) capable
  - Grown on Si wafers (low-cost) and micromachining/fab ~ identical to Si
  - Offers larger junction voltages (1.6 V vs. only 0.7V for Si) → stimulation possible?
- No measured chronic inflammatory response in 2 animal models
- Multitude of solid-state forms:
  - Poly-crystalline and amorphous SiC ( $\alpha$ -SiC which is an excellent insulator)
  - Single crystal polymorphs (hexagonal and cubic): 3C-SiC with 2.3 eV
  - Allows for microelectrode support, conductor and insulator in single material system



No Immune response in 3 animal models (Mouse, Rat, Pig) to date...

# 3C-SiC probes vs. coated Si probes



Si and 3C-SiC probes fabricated using same technology  
3C-SiC 3X as hard and 3X as flexible:

## Measured Mechanical Properties\*

Material Type	Hardness [GPa]	Elastic Mod. [GPa]	Fracture tough. [MPa·m <sup>1/2</sup> ]**
(100)Si	12.46 ± 0.78	172.13 ± 7.76	1.59 ± 0.21
(100)3C-SiC	31.19 ± 3.7	433 ± 50	4.6
Poly-3C-SiC	33.54 ± 3.3	457 ± 50	2.18

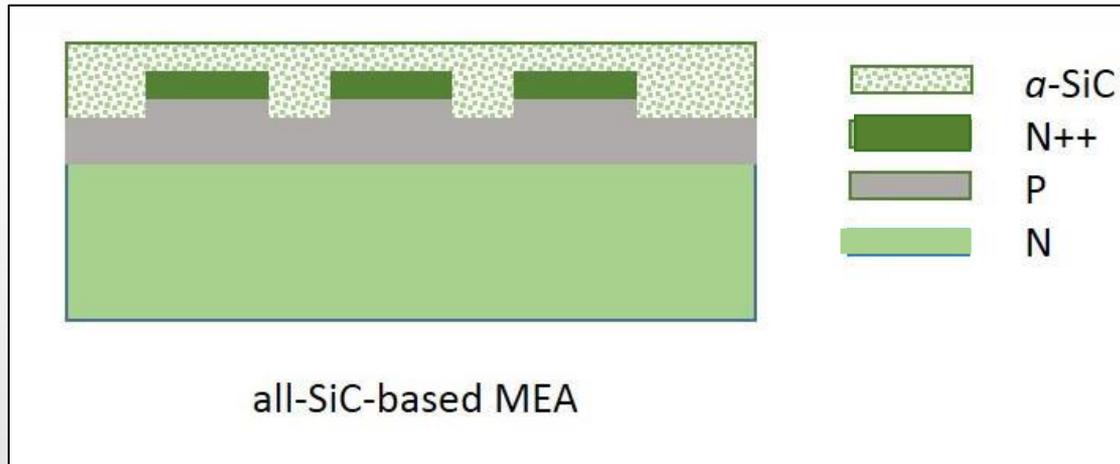
\* Measured via nanoindentation.

\*\* Crack lengths used to calculate the film fracture toughness.

Main advantage of 3C-SiC instead of polymer-coated Si is thinner probe thickness (**6 um vs. 15 um for Si**)

# Monolithic All-SiC MEA: a robust solution

- In all-SiC technology, a pn diode blocks current flow and an amorphous SiC ( $\alpha$ -SiC) insulator caps the metallic-like electrodes:

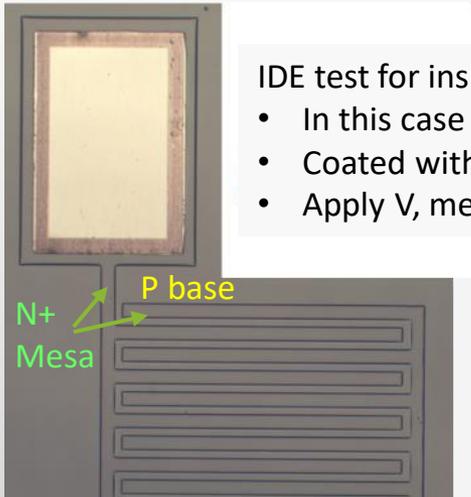


No metals or plastics → robust SiC only

# How does this work?

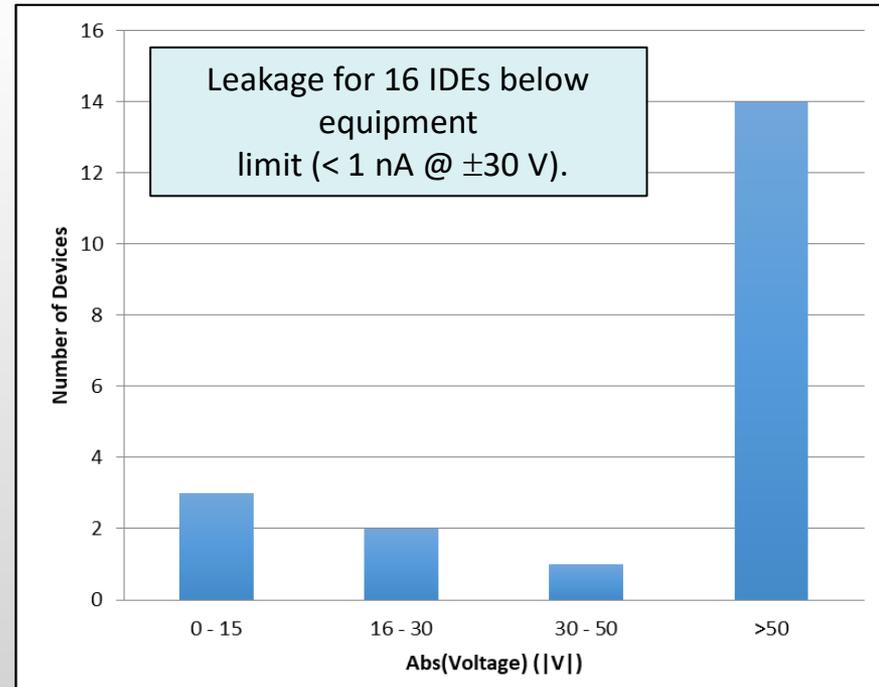
- Degenerately doped semiconductors → semi-metallic conduction
  - no need for metal electrodes to carry bi-directional signals
- Metal electrodes, such as PtIr, typically processed to form ceramic-like properties
  - 3C-SiC is already a ceramic
- $\alpha$ -SiC is highly insulating
  - All-SiC materials integrated to create a monolithic device

## All-SiC IDE

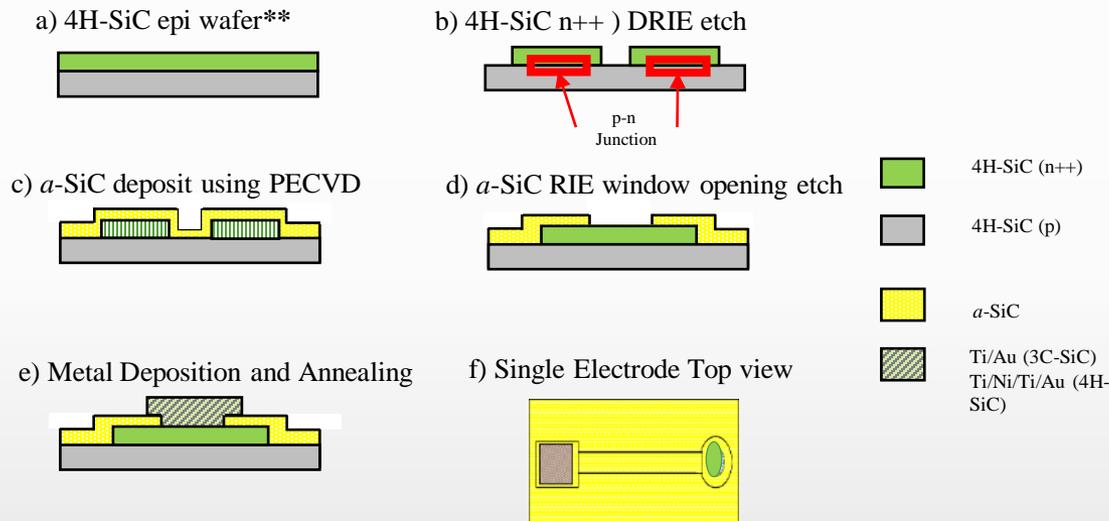


IDE test for insulation

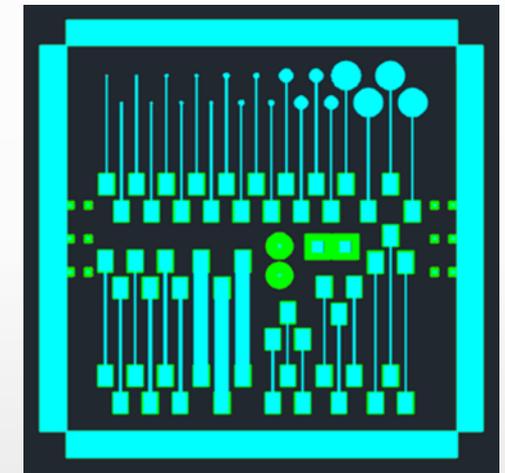
- In this case also isolation
- Coated with  $\alpha$ -SiC
- Apply V, measure I



# All-SiC INI Fabrication flow



Fabrication flow (a through f) for 4H- all-SiC planar neural microelectrode.  
 Fab for 3C-SiC devices identical with underlying Si substrate.

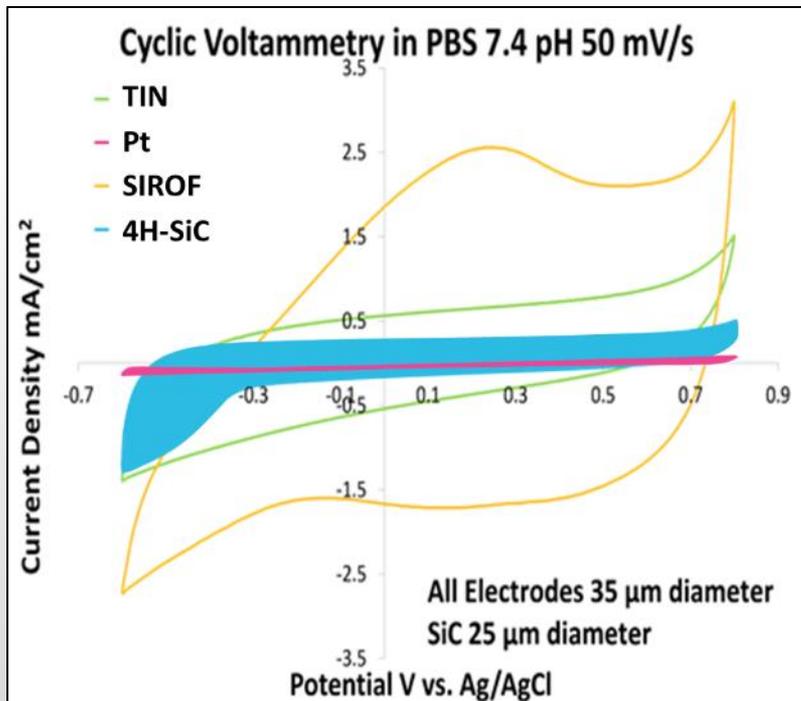


## Planar MEA

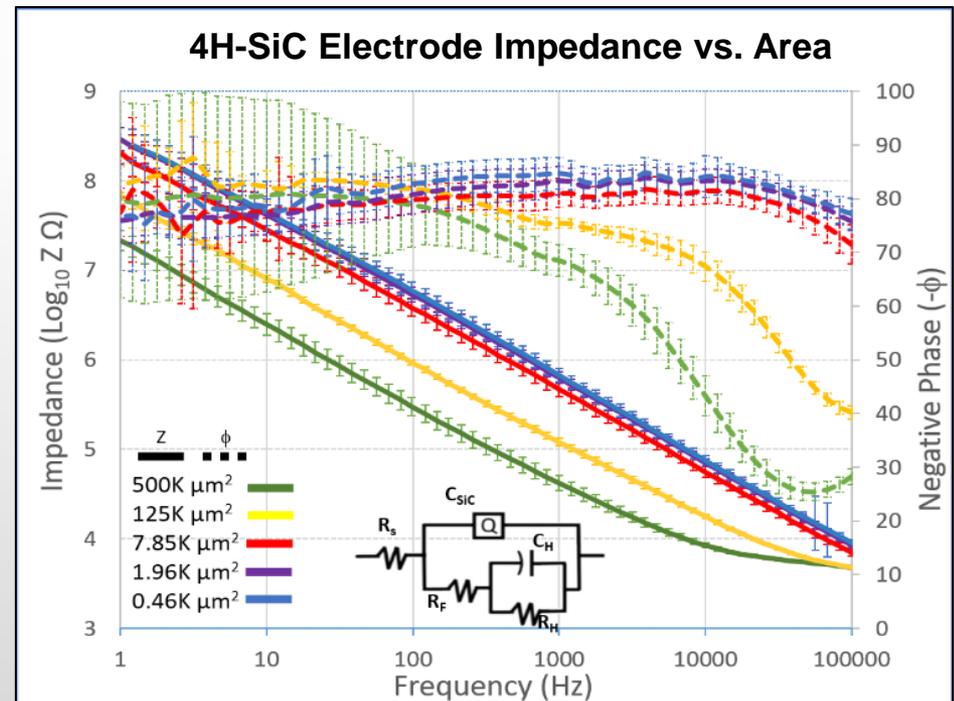
Single ended electrodes  
 Double ended resistors  
 PN Diodes

# Electrochemical Performance

- Impedance and cyclical voltammetry performed
- Planar all-SiC MEA consistently displayed electrode-like performance
- Dependence on electrode tip area studied
- Capacitive characteristic, as expected, observed



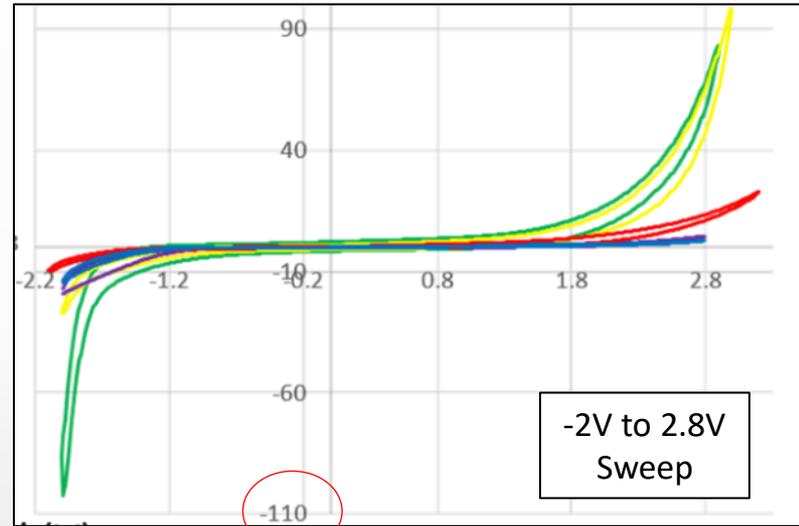
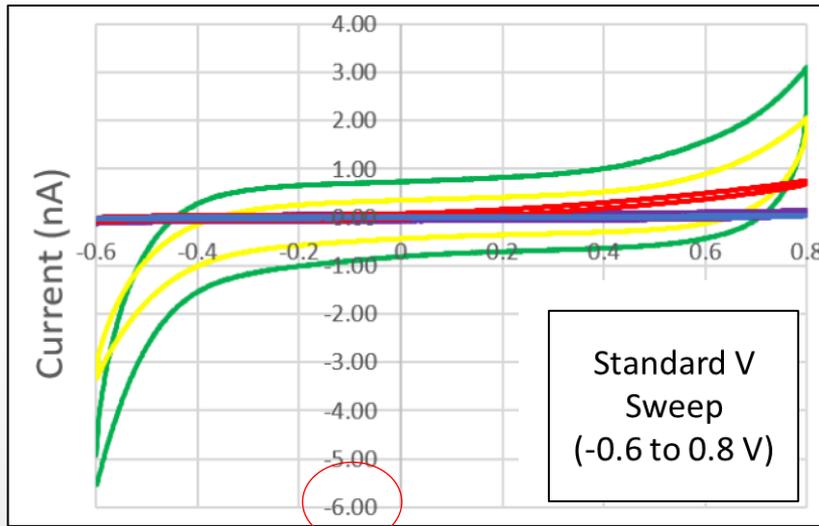
4H-SiC performed better than Pt electrode



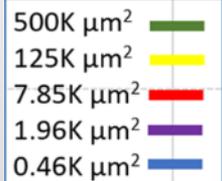
$|Z| \sim 675\text{k}\Omega$  ( $496 \mu\text{m}^2$ ) and  $\sim 46\text{k}\Omega$  ( $500\text{K} \mu\text{m}^2$ )

# Electrochemical Performance

## 4H-SiC Electrode CV vs. Area



Note scale difference

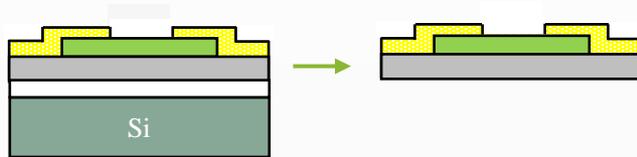


Increasing recording/stim tip area decreases Z and increases Charge capacity, as expected.

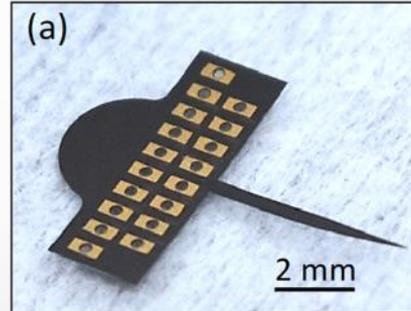
# Advantages of Cubic SiC over 4H-SiC

- Biggest challenge is removal of the substrate for implantable MEA's
- One solution is to grow 3C-SiC on SOI → oxide release layer
- Films grown at IMM-CNR (Catania)
- Allows for integration with electronics (Si) on tab.

All-SiC (3C-SiC) Device on SOI



Probe release (HF)



Shank → 5.1 mm long

Tab → 6.64 x 2.3 mm

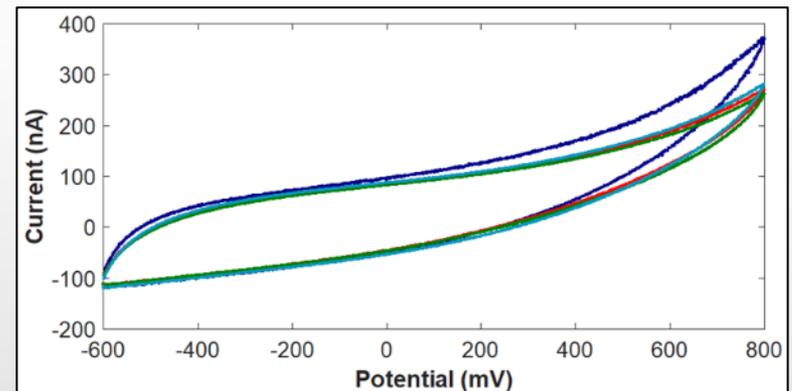
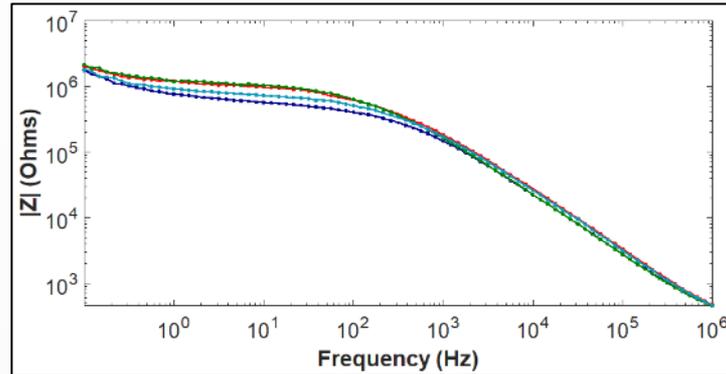
Newest 16 electrode Monolithic 3C-SiC Implants



# Fabrication of a Monolithic 3C-SiC/SOI Implantable Neural Interface

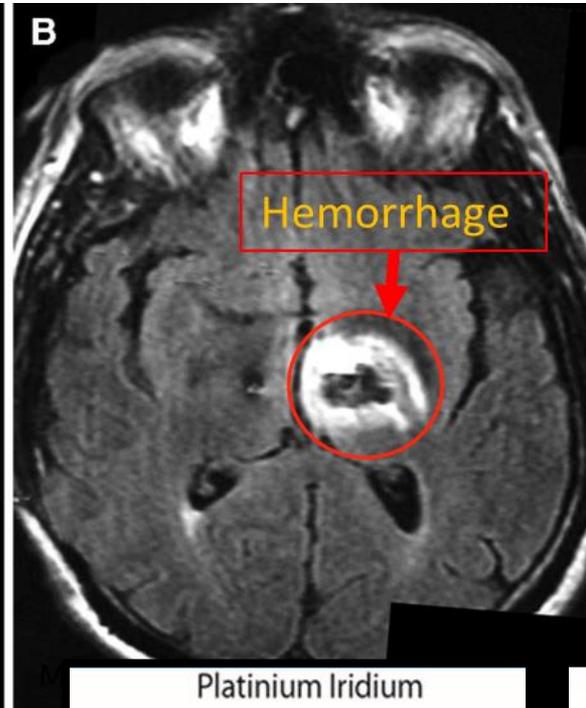
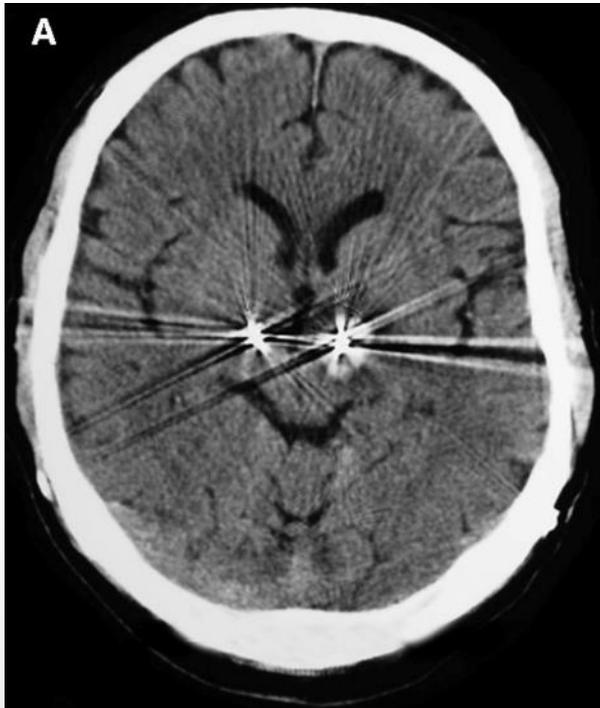
## EIS & CV measurements

- Results of 4 microelectrodes
- Average of 3 replicates
- $|Z|$  @ 1kHz  $\rightarrow$   $\sim 165$  k $\Omega$
- Electrode-electrolyte shows a predominantly capacitive behavior
- Rate of 50 mV/s

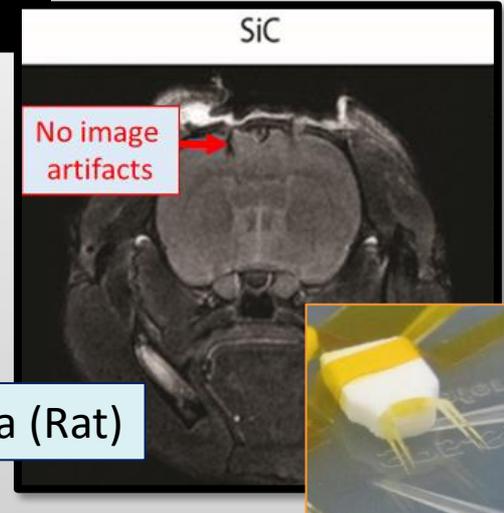
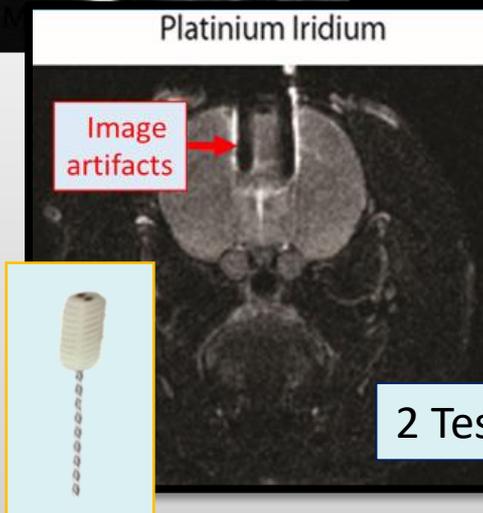


	Anodic	Cathodic
Average Charge Storage Capacity (mC/cm <sup>2</sup> )	15.4 $\pm$ 1.46	15.2 $\pm$ 1.03
Average Charge Per Phase (nC)	75.4 $\pm$ 5.06	74.8 $\pm$ 5.06

# MRI compatible neural interfaces



**Left:** Dual-shank MRI compatible PtIr electrodes (12.1 mm L, 160  $\mu\text{m}$  diameter)  
**Right:** 3C-SiC dual passive probe (7mm L, 15  $\mu\text{m}$  thick,  $\sim$  1015 n-doped)

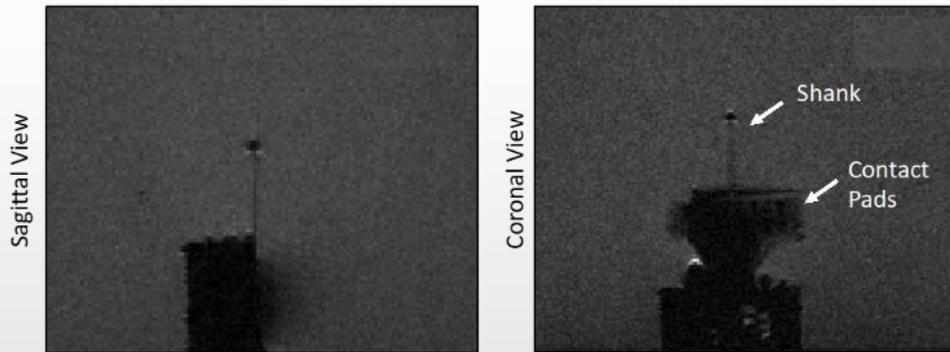


2 Tesla (Rat)

# MRI Images @7T

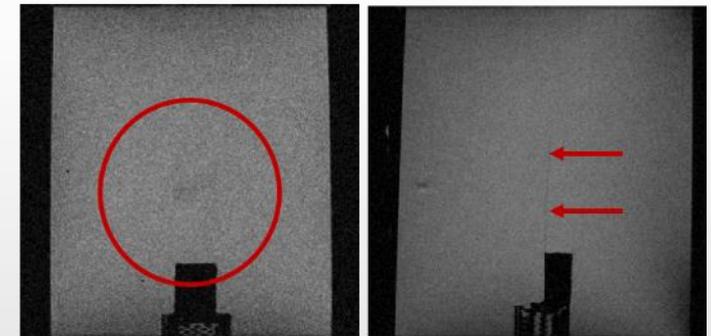


- Even a thin (~27  $\mu\text{m}$ ) Si layer results in noticeable image artifacts
- All-SiC free-standing probe displays no artifact @7T and is barely visible!



All-SiC INI  
(Si device layer)

$B_0$



Free-standing All-SiC INI  
No Si device layer

Beygi, M.; Dominguez-Viqueira, W.; Feng, C.; Mumcu, G.; Frewin, C.L.; La Via, F.; Sadow, S.E. Silicon Carbide and MRI: Towards Developing a MRI Safe Neural Interface. *Micromachines* 2021, **12**, 126.

<https://doi.org/10.3390/mi12020126>

# Summary

- Silicon Carbide is highly neuro-compatible
  - In-vitro and in-vivo (3 animal models) → no immune system trigger
- It is possible to create a monolithic INI with only SiC
  - No plastics (polymers) or metals to degrade in-vivo
  - Use of PN junction substrate isolation
  - Use of amorphous SiC capping layer
    - IDE data shows greater than  $\pm 50V$  breakdown ( $I < 1 \text{ nA}$ ) in 4H-SiC devices
- 3C-SiC on Si and SOI promising to allow for low-cost manufacturing
  - SOI → HF dip probe harvest
  - Higher CSC than 4H-SiC but with higher leakage current (Gen 1)
  - Gen 2 fabricated – packaging and testing pending
- Preliminary MRI compatibility testing in tissue phantom @7T
  - No visible image artifacts (SiC only)
  - Numerical modeling → below SAR limit (not presented)
  - In-vivo confirmation planned (summer 2021)

# Acknowledgments

## SiC Bio/Materials Studies

C. Coletti (Tissue)

N. Schettini (Blood)

C. Frewin (Brain)

## Glucose Sensing

S. Afroz, F. Cespedes, G. Mumcu

## Biosensors

S. Iannota, IMEM-CNR

R. Bange, E. Bano, V. Stambouli (DNA)

## Simulations

M. Beygi

## Deep-Tissue Cancer (NIH R21)

P. Choyke, NCI (Bethesda)

A. Gali, Wigner (Budapest)

G. Salviati, IMEM-CNR (Parma)

## Implantable Neural Interfaces

E. Bernardin (all-SiC)

C. Frewin, NeuroNexus

J. Hassan, LIU (Sweden), 4H-SiC epi

M. Beygi, MRI compatible interfaces

Chenyin Feng (C electrodes on SiC)

## Fabrication and Processing

R. Everly, NREC

F. La Via, IMM-CNR, 3C-SiC epi

K. Zekentes, E. Bano, V. Stambouli,

IMEP & FORTH, nanopillars

# Our team at USF



Spring 2020



## USF Silicon Carbide Biotechnology Group

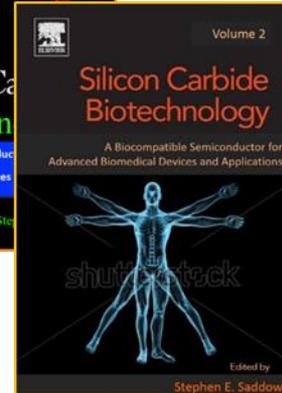


# Thank you for your kind attention!

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"THE COMPUTER SAYS I NEED TO UPGRADE MY BRAIN  
TO BE COMPATIBLE WITH ITS NEW SOFTWARE."

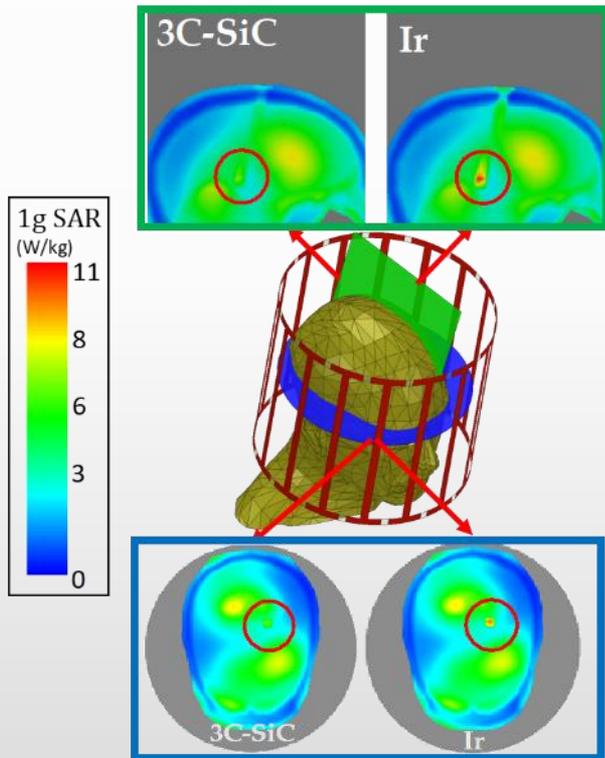


# Prof. Dr. Saddow Overview

- PhD in Electrical Engineering (electrophysics) 1993 (Uni of Maryland)
- Professor of Electrical and Medical Engineering, Uni of South Florida, Tampa, FL
- Develop silicon carbide (SiC) materials and devices for biomedical applications
  - Neural interfaces: Bionics, BMI, etc.
  - In-vivo sensors: blood, etc.
  - Bioelectronics: wearable sensors (wireless sleep, personal locator beacon, etc.)
  - Nanotechnology to treat deep-tissue cancer
- Innovation comes when you work at the nexus of different technologies/fields of endeavor
- In my case EE, physics, chemistry, medicine, material science, mechanics...

# Simulation of INI Materials – Brain Phantom

Induced heating caused by interaction with MRI fields → tissue damage



Simulated SAR\* vs. implant probe material

Material	SAR (W/kg)			
	Whole Head	Inside the box		
		Max 10 g	Max 1 g	Max 0.1 g
Ref.	2.55	5.83	6.68	7.28
All-3C-SiC	2.54	5.91	7.16	21.15
3C-SiC Tip	2.55	5.87	6.75	7.32
iridium	2.55	6.01	10.82	39.24
titanium	2.54	5.98	9.51	32.73
platinum	2.54	5.97	10.36	37.05
IrO <sub>2</sub>	2.55	6.00	9.39	32.19
TiN	2.55	5.98	8.87	30.04

\*SAR Specific Absorption Rate (W/kg)

# Simulation of INI Materials – Brain Phantom

Image Artifacts caused by interaction with MRI fields → difficult to 'see' detail near INI

- Estimated  $\Delta B_0$  caused by  $\Delta\chi$
- Assumed  $B_0=7$  T
- FOV= $256\times 256$  pixels
- Voxel size  $1\text{mm}\times 1\text{mm}\times 1\text{mm}$
- Max  $\Delta B_0=100\mu\text{T}$  & Min  $\Delta B_0=-0.3\mu\text{T}$
- Averaged  $\chi$  from literature

1) 3C-SiC

2) Si

3) Pt

